

1      **Modulating dream experience: Noninvasive brain stimulation over the**  
2      **sensorimotor cortex reduces dream movement**

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25

26 **Abstract**

27

28 Recently, cortical correlates of specific dream contents have been reported, such as the  
29 activation of the sensorimotor cortex during dreamed hand clenching. Yet, the causal  
30 mechanisms underlying specific dream content remain largely elusive. Here, we investigated  
31 how alterations in the excitability of sensorimotor areas through transcranial direct current  
32 stimulation (tDCS) might alter dream content. Following bihemispheric tDCS or sham  
33 stimulation, participants who were awakened from REM sleep filled out a questionnaire on  
34 bodily sensations in dreams. tDCS, compared to sham stimulation, significantly decreased  
35 reports of dream movement, especially repetitive actions. Contrary to this, other types of  
36 bodily experiences, such as tactile or vestibular sensations, were not affected by tDCS,  
37 confirming the specificity of stimulation effects. In addition, tDCS reduced interhemispheric  
38 coherence in parietal areas and altered the phasic electromyography correlation between the  
39 two arms. These findings reveal that a complex reorganization of the motor network co-  
40 occurred with the reduction of dream movement, confirming spatial specificity of the  
41 stimulation site. We conclude that tDCS over the sensorimotor cortex causally interferes with  
42 dream movement during REM sleep.

43

44 **Keywords**

45 Dreaming; motor processing; sensorimotor cortex; REM sleep; transcranial direct current  
46 stimulation.

47

## 48    **Introduction**

49    Dreams are vivid, often emotionally intense and narratively complex experiences occurring in  
50    sleep. In our dreams, we feel immersed in alternative worlds and have the experience of  
51    interacting with other persons and objects. Often this involves the subjective experience of  
52    moving through the dream world, and movement is among the most frequently reported  
53    dream experiences, second only to visual imagery. Yet these rich subjective experiences  
54    stand in stark contrast to the outward unresponsiveness and lack of observable behaviour  
55    during sleep. This study aimed to investigate the causal mechanisms underlying dream  
56    movement and bodily experience in dreams by using tDCS over sensorimotor areas. While  
57    most existing studies of the neural underpinnings of bodily experience in dreams and dream  
58    movement are correlational, our approach allowed us to manipulate dream content and draw  
59    conclusions about its underlying causes.

60    Specifically, our goal was to characterize the role of sensorimotor cortex in the generation of  
61    bodily sensations in dreams. We aimed to experimentally inhibit motor and other bodily  
62    experiences as an important aspect of self-simulation in dreams through bihemispheric  
63    transcranial direct current stimulation (tDCS) during REM sleep. After awakening from REM  
64    sleep, subjective dream experience was examined through the collection of dream reports and  
65    a questionnaire specifically designed to investigate bodily experiences in dreams; neural  
66    measures were obtained through electrophysiological sleep data.

67    This experimental protocol was guided by theoretical and empirical considerations. Our focus  
68    on bodily experience was motivated by the centrality of self-experience and subjective  
69    presence to dreaming (Strauch and Meier 1996; Occhionero et al. 2005; Speth et al. 2013).  
70    The immersive structure of dreaming is foregrounded in simulation theories (Revonsuo et al.  
71    2015), in which dreams are described as mental simulations characterized by the experience

72 of a virtual world. Typically, this virtual world is centered on a virtual self and experienced  
73 from an internal first-person perspective. The dream self is typically described as actively  
74 engaged in dream events, and movement is reported in 75% of dreams (Strauch and Meier  
75 1996; Cicogna and Bosinelli 2001). This immersive *here and now* quality is regarded as a  
76 defining characteristic of dreaming. It is also striking that with few exceptions, both the  
77 virtual world and the virtual self in dreams are experienced as real. Simulation views  
78 advocate the idea that “being-in-a-dream” feels the same as “being-in-the-world” during  
79 wakefulness. Moreover, bodily experience and movement sensations appear to be central to  
80 the feeling of subjective presence both during the waking and dream state, and sensorimotor  
81 interaction modulates subjective presence both in real and virtual environments (Sanchez-  
82 Vives and Slater 2005).

83 Our focus on bodily experience was further guided by findings suggesting high-level activity  
84 of the motor cortex during REM sleep (Hobson 1988; Maquet et al. 2000; Dang-Vu et al.  
85 2005). Generally, REM sleep dreaming has been associated with relative deactivation of  
86 executive networks and frontal areas, and with high levels of activity in sensory, motor, and  
87 emotional networks as compared to wakefulness (Schwartz and Maquet 2002; Nir and  
88 Tononi 2010; Cipolli et al. 2017). Studies focusing on the neural correlates of specific types  
89 of bodily dream experiences have shown the sensorimotor cortex to be activated during hand  
90 clenching in dreams (Dresler et al. 2011), and the right superior temporal sulcus, a region  
91 involved in the biological motion perception, to be activated in dreams with a sense of  
92 movement (Siclari et al. 2017). Furthermore, smooth pursuit eye movements during tracking  
93 of a visual target are highly similar during waking perception and lucid REM sleep dreaming  
94 (LaBerge et al. 2018). Taken together, these studies suggest a remarkable isomorphism of the  
95 neural mechanisms underlying motor control in wakefulness and dreaming. However, the

96 correlative nature of these studies limits their potential to uncover the causal contribution of  
97 specific brain regions to dream content.

98 Older studies attempted to experimentally induce different kinds of dream experience via  
99 peripheral and bodily stimulation during sleep. Causal manipulations that have been shown to  
100 have an effect on dream content include vestibular stimulation in rotating chairs (Hoff 1929;  
101 Hoff and Pötzl 1937) or hammocks (Leslie and Ogilvie 1996); light flashes or sprays of water  
102 applied to the skin (Dement and Wolpert 1958); thermal stimulation (Baldridge et al. 1965;  
103 Baldridge 1966); tactile stimulation via a blood pressure cuff inflated on the leg (Nielsen  
104 1993; Sauvageau et al. 1998); and olfactory stimulation (Schredl et al. 2009). The frequency  
105 of stimulus incorporation in dreams is variable and dependent both on the kind of stimulus  
106 and the sensory modality. Particularly high incorporation rates were achieved in studies using  
107 blood pressure cuff stimulation (40-80%) (Nielsen 1993; Sauvageau et al. 1998). This method  
108 of causally manipulating dream content is promising. However, because the processing of  
109 external and peripheral stimuli is attenuated in REM sleep, the precise effect of sensory  
110 stimulation on dream content is often nonspecific and unpredictable.

111 As a more direct method for manipulating dream content that avoids the possibly distorting  
112 effect of reduced sensory processing during REM sleep, we previously suggested using tDCS  
113 (Noreika et al. 2010). We argued that this method might complement previous attempts to  
114 manipulate dream content through sensory and bodily stimulation in sleep. Unihemispheric  
115 tDCS has been shown to facilitate motor imagery during REM sleep (Speth and Speth 2016)  
116 and to modulate visual imagery during Stage 2 NREM sleep (Jakobson, Fitzgerald, et al.  
117 2012a), but not during slow wave sleep (Jakobson, Fitzgerald, et al. 2012b) or REM sleep  
118 (Jakobson, Conduit, et al. 2012). Furthermore, frontal tDCS increases lucidity in experienced  
119 lucid dreamers (Stumbrys et al. 2013); and frontal transcranial alternating current stimulation  
120 (tACS) increases dissociation, insight and control in novice lucid dreamers (Voss et al. 2014).

121 tDCS has also been reported to modulate mind wandering in wakefulness (Axelrod et al.  
122 2015). This is promising, as dreaming has been proposed to be an intensified form of mind  
123 wandering, based on phenomenological and neurophysiological similarities (Fox et al. 2013).

124 Here, we applied tDCS over the sensorimotor cortex, aiming to understand its causal role in  
125 dream content generation. Since tDCS modulates neural processes associated with motor  
126 imagery during wakefulness (Quartarone et al. 2004; Matsumoto et al. 2010; Feurra, M. et al.  
127 2011), we expected a similar effect during REM sleep. However, instead of planned  
128 facilitation of movement sensations in dreams with unilateral anodal tDCS (Speth and Speth  
129 2016), our stimulation protocol was designed to interfere with motor processing during sleep,  
130 enabling a more focused analysis of the electrophysiological mechanisms underlying dream  
131 movement. Given that unilateral cathodal tDCS does not disrupt motor imagery during REM  
132 sleep (Speth and Speth 2016), we adopted a bihemispheric tDCS protocol, which is known to  
133 interfere with cortical and cerebellar motor networks more effectively than unilateral tDCS,  
134 particularly when applied during the resting state (Lindenberg et al. 2013, 2016).

135 To investigate possible effects of bihemispheric tDCS on outward muscular activity, we  
136 obtained electromyographic (EMG) measures from the arms. REM sleep is typically  
137 characterized by near-complete muscle atonia (Pompeiano 1967) and a partial blockade of  
138 sensory input (Hobson 1988; Wu 1993). At the same time, subtle muscular activity in the  
139 form of twitching is frequent in REM sleep and may play a role in the development and  
140 maintenance of motor behaviour (Blumberg 2015). A relation to dreaming seems plausible,  
141 but remains incompletely understood (Windt 2018).

