

# Cooperative *cis*-interactions between ectodomains of TCR $\alpha\beta$ CD3 subunits enable mechanotransduction

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# **ABSTRACT** (220 words)

TCR signaling poses a mechanical problem: pMHC binding occurs at the TCR $\alpha\beta$  ectodomain (ECD) head, whereas ITAM phosphorylation occurs on CD3 cytoplasmic tails. Chemistry cannot bridge this >10 nm gap, requiring the two events to be coupled through the TCR–CD3 interface, thus involving conformational allostery and being regulatable by force. Although weak ECD *cis*-interactions between TCR $\alpha\beta$  and CD3 have been proposed to contribute to this coupling, their kinetics and mechanical competence remain elusive. Here, we quantify TCR $\alpha\beta$ –CD3 ECD *cis*-interactions in a pseudo-*cis* configuration using two-dimensional binding and single-bond force spectroscopy, finding that TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ –CD3 $\delta\epsilon$  interactions have low affinity and rapid kinetics, yet form catch bonds. Critically, concurrent engagement of CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  produces high *cis*-cooperativity, yielding a stronger and longer-lasting CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  trimolecular catch bond than the sum of the two dimeric bonds, with force-stabilized lifetimes matching those of agonist TCR–pMHC *trans*-interaction. Molecular dynamics simulations reveal an expanded, cooperative, and asymmetric contact network, making CD3 $\delta\epsilon$  more force-responsive and susceptible to conformational change than CD3 $\gamma\epsilon$ . Interface mutations do not alter force-free affinities but remodel cooperative *cis*-bond profiles, leading to an inverse correlation with *trans*-bond profiles and T cell signaling. These results identify cooperative ECD *cis*-interaction as a mechanically regulatable allosteric coupling element at the TCR–CD3 junction important to antigen recognition and signal initiation.

# INTRODUCTION (main text 8207 words)

Antigen recognition by the T-cell receptor (TCR) results in T cell activation, leading to proliferation, differentiation, and effector functions (1). Signaling is initiated by ligation of peptide-major histocompatibility complex (pMHC) with TCR at its extracellular ligand-binding site, where the antigen information is received, then transmitted across the membrane along the octameric TCR–CD3 complex (TCR $\alpha\beta$  associated with CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , and CD3 $\zeta\zeta$ ) to the CD3 cytoplasmic tails (2). Concurrently, coreceptor CD8 or CD4 places the Src family kinase Lck close to the exposed CD3 tails to phosphorylate their immunoreceptor tyrosine-based activation motifs (ITAMs) (3). Phosphorylated ITAMs recruit Zap70, starting downstream signaling cascades (1, 4). Despite our detailed knowledge of the structural components of the TCR signaling machinery (5, 6), the mechanism of how pMHC binding at the TCR $\alpha\beta$  head leads to phosphorylation of CD3 ITAMs, two events separated by ~15 nm in space, precluding the action of local chemistry, remains unclear.

Two of the TCR triggering models—conformational change and mechanosensor models (7-9)—share a common requirement: a physical coupling pathway must link ligand binding to ITAM phosphorylation. Structurally, this pathway must traverse the interface between TCR $\alpha\beta$  and CD3s that includes ectodomains (ECDs), connecting peptides (CP), transmembrane (TM) bundle, and cytoplasmic tails. Yet identifying this coupling has been challenging because the TCR is subject to two seemingly opposing design constraints. On one hand, the complex must be sufficiently connected to maintain quaternary integrity and transmit information. On the other hand, it must remain sufficiently dynamic to permit state transitions that gate signaling. Resolving how molecular architecture balances connectivity with mobility is a central obstacle to a unified physical mechanism of TCR triggering.

A likely candidate for this coupling is *cis*-interaction (between proteins anchored to the same cell surface) between the TCR $\alpha\beta$  constant domains and the CD3 ECDs. Multiple lines of evidence support this notion: the functional sidedness of CD3s (10) and the importance of the TCR $\alpha\beta$  constant domains (C $\alpha$ /C $\beta$ ) (11, 12) indicate that TCR–CD3 *cis*-interactions are crucial for signal transmission. Disrupting these interactions with anti-CD3 antibodies can change how T cells are activated (13-15). The membrane-proximal ECD “ring” may act as the starting point for signal propagation and influences downstream elements such as the CPs (16), TM bundle (17, 18), and cytosolic tails (2, 19). Mutations affecting these *cis*-interactions can impact TCR assembly stability (20, 21), surface expression (22), down-modulation (23), and cellular responses (10, 21, 24-27). However, direct mechanistic interpretation has been limited by two gaps. First, ECD interactions appear very weak and transient, raising doubts about their ability to support sustained signal transmission. Second, the subtle coupling may reside in force-dependent dynamic allostery that is sensitive to experimental perturbations, rather than in easily-captured large, stable structural changes, as suggested by discrepant results from different experiments: Early cryo-electron microscopy (cryo-EM) structures (28-31) and crosslinking experiments have shown minimal stable rearrangements upon ligation (27), whereas nuclear magnetic resonance (NMR) (32, 33) and molecular dynamics (MD) (33, 34) studies indicate dynamic allostery in the TCR constant domains and at the CD3 interfaces upon pMHC binding.

More recent cryo-EM structures of the TCR–CD3 complex reconstituted in nanodiscs suggest unliganded TCR–CD3 adopts “compact/closed” conformations (35). Upon pMHC engagement the complex shifts to an “extended/open” architecture, and restricting ECD opening can impair activation (35). These findings support the plausibility of activation-linked allosteric transitions, but they do not identify the mechanical mechanism that stabilizes and coordinates this closed-to-

open transition across the TCR–CD3 junction, nor do they establish whether the implicated ECD interfaces are mechanically competent to support TCR–pMHC *trans*-interaction in the presence of force (1, 6, 18, 36-39).

Mechanical forces have been suggested to induce conformational allostery (40-42), regulate lifetimes of TCR–pMHC *trans*-bonds (40, 41, 43-46), and trigger signaling (43, 47-49), which, in turn, modulate effector functions (41, 43, 45, 50, 51). T cells exert endogenous forces on the TCR–CD3 via engaged pMHC (52-55), which must be mediated, at least in part, by TCR–CD3 ECD *cis*-interactions, therefore allowing force to play a role. Thus, mechanical force naturally fits the allosteric framework, likely as a regulator rather than an alternative to allostery. T cells exert forces on engaged ligands, and mechanical load can bias conformational ensembles by stabilizing specific bound states and pathways. In this view, force is a control parameter that can reveal latent allosteric couplings that are otherwise too fleeting to detect at equilibrium. If ECD *cis*-interactions participate in signal transmission, they must satisfy a stringent mechanical criterion: they must remain connected long enough under physiological loads to couple ligand engagement to downstream phosphorylation, while permitting the local rearrangements and fluctuations required for gating. This criterion turns our inquiry into a quantitative question—what are the kinetic and force-dependent properties of the TCR $\alpha\beta$ –CD3 ECD *cis*-bonds, and can cooperative assembly transform weak pairwise contacts into a durable, force-stabilized coupling element?

Addressing this question has been difficult because TCR $\alpha\beta$ –CD3 ECD *cis*-interactions are too weak and transient to be measured by three-dimensional (3D) methods (24, 56-58) such as SPR (Supplementary Fig. 1A, B). Moreover, most prior characterizations have been performed without controlling mechanical load, obscuring whether force reshapes the interaction landscape in ways relevant to mechanotransduction. Thus, despite longstanding hypotheses that ECD *cis*-interactions

link antigen recognition to CD3 signaling, direct measurements of their 2D kinetics, cooperativity, and force response have been lacking.

Here we combine ultrasensitive biophysical measurements with molecular dynamics (MD) simulations to define the kinetic and mechanical properties of TCR $\alpha\beta$ –CD3 ECD *cis*-interactions. Using micropipette adhesion frequency (MAF) assay (59, 60) and biomembrane force probe (BFP) thermal fluctuation and force-clamp assays (43, 61), we analyzed two-dimensional (2D) binding kinetics of TCR $\alpha\beta$  interactions with either CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , or both in a pseudo-*cis* configuration. We find that the bimolecular interactions are low-affinity and short-lived yet form catch bonds, indicating the presence of force-favored bound states. Crucially, co-engagement of CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  produces strong synergy in both bond formation and lifetime, resulting in a long-lived cooperative CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  trimolecular catch bond. Complementary analyses at the atomic level using conventional MD (CMD) and steered MD (SMD) simulations corroborate cooperative stabilization through an expanded contact network and reveal asymmetric force responses between CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$ . Finally, targeted mutations at the trimeric interface remodel force-dependent *cis*-bond profiles without altering force-free affinity, allowing us to relate mechanical coupling at the TCR–CD3 junction to T cell signaling. Together, these results establish cooperative ECD *cis*-interaction as a mechanically regulatable allosteric coupling element that can stabilize and shape information transmission across the TCR–CD3 interface.

# RESULTS

## 2D kinetic measurements reveal weak TCRαβ–CD3 *cis*-interactions.

To directly measure physical interactions among TCRαβ, CD3γε, and CD3δε (ECDs; hereinafter omitted for simplicity), we utilized the ultra-sensitive MAF assay (59, 60) and BFP thermal fluctuation assay (60, 62). To compensate for the anticipated low affinities, we coated high densities of hybrid 2B4 TCRαβ (mouse 2B4 TCRαβ variable domains fused with human LC13 TCRαβ constant domains) (26, 63) and human CD3γε or CD3δε onto opposing surfaces (Fig. 1A, B). To mimic *cis*-interactions, N-terminal biotinylated TCRαβ was coated on one side (*left*), while C-terminal biotinylated CD3s were coated on the opposing side (*right*), allowing head-to-tail alignment for “pseudo-*cis*” contacts. In the MAF assay (Fig. 1A), one red blood cell (RBC) was driven to cyclically contact the other RBC with a consistent contact area ( $A_c$ , in  $\mu\text{m}^2$ ) and time ( $t_c$ , in s) and separated to detect binding events from visually observed RBC elongations. An adhesion frequency,  $P_a$  (*i.e.*, number of binding events divided by total touches) enumerated from a sequence of repeated contact cycles was measured. Assuming second-order forward and first-order reverse reaction between monomeric TCRαβ and CD3γε or CD3δε, we previously showed that  $P_a = 1 - \exp(-\langle n \rangle)$ , where  $\langle n \rangle = m_r m_l A_c K_a [1 - \exp(-k_{\text{off}} t_c)]$  is the average number of bonds per contact. Here,  $m_r$  and  $m_l$  (in  $\mu\text{m}^{-2}$ ) are the respective densities of TCRαβ and CD3γε or CD3δε,  $K_a$  (in  $\mu\text{m}^2$ ) is 2D affinity, and  $k_{\text{off}}$  (in  $\text{s}^{-1}$ ) is off-rate (59, 60). When  $k_{\text{off}} t_c \gg 1$ ,  $\exp(-k_{\text{off}} t_c) \approx 0$ , the effective 2D affinity  $A_c K_a$  (in  $\mu\text{m}^4$ ) can be solved explicitly as  $A_c K_a = -\ln(1 - P_a) / m_r m_l$ .

The effective affinities of TCRαβ–CD3γε and TCRαβ–CD3δε *cis*-interactions were similar (3.78 and  $2.78 \times 10^{-6} \mu\text{m}^4$ , respectively), which are reliable because they are about an order of magnitude above the detection limit of our current MAF setups (Fig. 1C, *orange* and *blue*) (46). For comparison, we measured the 2B4 TCR–K5:IE<sup>k</sup> *trans*-interaction side-by-side using the C-

terminal biotinylated pMHC-coated RBC to test against the intact TCR–CD3 complex expressed on hybridoma cells. The resulting effective 2D affinity was tens to hundreds of folds higher ( $\sim 5.87 \times 10^{-4} \mu\text{m}^4$ , Fig. 1C, *gray*) even though the hybridoma cell surface is rough and the TCR $\alpha\beta$ -bearing RBC is smooth, which could result in one to two orders of magnitude lower effective 2D affinity for the rough than smooth cells (64). In addition, using C-terminal biotinylated CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  coated on the opposing surfaces, we quantified the CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$  heterotypic interaction ( $\sim 1.10 \times 10^{-5} \mu\text{m}^4$ , Fig. 1C, *green*), which was higher than the TCR–CD3 heterotypic interactions. Similarly, the effective 2D affinities for the CD3 $\gamma\epsilon$ –CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ –CD3 $\delta\epsilon$ , and TCR $\alpha\beta$ –TCR $\alpha\beta$  homotypic interactions were measured with lower values or undetectable (Supplementary Fig. 1C).

To further determine the on- and off-rate, we used the BFP thermal fluctuation assay to measure off-rate,  $k_{\text{off}}$  (60, 62). We attached a functionalized glass bead to the apex of the micropipette-aspirated ultra-soft hypotonic RBC to form the probe on the left (Fig. 1B), whose thermally driven fluctuations were monitored in real time with high spatial-temporal precision (few nanometers and sub-milliseconds) (65). The target bead coated with the corresponding binding partner was brought close to the probe to allow molecular contacts via thermal fluctuations, facilitating bond formation. Upon binding, the receptor–ligand (*i.e.*, either TCR $\alpha\beta$  vs. CD3, CD3 vs. CD3, or pMHC vs. TCR–CD3) bond acted as an additional spring in parallel with the RBC spring, dampening the confined Brownian motions (60, 62). The sudden reduction in thermal fluctuations indicated bond formation, while the restoration to the original fluctuation amplitude marked bond dissociation. The durations in between represent bond lifetimes, which were exponentially distributed, and the reciprocal of the mean bond lifetime is equal to the  $k_{\text{off}}$ . The 2D off-rates for TCR $\alpha\beta$ –CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ –CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$  *cis*-interactions measured in this way were very rapid ( $> 10 \text{ s}^{-1}$ ) compared to the slower  $k_{\text{off}}$  of the 2B4 TCR–K5:IE<sup>k</sup> *trans*-interaction plotted alongside in Fig. 1D. These



results also validated the  $\sim 2$  s contact time used in our MAF assay, which was sufficiently long to ensure the measured adhesion frequencies had reached steady-state. Finally, the effective 2D on-rates,  $A_c k_{on}$ , were calculated as  $A_c k_{on} = A_c K_a \times k_{off}$  for the corresponding interactions (Fig. 1E). Together, the very low affinities and fast off-rates explain why SPR failed to detect these weak and rapid TCR $\alpha\beta$ –CD3 interactions, underscoring the ultra-sensitivity of our 2D assays (66).

# **Pairwise *cis*-interactions among TCR–CD3 ECDs form bimolecular catch bonds.**

We (41-44, 46, 50) and others (40, 45, 51, 67, 68) have shown that mechanical force modulates TCR–pMHC *trans*-interactions and amplifies antigen discrimination (40, 43, 44). To test whether force also modulates dissociation of the TCR–CD3 *cis*-interactions, we used the BFP force-clamp assay (41, 43-45) to measure the force-dependent lifetimes of TCR $\alpha\beta$ –CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ –CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$  *cis*-bonds (Fig. 1B). Like in the thermal fluctuation assay, we also used bead-mounted RBCs as ultra-sensitive force transducers to measure molecular interactions in the force-clamp assay. Unlike the thermal fluctuation assay, which positioned the target bead at the null position for bond formation and dissociation at zero force, the force-clamp assay retracted the target by a pre-set distance to exert a constant tensile force onto the bond. To enhance stability of force measurement, a dual-edge tracking system was implemented to monitor the positions of both the BFP micropipette and the probe, allowing us to subtract the micropipette drifts from the force signals. The target was programmed to move in repeated “approach-touch-retract-hold-return” cycles, generating a force *vs.* time trace (Fig. 1F) that exemplified both non-binding and binding events. The compressive (negative) force indicates bead-target contact during which bond formation can occur. Upon retraction, the compressive force either returns to zero (no binding) or converts to tensile (positive) force (binding). In the latter case, retraction was halted at the designated force level until bond dissociation, indicated by the sudden return of force to zero.

Interestingly, BFP measurements revealed that all three *cis*-interactions formed catch bonds, with mean lifetimes prolonged by low forces (< 7-17 pN, depending on the specific interaction) until being overpowered by higher forces that turned the bond profiles into slip bonds (*i.e.*, mean bond lifetimes shortened by forces, Fig. 1G). These findings demonstrate that TCR-CD3 *cis*-interactions can bear durable force, supporting the notion that information on antigen recognition can be transmitted mechanically through TCR $\alpha\beta$ -CD3 interactions.

Notably, these TCR $\alpha\beta$ -CD3 *cis*-interactions exhibited shorter bond lifetimes across the entire force range than our previously reported TCR $\alpha\beta$ -pMHC *trans*-bonds here (replotted from (42) in Fig. 1G, *gray*), suggesting that individual TCR $\alpha\beta$ -CD3 bimolecular *cis*-interactions alone may not persist long enough to fulfill the proposed mechanical transmission requirements. The 1:1:1 stoichiometry of TCR $\alpha\beta$ :CD3 $\gamma\epsilon$ :CD3 $\delta\epsilon$  revealed by the cryo-EM structures (28, 29, 31) and our direct kinetic measurements of CD3 $\gamma\epsilon$ -CD3 $\delta\epsilon$  interactions (Fig. 1C-E, G, *green*) prompted us to ask: Does TCR $\alpha\beta$  bind CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  concurrently to form stronger bonds? If so, is this concurrent binding independent or cooperative? If cooperative, how much is the bond stability enhanced, and does this enhancement meet the mechanical transmission requirements?

# **CD3 $\delta\epsilon$ and CD3 $\gamma\epsilon$ interact with TCR $\alpha\beta$ cooperatively in bond formation and bond lifetime.**

To test whether CD3 $\delta\epsilon$  and CD3 $\gamma\epsilon$  interact with TCR $\alpha\beta$  cooperatively in *cis*, we applied affinity- and lifetime-based measurements with MAF and BFP while co-presenting both CD3s. The results were compared against predictions from a non-cooperative binding model. Significant deviations from these predictions are taken as evidence for positive *cis*-cooperativity.

To ensure rigorous comparison of adhesion frequencies, a single TCR $\alpha\beta$ -bearing RBC was sequentially brought into contact with a RBC coated with CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , or an equimolar mixture of both (denoted CD3m) in randomized order (Fig. 2A). Streptavidinylated RBCs were prepared

from the same batch and coated using excess amounts of biotinylated CD3s to ensure saturated mounting to SA with equivalent density. Adhesion frequencies were measured over 30 touches per pairing for TCR $\alpha\beta$ -CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ -CD3 $\delta\epsilon$ , and TCR $\alpha\beta$ -CD3m (Fig. 2B, connected by *solid lines*) before switching to a new TCR $\alpha\beta$ -bearing RBCs (specificity checks of all interactions are shown in Supplementary Fig. 1D). Across eight TCR $\alpha\beta$  RBCs tested, the adhesion frequency to CD3m was consistently higher than either subunit alone. To interpret this result, we transformed  $P_a$  into the average number of bonds per contact,  $\langle n \rangle = -\ln(1 - P_a)$ , which is additive for independent, concurrent binding (69, 70). Under this non-cooperative assumption, the predicted bond number for CDm is  $\langle \hat{n}_m \rangle = 1/2\langle n_{\gamma\epsilon} \rangle + 1/2\langle n_{\delta\epsilon} \rangle$ , where  $\langle n_{\gamma\epsilon} \rangle$  and  $\langle n_{\delta\epsilon} \rangle$  were measured from respective bimolecular TCR $\alpha\beta$  interactions with the single CD3 species indicated by the subscripts (Fig. 2B, *horizontal dotted line*). Strikingly, the observed  $\langle n_m \rangle$  significantly exceeded the predicted  $\langle \hat{n}_m \rangle$ , falsifying the independent binding hypothesis and demonstrating cooperative binding. The degree of cooperativity can be calculated as  $\langle n_m \rangle / \langle \hat{n}_m \rangle - 1$ , yielding a value of 170%, substantially higher than zero (Fig. 2C), confirming pronounced positive *cis*-cooperativity.

Next, we used BFP thermal fluctuation and force-clamp assays to measure the average lifetimes of TCR $\alpha\beta$ -CD3m bonds (denoted as  $\tau_m$ ) in the absence and presence of force. The BFP target beads were functionalized similarly to the target RBCs in the MAF assay, except that the surface density of TCR $\alpha\beta$  was adjusted to maintain infrequent adhesion events ( $\leq 20\%$ ), ensuring a high probability ( $\sim 90\%$ ) of single specific bonds (59) (Supplementary Fig. 1E-H). The lifetime scattergram was globally fitted by the previously described two-state, two-pathway dissociation models (Supplementary Fig. 2A-I) (46). TCR $\alpha\beta$ -CD3m bonds persisted significantly longer than single-ligand TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  or TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bonds across all force levels tested (Fig. 2D; single-ligand curves replotted from Fig. 1G). The  $\tau_m$  vs.  $f$  curve peaked at  $\sim 13$  pN with a lifetime

of  $\sim 1.5$  s, whereas the  $\tau_{\gamma\epsilon}$  and  $\tau_{\delta\epsilon}$  vs.  $f$  curves peaked at  $\sim 7$  and  $15$  pN, respectively, with lower values of  $\sim 0.6$  s for both. Notably, the  $\tau_m$  bond profile exhibited a more pronounced catching behaviour, closely matching that of the TCR $\alpha\beta$ -pMHC *trans*-interaction (Fig. 1G, *gray*; peak at  $\sim 10$  pN with a lifetime  $\sim 1.6$  s). These results indicate that dual ligands are able to provide sufficient *cis*-stability for mechanotransmission, whereas single ligands are not.

To investigate the basis of this prolonged dual-ligand lifetime, we performed survival analysis on bond lifetime distributions (60, 62, 65). The survival probability curve of zero-force lifetimes for TCR $\alpha\beta$ -CD3m displayed two distinct decay phases, in stark contrast to the log-linear decay observed for single-ligand *cis*-interactions (Fig. 2E). The presence of a slow-decaying subpopulation confirms the existence of the long-lived bond states, bond species, or both. Similar subpopulations of longer-lasting bonds in dual-ligand were also observed in the survival curves of low- and high-force lifetimes (Supplementary Fig. 2J, K). These longer-lived events likely represent trimolecular CD3 $\delta\epsilon$ -TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  bonds that substantially prolong  $\tau_m$ , and result in positive cooperativity. To quantify this cooperativity in terms of bond lifetime, we calculated the average lifetime of TCR $\alpha\beta$ -CD3m bonds as the weighted sum of the bond lifetimes of two bimolecular interactions expected from no cooperativity,  $\tau_{\gamma\epsilon}$  and  $\tau_{\delta\epsilon}$ , by  $\hat{\tau}_m = P_{\gamma\epsilon} \times \tau_{\gamma\epsilon} + P_{\delta\epsilon} \times \tau_{\delta\epsilon}$  (Fig. 2D, *dotted curve*), where the bond formation possibilities,  $P_{\gamma\epsilon}$  and  $P_{\delta\epsilon}$ , equal the respective fractions of TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bond numbers,  $\langle n_{\gamma\epsilon} \rangle / (\langle n_{\gamma\epsilon} \rangle + \langle n_{\delta\epsilon} \rangle)$  and  $\langle n_{\delta\epsilon} \rangle / (\langle n_{\gamma\epsilon} \rangle + \langle n_{\delta\epsilon} \rangle)$ . The assumption of independent binding predicts  $\tau_m = \hat{\tau}_m$ , but the cooperative analysis,  $\Delta\tau/\hat{\tau}_m = (\tau_m - \hat{\tau}_m)/\hat{\tau}_m$ , revealed  $\sim 74\%$  to  $328\%$  increments in the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimolecular *cis*-bond lifetime over the force range of 0-30 pN (Fig. 2F), highlighting the strong force-enhanced positive cooperativity.

## MD simulations corroborate cooperative interaction of CD3 $\gamma\epsilon$ and CD3 $\delta\epsilon$ with TCR $\alpha\beta$ .

To corroborate the experimentally observed *cis*-cooperativity, we performed force-free conventional MD (CMD) simulations (71) on TCR $\alpha\beta$ -CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ -CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  complexes. The initial full-atomic model of TCR-CD3 ECDs, including the trimeric and dimeric structures (Fig. 3A and Supplementary Fig. 3A), were extracted from the cryo-EM structure (PDB: 6JXR) (28). All equilibrated complexes remained bound after 200 ns CMD simulations. Their binding interfaces were analyzed in terms of contact areas (Fig. 3B and Supplementary Fig. 3B) and binding free energies (Fig. 3C and Supplementary Fig. 3C), which were inversely correlated. Using cooperative analyses similar to Fig. 2C, F, we found these two measures also exhibited positive *cis*-cooperativities (Fig. 3D). Because binding affinity,  $K_a$ , is related to free energy change,  $\Delta E$  by  $K_a \propto \exp(-\Delta E/k_B T)$ , where  $k_B$  is the Boltzmann constant and  $T$  is the absolute temperature, these simulations provide independent verification of cooperative 2D affinity measurements.

We next simulated force-induced dissociations of TCR $\alpha\beta$ -CD3 complexes using steered MD (SMD) (72). A pulling force was applied on the TCR $\alpha\beta$  N-terminus, while the C-termini of CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$  or both were anchored (Fig. 3E, *insets* and Supplementary Fig. 4A). To complete simulation within accessible computational timescales, we used relatively high clamping forces (100-200 pN) to accelerate dissociations, which were detected as sudden increases in the minimum distances between TCR $\alpha\beta$  and either or both CD3s (Fig. 3E, *curves* and Supplementary Fig. 4B). The times to dissociate ranked as TCR $\alpha\beta$ -CD3 $\delta\epsilon$  < TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  < CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$ . Simulated force effects on times to dissociation (Fig. 3F) were consistent with experimental lifetime trends, following expected slip behaviors beyond 15 pN (Fig. 2D). The trimolecular CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bonds dissociated at 626, 404, and 233 ns under 150, 175, and 200 pN,

respectively, which persisted at least an order of magnitude longer than the two dimeric bonds. To quantify cooperativity, we calculated  $\Delta t / \hat{t}_{\delta\gamma}$ , which compares observed times to dissociation,  $t_{\delta\gamma}$ , to the predicted times to dissociation for the non-cooperative trimolecular complex  $\hat{t}_{\delta\gamma} = t_{\gamma\epsilon} + t_{\delta\epsilon} - t_{\gamma\epsilon}t_{\delta\epsilon}/(t_{\gamma\epsilon} + t_{\delta\epsilon})$ , calculated using the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ -CD3 $\delta\epsilon$  dissociation times,  $t_{\gamma\epsilon}$  and  $t_{\delta\epsilon}$ , respectively. Observed dissociation times exceeded this prediction by from 1,200% at 150 pN to 1,900% at 200 pN, demonstrating strong *cis*-cooperativity and mechanical reinforcement (Fig. 3G). Force-ramp SMD simulations on partial and full TCR-CD3 assemblies yielded rupture forces in the same order, TCR $\alpha\beta$ -CD3 $\delta\epsilon$  < TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  < CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  (Supplementary Fig. 4C, D), further confirming the higher stability of the trimolecular complex. Together, complementary experimental and computational approaches demonstrate positive *cis*-cooperativity between CD3 $\delta\epsilon$  and CD3 $\gamma\epsilon$  in their co-binding to TCR $\alpha\beta$ .

#### **Structural basis of *cis*-cooperativity quantified by atomic-level contacts.**

To elucidate the structural basis of *cis*-cooperativity, we analyzed interface contacts within the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ -CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ -CD3 $\delta\epsilon$  dimers and compared them with those within the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimer. The contact area sizes were preserved from the dimer to trimer interfaces with only modest alteration upon incorporation of the third subunit. Because CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  bind TCR $\alpha\beta$  orthogonally with minimal overlap, their combined contact area in the trimer was only slightly smaller than the sum of dimers. This slight steric loss was more than offset by the gain of the CD3 $\gamma\epsilon$ -CD3 $\delta\epsilon$  contact area in the trimer, which substantially increased the total contact area and lowered the binding free energy (Fig. 3B, C), consistent with *cis*-cooperativity. Similarly, we analyzed hydrogen (H) bonds within the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ -CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ -CD3 $\delta\epsilon$  dimers and compared them with those within the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimer,

finding substantially more H-bonds in the trimer than in the dimers at the start and in the middle, but not near the end of SMD simulations (Supplementary Fig. 4E). Similar cooperativity calculations found > 100% and 180% more H-bonds in the trimer without and with force, respectively (Supplementary Fig. 4F).

We further quantified the level of interfacial contact using dynamic distances from each residue to its binding partner. We termed this quantification occupancy, defined as the fraction of simulation time during which the center of mass of that residue remains within 4 Å of any atom of the *cis*-interacting ECDs. As such, the occupancy of an individual residue ranks from 0% to 100% as interaction strengthens.

To reveal dynamic binding footprints, we mapped these occupancies onto the molecular surfaces, with color intensities proportional to occupancy percentages (Fig. 4A). To expose the respective TCRαβ-CD3γε and TCRαβ-CD3δε interfaces, a pair of the same trimer with different views formed the mirror images, where CD3γε (Fig. 4A, *left*) and CD3δε (Fig. 4A, *right*) were rotated outward away from fixed TCRαβ. Differential color coding was used to indicate CMD-derived occupancy levels on interfaces of CD3γε-TCRαβ-CD3δε trimer (*cyan*), TCRαβ-CD3γε dimer (*magenta*, after CD3δε removal), and TCRαβ-CD3δε dimer (*yellow*, after CD3γε removal), respectively. Overlay of dual-color maps (*blueish* overlap for TCRαβ-CD3γε; *greenish* overlap for TCRαβ-CD3δε) highlighted conserved interactions. These analyses revealed the shifts in residue contacts from residing in the respective dimeric structures to the trimeric structure in the absence of force. Interestingly, the interface of TCRαβ with CD3γε was nearly unchanged by the presence of CD3δε (Fig. 4A, *left*, *magenta* vs. *cyan*), whereas that with CD3δε exhibited a marked reorientation in the presence of CD3γε (Fig. 4A, *right*, *yellow* vs. *cyan*). This was consistently observed in all three independent CMD runs.



To quantify occupancy footprint colocalization between dimer and trimer states, we calculated Manders' overlap coefficients (73), finding significantly greater values for CD3 $\gamma\epsilon$  than CD3 $\delta\epsilon$  (Fig. 4B). The higher Manders' coefficient for  $\gamma\epsilon$  than  $\delta\epsilon$  revealed a higher level of overlapping contact interfaces between trimer and dimer of TCR $\alpha\beta$  with CD3 $\gamma\epsilon$  than CD3 $\delta\epsilon$ , which negatively correlated with the level of contact adjustments going from dimer to trimer after adding the missing CD3. This indicates that, structurally, the TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  interface remains unchanged with or without CD3 $\delta\epsilon$ , whereas the TCR $\alpha\beta$ –CD3 $\delta\epsilon$  interface must reshape to accommodate the incorporation of CD3 $\gamma\epsilon$  during trimeric assembly. Asymmetric TCR $\alpha\beta$  interactions with two CD3s may result in unequal contributions to *cis*-cooperativity.

### **Asymmetric responses of CD3 $\epsilon$ under *cis*-cooperativity and mechanotransmission.**

To further elucidate the asymmetric roles of CD3s during cooperative binding and force transmission, we investigated the differential dynamic responses of CD3 $\gamma\epsilon$  vs. CD3 $\delta\epsilon$  using occupancy and fluctuation analyses. We first compared the occupancies determined using SMD simulations in the presence of force with values determined in previous section using CMD simulations for every single  $\alpha$ ,  $\beta$ ,  $\gamma$ ,  $\epsilon$ ,  $\delta$ , and  $\epsilon'$  chains (note the omissions of TCR and CD3 designations for simplicity). Hereinafter, we use  $\epsilon'$  to denote the  $\epsilon$  chain that forms the heterodimer with the  $\delta$  chain to distinguish it from the  $\epsilon$  chain that forms the heterodimer with the  $\gamma$  chain, despite their identical sequences. Notwithstanding the average occupancies of  $\epsilon'$  and  $\epsilon$  chains of the trimer were similar in the absence of force,  $\epsilon'$  had far fewer contact residues with  $\alpha\beta$  than  $\epsilon$  both in the absence and presence force, indicating asymmetry (Fig. 4C). Interestingly, under pulling force applied to the TCR $\alpha\beta$ , both the number of residues with non-zero values and the domain average of  $\epsilon'$  occupancies declined sharply, whereas those of  $\epsilon$  remained stable (Fig. 4C).



These data suggest that  $\epsilon'$  is more sensitive to force, whereas  $\epsilon$  provides more mechanical support for *cis*-cooperativity.

To expand the  $\epsilon$  and  $\epsilon'$  occupancy data (Fig. 4C), we similarly calculated mean occupancies of  $\alpha\beta$  residues contacting  $\gamma$  and  $\delta$  domains from CMD and SMD simulated  $\gamma\epsilon$ - $\alpha\beta$ - $\delta\epsilon$  trimer. We also performed parallel occupancy calculations using simulated  $\alpha\beta$ - $\delta\epsilon$  and  $\alpha\beta$ - $\gamma\epsilon$  dimers for all CD3 chains. We then plotted these paired occupancies as points using values obtained from CMD (without force) and SMD (with force) as *x*- and *y*-coordinates and drew vectors connecting any two points for the same CD3 chains with the start- and end-point coordinates calculated from simulated dimeric and trimeric structures, respectively (Fig. 4D). The magnitude of a vector represents the amount of occupancy change for a single CD3 chain ( $\gamma$ ,  $\epsilon$ ,  $\delta$ , or  $\epsilon'$ ) from before (as  $\alpha\beta$ - $\gamma\epsilon$  or  $\alpha\beta$ - $\delta\epsilon$  dimer) to after (as  $\gamma\epsilon$ - $\alpha\beta$ - $\delta\epsilon$  trimer) incorporating the missing CD3 heterodimer ( $\delta\epsilon$  or  $\gamma\epsilon$ ). Remarkably, the  $\delta$  (*red*) and  $\epsilon'$  (*blue*) vectors were of much larger magnitudes than the  $\gamma$  (*green*) and  $\epsilon$  (*orange*) vectors, revealing much larger cooperativity-induced occupancy changes in the  $\delta$  and  $\epsilon'$  than the  $\gamma$  and  $\epsilon$  chains. This quantitatively depicts the strength of larger non-overlapping trimer and dimer footprints (*cyan areas*) of  $\delta\epsilon$  (Fig. 4A, *right*) than  $\gamma\epsilon$  (Fig. 4A, *left*), re-emphasizing that, to form a  $\gamma\epsilon$ - $\alpha\beta$ - $\delta\epsilon$  trimer via cooperative *cis*-interaction among ECDs, it requires more contact adaptation from incorporating  $\gamma\epsilon$  into the  $\alpha\beta$ - $\delta\epsilon$  dimer than incorporating  $\delta\epsilon$  into the  $\alpha\beta$ - $\gamma\epsilon$  dimer.