142 We hypothesized that if the sensorimotor cortex has a causal role in generating sensorimotor  
143 dream content, bihemispheric tDCS over the sensorimotor cortex during REM sleep should  
144 attenuate movement and other bodily experiences in dreams reported immediately after timed

145 awakenings in the laboratory. To test this hypothesis, we developed an empirically informed  
146 questionnaire focused specifically on bodily sensations in dreams. This allowed us to probe  
147 bodily experiences more systematically than the more common methods of content analysis  
148 or quantitative linguistic analysis of dream reports (Speth and Speth 2016). Furthermore, we  
149 hypothesized that bihemispheric tDCS during REM sleep would interfere with  
150 interhemispheric motor networks as well as with spontaneous peripheral muscle activity,  
151 which are possible neural pathways to the reduction of dream movement.

152

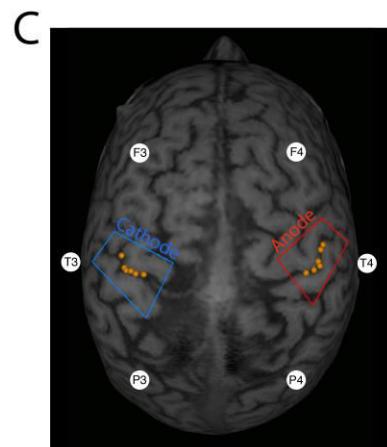
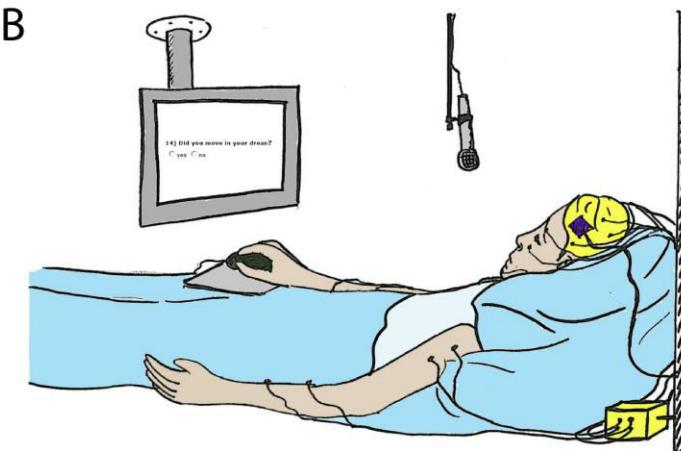
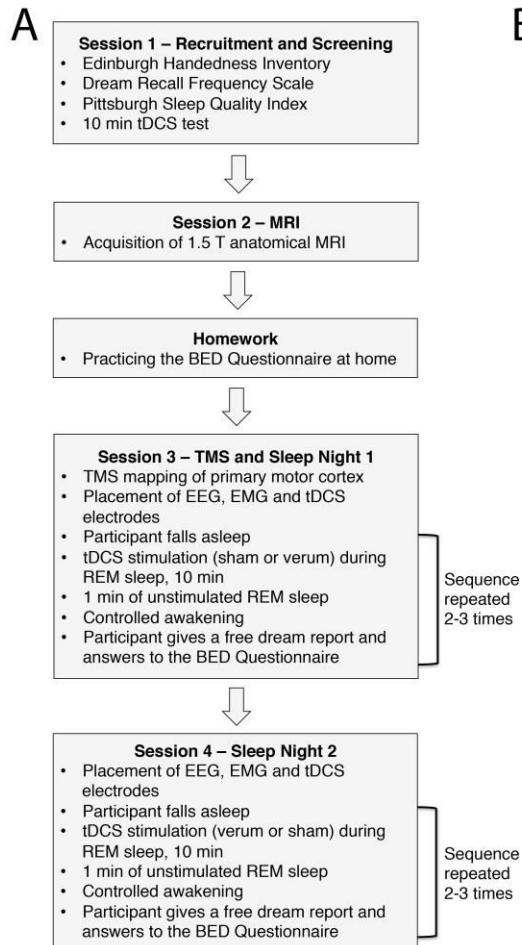
## 153 **Methods and Materials**

154

### 155 **Methods outline.**

156 The study protocol consisted of a recruitment and screening session, an MRI session, and two  
157 sleep sessions on non-consecutive nights (see Figure 1A). In addition, a TMS assessment of  
158 motor cortical excitability took place on the evening of the first sleep session. Ten  
159 participants were awakened from REM sleep two or three times per night and asked to give  
160 free dream reports and to answer to the Bodily Experiences in Dreams (BED) Questionnaire,  
161 which targeted the dream immediately preceding awakening (see Figure 1B). Participants  
162 received sham-stimulation during REM sleep on one night and bihemispheric tDCS on the  
163 other night. Bihemispheric tDCS montage included a cathode placed over the left  
164 sensorimotor cortex and an anode placed over the right sensorimotor cortex (see Figure 1C).  
165 In addition to standard polysomnography, central and peripheral electrophysiological data  
166 were recorded using 16 EEG channels and 4 EMG channels measuring flexor and deltoid  
167 muscles in both arms.

168



169

170 **Figure 1 | Experimental design.** (A) Time course of the study. (B) Experimental setup  
171 during sleep sessions. (C) Primary sensorimotor hand areas of a representative participant.  
172 Orange dots indicate stimulation sites where TMS pulses induced a subjectively experienced  
173 hand movement and/or muscle twitch (located approximately at the central sulcus between  
174 the somatosensory and somatomotor cortices). The blue box drawing over the left hemisphere  
175 represents the cathode tDCS electrode placement site, and the red box drawing over the right  
176 hemisphere represents the anode electrode placement site. White circles depict the  
177 approximate location of 6 electrodes used for the EEG inter-hemispheric coherence analysis.

178

## 179 **Participants.**

180 Aiming to recruit 10 right-handed individuals with high dream recall frequency and good  
181 sleep quality, potential participants were screened with the Edinburgh Handedness Inventory

182 (Oldfield 1971) and the Dream Recall Frequency (DRF) scale (Schredl 2002), which assesses  
183 the frequency with which people are able to remember dreams at home. The DRF scale  
184 consists of a single question “How often do you remember your dreams?” and 7 possible  
185 answers: 0=never, 1=less than once a month, 2=about once a month, 3=twice or three times a  
186 month, 4=about once a week, 5=several times a week, and 6=almost every morning.  
187 Furthermore, potential participants filled in the Pittsburgh Sleep Quality Index (PSQI)  
188 (Buysse et al. 1989). We aimed to recruit individuals whose global PSQI score did not exceed  
189 4 (with 0 indicating no sleep difficulty and 21 indicating severe difficulties in sleep) and  
190 whose sleep latency score indicated they typically needed less than 30 minutes to fall asleep.  
191 Given that the application of tDCS may occasionally induce itching, tickling, heat sensations  
192 under the electrodes, or even a temporary headache (Priori 2003), we introduced potential  
193 participants to the tDCS technique before they made their final commitment to take part in  
194 the study. After screening for MRI and tDCS contraindications, they were given the  
195 opportunity to familiarize themselves with the tDCS procedure before spending their first  
196 night in the laboratory. Participants were stimulated for 10 min with tDCS of 1 mA current  
197 over the C3 and C4 electrode sites according to the 10-20 EEG system (approximately over  
198 the sensorimotor cortex), which helped them decide whether they wanted to participate in the  
199 actual experiment. This also helped minimize the risk that tDCS during REM sleep would  
200 lead to awakening.

201 After screening 16 potential participants, we were able to recruit 10 healthy right-handed  
202 university students (4 men and 6 women, mean age 26.8, range 4.4 years). The mean  
203 handedness index was 0.9 (SD=0.11; range 0.73 to 1). The mean DRF score was 5.4  
204 (SD=0.79, Min=4, Max=6), indicating high spontaneous dream recall. While this might  
205 introduce bias towards high recallers’ dreams, it is arguably the most feasible recruitment  
206 strategy for a costly and time-consuming sleep laboratory study. All participants gave their

207 written informed consent according to the Declaration of Helsinki, and the protocol of the  
208 study was approved by the Ethics Committee of the Hospital District of Southwest Finland.  
209 Participants were financially compensated with 40 euros per night and 10 euros per hour for  
210 daytime testing.

211

212 **MRI-TMS mapping of the primary sensorimotor hand area.**

213 ECoG measurement of the electric field induced by tDCS in a human patient as well as  
214 computational modelling of tDCS effects in healthy participants suggest that the spatial  
215 focality of tDCS decreases if stimulation electrodes are misplaced by >1cm (Opitz et al.  
216 2018). Thus, aiming to constrain between-participant variance of the stimulation focus below  
217 1cm, the location of the hand area in the primary sensorimotor cortex in both hemispheres  
218 was determined individually for each participant with the help of magnetic resonance  
219 imaging (MRI) and transcranial magnetic stimulation (TMS). Anatomical brain images were  
220 acquired with a 1.5 T MRI scanner Philips Intera at the Turku PET Centre. 3D models of the  
221 brain were created using 3D T1-weighted MR sequence. A hospital radiologist confirmed  
222 that the brain MRI was normal in all cases. Afterwards, the approximate location of primary  
223 sensorimotor hand representations was visually determined from anatomical brain images  
224 based on macro-anatomical landmarks (Yousry et al. 1997).