The directions of these vectors indicate whether the changes are positive (increasing) or negative (decreasing). Their *x*- and *y*-components represent the changes occurring in the absence and presence of a 175 pN force, respectively. On Fig. 4D, points below (*light blue*) or above (*light red*) the diagonal line indicate domain contacts of  $\alpha\beta$  with CD3 chains that are suppressed or enhanced by force, respectively. Interestingly,  $\delta$  switched from a force-suppressed to a slightly force-

enhanced state (moving from below to above the diagonal line), while  $\epsilon'$  redirected from slightly force-enhanced to force-suppressed (moving from above to below the diagonal line); by comparison, hardly any changes of force-induced contacts, and neither switches of their force-enhanced ( $\gamma$ ) and force-suppressed ( $\epsilon$ ) states were seen in either  $\gamma$  or  $\epsilon$  chain. (Fig. 4D). These results reveal that  $\delta\epsilon$  is more force-sensitive and  $\gamma\epsilon$  is more mechanically stable, indicating their different roles in transmitting force across the interfaces between TCR $\alpha\beta$  and the two CD3 ECDs. In addition to occupancy analysis, which measures contact stability, we analyzed root-mean-square fluctuations (RMSF) in the absence and presence of a 175 pN clamp force, which reflect residue flexibility. By averaging across the entire chain, we assessed the mobility changes of different chains before and after applying force, revealing another layer of mechano-responsiveness for the trimer.  $\epsilon'$  showed a larger mean RMSF than  $\epsilon$  (Fig. 4E), and force-enhanced RMSF in both  $\epsilon'$  and  $\epsilon$  residues, but much more for  $\epsilon'$  than  $\epsilon$  (Fig. 4E). These results inverted the trends of the occupancy data (Fig. 4C), showing a negative correlation expected intuitively. The differences in RMSF values calculated in the presence and absence of force ( $\Delta$ RMSF) were projected onto the TCR–CD3 quaternary ECD structure, where force-enhanced (*blue*) and force-suppressed (*red*) fluctuations were indicated by color, and absolute  $\Delta$ RMSF values in response of force were indicated by backbone thickness (Fig. 4F). Under pulling,  $\delta\epsilon$  exhibited more amplified dynamics than  $\gamma\epsilon$ , forming a hinge in  $\delta$  (*red*) and promoting an out swinging of the semi-detached  $\epsilon'$  (*blue*), further revealing asymmetry between  $\gamma\epsilon$  and  $\delta\epsilon$ .

### Identifying residues critical to *cis*-cooperativity and their distinctive force-responses.

To pinpoint the structural determinants of *cis*-cooperativity, we developed a modified occupancy analysis (*i.e.*,  $\Sigma$ Occupancy) that integrated occupancies from CMD and SMD simulations, weighted by the number of connections from that residue to all residues in the binder. Briefly,

instead of residue-to-domain occupancy, we quantified residue-to-residue occupancy in a matrix format (Supplementary Fig. 5A). Subsequently, we summed over all possible contacts with the interacting domain (Supplementary Fig. 6, *gray*) to account for one-to-many interactions. This approach broadened the dynamic range of detection and identified ~10 and 14% more contacting residues in CMD and SMD, respectively, compared with cryo-EM static structure. We used  $\Sigma$ Occupancy to map the high-contact residues at the TCR-CD3 interface, visualized by sidechain color-coding on the structure, thereby highlighting candidate residues with strong interface connectivity (Fig. 4G).

To assess force sensitivity, instead of integrating the CMD and SMD results, we calculated the difference between the CMD- and SMD-derived occupancy matrix (Supplementary Fig. 5B). Summing over by row or column yielded  $\Delta$ Occupancy, in turn identified force-sensitive residues whose contacts were strengthened (*red*) or weakened (*blue*) by pulling (Supplementary Fig. 6 *red* and *blue*). We mapped these force-sensitive residues on the TCR-CD3 interface by color-coding (Fig. 4H). From a top-down view, force preferentially reduced TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  contacts, whereas TCR $\alpha\beta$ -CD3 $\delta\epsilon$  contacts were more dynamic. It seems reasonable to suspect that these force-sensitive residues play key roles in mediating force transmission across the TCR-CD3 interface.

# **Mutating interfacial residues alters catch bond but not affinity of TCR $\alpha\beta$ -CD3 interactions.**

Among all *cis*-contact residues, two regions of the TCR $\beta$  constant domain (C $\beta$ ) stood out by their strikingly opposite mechano-responses. Both the CC' loop (residues 182-187) and the Helix 4-F strand segment (residues 221-226) were highly conserved and enriched in high  $\Sigma$ Occupancy residues; however, the CC' loop showed negative  $\Delta$ Occupancy and the Helix 4-F strand displayed positive  $\Delta$ Occupancy (Fig. 5A). This suggests that force applied from the TCR $\beta$  N-terminus to the

C $\beta$  domain elicits residue-specific allostery with opposite effects in adjacent structural regions, moving the CC' loop away from, and the Helix 4–F strand closer to, the CD3s.

We targeted the C $\beta$  CC' loop and Helix 4–F strand regions, highlighted on the TCR $\alpha\beta$  structure (Fig. 5B), and introduced double-alanine mutations: G182A/K183A (GK), N222A/P223A (NP), and N225A/H226A (NH), made to alter residues with both strong (large  $\Sigma$ Occupancy) and force-sensitive (high absolute  $\Delta$ Occupancy) contacts. As previously reported (26), mutant mouse 2B4 TCR $\alpha\beta$  chains assembled normally with CD3 chains in transduced hybridoma cells, yet altered T cell activation, measured by interleukin-2 (IL-2) secretion upon co-culture with K5:IE<sup>k</sup> expressing CHO cells (Fig. 5C, reformatted IL-2 dose-dependent response curves from Ref. (26)). Among these, NP acted as a gain-of-function (GOF) mutation, whereas GK and NH behaved as loss-of-function (LOF) mutations. The IL-2 alterations underscore the functional relevance of TCR $\alpha\beta$ –CD3 *cis*-interaction in effectively relaying the ligation signals for downstream T cell activation.

To scrutinize how *cis*-interactions regulate signaling propagation, we measured *cis*-interactions between WT and mutant (MT) N-terminally biotinylated 2B4 TCR $\alpha\beta$  with C-terminally biotinylated CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , or both. To ensure the 1:1 ratio of CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  constructs, we engineered flexible amino acid linkers to covalently tether the two CD3 heterodimers, thereby avoiding heterogeneous CD3 mixtures (*i.e.*, *in vitro* CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$ , see Methods). Comparing MTs to WT TCR $\alpha\beta$ , statistically indistinguishable normalized numbers of bonds were observed for bimolecular interactions with CD3 $\gamma\epsilon$  ( $7.52 - 10.94 \times 10^{-7} \mu\text{m}^4$ ; Fig. 5D, *first group*) and CD3 $\delta\epsilon$  ( $6.25 - 9.11 \times 10^{-7} \mu\text{m}^4$ ; Fig. 5D, *second group*) and much higher but similarly valued were observed for trimolecular interactions with both CD3s ( $22.75 - 27.82 \times 10^{-7} \mu\text{m}^4$ ; Fig. 5D, *third group*). The cooperative analysis also revealed similar positive cooperativity measures in WT and MT trimers (Supplementary Fig. 7A). Furthermore, *trans*-interactions between complete WT and

MT 2B4 TCR–CD3 complexes expressed on hybridoma cells with C-terminally biotinylated K5:IE<sup>k</sup> pMHC reported orders of magnitude higher than *cis*-counterparts but near-identical values with each other ( $5.59 - 5.87 \times 10^{-4} \mu\text{m}^4$ ; Fig. 5D, *fourth group*). These results rule out zero-force kinetics of TCRαβ–CD3 *cis*-interaction and TCR–pMHC *trans*-interaction as a possible reason for the altered T cell activation by the mutations.

However, under force, more pronounced kinetic differences emerged in terms of the catch-slip bond. Bond lifetime vs. force curves for WT and MT TCRαβs with CD3γε were similar (Fig. 5E); so were those with CD3δε, except for the NP mutation (Fig. 5F), which exhibited a markedly enhanced catch bond. Interestingly, when comparing against each other, their force-dependent bond lifetimes demonstrated asymmetry again, as measured by the optimal forces where bond lifetime peaks and the catch bond intensities (a metric summarizing force-dependent bond lifetime changes (42)), both showing significantly higher values for four TCRαβ mutants interacting with CD3δε than CD3γε (Supplementary Fig. 7B, C). This validates the results from structural analysis and MD simulations (Fig. 4C-F), confirming that CD3δε is more force-responsive than CD3γε.

In the case of co-presenting both CD3s, bond lifetime profiles revealed marked mutational effects (Fig. 5G). Notably, the NH LOF TCRαβ mutant formed exceptionally stable bonds with CD3γε–CD3δε, sometimes exceeding 100 seconds, resulting in an average bond lifetime several-fold longer than the WT TCRαβ. Similarly, the GK LOF mutant exhibited an enhanced catch bond with longer lifetimes across the entire force range, whereas the NP GOF mutant displayed a bond profile resembling WT. Recalling our bond measurements for corresponding *trans*-interactions (Fig. 5H, replotted from Ref. (42)), the mutational effects on TCR–pMHC *trans*-interactions and TCRαβ–CD3 ECD *cis*-interaction seem exhibit a reverse correlation: the longer the *cis*-bond, the shorter the *trans*-bond and vice versa.

# **Correlating *cis*- and *trans*-interactions between TCRαβ and CD3s with T cell signaling.**

We next inspected possible correlations between IL-2 secretions (Fig. 5C) and the kinetic measures of the ECD *cis*-interactions of WT and MT TCRαβs with either CD3γε, CD3δε, or both in the absence and presence of force. For bimolecular *cis*-interactions, as expected from their statistically indistinguishable values across each group, the effective 2D affinities (Fig. 5D, *first two groups*) showed poor predictive power for normalized IL-2 AUC, with steep regression slopes and/or low  $R^2$  values (Fig. 6A). Here, the inverse of the slope indicates the sensitivity-of-prediction, and  $R^2$  reflects the goodness-of-fit (see Methods). Poor predictive powers for T cell function were similarly observed from lifetimes measured at zero force and optimal force (Fig 5E, F) for both TCRαβ–CD3γε and TCRαβ–CD3δε bimolecular *cis*-bonds (Fig. 6B, *orange and blue*, respectively; Supplementary Fig. 7D). Of note, slightly better correlation with T cell signaling was observed for TCRαβ bonds with CD3δε than CD3γε at both types of lifetime measures, with higher  $R^2$  values and more gradual slopes (Fig. 6B, *dotted vs. solid lines*), potentially because of the differential force-responsiveness.

To examine the contribution of cooperativity of the CD3γε–TCRαβ–CD3δε ECD *cis*-interaction to T cell activation, the normalized bond numbers (Fig. 5D, *third group*) and lifetimes at zero force (Fig. 5H, 0 pN) of the trimeric interaction were analyzed, but again found lacks of functional correlations due to their comparable values (Fig. 6C, *red*), similar to their bimolecular counterparts. In contrast to the poor function correlations with the peak lifetime at optimal force of the two bimolecular bonds (Fig. 6B, *solid lines*), a significant reverse correlation was observed between peak lifetime of the cooperative trimolecular bond (Fig. 5H, *optimal force*) and IL-2 production, with a much higher  $R^2$  value and a much flatter slope (Fig. 6C, *black*).

The sharp contrast between the differential predictive powers at zero and optimal forces prompted us to analyze the force effect more rigorously by plotting vs. IL-2 AUC, the goodness-of-fit and sensitivity-of-prediction based on WT and MT lifetimes under each force, finding that the negative correlation persisted across nearly the entire force range tested (Fig. 6D). Because of the negative correlations, the sensitivity-of-prediction followed the reverse trends of catch bonds, with biphasic behavior most pronounced at optimal force, where force-dependent lifetimes diverged the most between TCR WT and MTs. The Pearson coefficient rapidly approached -1 upon application of force and remained strongly correlated across  $\sim 5$ -20 pN. These results underscore a mechanotransduction role of the cooperative trimeric *cis*-catch bond.

Since IL-2 produced by T cells expressing these WT and MT TCRs correlates with the peak lifetime of TCR-K5:IE<sup>k</sup> *trans*-bonds (42), we correlated the peak lifetimes of *trans*- against *cis*- interactions, finding strong anti-correlations with those of the trimer ( $R^2 \sim 0.8$ , Fig. 6E, *black*), but not dimers ( $R^2 < 0.5$ , Fig. 6E, *orange* and *blue*). To confirm the force effect on *cis*- and *trans*- coordination, we plotted the force-dependent fitting of *cis*- vs. *trans*- bond profiles for WT and NP, GK, and NH mutants indicated no correlation in the absence of force (Pearson coefficient,  $r \sim 0$  at zero force), and weak correlations in the presence of force for the bimolecular *cis*-bonds ( $0.33 < r < 0.73$  for  $\gamma\epsilon$ , and  $-0.03 < r < 0.82$  for  $\delta\epsilon$ ; Supplementary Fig. 7E), but strong negative-correlations in the presence of force for the trimolecular *cis*-bond ( $r$  dropped sharply, reaching  $\sim -1$  at 10 pN before rebounding; Fig. 6F). Such correlation analysis reveals an interesting synergy between *trans*- and *cis*-interactions, suggesting a possible feedback mechanism of the TCR mechanosensory machine: from the constant domains, the downstream mechanotransduction region transmitting back to the variable domains, the antigen recognition region.



# DISCUSSION

Noncovalent *cis*-interactions between the TCR $\alpha\beta$  and CD3 chains are essential because they not only hold the octameric TCR–CD3 complex together stably but also provide the “wiring” bridging the >10 nm spatial gap between ligand engagement at the TCR $\alpha\beta$  N-termini and ITAM phosphorylation at the CD3 cytoplasmic tails (Supplementary Fig. 8A, *right*). NMR chemical-shift perturbation experiments revealed TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ –CD3 $\delta\epsilon$  ECD dimeric interactions (26), but their functional relevance has been difficult to test because these contacts are exceptionally weak and fast. Using MAF and BFP assays that measure direct physical interactions in the same membrane-proximal geometry where these interfaces exist, we quantified the kinetics of TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ –CD3 $\delta\epsilon$  bimolecular binding and CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  trimolecular binding both in the absence and presence of force, showing that these ECD *cis*-interactions are not merely structural accessories but are force-bearing, force-regulated bonds. A key indication that the TCR–CD3 ectodomain junction can function as a mechanically addressable coupling element—capable of transmitting, filtering, and stabilizing information under load rather than simply holding the complex together at rest—is the discovery that these interactions form *cis*-catch bonds (Supplementary Fig. 8A, *left*).

However, the individual TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ –CD3 $\delta\epsilon$  bimolecular catch bonds are too short-lived to sustain mechanotransmission over the lifetime of an agonist TCR–pMHC interaction. We showed that the solution to this paradox is cooperativity: When CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  engage TCR $\alpha\beta$  concurrently, the resulting trimolecular assembly exhibits strong positive *cis*-cooperativity, more likely forming a long-lived *cis*-catch bond whose mechanical stability matches that of the TCR–pMHC *trans*-catch bond (Supplementary Fig. 8B). While early assembly studies suggested *cis*-interaction cooperativity among the TM bundles in the TCR–CD3 intra-complex (17, 74) since



both CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  were required for their enhanced assembly with the TCR $\alpha\beta$  (25), the present work qualitatively demonstrated and quantitatively evaluated the trimolecular binding cooperativity, using a kinetic approach that follows our previous analysis of positive cooperativity in the TCR–pMHC–CD8 (50, 75, 76) and TCR–pMHC–CD4 (46) trimolecular interactions, as well as the negative cooperativity between two distinct sets of immuno-*trans*-interactions: TCR–pMHC–CD8 and PD-1–PD-ligands (77). Note that our measurements are likely underestimated because the TCR and CD3 ECDs were measured under pseudo-*cis* configurations without TM bundling, which would place them in the most appropriate orientations, especially when CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  were captured randomly as CD3m on the beads. In addition to biophysical measurements, CMD and SMD simulations provide multiple lines of corroborative evidence for strong synergy. These include contact areas, free energies, dissociation times, distinct dynamic footprints, and contact residues between the ECDs of TCR $\alpha\beta$  and two CD3s separately or concurrently. Regardless of the metrics used, our results definitively demonstrated positive cooperativity in the TCR–CD3 *cis*-interactions, as the integrated response of the complex exceeded that of its individual components. Specifically, the whole trimolecular interaction forms more H bonds with larger footprints and stronger contacts that are mechanically more stable and longer lasting than even the sum of the two bimolecular interactions. Conceptually, cooperativity converts two weak, transient tethers into an integrated “mechanical clutch”: force preferentially stabilizes the coupled state, enabling sustained load sharing and extending the time window for downstream signaling to commit (Supplementary Fig. 8B).

The ability of the cooperative TCR–CD3 ECD *cis*- catch bond to support force for times that match the lifetime of cognate TCR–pMHC *trans*-catch bond implies their importance in signal relay. This may be significant in light of our current perspectives on the role of the *trans*-catch bond in

TCR mechanosensing, which enhances the predictive power for T cell response beyond that of binding affinity in the absence of force (9, 39, 78). By comparison,  $\gamma\delta$ TCR–CD3 complexes lack interactions among ECDs with flexible CPs (79–81); correspondingly,  $\gamma\delta$ TCR–ligand *trans*-interactions form slip bonds and lack mechanosensing (12). This contrast highlights the importance of the cooperative trimolecular *cis*-catch bond revealed here, which must contribute, at least in part, to the “mechanical conduit” with the needed structural connectivity among various  $\alpha\beta$ TCR–CD3 chains important for signaling. Such connectivity must be critical for supporting force, regardless of whether applied externally by pMHC or generated endogenously via CD3 cytosolic tails. An interrelated dual role may be envisioned for the cooperativity-reinforced *cis*-catch bond: First, force does not merely test bond strength; it selects bond state. Catch behavior implies an underlying force-favored bound conformation (or pathway) that is accessed more frequently or stabilized under loads. Second, because the cooperative *cis*-catch bond is maximally stabilized within a defined force regime, the TCR–CD3 junction can act as a “force band-pass filter,” preferentially transmitting signals within the physiological force window and rejecting either insufficient load (no stabilization) or excessive load (slip-driven rupture). In this view, the mechanistic role of *cis*-cooperativity is not simply to strengthen the complex, but to shape how mechanical information is encoded in bond lifetimes and, thus, signaling probability. Therefore, our findings support the TCR mechanotransduction hypothesis (9, 39) and are also consistent with the allostery hypothesis (82).

Further support for this view comes from observed fluctuations that are inversely correlated with the cooperatively enhanced contact stability, consistent with dynamic allostery rather than purely elastic linkages within both TCR and CD3 ECDs. NMR (32, 33) and CMD (33, 41) studies have observed long-range allosteric communication across the TCR $\alpha\beta$  ECD upon ligand engagement,

manifesting as chemical shift changes and increased dynamics at the CD3 binding site, suggesting regulatory capacity via distant conformational coupling. Dynamics of CD3s have been hypothesized to be the primary drivers of cross-membrane signal transmission, based on their more structured CP regions compared to the flexible TCR anchors (83). Although early cryo-EM (29, 30) and photo-crosslinking (27) studies failed to detect a different stable conformation upon pMHC or activating antibody ligation in the absence of force, a recent cryo-EM study observed distinct conformations of the TCR–CD3 complex preserved in native states using nanodiscs (35). The conceptual connection is that cooperative *cis*-coupling provides a plausible means to stabilize and mechanically gate such large-scale ECD rearrangements: weak pairwise contacts would be insufficient to sustain coordinated motion, whereas a cooperative *cis*-catch bond could maintain quaternary integrity while allowing force to bias transitions between compact and open ensembles.

Consistent with the mechanically regulated dynamic allostery is the asymmetric responses of the two CD3 ECDs, arising from their dissimilar molecular architectures and distinct interactions with the TCR  $\alpha$  and  $\beta$  chains (Supplementary Fig. 8A, *right*). The C $\beta$  FG loop has been suggested to be important for TCR mechanosensing, partly because of its proximity to the CD3 $\gamma$  ECD, which may restrict domain motions (40, 84, 85). Additionally, CD3 $\delta\epsilon$  exhibits heavier glycosylation than CD3 $\gamma\epsilon$  (57, 86), suggesting a tighter association of CD3 $\gamma\epsilon$  with TCR $\beta$  than CD3 $\delta\epsilon$ . Here, we found that across SMD and BFP (but not CMD and MAF) measurements, CD3 $\delta\epsilon$  is more force-responsive and undergoes greater contact reshaping and fluctuation changes, whereas CD3 $\gamma\epsilon$  maintains a more invariant interface with TCR $\alpha\beta$  and appears mechanically more stable. This division of labor suggests a useful conceptual model: CD3 $\gamma\epsilon$  behaves as a stabilizing strut that preserves the coupled architecture under load, while CD3 $\delta\epsilon$  behaves as a compliant hinge that accommodates force-induced rearrangements. Such asymmetric compliance provides a plausible

way to meet two competing requirements of mechanotransduction: the complex must remain connected long enough to transmit load, yet must also remain dynamic enough to permit conformational/dynamical transitions that ultimately gate tail exposure and ITAM phosphorylation. Indeed, the ECD asymmetry revealed here may be related to the structural (35) and functional (87) differences of CD3 chains during TCR triggering. Our findings shed light on the asymmetric behaviors of  $\epsilon$  chains, warranting further investigation: upon TCR–pMHC binding, the cytoplasmic tail of  $\gamma$ -associated  $\epsilon$  is kept in a constrained, inactive conformation by binding to the inner leaflet of the plasma membrane, while that of  $\delta$ -associated  $\epsilon'$  is exposed to the cytoplasm, ready to be phosphorylated by Lck to initiate TCR signaling.

Mutagenesis was used to perturb the ECD *cis*-bonds within the TCR–CD3 assembly to further elucidate their potential mechanotransduction role. Three double mutations at the TCR $\alpha\beta$  constant domains were examined due to the high dynamic contacts of these residues with the CD3s, which also show GOF (NP) and LOF (GK and NH) effects as measured by IL-2 production in antigen-stimulated T hybridoma cells (26). Interestingly, none of these mutants altered their effective 2D affinities with either CD3 or the normalized average number of bonds with both CD3s when measured in the absence of force. A similar lack of effect was observed with these mutants for bimolecular catch bonds. The only exception was the NP mutation, which forms a much more pronounced catch bond with CD3 $\delta\epsilon$  but not CD3 $\gamma\epsilon$ . Again, this force-dependent asymmetry may be related to the asymmetric behavior of the two  $\epsilon$  cytoplasmic tails, for the more adaptive TCR $\alpha\beta$ –CD3 $\delta\epsilon$  *cis*-bond may serve as the preferred path of force transmission to enable the larger share of total force through the  $\epsilon'$  chain, facilitating the release of its cytoplasmic tail for signal initiation. Hypothetically, the mechanotransmission of information requires the TCR–CD3 complex to have a mechanically integrated architecture with directional constraints, achieved by asymmetric

coupling, to allow binding of different ligands to tip the balance among pre-existing states of an energetically metastable structure, enabling force-regulated conformational changes to propagate allosterically. Thus, the C $\beta$  mutants further sharpen the mechanistic picture by separating equilibrium binding from mechanical coupling. Despite leaving force-free *cis*-affinity/bond number largely unchanged, these substitutions remodel the force-dependent lifetime landscape—most prominently for the cooperative trimolecular *cis*-catch bond—demonstrating that the functional lever resides in force-activated dynamics rather than in static affinity. In other words, these mutations tune the mechanical impedance of the TCR–CD3 junction: they alter how the interface redistributes force and stabilizes (or destabilizes) mechanically favored bound states. This also provides a practical design principle: mechanotransduction can be engineered by targeting residues that modulate the “force-response” of *cis*-coupling, without necessarily perturbing antigen recognition chemistry.

Surprisingly, the GOF mutation suppressed the trimolecular *cis*-catch bond, whereas both LOF mutations enhanced it. This apparent paradox is explained by our MD simulation results, showing that the GOF mutant enables, whereas the LOF mutants disable the TCR $\alpha\beta$  synergistic associations with the CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$ . These opposing effects enhance and restrict CD3 flexibility, respectively, thereby amplifying and attenuating downstream signaling, correspondingly. Indeed, this explanation is consistent with cryo-EM and crosslinking studies, which show that TCR mutants that strengthen the TCR–CD3 interface paradoxically impair T-cell function (27), underscoring the functional relevance of CD3 motions.

Previously, we found the same mutations produced a positive correlation between T-cell function and *trans*-bond profile: the GOF mutant TCR (NP) formed a stronger catch bond than WT, whereas the LOF mutants (GK and NH) formed a weaker catch bond or even a slip bond, supporting the

predictions from our structural and biophysical model of TCR–pMHC bond profile (42). The model suggests that domain stretching, tilting, and rotating near the hinges of the V $\alpha$ /V $\beta$  and C $\alpha$ /C $\beta$  domains facilitate *trans*-catch bond formation. A striking finding of the present work is the inverse relationship between the cooperative *cis*-catch bond and T-cell function, together with the anti-correlation between the *cis*- and *trans*-bond profiles (Supplementary Fig. 8C). These trends suggest a tradeoff between internal complex stability and external ligand sensitivity: excessive stabilization of the intra-complex *cis*-junction may “over-clutch” the receptor, restricting the structural compliance that supports optimal *trans*-catch bond formation and antigen discrimination, whereas a more labile *cis*-junction may permit the conformational freedom needed to maximize *trans* mechanosensing—up to the point where connectivity becomes limiting. Thus, the unexpected results from this work actually validate our previous model, for the weaker the *cis*-catch bond, the more flexible the TCR–CD3 complex, the stronger the *trans*-catch bond, and the more potent the T cell function. This view is also consistent with the findings of previous studies, which show that LOF and GOF mutations in TM residues correspond to those that stabilize and destabilize the TCR–CD3 complex, respectively (18, 88). We therefore propose that TCR triggering requires not maximal *cis*-stability per se, but a balance between connectivity and mobility, such that force can be transmitted while motion remains permissible.

# **MATERIALS AND METHODS**

## **Proteins, cells, and antibodies**

A biotinylation sequence (GLNDIFEAQKIEWHE) was added to the N-terminus of ECD constructs of 2B4 TCR $\alpha\beta$  and the C-terminus of human CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$  subunits through PCR. For the single heterodimer CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$ , a 26-residue peptide linker, C-GSADDAKKDAKKDDAKKDDAKKDGS-N, was engineered to connect different CD3 chains (89). For the CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$  heterodimer–heterodimer, a different 25-residue peptide linker, C-GSSPNSASHSGSAPQTSSAPGSQGS-N, was added to join the two dimers (90). Proteins were expressed in One Shot™ *E. coli* BL21 (DE3) (Invitrogen) as insoluble inclusion bodies, refolded, and purified as previously described (26). Inclusion bodies for IE<sup>k</sup>  $\alpha$  (with C-terminal biotinylation sequence) and  $\beta$  chains were produced in One Shot™ *E. coli* BL21 (DE3), refolded with K5 peptide (ANERADLIAYFKAATKF), and purified as described previously (91). For all proteins, purified fractions were biotinylated using a BirA protein ligase kit (Avidity LLC). The biotinylated proteins were further purified by gel filtration (S200, GE Life Sciences) in PBS (pH 7.4). The proteins were tested for biotinylation efficiency by gel-shift analysis after incubation with excess streptavidin.

Mouse 58<sup>-/-</sup> T cell hybridoma cells (92) expressing mouse CD3 but not TCR $\alpha\beta$  were a generous gift from Dr. Bernard Malissen (Centre d'immunologie de Marseille-Luminy, France). 58<sup>-/-</sup> cells were transfected with mutant mouse 2B4 TCR constructs through retroviral transduction and cultured as described previously (26). The transduced cells were stained with PE anti-mouse CD3 $\epsilon$  (clone 145-2C11, eBioscience) and allophycocyanin (APC)-conjugated anti-TCR $\beta$  (clone H57-597, eBioscience) mAbs, then sorted for dual expression of CD3 and TCR. The sorted cells were expanded for 6 days and quantified for TCR and CD3 $\epsilon$  expression.

## Flow cytometry and site density

Samples were stained using 10 µg/ml (as indicated below) of antibodies in 100 µl of FACS buffer (PBS or Hanks Ca<sup>2+</sup>/Mg<sup>2+</sup> free, 2% FBS, 5 mM EDTA, and 0.1% NaN<sub>3</sub>) for 30 min at 4 °C. Subsequently, samples were washed twice in 500 µl and then resuspended in 300 µl of FACS buffer. High-performance analysis and sorting were conducted using BD FACS Aria™ III, then flow cytometric data were processed using FlowJo™ Software. PE-conjugated anti-mTCRβ (clone H57-597, BD Biosciences), anti-mIE<sup>k</sup> (clone 14-4-4S, BD Biosciences), and PE-Cy7-conjugated anti-mCD3ε (clone 145-2C11, BD Biosciences) were used for *trans*-interactions. PE-conjugated anti-mTCR Vα11.1, 11.2 (clone RR8-1, Biolegend), anti-hCD3ε (clone UCHT1, Biolegend), isotype rat IgG2b,κ (clone RTK4530, Biolegend), isotype mouse IgG1,κ (clone MOPC-21, Biolegend) were used for *cis*-interactions.

## Micropipette adhesion frequency assay

The MAF assay for measuring 2D affinity has been described previously (59, 60). Briefly, human RBCs were isolated from whole blood obtained from healthy donors using a protocol approved by the Institutional Review Board of the Georgia Institute of Technology. RBCs were biotinylated with various concentrations of biotin-X-NHS linker (Millipore/Sigma) to achieve different levels of surface functionalization. Then, the biotinylated RBCs were incubated with a saturating amount of tetrameric streptavidin (Thermo Fisher) and the biotinylated protein of interest for 30 min at room temperature for each step. Based on available biotin sites, the protein was fully coupled to RBCs via biotin-streptavidin-biotin conjugations, and the resulting surface density was quantified by flow cytometry.

An experiment chamber was assembled by sandwiching coverslips onto short-edge metal spacers, leaving long-edge gaps open for inserting solutions and reagents. The channel bridging two metal



spaces was created by filling the center space with Leibovitz's L-15 Medium (Gibco) and sealing the solution with mineral oil. The chamber was mounted on the stage of an inverted microscope (a 40×/NA 0.75 objective with a 4× TV tube, Nikon, Eclipse Ti) and imaged at 200 frames per second (Basler, Ace 2). RBCs, beads, and hybridoma cells were loaded into different regions of the channel; the forged micropipettes (Sutter Instrument, P-97) were inserted from each side of the openings to form opposing alignments.

Using suction pressures from the manometer systems, a pair of RBCs (or a RBC and a bead or a hybridoma cell), bearing receptor and ligand, respectively, were captured by two opposing capillary micropipettes (Fig. 1A). The piezo-driven target RBC on the right was brought into contact with the stationary probe RBC on the left in the repeated “approach-contact-retract” testing cycles. Binding vs. non-binding events were sampled at a constant contact time and a consistent contact area: upon retraction, RBC elongations reflect binding as 1, and no deformations indicate non-binding as 0. The adhesion frequency ( $P_a = \langle s \rangle$ ) is the mean of the obtained Bernoulli sequence (*i.e.*,  $\{s_1, s_2, s_3, \dots, s_n\}$ ), in other words, the probability of the occurrence of binding events.

Due to the ultra-low affinities, the *cis*-bond formations are *i.i.d.* and rare. Thus, the probability of forming  $n$  bonds obeying the Poisson distribution,  $p_n = (\langle n \rangle^n / n!) \exp(-\langle n \rangle)$ , with a single parameter,  $\langle n \rangle$ , the mean number of bonds formed during contact time. As a result, the adhesion frequency is expressed as,

$$P_a = 1 - p_0 = 1 - \exp(-\langle n \rangle). \quad (1)$$

To further relate the characteristic  $\langle n \rangle$  to pairwise *cis*-binding kinetics, we established the kinetic differential equation that is governed by the second-order forward and first-order reverse reactions,

$$\frac{d\langle n \rangle}{dt} = m_r m_l A_c k_{on} - k_{off} \langle n \rangle \quad (2)$$

733 , where  $m_r$  and  $m_l$  ( $\mu\text{m}^{-2}$ ) are site densities of receptors and ligands on the RBC surfaces,  $A_c$  ( $\mu\text{m}^2$ )  
734 and  $t$  (s) are contact area and time;  $k_{on}$  ( $\mu\text{m}^2 \text{ s}^{-1}$ ) and  $k_{off}$  ( $\text{s}^{-1}$ ) are 2D on-rate and off-rate, whose  
735 ratio gives 2D affinity  $K_a = k_{on}/k_{off}$  ( $\mu\text{m}^2$ ). Clearly, one of Eq. 2 solutions is,

$$\langle n \rangle = m_r m_l A_c K_a [1 - \exp(-k_{off} t)] \quad (3)$$

736 , whose integration constant is zero, assuming there is no bond initially. Because of the rapid off-  
737 rates of *cis*-interactions, the exponential term vanishes at steady-state with a long contact time (2  
738 s). As a result, effective 2D affinity  $A_c K_a$  can be simply derived from  $P_a$  by,

$$A_c K_a = \frac{\langle n \rangle}{m_r m_l} = \frac{-\ln(1 - P_a)}{m_r m_l}. \quad (4)$$

739 Here,  $m_r$  and  $m_l$  were determined by calibrating the mean fluorescence intensity (MFI) of a  
740 protein of interest fully stained with a PE-tagged antibody against the MFI of PE quantitation beads  
741 (BD Biosciences) by flow cytometry.

## 742 **Biomembrane force probe (BFP)**

743 The BFP thermal fluctuation (60, 62) and force-clamp (43, 50) assays for measuring bond lifetime  
744 in the absence and presence of force, respectively, have been described in detail previously. Briefly,  
745 isolated human RBCs were treated and functionalized to form ultra-sensitive mechanotransducers.  
746 Probe RBCs were fully biotinylated with a saturated amount of biotin-PEG-NHS (JenKem), then  
747 inflated into hypotonic states by nystatin (ThermoFisher). Next, the probe beads were prepared for  
748 dual roles: to attach to the RBCs and to display the protein of interest. In short, streptavidin-  
749 maleimide (Sigma) was clicked onto thiol-functionalized glass beads (MPTMS, Thermo Fisher)  
750 overnight at 4°C. Afterward, the biotinylated protein-of-interest was partially coupled to the  
751 streptavidin beads (90 minutes at room temperature), leaving enough vacancies for RBC

attachments through biotin-streptavidin interactions. Lastly, either beads, RBCs, or cells were used as the targets, on which the binding partners were either chemically conjugated or naturally assembled for the probe to test against.

A similar experiment chamber (see MAF section) was prepared prior to loading the probe RBCs, probe beads, and targets. In addition to the two opposing micropipettes, a third helper pipette was inserted to assist probe assembly: capturing smaller probe beads and attaching them to the apex of RBCs. The microscope was set up in the same way, but aside from Basler visualization, another high-speed CCD camera (Mako G040B, Allied Vision) was utilized to trace any deformations of the probe RBCs. To do so, a 60-line strip window across the probe was imaged at 1,200 frames per second, where a homemade dual-edge tracking program (LabVIEW, Texas Instruments) scanned the real-time bead positions relative to the reference on the pipette (*i.e.*, the axial length of probe RBCs). This drift-prone design allows ultra-stable and ultra-sensitive micro-manipulations with  $\sim 2$  nm spatial and  $\sim 1$  ms temporal resolutions.

# 1. Thermal fluctuation assay

This assay is based on the equipartition theorem (62, 65), where the RBCs elastic energy is quadratic under small deformations,

$$\frac{1}{2}\kappa_x\langle\Delta x^2\rangle = \frac{1}{2}k_BT \quad (5)$$

, where  $\kappa_x$  is the spring constant of RBC's simple harmonic motion, and  $k_B$  is the Boltzmann constant that scales absolute temperature to energy. The union of the target with the probe, via bond formation, dampens its Brownian motion, equivalent to adding a parallel spring that stiffens the system with a ramped-up spring constant. Whereas bond breakage leads to the restoration of  $\kappa_x$ . Due to the anti-correlation between  $\kappa_x$  and  $\langle\Delta x^2\rangle$ , the bond association and dissociation events

were pinpointed by the sudden decreases and increases in the variance of probe displacements, respectively.