225 Based on this analysis, the location of the primary sensorimotor hand area was determined for  
226 each participant in a separate TMS session, which was carried out on the evening of the first  
227 experimental night at the Department of Psychology at the University of Turku. TMS pulses  
228 were delivered using eXimia™ TMS stimulator with NBS navigation system (Nexstim Ltd.,  
229 Helsinki, Finland), which allowed us to navigate within individual anatomical MRI with an  
230 approximately 6-mm spatial resolution containing all sources of errors (Ruohonen and Karhu

231 2010). Participants sat on a reclining chair with their eyes closed and both arms supported by  
232 a pillow to ensure that their arm muscles were relaxed. TMS was carried out in a single pulse  
233 mode using a figure-of-eight-shaped coil that was held tangentially against the participant's  
234 head. The current direction of the second phase of the biphasic pulse was oriented  
235 perpendicularly to the post-central gyrus in the posterior to the anterior direction at the bank  
236 between pre-central and post-central sulci (Richter et al. 2013) (see Figure 1B).

237 First, a rough location of the hand area was estimated by asking participants to report whether  
238 they experienced any hand movement following a TMS pulse over the motor cortex in the  
239 contralateral hemisphere. Once a reliable hotspot was found, an individual motor threshold,  
240 i.e. the minimum TMS intensity required to induce the subjective experience of a hand  
241 movement, was determined with the maximum likelihood threshold hunting (MLTH)  
242 procedure (Awiszus, 2003). In this process, 20 pulses were delivered to the hand area with  
243 different stimulus intensities, starting at 60% of maximal TMS intensity. The mean motor  
244 threshold was 56.1% (SD=12.4, Min=28, Max=76.7) of maximal TMS intensity for the left  
245 hemisphere, and 59.2% (SD=16.5, Min=24.8, Max=77.12) for the right hemisphere. While  
246 motor thresholds did not differ systematically between the hemispheres (paired samples t test:  
247  $t(9)=1.02$ ,  $p=0.34$ ,  $Bf$  in favor of the null=2.2), there was a strong inter-hemispheric  
248 correlation of motor thresholds (Pearson correlation:  $r=0.82$ ,  $p=0.004$ ).

249 Following estimation of individual motor thresholds, the most ventral and caudal points of  
250 the hand representation in the primary motor cortex were estimated by delivering TMS pulses  
251 with the intensity of 10% above the level of the individual motor threshold. This procedure  
252 was consecutively performed for both hemispheres, yielding bilateral hand representation  
253 maps that were later used to place tDCS electrodes (see Figure 2B).

254

255 **tDCS over the primary sensorimotor cortex during REM sleep.**

256 tDCS and sham-stimulation sessions were conducted in the Sleep Laboratory of the Centre  
257 for Cognitive Neuroscience at the University of Turku over two non-consecutive nights with  
258 each participant. Microprocessor-controlled programmable 1-channel Eldith DC-Stimulator  
259 PLUS (Electro-Diagnostic & Therapeutic Systems GmbH, Ilmenau, Germany) was used as a  
260 stimulation device.

261 tDCS was applied bilaterally to the hand area in order to modulate the excitability level of the  
262 primary sensorimotor cortex during REM sleep. Participants were asked to avoid caffeine for  
263 6 hours and alcohol and other CNS-affecting drugs for 24 hours prior to the experiment. To  
264 ensure these requirements were met, participants filled out the custom-made Pre-Sleep  
265 Questionnaire before each session. For each participant, the two stimulation sessions were  
266 separated by at least one week in order to avoid interference effects.

267 Two 35 cm<sup>2</sup> sized sponge-covered rubber electrodes were soaked with water, and Ten20  
268 electrode paste (Weaver and Company) was applied on both sides of the sponge. The  
269 electrodes were placed bilaterally along the central sulcus posterior to the primary motor  
270 hand areas, which was determined with the help of MRI-guided TMS (see Figure 1B). They  
271 were supported with a comfortable bandage throughout the night. tDCS was carried out on  
272 one experimental night and sham-stimulation took place on another night. Participants were  
273 blind to the experimental conditions, i.e. whether the tDCS session was followed by the sham  
274 session (N=5) or vice versa. An equal number of participants was assigned randomly to each  
275 condition.

276

277 During the tDCS night, 1mA electric current was delivered to participants' scalp two or three  
278 times per night for 10 min during REM sleep, starting with the second sleep cycle. It has been

279 reported that changes in current direction may result in qualitatively different motor effects,  
280 with cathodal stimulation being more effective and largely inhibitory and anodal stimulation  
281 being less effective and largely facilitatory (Nitsche et al. 2008). Furthermore, tDCS induced  
282 neuroplasticity may accumulate over time (Nitsche and Paulus 2000). In order to keep the  
283 stimulation effects consistent throughout the night, the electrode over the right sensorimotor  
284 area was always the anode, and the electrode over the left sensorimotor area was always the  
285 cathode. This procedure ensured that the asymmetric stimulation during one sleep cycle  
286 would not interfere with or cancel stimulation effects during another cycle. We chose to place  
287 the cathode over the dominant left hemisphere with the aim to disrupt dream movements.

288

289 During the sham-stimulation night, stimulation was conducted by switching on the DC device  
290 and stimulating only for 10 sec each at the beginning and end of a 10 min period during REM  
291 sleep. Stimulation that lasts only a few seconds has been shown to produce a minimal effect  
292 on the brain, if any (Hummel et al. 2005). The aim of sham stimulation was to mimic the skin  
293 sensation that is occasionally experienced during the onset and offset of tDCS. This  
294 procedure is thought to make the two conditions subjectively indistinguishable (Gandiga et  
295 al. 2006). The same procedure was repeated two or three times starting with the second sleep  
296 cycle.

297

298

299 **Electrophysiological recordings.**

300 To record EEG activity, 16 electrodes (Fp1, Fp2, F7, F3, Fz, F4, F8, T3, T4, T5, P3, Pz, P4,  
301 T6, O1, O2) were placed on the scalp following the standard 10-20 system (Jasper 1958). C3,  
302 Cz and C4 electrode locations were left empty for the placement of tDCS electrodes. To  
303 record eye blinks and vertical saccades, two electrooculography (EOG) electrodes were

304 placed below and above the left eye, while two other electrodes placed adjacent to the lateral  
305 canthi of each eye were used to measure horizontal saccades. An electromyography (EMG)  
306 electrode placed on the chin was used to record muscle tone, which was used for the scoring  
307 of sleep stages. The reference for all these electrodes was placed on the right ear mastoid and  
308 the ground electrode was placed on the temple. In addition, two bipolar EMG channels were  
309 used to record muscle activity in the right and the left arm flexor digitorum profundus, which  
310 were later used to analyze peripheral motor activity. Another two EMG channels recorded  
311 activity of the deltoid muscles in both arms. Electrophysiological recordings were  
312 continuously monitored on a computer screen and all electrodes were regularly checked  
313 throughout the night to ensure that the impedance remained under 5 k $\Omega$ . All data were  
314 recorded at 500 Hz sampling rate with Ag/AgCl electrodes using NeuroScan amplifier  
315 SynAmps Model 5083. Given that tDCS onset induces a slow frequency artifact in the EEG  
316 that may preclude online polysomnographic scoring, a 1-Hz high-pass filter was applied  
317 during recording for online monitoring of sleep stages (Marshall 2004). As expected, tDCS  
318 onset- and offset-induced artifacts always faded away after 5-10 sec.

319

320 **Collection of dream reports.**

321 One minute after the termination of tDCS or sham-stimulation, participants were awakened  
322 from REM sleep with a standard awakening tone. They were then asked to give a verbal  
323 dream report of “everything that was going through their minds before awakening”, aiming to  
324 facilitate dream recall. Afterwards, participants were asked if they remembered anything else  
325 about their dream. To avoid a possible bias between stimulation conditions, these questions  
326 were played from a pre-recorded computer audio file. Following the free dream report,  
327 participants were asked to fill in the Bodily Experiences in Dreams (BED) Questionnaire.

328 The questionnaire was designed as an internet survey programmed on [www.webropol.com](http://www.webropol.com)  
329 and was projected on a screen above the bed in the sleep laboratory. Participants navigated  
330 and responded to the BED Questionnaire by controlling a mouse while lying in bed.

331 Participants were stimulated and awakened two or three times per night, depending on how  
332 many REM sleep periods they had. The number of awakenings was balanced across the first  
333 and the second night and across the two stimulation conditions (see Table S3). White dream  
334 reports (i.e. cases when a person reports the occurrence of dream experiences but cannot  
335 recall any specific details) as well as sleep mentation reports (i.e. when a person reports non-  
336 perceptual subjective experiences, such as thinking) were excluded from the analysis. A total  
337 of 50 dreams reported during a total of 20 nights were available for analyses.

338

### 339 **Bodily Experiences in Dreams (BED) Questionnaire.**

340 The 41-item BED Questionnaire was designed to gather detailed information about  
341 kinaesthetic and other bodily experiences in dreams (see Appendix 1). The BED  
342 Questionnaire consists of 5 general questions with respective sub-scales (see Table 1). Each  
343 of the general questions targets a particular category of body-related experience: vestibular  
344 sensations, tactile and somatosensory experiences, movement, movement alterations, and  
345 body schema alterations. Each general question, if answered positively, is followed by sub-  
346 scales targeting more specific instances of this category of experience. For example, if a  
347 participant indicated that they had experienced movement sensations, they would then be  
348 asked about the occurrence of specific types of movement sensations, such as single,  
349 repetitive, and passive movements. In addition, participants were asked whether the reported  
350 sensation concerned the whole body, the right or left hand, the right or left side of the face, or  
351 another body part (see Appendix 1). If they answered negatively, they would skip to the next

352 general category. Depending on whether a sub-scale asked about the intensity or the duration  
353 of experience, 9 point Likert-scales for answering ranged either from “1=Low intensity” to  
354 “9=High intensity” or from “1=Never” to “9=Throughout”.

355

356

357 **Table 1.** The BED Questionnaire: General questions and exemplary sub-scales

---

*Five general questions (Yes/No)*

---

5. Did you experience any tactile or somatosensory sensations in your dream?

---

11. Did you experience any vestibular or balance sensations in your dream?

---

14. Did you move in your dream (including active as well as passive movements (for instance in a vehicle) of the whole body or body parts)?

---

18. Were your movements (either of the whole body or of certain body parts) altered or impaired compared to wakefulness?

---

26. Was your dream body or were certain body parts altered compared to wakefulness?

---

*Movement sub-scales (from 1=Never to 9=Throughout)*

---

15. How frequently did you move in your dream (including active as well as passive movements (for instance in a vehicle) of the whole body or body parts)?

---

16. How frequently did you perform the following types of movements in your dream?

---

16.1 – single actions (e.g. placing a book on the table)

---

16.2 – repetitive actions (e.g. running)

---

16.3 – passive movements (e.g. going by car)

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358

359

360

361 **Word count of verbal dream reports.**

362 The length of dream reports was assessed by two blind judges (authors JW and KV), who  
363 independently calculated the meaningful word count of each dream report. Murmurs,  
364 repetitions of words, and any secondary reflections or comments about the dream were not  
365 included in the word count. The judges initially agreed on the word count of 47 out of 50  
366 dream reports (94% agreement). The judges discussed the reasons for the mismatch in the  
367 remaining 3 cases and reached an agreement.

368

369 **Content analysis of movement sensations in verbal dream reports.**

370 Following the findings from the BED Questionnaire, we carried out content analysis of verbal  
371 dream reports, focusing on the specific types of movement (single actions, repetitive actions,  
372 passive movement) performed by the dream self. To compare the type and frequency of  
373 movements reported in the BED Questionnaire to those explicitly mentioned in dream  
374 reports, two blind judges (authors VN and BL) carried out a content analysis of verbal  
375 reports. First, the judges scored whether each dream report contained at least one movement  
376 produced by the dream self, excluding facial movements such as talking, drinking, and  
377 blinking, as we reasoned that individuals do not typically consider facial musculature when  
378 asked to report their movements. Movements attributed to the first-person plural "we" were  
379 treated as involving movements of the dream self. Second, the judges identified individual  
380 movements produced by the dream self in each dream that, in the first step, was judged to  
381 contain movement. Third, they scored the type of the identified movements (single action,  
382 repetitive action, passive movement). All three stages of the content analysis were first  
383 carried out individually and the obtained results were then compared between the judges. In  
384 the case of disagreement, the judges discussed it until an agreement was achieved.

385 Regarding the presence or absence of movement in a given report, the judges initially agreed  
386 on 45 out of 50 dream reports (90% agreement). After discussion, the judges agreed that the  
387 remaining 4 dreams contained references to movements produced by the dream self, while  
388 one report had no explicit references to such movement. Regarding individual movements,  
389 judges initially agreed on the identification of 33 movements, and disagreed on 19  
390 movements (63.5% agreement). The disagreement was caused by one judge either missing a  
391 movement or treating it as part of a longer sequence of movements, e.g. treating walking  
392 from A to B and from B to C as a single movement. After discussion, the judges agreed that  
393 the dream reports contained a total of 48 individual movements executed by the dream self.  
394 Regarding specific types of movements (single action, repetitive action, passive movement),  
395 the judges initially agreed on 44 out of 48 movements (91.7% agreement). After discussion,  
396 the judges agreed that the remaining 4 movements should be scored as follows: “diving” -  
397 single action, “riding a bike downhill” - passive movement, “writing something” - repetitive  
398 action, “made some coffee” - single action.

399

#### 400 **EEG analysis: coherence and spectral power.**

401 To assess the electrophysiological effects of tDCS on brain functioning, we analyzed the full  
402 period of 1 min of EEG signal recorded between the termination of tDCS or sham-stimulation  
403 and controlled awakening. tDCS artifacts did not contaminate this EEG interval whilst sleep  
404 scoring ensured that REM sleep continued up to the point of awakening. On one occasion, a  
405 spontaneous awakening took place before the planned controlled awakening, and only 7 sec  
406 of stimulation-free sleep EEG were available for analysis. On another occasion, a  
407 spontaneous awakening took place immediately after the termination of stimulation; this  
408 recording was excluded, leaving 49 EEG recordings available for analysis.

409 Continuous recordings were first high-pass (0.5 Hz) and then low-pass (45 Hz) filtered using  
410 a FIR filter as implemented in EEGLab toolbox (Delorme and Makeig 2004). The data were  
411 then common average referenced, and excessively noisy periods of recording were manually  
412 deleted (an average of 743 ms per single recording). Detached or excessively noisy channels  
413 were deselected (an average of 0.2 channels per dataset), and an independent component  
414 analysis (ICA) was carried out on the remaining channels, using EEGLab toolbox (Delorme  
415 and Makeig 2004). Independent components reflecting eye movements and other sources of  
416 noise were manually deleted (an average of 3.3 ICs per recording), following which dropped  
417 noisy EEG channels were interpolated using spherical spline interpolation. Continuous EEG  
418 recordings were epoched into 2-sec segments with a 50% overlap between adjacent segments.  
419 Several epochs that still contained visible artifacts were manually deleted (an average of 0.5  
420 epochs per recording). Individual epochs were demeaned across the whole 2 sec interval.

421 We analyzed EEG inter-hemispheric coherence in the beta oscillation range (15-30 Hz) at the  
422 electrodes adjacent to the stimulation site (F3, F4, T3, T4, P3, P4). Magnitude-squared  
423 coherence was computed in the range from 2 Hz to 44 Hz with a maximum frequency  
424 resolution of 2 Hz between pairs of EEG channels adjacent to the stimulation site from the  
425 frontal (F3-F4), temporal (T3-T4) and parietal (P3-P4) side, using Brainstorm toolbox (Tadel  
426 et al. 2011). Coherence values obtained at a single 2 sec segment level were averaged across  
427 beta frequency range (15.6-29.3 Hz). Next, coherence values were averaged across each 1-  
428 min pre-awakening recordings. Afterwards, individual means were averaged over several  
429 awakenings for each participant according to the experimental condition, yielding 10 tDCS  
430 and 10 sham-stimulation values for each electrode pair.

431 In the case of a significant difference between tDCS and sham-stimulation conditions across  
432 the 1-min pre-awakening periods, coherence was computed at four separate 15 sec sub-  
433 intervals preceding controlled awakening: -60 to -46 sec, -45 sec to -31 sec, -30 to -16 sec,

434 and -15 to -1 sec. A significant difference between tDCS and sham conditions observed  
435 immediately after the termination of stimulation (-60 to -46 sec) was expected to reflect a  
436 tDCS-driven modulation of EEG activity, as an effect size of neurophysiological changes  
437 following motor tDCS decreases with increasing time (Nitsche and Paulus 2000). Contrary to  
438 this, a significant difference between tDCS and sham-stimulation conditions at the interval  
439 preceding awakening (-15 to -1 sec) with no difference at the -60 to -46 sec interval was  
440 expected to reflect an unspecific modulation of EEG activity, e.g. micro-arousals caused by  
441 tingling sensations could eventually trigger body movements in bed.

442 To control for a possible confound of EEG spectral power on coherence computation  
443 (Bowyer, 2016), we carried out a control analysis of EEG beta power. Spectral power was  
444 computed across 2 sec epochs using Hilbert transform, set from 1 Hz to 44 Hz in steps of 1  
445 Hz, for the same set of 6 electrodes adjacent to the stimulation site. Power values obtained at  
446 a single 2 sec segment level were averaged across beta frequency range (15-30 Hz), with  
447 subsequent data averaging steps repeating coherence analysis.