During the course of measurements, we adjusted the manometer system to lightly grab the probe RBC using the left micropipette, keeping the RBC ultra-soft with small  $\kappa_x$  to promote sensitive detections. Subsequently, the probe bead was aligned and pushed against the apex of probe RBC, where biotin-streptavidin firmly fused them to assemble the complete mechano-sensing probe (Fig. 1b, *left*). Then, we brought the target to the proximity of the probe, leaving a tiny gap between the target's receptor-presenting and the probe bead's ligand-presenting surfaces. Hence, the thermal-driven  $\Delta x$  occasionally closed the gap to allow the ligand-receptor binding. If bonds occurred, the durations between the onsets of  $\langle \Delta x^2 \rangle$  reductions and the moments of  $\langle \Delta x^2 \rangle$  resumptions (*i.e.*, sequence of events from the exponential random variable,  $\{t_1, t_2, t_3, \dots, t_n\}$ ) were sampled, whose mean reports the ligand-receptor lifetime,  $\tau = \langle t \rangle$ . Note that the adhesion frequency was kept low enough to ensure limited second bond formation before breaking the first bond.

To calculate the off-rate,  $k_{\text{off}}$  of pairwise interactions from sampled lifetime events, the kinetic differential equation of first-order reverse reaction is simplified by setting  $k_{\text{on}} = 0$  (Eq. 2) as,

$$\frac{d\langle n \rangle}{dt} = -k_{\text{off}}\langle n \rangle. \quad (6)$$

Its solution is scalable with the initial number of bonds,  $\langle n_0 \rangle$ , and reexpressed as the time-dependent survival probability,  $P_s(t)$ ,

$$P_s(t) = \frac{\langle n \rangle}{\langle n_0 \rangle} = \exp(-k_{\text{off}}t). \quad (7)$$

As a result,  $P_s(t)$ , the number of events lasting longer than  $t$  normalized by total lifetime events, starts from point (0, 1) and decays exponentially. After rearranging lifetime events chronologically, the linear regression slope of survival probability vs. time in logarithmic scale estimates  $k_{\text{off}}$ .

## 2. Force-clamp assay

The force-clamp assay utilized the same BFP micropipette apparatus, probe setups, and coating strategies as the thermal fluctuation assay (Fig. 1B). Nonetheless, instead of passively monitoring lifetime events without interference, we precisely quantified and interactively manipulated the force levels exerted on the ligand-receptor bonds to obtain the force-dependent lifetime,  $\tau(f)$ . The probe, as a harmonic oscillator, obeys Hooke's law,

$$f = \kappa_x \Delta x \quad (8)$$

, where  $\kappa_x$  converts the axial displacements into the force applied by the spring. To fine-tune probe stiffness, the suction pressure ( $\Delta p$ ) on probe RBCs modulates the hypotonic RBC membrane tension, which, in turn, relates to the spring constant by a geometric scaling factor as,

$$\kappa_x(\Delta p) \approx \frac{2\pi}{\ln\left(\frac{4R_0^2}{R_p R_c}\right)} \sigma = \frac{\pi R_p \Delta p}{\left(1 - \frac{R_p}{R_0}\right) \ln\left(\frac{4R_0^2}{R_p R_c}\right)} \quad (9)$$

, where  $\sigma$  is the membrane tension, and the characteristic measures of the probe,  $R_0$ ,  $R_p$ , and  $R_c$ , are radii of the outer RBC sphere, the inner RBC cap, and the bead-RBC circular contact, respectively. Typically, the designated  $\Delta p$  sets  $\kappa_x \sim 0.3$  pN/nm, which establishes the ultra-sensitive force sensor at a resolution of  $\pm 5$  nm in  $x$ -deformations.

During experiments, once fine-tuned to the specified stiffness, we utilized a high-precision piezoelectric linear actuator (Physik Instrumente) to micro-manipulate the target, allowing it to undergo “approach-contact-retract-hold-return” testing cycles against the stationary probe. Based on the instantaneous  $f(t)$ , automated subprograms (LabVIEW, Texas Instruments) made interactive decisions about the target’s sub-nanometer movements. The target **approached** the probe till  $f(t)$  dropped below zero. Next, the target was stopped at  $f(t) \sim -25$  pN and **contacted** the probe

to facilitate ligand-receptor associations for a fixed period of  $\sim 0.5$  s. At its end, the piezo **retracted** the target from the probe with two outcomes: a non-binding event was indicated by  $\langle f(t) \rangle \sim 0$ , and a binding event was detected by  $\langle f(t) \rangle \gg 0$  at the moment of separation (Fig. 1F). If the ligand-receptor formed a bond and the ramping-up force reached an expected level,  $f$ , the target was **held** in place to maintain the constant  $\Delta x$ , such that the tensile force on the bond was clamped until the spontaneous dissociation occurred (*i.e.*, the sudden decline of  $f(t)$ ). Later, the piezo **returned** the target to its origin to reinitiate the next testing cycle. Among 100s of cycles tested on a pair of targets and probes, lifetime events (*i.e.*,  $\{t_1^f, t_2^f, t_3^f, \dots, t_n^f\}$ ) were sampled as the time intervals between the instants of  $f(t)$  ramped up to the desired magnitudes, and the moments of  $f(t)$  suddenly dropped to zero. The mean of lifetime events reports the force-dependent ligand-receptor lifetime,  $\tau^f = \langle t^f \rangle$ , where the superscript denotes being subjected to the force-clamping of  $f$ . To ensure that most interactions represented single-bond events, the site densities of the molecules coated on the beads were adjusted to maintain the adhesion frequency below 20%.

## Cooperativity analysis

Multiple metrics were implemented to assess the cooperativity of *cis*-interaction, such as 2D affinity, force-dependent bond lifetime, *etc.* When CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  were co-presented, the comparisons between the actual measurements and the expected values assuming independence revealed the level of cooperativity of the TCR and CD3 mixture. To formulate a criterion and a quantitative index for cooperativity, we derived the general form as,

$$\frac{\Delta\langle Y \rangle}{\langle \hat{Y}_m \rangle} = \frac{\langle Y_m \rangle - \langle \hat{Y}_m \rangle}{\langle \hat{Y}_m \rangle} = \frac{\langle Y_m \rangle}{\langle \hat{Y}_m \rangle} - 1 \begin{cases} > 0 & \text{positive cooperativity} \\ = 0 & \text{zero cooperativity} \\ < 0 & \text{negative cooperativity} \end{cases} \quad (10)$$

, where  $Y$  is an arbitrary random variable about *cis*-interaction, and  $Y_m$  and  $\hat{Y}_m$  are the obtained and expected values from the CD3 mixture, respectively. Zero cooperativity indicates independent

binding, while positive or negative cooperativity signifies dependent binding, with the magnitude of cooperativity quantifying the level of dependency.

Three types of cooperativity analysis were employed to evaluate the *cis*-bindings between TCRαβ and CD3γε, CD3δε mixture using *in vitro* MAF, BFP, and *in silico* SMD dissociation assays. Under the assumption of independent bindings, the expected values for corresponding assays are listed below,

$$\text{MAF} \quad \langle \hat{n}_m \rangle = m_{\alpha\beta} m_{\gamma\epsilon} A_c K_a^{\gamma\epsilon} + m_{\alpha\beta} m_{\delta\epsilon} A_c K_a^{\delta\epsilon} \quad (11)$$

$$\text{BFP} \quad \hat{\tau}_m = \frac{m_{\gamma\epsilon} K_a^{\gamma\epsilon}}{m_{\gamma\epsilon} K_a^{\gamma\epsilon} + m_{\delta\epsilon} K_a^{\delta\epsilon}} \tau_{\gamma\epsilon} + \frac{m_{\delta\epsilon} K_a^{\delta\epsilon}}{m_{\gamma\epsilon} K_a^{\gamma\epsilon} + m_{\delta\epsilon} K_a^{\delta\epsilon}} \tau_{\delta\epsilon} \quad (12)$$

$$\text{SMD} \quad \langle \hat{t}_{\delta\gamma} \rangle = \langle t_{\gamma\epsilon} \rangle + \langle t_{\delta\epsilon} \rangle - \frac{\langle t_{\gamma\epsilon} \rangle \langle t_{\delta\epsilon} \rangle}{\langle t_{\gamma\epsilon} \rangle + \langle t_{\delta\epsilon} \rangle}. \quad (13)$$

Here,  $K_a$ ,  $\tau$ , and  $\langle t \rangle$  in expressions are characteristic kinetic parameters of pairwise *cis*-interactions quantified from corresponding TCRαβ–CD3γε and TCRαβ–CD3δε assays, while  $A_c$  and  $m$  are controllable factors. Note that  $\tau$  and  $\langle t \rangle$  distinguish the quantifications of lifetime using different approaches, where the former population study reports the ensemble average of multiple association states (subscript m), and the latter computer study is based on the single trimeric state (subscript δγ).

## Derivations of the expected value of trimeric dissociation lifetime

The expected values for the first two cooperativity analyses are straightforward, and we only show the derivations for Eq. 13 in detail here. The third cooperativity analysis is based on the waiting time of dissociations during SMD simulations. Again, this differs from the population mean of BFP lifetime measurements because we simulated a single-molecular construct at a time, either TCRαβ–CD3γε or TCRαβ–CD3δε, or CD3γε–TCRαβ–CD3δε complexes. Recall that the survival probabilities for the pairwise associations of TCRαβ–CD3γε and TCRαβ–CD3δε are,

$$P_s^{\gamma\epsilon} = \exp\left(-\frac{t}{\langle t_{\gamma\epsilon} \rangle}\right) \text{ and } P_s^{\delta\epsilon} = \exp\left(-\frac{t}{\langle t_{\delta\epsilon} \rangle}\right) \quad (14)$$

, respectively, where  $\langle t_{\gamma\epsilon} \rangle$  and  $\langle t_{\delta\epsilon} \rangle$  are their corresponding average waiting time till dissociation.

Assuming the CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  dissociations from the concurrently bound states are independent,

and the presence of high loads prevents any rebinding upon dissociations, the cumulative joint

probability for TCR $\alpha\beta$  to dissociate from both concurrently during  $(0, t)$  is,

$$\begin{aligned} F_{\delta\gamma}(t) &= \left(1 - P_s^{\gamma\epsilon}(t)\right)\left(1 - P_s^{\delta\epsilon}(t)\right) \\ &= 1 - e^{-t/\langle t_{\gamma\epsilon} \rangle} - e^{-t/\langle t_{\delta\epsilon} \rangle} + e^{-t(1/\langle t_{\gamma\epsilon} \rangle + 1/\langle t_{\delta\epsilon} \rangle)}. \end{aligned} \quad (15)$$

The corresponding probability density is,

$$\rho_{\delta\gamma}(t) = \frac{dF_{\delta\gamma}(t)}{dt} = \frac{e^{-t/\langle t_{\gamma\epsilon} \rangle}}{\langle t_{\gamma\epsilon} \rangle} + \frac{e^{-t/\langle t_{\delta\epsilon} \rangle}}{\langle t_{\delta\epsilon} \rangle} - \frac{e^{-t(1/\langle t_{\gamma\epsilon} \rangle + 1/\langle t_{\delta\epsilon} \rangle)}}{1/\langle t_{\gamma\epsilon} \rangle + 1/\langle t_{\delta\epsilon} \rangle}. \quad (16)$$

Thus, the expected value of trimeric dissociation lifetime under the non-coop assumption is,

$$\langle \hat{t}_{\delta\gamma} \rangle = \int_0^\infty t \rho_{\delta\gamma}(t) dt = \langle t_{\gamma\epsilon} \rangle + \langle t_{\delta\epsilon} \rangle - \frac{\langle t_{\gamma\epsilon} \rangle \langle t_{\delta\epsilon} \rangle}{\langle t_{\gamma\epsilon} \rangle + \langle t_{\delta\epsilon} \rangle}. \quad (17)$$

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## 860 Kinetic modeling of dual-species interaction

To model the dual-species scenario, in addition to the pairwise interactions in the single-species

scenario, only the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimolecular interaction is allowed as a concurrent

binding state. As such, for simplicity, the total TCR $\alpha\beta$  bonds with CD3m include only three

subpopulations.

$$\langle n_m \rangle = \langle n_{\gamma\epsilon}^m \rangle + \langle n_{\delta\epsilon}^m \rangle + \langle n_{\delta\gamma}^m \rangle. \quad (18)$$

, where  $n$  with different subscriptions denote the number of bonds for the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ -

CD3 $\delta\epsilon$  bimolecular interactions, and the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimolecular interaction,

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sequentially. Here, the concurrent mode exhibits unique kinetics, redistributing the probabilities of dimeric and trimeric bond formation.

The competitive kinetics between the pairwise and concurrent TCR $\alpha\beta$ -CD3s *cis*-interactions follow the two-step model. In the first step, the TCR $\alpha\beta$  interacts with either CD3 $\gamma\epsilon$  (kinetic rates  $k_1$  and  $k_{-1}$ ) or CD3 $\delta\epsilon$  (kinetic rates  $k_2$  and  $k_{-2}$ ) to form TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  or TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bimolecular bonds. In the second step, the TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bond interacts with CD3 $\gamma\epsilon$  (kinetic rates  $k_3$  and  $k_{-3}$ ) or the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  bond interacts with CD3 $\delta\epsilon$  (kinetic rates  $k_4$  and  $k_{-4}$ ) to form CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  trimolecular bonds. Refer to Eq. 2, the modified kinetic differential equations for the steady state are,

$$\frac{d}{dt} \begin{pmatrix} \langle n_{\gamma\epsilon}^m \rangle \\ \langle n_{\delta\epsilon}^m \rangle \\ \langle n_{\delta\gamma}^m \rangle \end{pmatrix} + \begin{bmatrix} m_{\delta\epsilon}k_4 + k_{-1} & 0 & -k_{-4} \\ 0 & m_{\gamma\epsilon}k_3 + k_{-2} & -k_{-3} \\ -m_{\delta\epsilon}k_4 & -m_{\gamma\epsilon}k_3 & k_{-3} + k_{-4} \end{bmatrix} \begin{pmatrix} \langle n_{\gamma\epsilon}^m \rangle \\ \langle n_{\delta\epsilon}^m \rangle \\ \langle n_{\delta\gamma}^m \rangle \end{pmatrix} = \begin{pmatrix} m_{\alpha\beta}m_{\gamma\epsilon}A_c k_1 \\ m_{\alpha\beta}m_{\delta\epsilon}A_c k_2 \\ 0 \end{pmatrix} \quad (19)$$

, whose solutions are derived as,

$$\langle n_{\gamma\epsilon}^m \rangle = \frac{m_{\alpha\beta}m_{\gamma\epsilon}A_c}{m_{\delta\epsilon}k_4 + k_{-1}} \left[ k_1 + m_{\delta\epsilon}k_{-4} \frac{k_1k_4(m_{\gamma\epsilon}k_3 + k_{-2}) + k_2k_3(m_{\delta\epsilon}k_4 + k_{-1})}{k_{-1}k_{-4}(m_{\gamma\epsilon}k_3 + k_{-2}) + k_{-2}k_{-3}(m_{\delta\epsilon}k_4 + k_{-1})} \right] \quad (20)$$

$$\langle n_{\delta\epsilon}^m \rangle = \frac{m_{\alpha\beta}m_{\delta\epsilon}A_c}{m_{\gamma\epsilon}k_3 + k_{-2}} \left[ k_2 + m_{\gamma\epsilon}k_{-3} \frac{k_1k_4(m_{\gamma\epsilon}k_3 + k_{-2}) + k_2k_{(45)}(m_{\delta\epsilon}k_4 + k_{-1})}{k_{-1}k_{-4}(m_{\gamma\epsilon}k_3 + k_{-2}) + k_{-2}k_{-3}(m_{\delta\epsilon}k_4 + k_{-1})} \right] \quad (21)$$

$$\langle n_{\delta\gamma}^m \rangle = m_{\alpha\beta}m_{\gamma\epsilon}m_{\delta\epsilon}A_c \frac{k_1k_4(m_{\gamma\epsilon}k_3 + k_{-2}) + k_2k_3(m_{\delta\epsilon}k_4 + k_{-1})}{k_{-1}k_{-4}(m_{\gamma\epsilon}k_3 + k_{-2}) + k_{-2}k_{-3}(m_{\delta\epsilon}k_4 + k_{-1})} \quad (22)$$

, where  $m$  with different subscriptions indicates the site densities of TCR $\alpha\beta$ , CD3 $\gamma\epsilon$ , and CD3 $\delta\epsilon$ , respectively.

The cooperativity resides in the second step by allowing the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  concurrent *cis*-engagements. As expected, letting  $k_3 = k_4 = 0$  abolishes the trimolecular bonds and reduces Eq. 20, 21 to the forms of Eq. 3 for the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bimolecular bonds.

Note that the comparison between the gain in  $\langle n_{\delta\gamma}^m \rangle$  and the loss in  $\langle n_{\gamma\epsilon} \rangle - \langle n_{\gamma\epsilon}^m \rangle$  and  $\langle n_{\delta\epsilon} \rangle - \langle n_{\delta\epsilon}^m \rangle$

defines the sign of cooperativity. Furthermore, the reduction of bimolecular bond fraction leads to the inequality of  $\langle n_{\delta\gamma}^m \rangle \geq \Delta \langle n \rangle$ . From which, the lower bound for the trimolecular bond fraction can be estimated using solely the value of cooperativity by  $\langle n_{\delta\gamma}^m \rangle / \langle n_m \rangle \geq \Delta \langle n \rangle / (\Delta \langle n \rangle + \langle \hat{n}_m \rangle)$  (i.e., cooperativity divided by one plus cooperativity). For example, based on the bond number cooperativity of 170% that we measured, the chance of trimolecular bond formation is higher than 62% of the total bonds.

To model the dual-species dissociation processes, similar to the off-rate analysis in the thermal dynamic assay, by setting the right-hand side of Eq. 19 master equations to zero, we obtained the two-step dissociation of dual-species following a multi-exponential decay. Again, letting the second-step kinetic rates  $k_3 = k_{-3} = k_4 = k_{-4} = 0$  reduces the master equations to two uncoupled first-order reverse reactions for the TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ -CD3 $\delta\epsilon$  *cis*-dissociation, following single-exponential decays.