448

449 **Phasic EMG analysis.**

450 We investigated the effects of tDCS on peripheral muscle tone by analyzing EMG activity  
451 from the left/right arm flexor and deltoideus muscles during the 1 min interval between the  
452 termination of tDCS or sham-stimulation and the controlled awakening of participants. We  
453 were specifically interested whether EMG traces following tDCS and sham-stimulation  
454 showed increased phasic muscle activity compared to the pre-stimulation baseline window,  
455 and whether bihemispheric tDCS modulated interaction between the left/right arm EMG.  
456 Since phasic EMG activity manifests during REM sleep as short-lasting muscle bursts  
457 recorded by surface electrodes (Fairley et al. 2012), we split the 1-min epochs into 60 non-

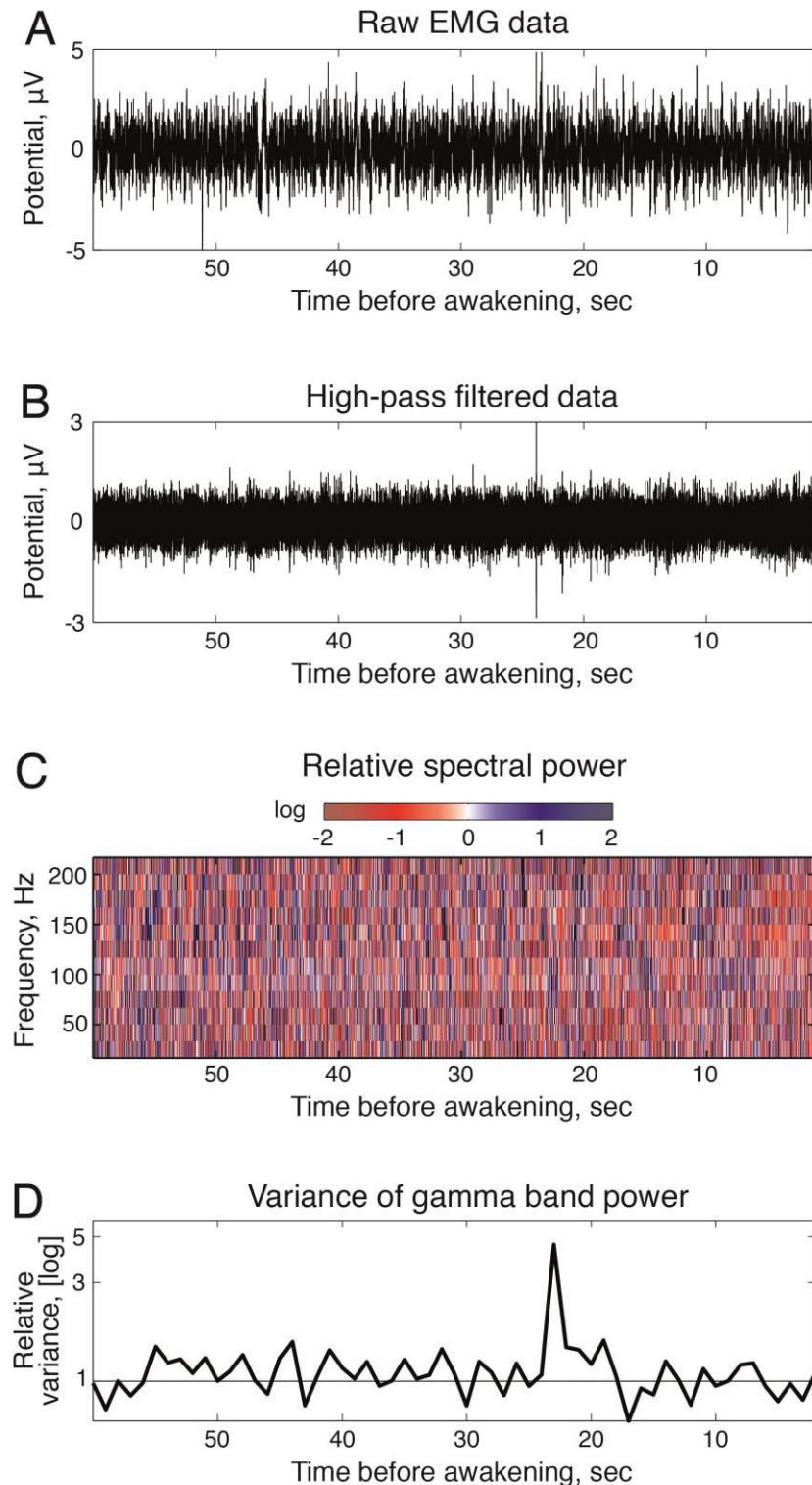
458 overlapping 1-sec segments and carried out a binary assessment whether each segment  
459 contained phasic EMG activity. Segments with phasic EMG activity were then assigned a  
460 value of one, segments without phasic EMG activity a value of zero. The mean overall 60  
461 binary values were then used to define the ratio of phasic EMG activity within the respective  
462 epoch.

463 More specifically, since phasic EMG activity is reflected in broadband spectral power  
464 changes, we used the variance of gamma band (50-250 Hz) power for the detection of short-  
465 lasting bursts of muscle activity. In a first step we high-pass filtered the raw data with a 3rd  
466 order butterworth filter with a cutoff-frequency at 50Hz (Suppl. Fig. 1 a-b). For the  
467 subsequent time-frequency analysis, we used a single-tapered spectral analysis method  
468 (Percival and Walden 2000) with a time window of 50 ms and 10-ms time steps. The relative  
469 power changes were then calculated by dividing the time-resolved amplitude for each  
470 frequency bin by the frequency-specific average of the whole 1 min epoch (Suppl. Fig. 1 c).  
471 After splitting the epochs in 1-s segments, the variance of relative power was calculated for  
472 each segment and every frequency. The variance of gamma band power was then defined as  
473 the mean over all frequencies between 50 Hz and 250 Hz.

474 To assess a relative shift towards more phasic/tonic activity in response to stimulation, the  
475 variance of gamma band power was calculated both for the 60 sec epochs after the  
476 termination of tDCS or sham-stimulation and for a 30 sec baseline time window before tDCS  
477 or sham-stimulation. The relative variance of gamma band power was then calculated by  
478 dividing the variance by the averaged variance in the baseline time window (Suppl. Fig. 1 d).  
479 This way, post-stimulation segments with the variance of gamma band power higher than the  
480 corresponding average (median) in the stimulation-free 30 sec baseline time window received  
481 a relative variance value greater than one and were defined as segments shifting towards  
482 phasic EMG, while segments with a relative variance between zero and one were defined as

483 segments shifting towards tonic EMG. Finally, a proportion of phasic segments was  
484 calculated across the whole 60 sec post-stimulation epoch, yielding values ranging from 0,  
485 indicating a complete shift towards tonic EMG, to 1, indicating a complete shift towards  
486 phasic EMG.

487



488

489 **Figure S1 | Analysis of peripheral EMG activity.** **a)** Exemplary 60 sec EMG recording of  
490 the right hand flexoris muscle between termination of tDCS and the awakening. **b)** The same  
491 EMG recording after a high-pass filter with a 50 Hz cutoff-frequency. **c)** Relative spectral  
492 power of the high-pass filtered EMG recording. **d)** Relative variance of gamma band power,  
493 i.e., divided by the average variance of gamma band power in the baseline time window.

494 Values greater than one (above the grey solid line) depict 1 sec segments with a shift towards  
495 phasic EMG, values equal or smaller than one depict segments with a shift towards tonic  
496 EMG.

497

498 **Statistical analysis.**

499 All dependent measures were averaged per individual participant separately for the sham-  
500 stimulation and tDCS conditions. A Shapiro-Wilk test was used to assess the distribution  
501 normality of dependent variables. Paired-samples t test and Pearson correlation were carried  
502 out when distribution of given variables (or their difference in a case of t test) was normal,  
503 and Wilcoxon signed-rank test (Z statistic) and Spearman rank order correlation were used in  
504 the cases of non-normal distribution of one or both variables. For the paired-samples t-test,  
505 Cohen's  $d$  was calculated as an effect size estimate using pooled variance. For the Wilcoxon  
506 signed-rank test,  $r=Z/\sqrt{N}$  was calculated as an effect size estimate. All statistical tests  
507 were two-tailed. To control for multiple comparisons, Bonferroni correction was applied by  
508 multiplying the obtained p value by the number of comparisons with a given set of tests.  
509 Bonferroni corrected p values are denoted as  $p_{B-N}$  where N indicates the number of multiple  
510 comparisons. For all control analyses, we report uncorrected p values. For the control t tests  
511 where we expected null findings, we additionally report Bayes factor in favor of the null.  
512 Statistical analyses were carried out with SPSS 22 and JASP 0.8.2.

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516 **Results**

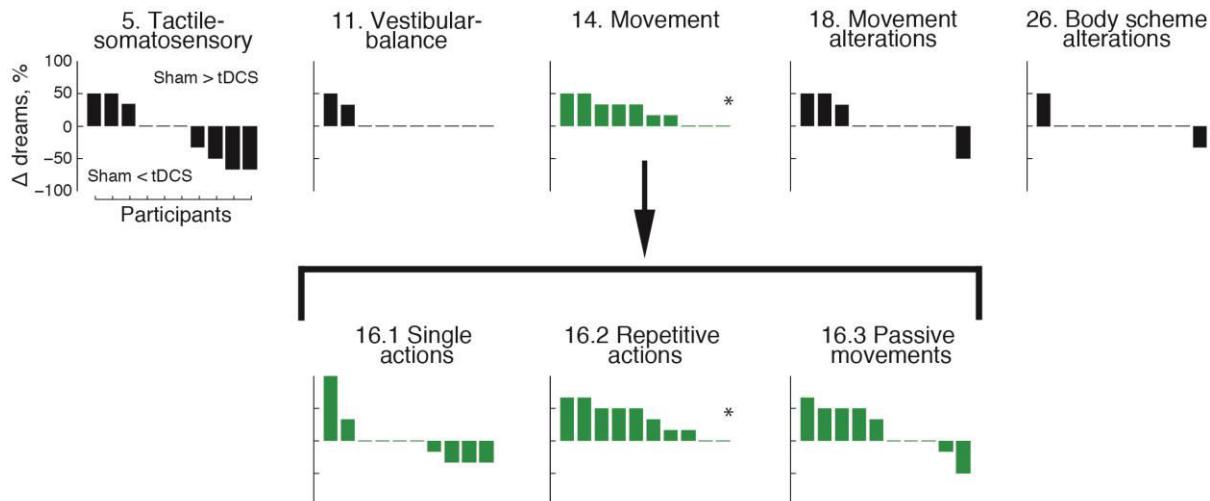
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518 **tDCS modulates dream movement.**

519 The first research question addressed whether the sensorimotor cortex is involved in the  
520 generation of bodily experiences in dreams. To answer this, we compared the percentage of  
521 dreams with different types of bodily experiences reported in the BED Questionnaire between  
522 the tDCS and sham stimulation. Among the general dimensions of bodily experience in  
523 dreams (tactile/somatosensory, vestibular/balance, movement, movement alterations, body  
524 scheme alterations), we found a significant difference only for movement (see Fig 2 and  
525 Table 2). Specifically, the proportion of dreams with movement was significantly lower in  
526 the tDCS ( $M=63.1\%$ ,  $SEM=10.2\%$ ) compared to the sham-stimulation ( $M=86.6\%$ ,  
527  $SEM=7\%$ ) condition (paired samples  $t$  test:  $t(9)=3.77$ ,  $p_{B,5}=0.022$ ,  $d=0.85$ ). That is,  
528 participants were less likely to answer YES to the question “Did you move in your dream?”  
529 when they were awakened 1 min after termination of bihemispheric tDCS. At the individual  
530 level, 7 out of 10 participants showed this effect, whereas the remaining 3 participants had  
531 equal proportions of dreams with movements between the two conditions (see Fig. 2).