### Kinetic modeling of catch-bonds

The *cis*-bond profiles of TCR $\alpha\beta$  interacting with CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , or both all demonstrate catch-slip behaviors, with bi-exponential-decay survival probabilities, suggesting the presence of two bound species (93-95), particularly under the effects of clamping force. Therefore, for the analysis of force-dependent dissociations of bimolecular bonds, we assumed that a single bond might undergo either a fast-dissociation pathway from a weak state or a slow-dissociation pathway from a strong state (indicated by \*), also allowing them to exchange with each other. For the analysis of the mixture bond data, besides combining the two-pathway models obtained for the pairwise TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  and TCR $\alpha\beta$ -CD3 $\delta\epsilon$  dissociations, we added a third population of trimolecular CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  bonds using the same modeling scheme. The corresponding reaction diagrams for all scenarios are depicted in Supplementary Fig. 2A.

906 The force dependency of kinetic rates follows Bell's equation (96),

$$k_{i,j}(f) = k_{i,j}^0 \exp\left(\frac{fx_{i,j}}{k_B T}\right) \quad (23)$$

907 , where the subscript  $i$  denotes rates of dissociation along fast (-f) or slow (-s) pathways and of  
 908 activation into (a) or deactivation from (-a) the strong states; the subscript  $j$  denotes different bond  
 909 types of TCR $\alpha\beta$ -CD3 $\gamma\epsilon$  ( $\gamma$ ), TCR $\alpha\beta$ -CD3 $\delta\epsilon$  ( $\delta$ ), and CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  ( $\delta\gamma$ ); the superscript  
 910 0 denotes the respective force-free kinetic rates. According to transition state theory, the force  
 911 linearly modulates the free energy of the transition barrier,  $\Delta E^\ddagger(f) = \Delta E_0^\ddagger - fx$ , and subsequently  
 912 regulates the kinetic rates,  $k(f) = \exp(-(\Delta E_0^\ddagger - fx)/k_B T)$ , where  $x$  is the characteristic  
 913 transition distance, and  $k^0$  is proportional to  $\exp(-\Delta E_0^\ddagger)$ .

914 This two-state, two-pathway dissociation model (46) recapitulated the lifetime of catch bonds and  
 915 the bi-exponential decay of survival probabilities. Here, the force-free fast dissociation rates for  
 916 the dimeric bonds were obtained from the thermal fluctuation assay, and the remaining parameters  
 917 were then evaluated by globally fitting the model to the force-lifetime distributions via maximum  
 918 likelihood estimation (MLE). The initial proportions of the two states were determined from the  
 919 ratios of the kinetic rates, assuming equilibrium. A two-step optimization procedure was employed  
 920 to minimize the MLE: an extensive parameter space was explored using differential evolution to  
 921 obtain an approximate solution, followed by L-BFGS to hone in on the minimum (Supplementary  
 922 Fig. 2E-G). The resultant kinetic rates vs. force relationships are presented in Supplementary Fig.  
 923 2B-D, and Bell's parameters are summarized in Supplementary Table 2. The standard deviation  
 924 for each parameter was obtained by inverting the Hessian matrix at the MLE to approximate the  
 925 covariance matrix, whose diagonal entries correspond to the variance of the fitted parameters.

926 **Molecular dynamics simulations**

## 1. Molecular constructs

All simulations were based on the cryo-EM structure (PDB ID: 6JXR) (28). The TCR $\alpha\beta$ , CD3 $\gamma\epsilon$ , and CD3 $\delta\epsilon$  were truncated near the CPs between extracellular and intracellular regions, leaving the complete TCR–CD3s ECD in its trimeric assembly. The TCR $\alpha\beta$  were trimmed at their C-termini, leaving the  $\alpha$ -chain Gly22-Glu237 and the  $\beta$ -chain Val26-Glu269. The CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  were obtained by truncating the  $\gamma$ -chain after Cys107,  $\epsilon$ -chain after Asn121,  $\delta$ -chain after Glu98, and  $\epsilon'$ -chain after Glu124. To minimize potential trimming effects, all chain ends were modified to prevent the exposure of charged residues. An acetyl group was added in front of the N-terminus, and an N-methylamine group capped the C-terminus of every chain. All hydrogen atoms, as well as any missing atoms, were added back through Gromacs utilities (28). The disulfide bonds in the original cryo-EM structure were preserved through Gromacs interactive S-S bridge selection procedures (28). The resulting CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  trimeric assembly was used to simulate the concurrent *cis*-binding. Then, three partial assemblies were generated to simulate the pairwise *cis*-interactions by removing CD3 $\delta\epsilon$ , CD3 $\gamma\epsilon$ , and TCR $\alpha\beta$  individually from the fully-assembled ECDs, yielding dimeric TCR $\alpha\beta$ –CD3 $\gamma\epsilon$ , TCR $\alpha\beta$ –CD3 $\delta\epsilon$ , and CD3 $\gamma\epsilon$ –CD3 $\delta\epsilon$ , respectively.

## 2. Unit cell preparation

Unit cells enclosing molecular systems of interest were built with physiologically realistic surroundings and then brought into thermodynamically favorable states. The initial structures were oriented and centered within optimized orthorhombic cells, which accommodated the physical extensions in all directions with a  $\geq 1.6$  nm buffering zone apart from the box sides to ensure the protein was well-isolated. The molecules in unit cells were solvated using the TIP3P water model (97). The negative charges were counterbalanced using sodium ions, and then the ionic strength was set to  $\sim 150$  mM with sodium chloride. To further prepare the system thermodynamically,

energy-unfavorable close contacts were eliminated through the steepest descent and conjugate gradient energy minimization cycles. While restraining the heavy atoms in macromolecules, the unit cell was brought to a suitable ensemble employing a 200-ps velocity rescaling simulation to adjust the temperature and a 200-ps Berendsen Barostat simulation to correct the pressure (300 K, 1.01325 bar). After releasing the heavy-atom restraints, the systems were considered ready for subsequent equilibration and production runs.

### 3. Conventional molecular dynamics

CMD simulations were performed using GROMACS (version 2019.6) (98-100) under the recent AMBER99SB\*-ILDNP force field with improved helix-coil transitional and side-chain torsional dynamics (101). From previously prepared unit cells, the set of initial velocities was randomly sampled from the Maxwell-Boltzmann distribution. The molecular trajectories were self-evolved under the leap-frog algorithm by integrating Newton's law of motion every 2 fs. For CMD, the individual simulation runs were executed under periodic boundary conditions to sample the NVT ensemble under corresponding constant volumes (*i.e.*, CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$ :  $12.5 \times 10.8 \times 9.9$  nm<sup>3</sup>; TCR-CD3 $\gamma\epsilon$ :  $12.6 \times 9.8 \times 8.6$  nm<sup>3</sup>; TCR-CD3 $\delta\epsilon$ :  $11.9 \times 10.3 \times 9.2$  nm<sup>3</sup>; CD3 $\gamma\epsilon$ -CD3 $\delta\epsilon$ :  $11.5 \times 8.1 \times 8.0$  nm<sup>3</sup>) and 300 K constant temperature. The neighborhood lists were refreshed every 10 steps using the buffered Verlet scheme, with a 1.2 nm non-bonded cutoff for Coulomb and van der Waals interactions. The long-range potentials of electrostatic interactions were computed using the Particle Ewald Mesh summation method. All systems were simulated for 100s ns with three repeats, where each trajectory consists of at least a 50 ns equilibration stage and the remaining production run. Conformational snapshots every 0.1 ns during the production stage were extracted for subsequent analysis.

### 4. Steered molecular dynamics

SMD simulations were initiated from the well-equilibrated configurations from corresponding CMD simulations (*i.e.*, the conformational snapshots at 100 ns). They were prepared according to the Unit cell preparation section, but with a 20-nm box length to accommodate the molecular extension and separation under external pulling. The external forces with constant magnitudes (*i.e.*, force-clamp) or constant velocities (*i.e.*, force-ramp) along the fixed *z*-direction were added to the trimeric and dimeric complexes. The clamping or ramping forces were applied to the N-terminus of the TCR $\alpha$  chain to accelerate the dissociations while keeping the C-termini of CD3 $\epsilon$  chains fixed to mimic the anchor effect of their TM domains. For force-clamp simulations, five independent trajectories under 100, 125, 150, 175, and 200 pN were generated for each of the two dimeric systems, but only three independent runs under 150, 175, and 200 pN were executed for the trimeric complex. We aborted the CD3 $\gamma\epsilon$ -TCR $\alpha\beta$ -CD3 $\delta\epsilon$  simulations at smaller clamp forces of 100 and 125 pN due to the inability to observe dissociation events after the exceedingly long waiting time ( $> 1000$  ns). For force-ramp simulations, a 70 pN/nm pseudo spring was utilized to exert increasing levels of pulling to accelerate dissociations. One end of the spring was linked to the  $\alpha$  chain N-terminus of the targeting molecule, and the other free end departed in the *z*-direction at 1 nm/ns. Five repeats each for two dimeric and one trimeric ECD complexes were performed to assess the corresponding rupture forces as a consistency check.

## Occupancy analysis

Several variations of occupancy analysis were employed to dynamically evaluate the extent of a particular residue in dynamic contact with its binding partner throughout the simulation. At timestamp *i*, the residue being analyzed is defined to be in contact (denoted  $o_i = 1$ ) if the center of mass of this residue is within 4 Å of any atoms of its binding partner; otherwise, it is not in

touch (denoted  $o_i = 0$ ). The occupancy index (%) indicates the fraction of time in contact during a given period, as  $\sum_i o_i / N$ , where  $N$  is the total number of analyzed frames.

# **1. Residue-to-residue occupancy (Supplementary Fig. 5)**

By setting residues within a subunit as a reference group, this occupancy analysis quantifies the extent of dynamic interaction between each residue from one subunit and every single residue from the other subunit over a given period. Thus, it evaluated the level of any pairwise contacts, thereby forming a correlation matrix where the column indexes the residues from one subunit; the row indexes the residues from the other subunit, and the elements denote the values of residue-to-residue relative binding strength, ranging from 0 to 1.

# **1. Residue-to-domain occupancy (Supplementary Fig. 6)**

This occupancy analysis quantifies each residue against all residues within its binding partner, using the entire subunit as the reference group. It is usually smaller than the sum of residue-to-residue occupancy over the binding domain because the residue in question may simultaneously be in contact with multiple residues in the domain under consideration; on the other hand, these contact periods can only be counted once for residue-to-domain occupancy. To account for this disadvantage,  $\Sigma$ Occupancy is defined as the integration of the CMD and SMD row-/column-wise sums of residue-to-residue occupancies; while  $\Delta$ Occupancy is defined as the differentiation of the CMD from the SMD row-/column-wise sums of residue-to-residue occupancies, which were calculated to summarize and discriminate force-free and force-clamp interface dynamics (Fig. 4G, H).

# **2. Domain-to-domain occupancy**

1016 This occupancy analysis further reduces data presentation to examine the overall binding tendency  
1017 against the other domain by averaging over all interacting residues (*i.e.*, positive terms of residue-  
1018 to-domain occupancies), providing a measure of the overall domain-to-domain adhesion strength.

# 1019 **Linear regression**

1020 Linear regression was conducted to assess the correlations between *cis*-kinetic measures (as  $x$ ) and  
1021 functional outputs or *trans*-kinetic measures (as  $y$ ). The goodness-of-fit was quantified using  
1022 Pearson's correlation coefficient, *i.e.*,  $(n \sum xy - \sum x \sum y) / \sqrt{(n \sum x^2 - (\sum x)^2)(n \sum y^2 - (\sum y)^2)}$ ,  
1023 which preserves the sign of correlation, as well as its square, R-squared. The sensitivity-of-  
1024 prediction, *i.e.*,  $(n \sum x^2 - (\sum x)^2) / (n \sum xy - \sum x \sum y)$ , is the inverse of the linear-regression  
1025 slope.



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# **AUTHOR CONTRIBUTIONS**

C.Z., P.C., and C.G. conceived the study; C.Z. and M.K. directed the study; P.C., Z.Y., C.G., and A.N. performed experiments; P.C. performed simulations; P.C. and A.N. performed structural analysis; A.N., S.B, and D.G produced proteins; P.C. and S.T. analyzed data using mathematical models; P.C., A.N., Z.Y., M.K., and C.Z. analyzed data and wrote the paper with contributions from other authors.

# **STATEMENT OF COMPETING INTERESTS**

The authors declare no competing interests. M.K. serves on the scientific advisory boards of Genentech and Merck and Co. and received research support from Merck Sharp & Dohme Corp., a subsidiary of Merck and Co., Inc., Genentech, Biogen, Novartis, and the Mark Foundation.

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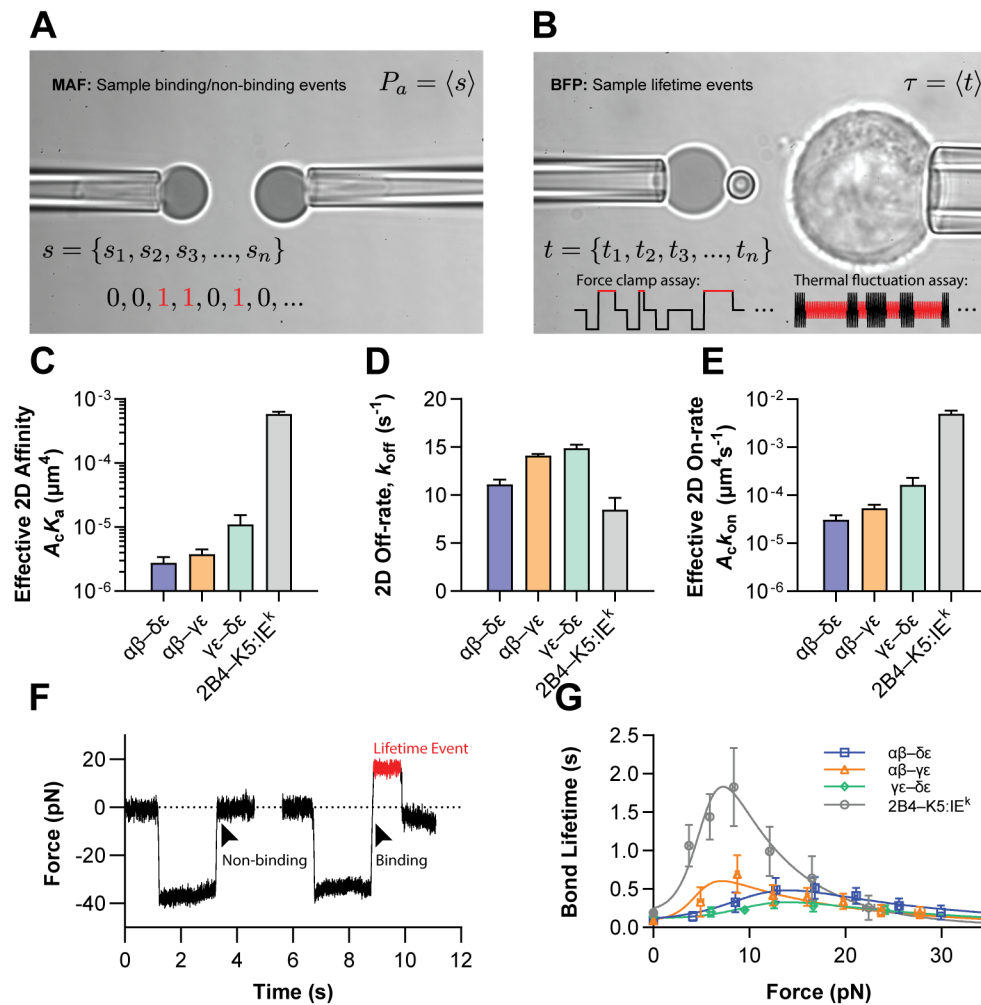
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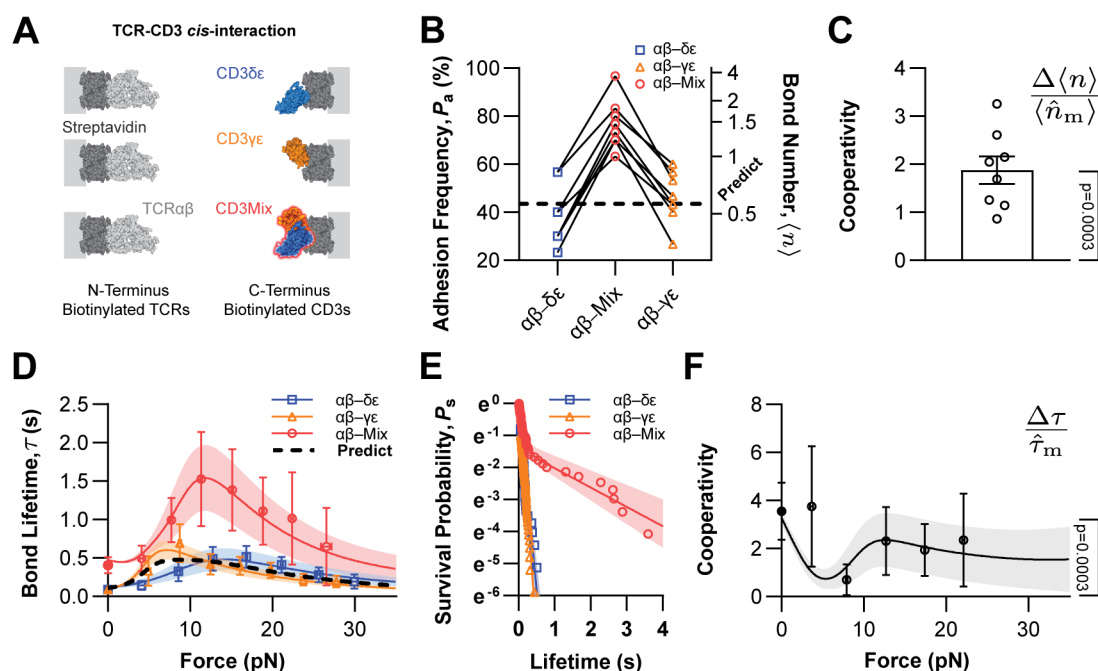
## FIGURE LEGENDS