532

533



535 **Figure 2 | tDCS effects on reported dream experiences.** Changes between sham-  
536 stimulation and tDCS conditions across the five general categories of dream content (A-E)  
537 and for particular kinds of movement (F-H) per participant. Positive and negative values  
538 indicate a higher proportion of dreams with a specific experience in the sham-stimulation and  
539 tDCS condition, respectively. Individual participants are sorted in descending order  
540 beginning with the participant with the highest proportion of dreams with a specific  
541 experience in the sham-stimulation condition, compared to the tDCS condition. Participants  
542 are sorted separately for each dimension of experience. \*  $p_B < 0.05$ .

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553 **Table 2.** The BED Questionnaire: Percentage of dream reports containing specific bodily  
554 experiences following sham-stimulation and tDCS during REM sleep

<i>Bodily experiences</i>	<i>Sham</i>	<i>tDCS</i>	<i>Statistical test</i>	
	<i>M (SEM)</i>	<i>M (SEM)</i>	<i>t/Z</i>	<i>p<sub>B</sub></i>
<i>Five general dimensions</i>				
5. Tactile- somatosensory	34.9 (12.3)	43.2 (12)	$t(9) = 0.59$	1
11. Vestibular- balance	8.3 (5.7)	0 (0)	$Z = 1.34$	0.9
14. Movement	86.6 (7)	63.1 (10.2)	$t(9) = 3.77$	0.022*
18. Movement alterations	13.3 (6.9)	5 (5)	$Z = 0.76$	1
26. Body scheme alterations	5 (5)	3.3 (3.3)	$Z = 0.45$	1
<i>Movement sub-scales</i>				
16.1 Single actions	53.3 (13.3)	51.7 (13.3)	$Z = 0.22$	1
16.2 Repetitive actions	65 (9.8)	30 (8.5)	$t(9) = 4.36$	0.006*
16.3 Passive movements	30 (8.5)	11.7 (7.9)	$t(9) = 1.56$	0.45

555 *Note.* t: paired samples t test; Z: Wilcoxon signed-rank test; \*  $p_B < 0.05$

556

557

558 To investigate whether specific types of movement were inhibited by tDCS, we compared the  
559 proportion of dreams with single actions (i.e. movements that are not repeated immediately  
560 after their execution, such as placing a book on the table), repetitive actions (i.e. the same  
561 movements repeated several times in a continuous sequence, such as running), and passive  
562 movements (i.e. movements determined by external forces, such as traveling by car) between  
563 tDCS and sham-stimulation conditions (see Table S1 for examples of movement descriptions  
564 in the verbal dream reports). There were significantly less dreams with repetitive actions in  
565 the tDCS condition ( $M=30\%$ ,  $SEM=8.5\%$ ) compared to the sham condition ( $M=65\%$ ,  
566  $SEM=9.8\%$ ) (paired samples t test:  $t(9)=4.36$ ,  $d=1.21$ ,  $p_{B,3}=0.006$ ) (see Fig. 2). There were no  
567 significant tDCS effects on the frequency of dreams containing single actions or passive  
568 movements (see Table 2).

569 Interestingly, we found no difference in movement frequency between the stimulation  
570 conditions in verbal dream reports that were content analysed by external judges (see Table  
571 S2). This could be due to a considerably smaller proportion of explicitly expressed  
572 movements in free reports compared to the BED Questionnaire answers. It is possible that  
573 participants tended to omit movements from the spontaneous verbal reports that were given  
574 before answering to explicit motor questions of the BED Questionnaire (see Supplementary  
575 Results).

576 According to our questionnaire data, a majority of dream movements involved the whole  
577 body ( $M=75.5\%$ ,  $SEM=7.62\%$ ) and more rarely the right hand ( $M=25\%$ ,  $SEM=8.23\%$ ) or  
578 both hands ( $M=15.83\%$ ,  $SEM=7.02\%$ ); another unspecified body part was mentioned in only  
579 one report. Repetitive actions typically involved the whole body ( $M=89.8\%$ ,  $SEM=6.8\%$ ),  
580 with only 5.6% of repetitive movements performed by the right hand (Wilcoxon signed-rank  
581 test:  $Z=2.71$ ,  $p=0.007$ , effect size  $r=0.64$ ). Contrary to this, the proportion of single actions  
582 was comparable for the whole body ( $M=43.8\%$ ,  $SEM=12.3\%$ ) and right hand movements

583 (M=34.4%, SEM=11.5%, Wilcoxon signed-rank test: Z=0.43, p=0.67, effect size  $r=0.11$ ). No  
584 systematic body part or laterality differences were observed between the sham-stimulation  
585 and tDCS conditions.

586 Importantly, the observed reduction of dream movement following tDCS was not related to  
587 the overall length of dream reports, which could have been a confounding factor. To test  
588 whether the reduction in dream movement was related to shorter dream reports following  
589 tDCS, we compared the subjectively reported duration of dreams during the tDCS and sham-  
590 stimulation conditions (BED Questionnaire - Q41, see Appendix 1). There was no difference  
591 in the subjectively reported duration of dream reports between tDCS (Median=9.17 min,  
592 range from 1.5 min to 97.5 min) and sham-stimulation (Median=9.67 min, range from 0.83  
593 min to 40 min) conditions (Wilcoxon signed-rank test: Z=0.36, p=0.72,  $r=0.11$ ). Furthermore,  
594 we compared the word count of dream reports. Once again, there was no significant  
595 difference between tDCS (M=76.1, SEM=16.31) and sham-stimulation (M=124.2,  
596 SEM=34.68) conditions (paired samples t test:  $t(9)=1.69$ ,  $p=0.124$ ,  $d=0.56$ , Bf in favor of the  
597 null=1.11). On four occasions, participants remembered and reported additional details of a  
598 dream after completing the original dream report and questionnaire, while they were trying to  
599 fall asleep again. When these secondary reports were included in the word count analysis,  
600 there was still no significant difference in word count between tDCS (M=89, SEM=19.83)  
601 and sham-stimulation (M=124.98, SEM=34.55) conditions (paired samples t test:  $t(9)=1.15$ ,  
602  $p=0.281$ ,  $d=0.4$ , Bf in favor of the null=1.91). We thus conclude that differences in the length  
603 of dream reports (and in the subjectively estimated duration of dreams) were not related to  
604 the observed reduction of dream movement following tDCS.

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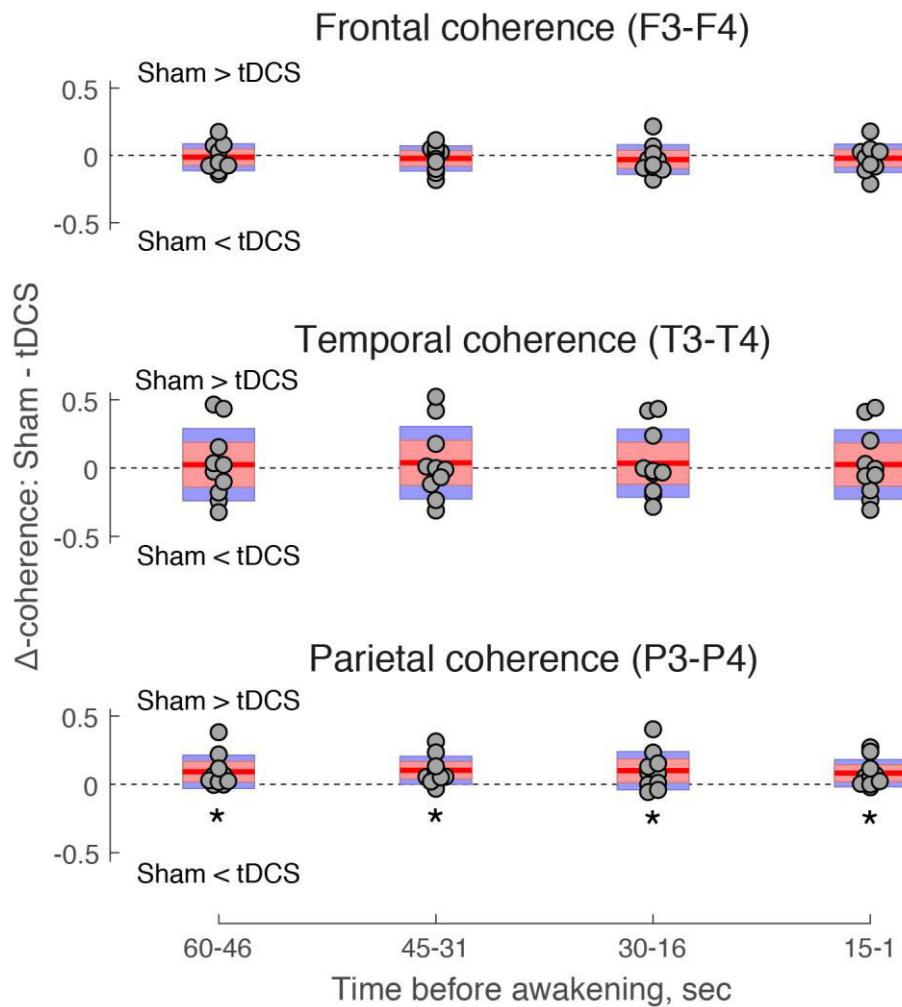
607 **tDCS modulation of EEG activity.**