**Figure 1. 2D kinetic quantifications of TCR $\alpha\beta$ –CD3 ECD *cis*-interactions.**

(A, B) Photomicrographs of the micropipette adhesion frequency (MAF) assay (A) and the biomembrane force probe (BFP) assay (B), overlain with legends indicating the measurement types. The two micropipettes held the probe (*left*) and the target (*right*), respectively, with each presenting one of the interacting pair. The target image shown in (B) is a hybridoma cell expressing full TCR–CD3 complexes, but beads coated with purified protein ECDs were also used, depending on the experiment. The target was brought into repeated contact with the probe to enable and interrogate ligand–receptor interactions. The probe, which was either a pressurized RBC (A) or a glass bead attached to the apex of the pressurized RBC (B), served a dual role of ligand presenter and force transducer, detecting the binding events to evaluate adhesion probability (A) and measuring bond lifetime (B), respectively, as indicated in the legends (see Methods). (C) Effective 2D affinities ( $A_c K_a$ ) of pairwise *cis*-interactions between the ECDs of TCR $\alpha\beta$  ( $\alpha\beta$ ), CD3 $\delta\epsilon$  ( $\delta\epsilon$ ), and CD3 $\gamma\epsilon$  ( $\gamma\epsilon$ ) measured by MAF. (D) 2D off-rates ( $k_{\text{off}}$ ) of the indicated *cis*-interactions quantified by the thermal fluctuation assay using BFP. (E) Calculated effective 2D on-rates ( $A_c k_{\text{on}} = A_c K_a \times k_{\text{off}}$ ) of the indicated *cis*-interactions. Data are presented as mean  $\pm$  SEM in (C)–(E), with the 2D affinity, off-

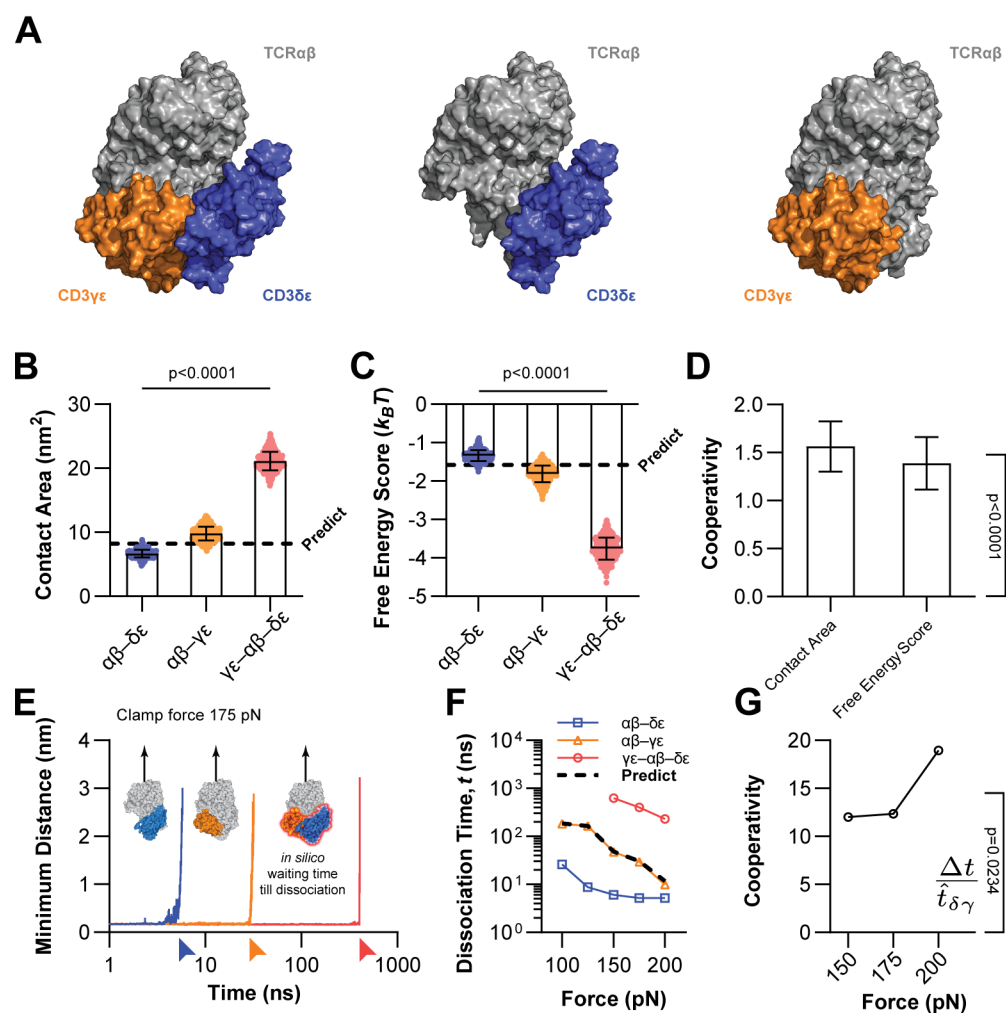
rate, and on-rate of the *trans*-interaction between cell-surface 2B4 TCR and its cognate pMHC K5:IE<sup>k</sup> (*gray*) also plotted in the corresponding panels for comparison. **(F)** Representative force traces of non-binding *vs.* binding events from the BFP force-clamp assay. The target, either a bead or a cell, was driven to approach the probe ( $\sim 0$  pN before contact), pressed against it for 1 s ( $\sim -35$  pN), which resulted in either a non-binding (returning to  $\sim 0$  pN) or a binding event (crossing 0 pN to a positive, tensile force) upon target retraction. The latter trajectory illustrates a lifetime event in which the ligand–receptor bond was clamped with a force of  $\sim 16$  pN for  $\sim 0.5$  s (*red*) until dissociation, indicated by a sudden drop in force to  $\sim 0$  pN. **(G)** Force-dependent average lifetimes of pairwise  $\alpha\beta$ – $\delta\epsilon$ ,  $\alpha\beta$ – $\gamma\epsilon$ , and  $\delta\epsilon$ – $\gamma\epsilon$  *cis*-bonds (*points*, mean  $\pm$  SEM of  $> 30$  lifetime events per force bin) at zero force by thermal fluctuation assay (*closed symbols*) and at non-zero forces by force-clamp assay (*open symbols*). The overlaid smooth curves are the global fits of the two-state dissociation model (Supplementary Fig. 2; see Methods). In contrast to *cis*-bonds, the points and curve in *gray* denote the previously published force-lifetime results of the 2B4–K5:IE<sup>k</sup> *trans*-interaction (42), which provides a direct comparison.



**Figure 2. Experimental demonstration of cooperativity in *cis*-interaction of CD3γɛ, CD3δɛ, and TCRαβ ECDs.**

(A) Experimental schemes. Purified protein ECDs were captured onto the RBC or bead surfaces through biotin-streptavidin (SA) coupling. N-terminally-biotinylated 2B4 hybrid TCRαβ was coated onto the probe (*left*), while C-terminally-biotinylated human CD3γɛ (*blue*), CD3δɛ (*orange*), or a 1:1 mixture of both (CD3m, *red*) was coupled onto the opposing target (*right*). These tail-to-head binding arrangements ensure preferred *cis*-interaction orientations for TCR-CD3 associations. (B) Adhesion frequency,  $P_a$  (*left ordinate*), and average bond number,  $\langle n \rangle = -\ln(1 - P_a)$  (*right ordinate*), measured by the MAF assay. The same TCRαβ-bearing RBC was tested sequentially against three RBCs bearing, respectively, CD3γɛ, CD3δɛ, or CD3m in random order (*points connected by solid lines*). These CD3-bearing RBCs were from the same batch of streptavidinylated cells, which were then incubated with saturating amounts of CD3γɛ, CD3δɛ, and CD3m, respectively, to equalize site density coating. Each probe-target pair was tested for 30 cycles, with a 2-s contact time per cycle. The predicted bond number of dual-ligand RBCs (*dotted line*),  $\langle \hat{n}_m \rangle$ , is the sum of the bond numbers of TCRαβ interacting with CD3γɛ and CD3δɛ, separately. Thus,  $\langle \hat{n}_m \rangle$  equals to the average of the bond numbers measured from the two RBCs bearing single CD3 species because the respective densities of CD3γɛ and CD3δɛ on the mixed ligand RBCs are half of the densities of CD3γɛ and CD3δɛ on the single-ligand RBCs under the assumption of concurrent and independent binding (see Methods). This no-cooperativity assumption is invalidated by the data, which clearly demonstrate that the actual measurements greatly outnumber the prediction (note that a log scale is used on the right ordinate). Several metrics were used to quantify cooperativity (*C*, *F*, and Fig. 3D, G), which is defined as the difference between the measurement and the prediction, normalized by the expected value assuming no cooperativity. (C) Positive 2D binding cooperativity of TCRαβ-CD3m *cis*-interaction.

Here,  $\Delta\langle n_m \rangle / \langle \hat{n}_m \rangle$  (*points*) utilized the bond number in (*B*) as the cooperative metric. The case of no cooperation corresponds to a zero value, whereas a greater than zero value reveals 2D binding cooperativity. **(D)** Force-dependent average bond lifetime,  $\tau(f)$ , for TCR $\alpha\beta$ -CD3m *cis*-interactions quantified using BFP. The predicted average bond lifetime of dual-species (*dotted line*),  $\hat{\tau}_m$ , is the weighted sum of the single-species force-lifetime curves of the  $\alpha\beta$ - $\delta\epsilon$  and  $\alpha\beta$ - $\gamma\epsilon$  bimolecular bonds (replotted from Fig. 1G for comparison). The weights are fractions of bond formation based on the 2D binding affinities of single-ligand *cis*-interactions (Fig. 1C) and corresponding amounts (1:1 ratio). The overlaid smooth curves are the global fits of the two-state, two-pathway dissociation models (Supplementary Fig. 2A-I; see Methods). **(E)** The bond survival probability for the TCR $\alpha\beta$ -CD3m *cis*-interactions derived from zero-force individual bond lifetimes (whose average is  $\tau(0)$ ) measured from the thermal fluctuation assay. The bond survival probability curves of the  $\alpha\beta$ - $\delta\epsilon$  and  $\alpha\beta$ - $\gamma\epsilon$  bimolecular bonds are shown for comparison (using pairwise lifetime data in Fig. 1D). **(F)** Positive bond lifetime cooperativity of dual-ligand *cis*-interaction,  $\Delta\tau/\hat{\tau}_m$ , using the bond lifetime in (*D*) as the cooperative metric. Again, the no cooperation case corresponds to a zero value, whereas a greater than zero value reveals cooperativity in force-dependent bond lifetime. In (*D*) and (*F*), data points are presented as mean  $\pm$  SEM from  $> 30$  lifetime-events per force bin; global-fitting force-lifetime and survival-probability curves (*D*, *E*, and *F*) are plotted with means (*solid line*) and standard deviations (*shaded area*). Significance in (*C*) and (*F*) was assessed using a one-sample t-test against zero.

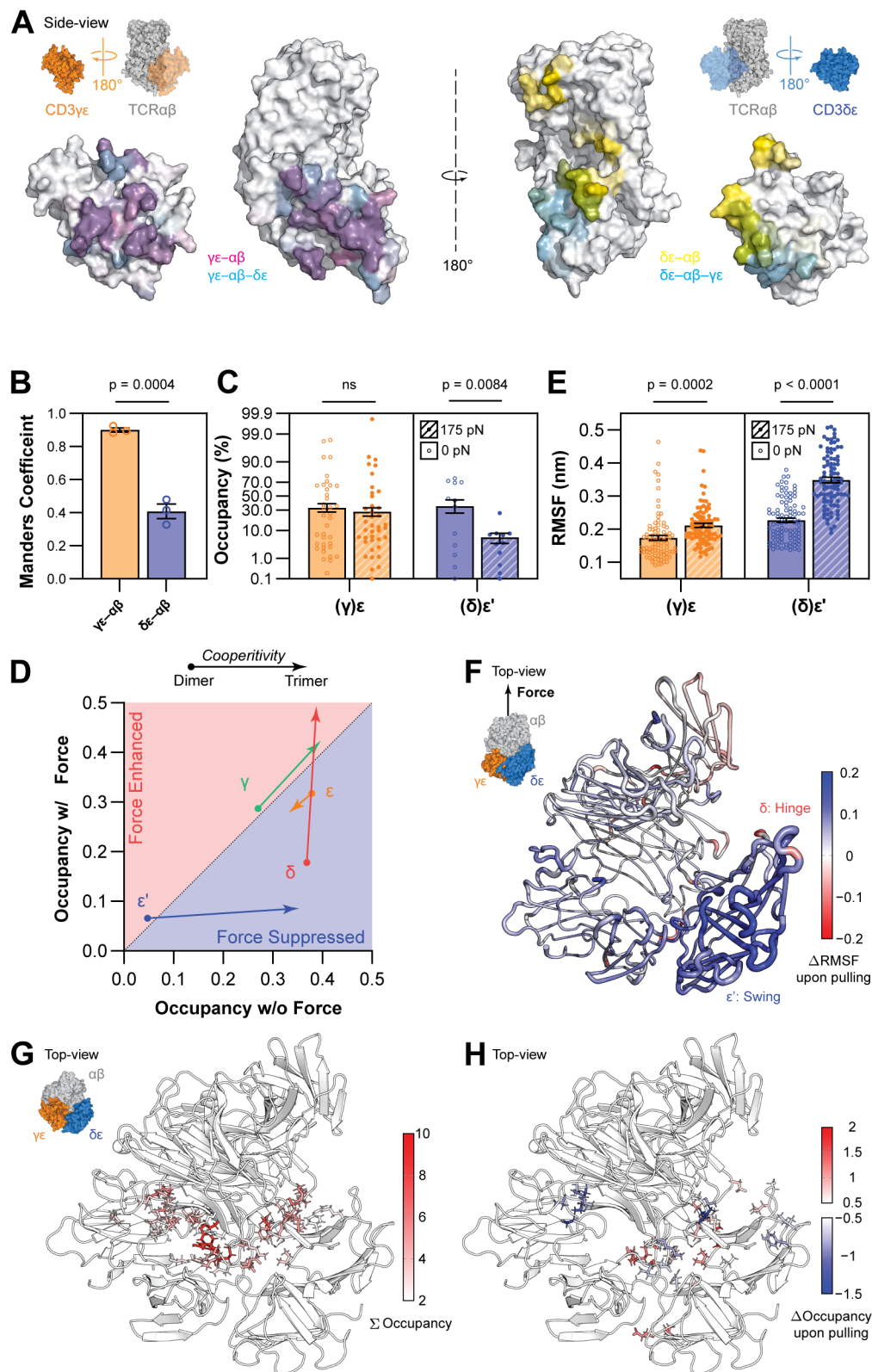


**Figure 3. Computational demonstration of cooperativity in *cis*-interaction of CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , and TCR $\alpha\beta$  ECDs.**

(A) Initial structures for MD simulations. The ECD of CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  trimolecular complex (*left*) was modeled based on the published cryo-EM structure (28), 6JXR. The two TCR $\alpha\beta$ –CD3 $\delta\epsilon$  (*middle*) and TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  (*right*) bimolecular structures were obtained by removing CD3 $\gamma\epsilon$  and CD3 $\delta\epsilon$  from the trimer, respectively. (B, C) Contact areas and interaction energies for the dimers and trimer from CMD simulations. Mean  $\pm$  SD of contact areas (B), defined by solvent accessible surface areas (101), and interaction energies (C), quantified using empirical free energy scores (102), were calculated from the TCR $\alpha\beta$ –CD3 $\delta\epsilon$  (blue), TCR $\alpha\beta$ –CD3 $\gamma\epsilon$  (orange), and CD3 $\gamma\epsilon$ –TCR $\alpha\beta$ –CD3 $\delta\epsilon$  (red) structures (Supplementary Fig. 3B, C). Statistics were obtained by comparing any two groups using unpaired t-tests. (D) Cooperative metrics of the  $\delta\epsilon$ – $\alpha\beta$ – $\gamma\epsilon$  trimeric complex in terms of contact areas (*left*) and free energy scores (*right*). The cooperative analyses were conducted similarly to that in Fig. 2C, but were based on contact areas and interaction energies in (B) and (C) rather than on bond numbers. (E) The minimum distances between TCR $\alpha\beta$  and corresponding CD3 $\delta\epsilon$  (blue), CD3 $\gamma\epsilon$  (orange), or both (red) vs. simulation time, calculated from representative trajectories of SMD-simulated TCR–CD3 ECD dissociation.

Initial molecular constructs of  $\alpha\beta$ - $\delta\epsilon$  and  $\alpha\beta$ - $\gamma\epsilon$  dimeric assemblies and of  $\delta\epsilon$ - $\alpha\beta$ - $\gamma\epsilon$  trimeric complex are indicated, where TCR $\alpha\beta$  N-termini were pulled away from corresponding C-terminal anchored CD3s during a 175-pN force-clamping SMD simulations (*insets*). The sudden rise of the trajectory from the baseline signifies the time point of dissociation (*arrows*). **(F)** *In silico* times required for the complex to dissociate,  $t(f)$ , under constant forces of 100-200 pN from SMD simulations. The predicted time-to-dissociation of the  $\gamma\epsilon$ - $\alpha\beta$ - $\delta\epsilon$  trimer (*dotted line*),  $\hat{t}_{\delta\gamma}$ , is the TCR dissociation time from both  $\delta\epsilon$  and  $\gamma\epsilon$ , under the assumption that the two bimolecular bonds are in parallel, and their dissociations are independent and concurrent (see Methods). **(G)** Cooperative metric  $\Delta t/\hat{t}_{\delta\gamma}$  vs. force of the  $\delta\epsilon$ - $\alpha\beta$ - $\gamma\epsilon$  trimeric complex. The cooperative analyses were conducted similarly to that in Fig. 2F but were based on the SMD simulated time-to-dissociation in (F) rather than on experimentally measured bond lifetimes. Significance was assessed using one-sample t-tests against zero in (D) and (G).







#### Figure 4. Structural basis of force-dependent cooperative TCR–CD3 ECD *cis*-interactions.

**(A)** Dynamic “footprints” of  $\alpha\beta$ – $\gamma\epsilon$  (*left*) and  $\alpha\beta$ – $\delta\epsilon$  (*right*) interfaces are defined by the CMD-derived occupancies, which were projected onto the light gray space-filling representations of TCR–CD3 ECDs. The *insets* depict the placements and orientations of  $\gamma\epsilon$  (*orange*) and  $\alpha\beta$ – $\delta\epsilon$  (*gray*),  $\alpha\beta$ – $\gamma\epsilon$  (*gray*) and  $\delta\epsilon$  (*blue*) from the far left to the far right: two sets of side-view images mirroring each other to allow CD3s to face outward. The respective  $\gamma\epsilon$  (*left*) and  $\delta\epsilon$  (*right*) binding interfaces with  $\alpha\beta$  are exposed by flipping the CD3s 180° while keeping the rest fixed (before *transparent*; after *opaque*). The pseudo-color maps are coded for interface footprints in the trimer (*cyan*; only the unobscured areas are visible) as well as in dimers with  $\gamma\epsilon$  (*magenta*) and  $\delta\epsilon$  (*yellow*), with intensity levels matching the occupancy values, ranging from 0% (white) to 100% (fully saturated). When comparing trimer *vs.* dimer, the unobscured *cyan* areas relative to the *magenta* and *yellow* areas represent the increased footprints of  $\alpha\beta$  with  $\gamma\epsilon$  (*left two panels*) or  $\delta\epsilon$  (*right two panels*) from dimer structures upon assembly of the trimer structure by incorporating the missing CD3. When comparing  $\gamma\epsilon$  *vs.*  $\delta\epsilon$ , the magenta area is larger than the yellow area, indicating a more stable  $\alpha\beta$ – $\gamma\epsilon$  than  $\alpha\beta$ – $\delta\epsilon$  dimer. Moreover, the overlapping areas are smaller on the right (*cyan + magenta*) than on the left (*cyan + yellow*), both in absolute values and percentages, indicating smaller cooperative effects due to adding  $\delta\epsilon$  to  $\alpha\beta$ – $\gamma\epsilon$  than adding  $\gamma\epsilon$  to  $\alpha\beta$ – $\delta\epsilon$  in the trimer and demonstrating asymmetry with less contact adjustment of  $\gamma\epsilon$  than  $\delta\epsilon$  after trimer assembly.

**(B)** Quantification of colocalization of occupancies between trimer and dimers by Manders’ overlap coefficient, defined by  $\sum D_i T_i / (\sum D_i^2 \sum T_i^2)^{1/2}$  where  $i$  denotes the residue index of  $\alpha\beta$ – $\gamma\epsilon$  (*orange*) and  $\alpha\beta$ – $\delta\epsilon$  (*blue*);  $D_i$  and  $T_i$  denote the  $i^{\text{th}}$  occupancy values of dimer and trimer, respectively, before and after *cis*-cooperative trimer assembly with the missing CD3. A Student t-test was used to assess significance based on three independent simulation repeats.

**(C)** Interfacial stabilities of two  $\epsilon$ -chains under 0 and 175 pN force, quantified by mean  $\pm$  SEM of  $\epsilon$  (*left*) or  $\epsilon'$  (*right*) chains residues with non-zero occupancies (*points*) interacting with  $\alpha\beta$  calculated from CMD (0 pN, *open bars*) or SMD (175 pN, *hatched bars*) simulated  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  trimeric structure. Here,  $\gamma$ -associated  $\epsilon$ -chain ( $\epsilon$ ) and  $\delta$ -associated  $\epsilon$ -chain ( $\epsilon'$ ) are distinguished using the prime superscript.

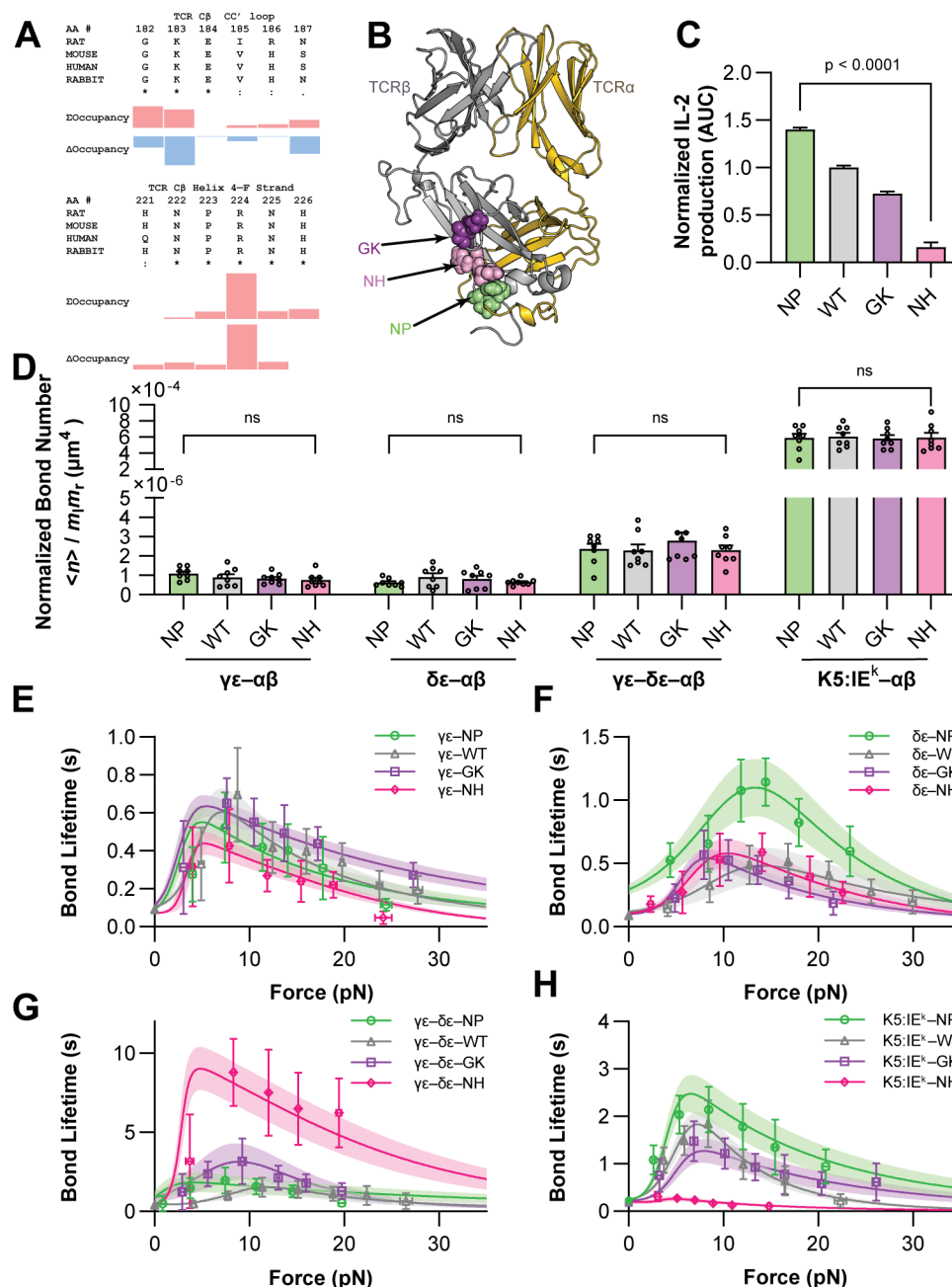
**(D)** Mean occupancies of  $\gamma$  (*green*),  $\epsilon$  (*orange*),  $\delta$  (*red*), or  $\epsilon'$  (*blue*) chains interacting with  $\alpha\beta$  quantified by averaging non-zero occupancies calculated from CMD (without force, *x*-axis) or SMD (with force, *y*-axis) simulated  $\alpha\beta$ – $\gamma\epsilon$  and  $\alpha\beta$ – $\delta\epsilon$  dimer structures (*arrow starting points*) or  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  trimer structure (*arrow ending points*).

**(E)** Fluctuations of two  $\epsilon$ -chains under 0 and 175 pN force, quantified by mean  $\pm$  SEM of residue RMSFs of  $\epsilon$  (*left*) or  $\epsilon'$  (*right*) chains calculated from CMD (0 pN, *open bars*) or SMD (175 pN, *hatched bars*) simulated  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  trimeric structure.

**(F)** Change of flexibilities in the TCR–CD3 complex upon pulling. The *inset* shows the top view of the  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  ECD structure under a 175 pN force. Differential RMSF profiles between SMD and CMD (*blue* for enhanced and *red* for suppressed fluctuations) are mapped onto the ribbon view of trimeric ECD. The residues’ absolute  $\Delta$ RMSF values are represented by the thickness of the protein backbone. Statistical significance levels were assessed by Welch’s t-test assuming non-equivalent SD.

**(G, H)** Critical interacting residues mapped onto the  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  interfaces showing the strong-interacting (*G*) and the force-sensitive (*H*) contacts.

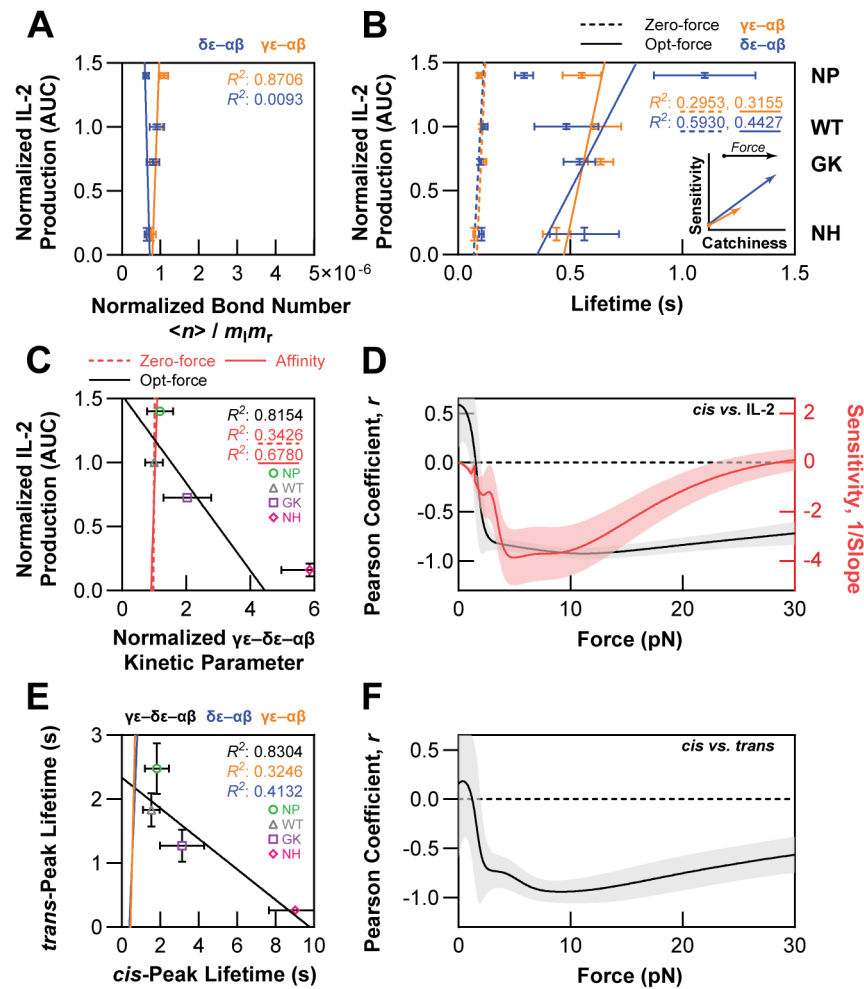
The *inset* in (*G*) is the top-view of the  $\gamma\epsilon$ – $\alpha\beta$ – $\delta\epsilon$  ECD structure. The same top-views of the full ECD assembly are shown in ribbon representation where tightly interacting residues are highlighted by sticks and colors. Only strong-interacting contact residues are shown in (*G*) using sidechains colored from *white* to *red*, based on their  $\Sigma$ Occupancy level. The force-sensitive residues with significant occupancy differences upon applying a 175 pN clamping force are shown in (*H*), with sidechains colored from *white* to *red* for increases and from *white* to *blue* for decreases in their  $\Delta$ Occupancy level (see Methods).



**Figure 5. Effects of mutating C $\beta$  contacting residues on *cis*-interaction affinity and bond lifetime.**

(A) TCR $\beta$  local segments with distinct force-responses. Residues in the CC' loop (*upper table*) and Helix 4 – F strand (*lower table*) of the C $\beta$  domain both contact CD3 (indicated by  $\Sigma$ Occupancy) but respond differently to 175 pN clamping force (indicated by  $\Delta$ Occupancy). (B) TCR $\alpha\beta$  structure with double-mutants listed in (A) highlighted on the C $\beta$  CC' loop and Helix 4-F strand, which contribute to the force-dependent cooperative TCR–CD3 *cis*-interaction according to (A). (C) Differential IL-2 cytokine productions of cells containing C $\beta$  mutations. The hybridoma

expressing 2B4 TCR WT and MTs were stimulated by K5:IE<sup>k</sup> displayed on CHO cells. The area under the dose-response curve (AUC), normalized by that of WT, quantifies the relative IL-2 secretion. This data has previously been reported (26) and is reformulated here to facilitate experimental design and correlative analysis. **(D)** Normalized average number of bonds of *cis*-interactions between CD3δ $\epsilon$  (*first group*), CD3γ $\epsilon$  (*second group*), or CD3δ $\epsilon$ –CD3γ $\epsilon$  (*third group*) and TCRαβ WT (*gray*) or β-chain double-mutants NP (*green*), GK (*purple*), or NH (*magenta*) MTs. Corresponding  $\langle n \rangle / m_l m_r$  of WT and indicated mutant 2B4 TCRs on hybridomas *trans*-interacting with K5:I-E<sup>k</sup> are plotted for comparison (*fourth group*). **(E-G)** Force-dependent bond lifetimes (*points*, mean  $\pm$  SEM of  $> 30$  lifetime events per force bin; *curves with shades*, mean  $\pm$  SD of globally fitted bond profiles) of *cis*-interactions of CD3γ $\epsilon$  (*E*), CD3δ $\epsilon$  (*F*), or both (*G*) with TCRαβ WT (*gray*), NP (*green*), GK (*purple*), or NH (*magenta*) MTs. **(H)** Corresponding  $\tau(f)$  of WT and indicated mutant 2B4 TCRs on hybridomas *trans*-interacting with K5:I-E<sup>k</sup> are shown for comparison. This data has previously been reported (42) and is replotted here to facilitate correlative analysis and mechanistic understanding.



**Figure 6. Correlating ECD *cis*-interaction parameters of TCR $\alpha\beta$  with CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$ , or both with T cell function and *trans*-interaction parameters between TCR and pMHC.**

(A) The correlations between the IL-2 secretion (in Fig. 5C) and effective 2D affinity for  $\alpha\beta$ - $\gamma\epsilon$  (orange) or  $\alpha\beta$ - $\delta\epsilon$  (blue) *cis*-interaction (in Fig. 4C, *first* and *second* group). (B) The correlations between IL-2 secretion and zero-force (dotted lines) vs. optimal-force (solid lines) bond lifetime for  $\alpha\beta$ - $\gamma\epsilon$  (orange) or  $\alpha\beta$ - $\delta\epsilon$  (blue) *cis*-interaction (in Fig. 5E, F). *Inset*: Different catchiness and sensitivity of CD3 $\gamma\epsilon$  (orange) vs. CD3 $\delta\epsilon$  (blue). The arrows display the effects of force. (C) Correlations between normalized  $\gamma\epsilon$ - $\delta\epsilon$ - $\alpha\beta$  *cis*-kinetics and T-cell signal. The mean  $\pm$  SEMs of relative IL-2 AUC (in Fig. 5C) are negatively correlated with the peak lifetimes of ECD *cis*-interactions of WT and MT TCR $\alpha\beta$ s (in Fig. 5G) when both CD3 $\gamma\epsilon$ , CD3 $\delta\epsilon$  co-presented (black). The poor correlations between IL-2 production and zero-force bond lifetime (red dashed line) or normalized number of bonds (red solid line) for  $\gamma\epsilon$ - $\delta\epsilon$ - $\alpha\beta$  *cis*-interactions are also plotted for comparison. (D) Goodness-of-fit and sensitivity of force-dependent bond lifetimes of  $\gamma\epsilon$ - $\delta\epsilon$  *cis*-interacting with WT and MT TCR $\alpha\beta$ s in predicting downstream IL-2 responses. The Pearson correlation coefficients (black) and inverse of the linear-regression slopes (red) between

normalized IL-2 AUC and  $\gamma\epsilon$ - $\delta\epsilon$ - $\alpha\beta$  *cis*-catch bonds are plotted for a range of forces (*curves with shades*, mean  $\pm$  SD). (E) Correlations between  $\gamma\epsilon$ - $\delta\epsilon$ - $\alpha\beta$  *cis*- and *trans*-bond lifetimes. The mean  $\pm$  SEMs of the peak lifetimes of trimolecular *cis*-interactions (in Fig. 5G) are negatively correlated with those of *trans*-interactions from WT and MT 2B4 TCRs expressed on hybridoma cells interacting with K5:IE<sup>k</sup> (in Fig. 5H). The poor correlations between the peak lifetimes of bimolecular *cis*-interactions (*orange*,  $\alpha\beta$ - $\gamma\epsilon$  and *blue*,  $\alpha\beta$ - $\delta\epsilon$ ) with the peak lifetimes of the WT and MT 2B4 TCRs *trans*-interacting with K5:IE<sup>k</sup> are plotted for comparison (in Fig. 5E, F). (F) Anti-correlation between the  $\gamma\epsilon$ - $\delta\epsilon$ - $\alpha\beta$  *cis*-interaction and the TCR-pMHC *trans*-interaction for WT and MT. The Pearson correlation coefficients of the *cis*- vs. *trans*-bond lifetime are shown for every single magnitude of force (*curves with shades*, mean  $\pm$  SD).