608 Given the opposing direction of bihemispheric tDCS in the current study, i.e. a cathodal  
609 inhibitory effect over the left motor cortex and anodal excitatory effect over the right motor  
610 cortex, we hypothesized that a reduction of repetitive whole-body actions in response to  
611 tDCS was due to a decreased inter-hemispheric coordination of motor processing. To  
612 investigate this hypothesis, we restricted EEG analysis to the beta frequency band, because  
613 (1) transient and tonic changes in EEG beta oscillatory activity underlie cortical processing of  
614 both real (Gerloff et al. 1998; Jenkinson and Brown 2011; Zaepffel et al. 2013) and imagined  
615 (Neuper et al. 2005; Nam et al. 2011) movements, (2) preparation and execution of  
616 movement involves inter-hemispheric functional coupling in the beta frequency range  
617 (Leocani et al. 1997; Mima et al. 2000), and (3) motor impairment and successful  
618 rehabilitation involve changes in the inter-hemispheric interaction in the beta frequency range  
619 (Pellegrino et al. 2012; Fortuna et al. 2013). We thus expected bihemispheric tDCS to  
620 destabilize motor processing by reducing inter-hemispheric coherence in the beta frequency  
621 range.

622 As predicted, we observed a significant decrease in coherence between parietal electrodes P3-  
623 P4 following tDCS compared to sham-stimulation during a 1-minute stimulation-free period  
624 before awakening (Wilcoxon signed-rank test:  $Z=2.5$ ,  $p_{B-3}=0.039$ , effect size  $r=0.79$ ). No  
625 inter-hemispheric tDCS effects were observed between frontal (paired samples t test:  
626  $t(9)=0.72$ ,  $p_{B-3}=1$ ,  $d=0.244$ ) or temporal electrodes ( $t(9)=0.38$ ,  $p_{B-3}=1$ ,  $d=0.114$ ). To control  
627 for temporal specificity of the decrease of parietal coherence, we repeated the same analysis  
628 in four separate time intervals following termination of stimulation: -60 to -46 sec, -45 to -31  
629 sec, -30 to -16 sec, and -15 sec to -1 sec prior to awakening. A significant effect observed  
630 only in the time window before awakening (i.e. -30 to -16 sec, and/or -15 sec to -1 sec) would  
631 indicate a non-specific effect of experimental stimulation. Compared to sham-stimulation, a

632 significant decrease of parietal coherence took place in the tDCS condition throughout all  
633 four sub-intervals between the offset of stimulation and the onset of awakening, confirming a  
634 direct and relatively long-lasting tDCS effect on parietal coherence in the beta-frequency  
635 range (see Fig 3).

636



637

638 **Figure 3 | EEG coherence following tDCS during REM sleep.** Inter-hemispheric EEG  
639 coherence between frontal (top), temporal (middle), and parietal (bottom) electrodes  
640 surrounding the tDCS site, expressed as a difference between sham-stimulation and tDCS  
641 conditions ( $\Delta$ -coherence). Jittered circles represent individual participants. Red lines depict  
642 the mean of  $\Delta$ -coherence, pink bars represent 1 standard deviation (SD), and blue bars  
643 represent 95% confidence intervals for the mean. Positive values indicate higher coherence in  
644 the sham-stimulation condition, whereas negative values indicate higher coherence in the  
645 tDCS condition.  $\Delta$ -coherence is plotted separately in four stimulation-free time intervals

646 preceding controlled awakenings from REM sleep. In the parietal region, coherence was  
647 reduced by tDCS compared to sham stimulation in -60- to 46 sec ( $Z=2.5$ ,  $p=0.013$ ,  $r=0.79$ ), -  
648 45 to -31 sec ( $t(9)=3.17$ ,  $p=0.011$ ,  $d=0.97$ ), -30 to -16 sec ( $t(9)=2.27$ ,  $p=0.05$ ,  $d=0.88$ ) and -15  
649 to -1 sec ( $t(9)=2.57$ ,  $p=0.03$ ,  $d=0.74$ ) time intervals. \*  $p < 0.05$ .

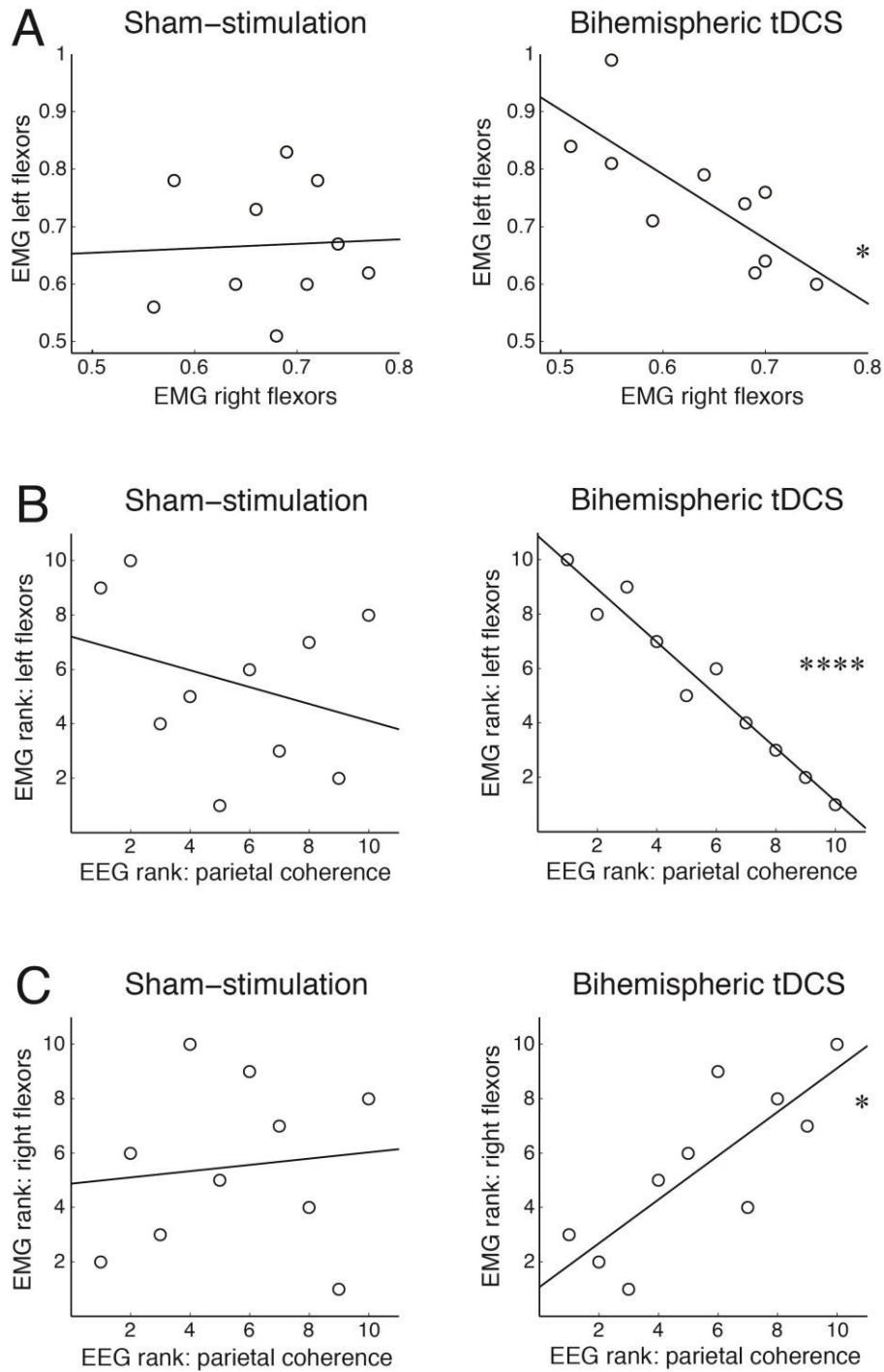
650  
651 Given that EEG coherence can be affected by spectral power differences between conditions  
652 (Fein et al. 1988), we carried out a control analysis to compare beta power in the electrodes  
653 adjacent to the stimulation site across a 1 min stimulation-free pre-awakening period. There  
654 was a significant decrease of beta power at the left parietal site (P3) in the tDCS compared to  
655 the sham-stimulation condition (paired samples t test:  $t(9)=2.29$ ,  $p=0.048$ ,  $d=0.37$ , Bf in favor  
656 of the null=0.64), whereas tDCS did not modulate beta power in the right parietal site (P4)  
657 ( $t(9)=0.73$ ,  $p=0.48$ ,  $d=0.088$ , Bf in favor of the null=2.93). The observed trend was  
658 investigated further across four 15 sec sub-intervals. No tDCS effects were observed  
659 regarding beta power in P3 electrode during time intervals immediately following motor  
660 cortex stimulation, i.e. -60 to -46 sec (paired samples t test:  $t(9)=1.159$ ,  $p=0.276$ ,  $d=0.25$ , Bf  
661 in favor of the null=1.89) and -45 to -31 sec ( $t(9)=1.172$ ,  $p=0.271$ ,  $d=0.3$ , Bf in favor of the  
662 null=1.87). Contrary to this, beta power decreased during time intervals preceding  
663 awakenings: -30 to -16 sec (paired samples t test:  $t(9)=2.433$ ,  $p=0.038$ ,  $d=0.433$ , Bf in favor  
664 of the null=0.46) and -15 to -1 sec ( $t(9)=2.829$ ,  $p=0.02$ ,  $d=0.379$ , Bf in favor of the  
665 null=0.28). Given that EEG beta coherence was modulated by tDCS across all four time  
666 intervals, we conclude that its decrease was not due to the temporally constricted changes in  
667 beta spectral power.

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672 **tDCS modulation of EMG activity.**

673 We observed a significant association in the proportion of phasic EMG activity in the flexors  
674 between the left and right arms during the 1-min period of REM sleep from the offset of  
675 tDCS to the controlled awakening (Pearson correlation: forearm flexors:  $r=-0.769$ ,  $p_{B-4}=0.037$ ;  
676 deltoids:  $r=-0.738$ ,  $p_{B-4}=0.06$ ). The negative correlation between the arms likely reflects the  
677 asymmetrical modality of stimulation with the cathode placed over the right sensorimotor  
678 cortex and the anode over the left sensorimotor cortex. Contrary to this, there was no  
679 association in the proportion of phasic EMG between forearms following sham stimulation  
680 (Pearson correlation: forearm flexors:  $r=0.095$ ,  $p_{B-4}=1$ ; deltoids:  $r=0.308$ ,  $p_{B-4}=1$ ), indicating  
681 that muscle activity varied independently (see Fig 4A). Regarding absolute EMG values,  
682 there was no difference between phasic activity in the left as compared to the right arm in  
683 either the sham-stimulation condition (paired samples t test: forearm flexors:  $t(9)=0.12$ ,  $p_{B-4}=1$ ,  $d=0.08$ ;  
684 deltoids:  $t(9)=1.52$ ,  $p_{B-4}=0.66$ ,  $d=0.57$ ) or following tDCS (forearm flexors:  
685  $t(9)=1.88$ ,  $p_{B-4}=0.37$ ,  $d=1.13$ ; deltoids:  $t(9)=1.96$ ,  $p_{B-4}=0.33$ ,  $d=1.08$ ).

686



687

688

689 **Figure 4 | Bihemispheric tDCS during REM sleep modulates phasic activity of the**  
690 **forearm muscles. (A)** Correlation of EMG shift towards phasic activity between the left and  
691 right forearm flexor muscles in the sham-stimulation and tDCS conditions. **(B-C)** Correlation  
692 between EMG shift towards phasic activity and EEG parietal coherence in the beta frequency  
693 band, plotted separately for the left and right forearm recordings, in the sham-stimulation and  
694 tDCS conditions. Ranked data are plotted in (B) and (C) as Spearman's rank order

695 correlations were carried between EMG and EEG measures. In all plots, the least-squares  
696 lines are plotted to visualize associations between variables. \*  $p_B < 0.05$ , \*\*\*\*  $p_B < 0.00005$ .

697

698 Next, we investigated whether peripheral EMG activity is associated with EEG parietal  
699 coherence in the beta frequency band, which decreased in response to tDCS during REM  
700 sleep (see Fig 4B-C). In the tDCS condition, EEG coherence was significantly associated  
701 with the proportion of phasic activity in the left flexor muscles (Spearman rank order  
702 correlation:  $\rho = -0.976$ ,  $p_{B-8} = 0.00001$ ), and the right flexor muscles ( $\rho = 0.806$ ,  $p_{B-8} = 0.039$ ).  
703 Interestingly, higher parietal coherence was associated with a larger proportion of phasic  
704 activity in the right forearm muscles and a lower proportion of phasic activity in the left  
705 forearm muscles, once again likely reflecting differential effects of anodal vs. cathodal  
706 stimulation. No association was observed between parietal EEG coherence and the proportion  
707 of phasic activity in flexor muscles in the sham stimulation condition (lowest  $p_{B-8} = 1$ ).  
708 Likewise, there was no association between parietal EEG coherence and deltoid EMG,  
709 neither during sham-stimulation (lowest  $p_{B-8} = 1$ ) nor tDCS conditions (lowest  $p_{B-8} = 0.72$ ),  
710 indicating a site specific interaction between EEG and EMG measures.

711

## 712 **Discussion**

713

714 The foremost aim of our study was to investigate the role of the sensorimotor cortex in  
715 generating bodily sensations in REM sleep dreams by modulating the excitability of the  
716 sensorimotor cortex with tDCS. We found that compared to sham stimulation, bihemispheric  
717 tDCS over the sensorimotor cortex reduced the frequency specifically of repetitive actions of  
718 the dream self in preceding REM sleep dreams, providing causal evidence that the  
719 sensorimotor cortex is involved in the generation of dream movement. Furthermore, tDCS

720 interfered with inter-hemispheric EEG coherence and peripheral EMG activity, pointing to a  
721 change in both the central and peripheral motor systems in response to bihemispheric tDCS  
722 during REM sleep.

723

724 **Frequency of bodily sensations and movement in dreams.**

725 To systematically assess and directly interfere with bodily sensations in dreams, we  
726 developed a questionnaire designed to capture various dimensions of bodily experiences in  
727 dreams (see Table 2 and Appendix 1 for the complete questionnaire). Interestingly,  
728 independently of tDCS, our data suggest that while dream movements were very common,  
729 other bodily sensations such as somatosensory sensations, vestibular sensations or body  
730 schema alterations were rather rare. This overall pattern of frequent dream movement  
731 coupled with rare reports of other bodily sensations has been found in previous studies  
732 (Hobson 1988; Schwartz 2000; Windt 2018). Our study extends the previous work based on  
733 spontaneous dream reports by showing that when different types of bodily experiences are  
734 specifically investigated through use of a questionnaire, movements and tactile sensations  
735 remain the predominant dimensions of bodily experience in dreams. Thus, content analysis-  
736 and questionnaire-based studies provide converging evidence for the important role of  
737 sensorimotor phenomena in dreams.

738 The predominance of dream movement in our data also seems to be in line with a recent  
739 suggestion that kinesthesia is central to the generation of dream experience, at least during  
740 sleep onset (Nielsen 2017). At the same time, in our study, 36.9 % of dream reports following  
741 tDCS contained no movements. It therefore seems that specifically self-movements are not  
742 strictly necessary to sustain REM sleep dreaming. Moreover, the decrease of dream

743 movement did not reduce the length of dream reports in our sample. Whether these dreams  
744 still involved e.g. observed movement is an open question.

745 **Electrophysiological effects of bihemispheric tDCS.**

746 Bihemispheric tDCS over the sensorimotor cortex, as compared to sham stimulation,  
747 specifically altered repetitive actions in dreams. Repetitive actions are typically dependent on  
748 implicit memory of learnt motor sequences (e.g., walking), the automatic processing of which  
749 does not require explicit awareness and monitoring of movements. Such learnt, automatic  
750 movements, as compared to more controlled and deliberate movements, are also associated  
751 with a smaller increase of activity in brain areas related to motor processing (Wu and Hallett  
752 2005). Thus, arguably, a relatively modest tDCS interference with cortical processing might  
753 have down-regulated motor cortex activity involved in the processing of automatic  
754 movements, reducing it to the baseline resting level and simultaneously inhibiting the  
755 occurrence of repetitive actions in dreams. Contrary to this, the relatively stronger cortical  
756 activation underlying single controlled actions might not have been reduced sufficiently by  
757 tDCS interference to significantly alter dream content. This would explain why our results  
758 showed a specific decrease in repetitive actions, while the frequency of single actions in  
759 dreams remained relatively high during tDCS and did not significantly differ from sham  
760 stimulation. Alternatively, bihemispheric stimulation might have interfered with the temporal  
761 coordination of dream movement, prohibiting long sequences of repetitive actions, but  
762 sparing temporally restricted single actions. Indeed, dream imagery is notoriously unstable  
763 and prone to change in discontinuous jumps (Revonsuo and Salmivalli 1995). Such  
764 possibilities should be more directly assessed in future studies, e.g. using motor imagery tasks  
765 during wakefulness that would allow for a more stringent control of movement complexity.

766 We found that bihemispheric tDCS interfered with neural processing in the beta frequency  
767 band, classically linked to motor processing (Leocani et al. 1997; Gerloff et al. 1998; Mima et  
768 al. 2000; Neuper et al. 2005; Jenkinson and Brown 2011; Nam et al. 2011; Pellegrino et al.  
769 2012; Fortuna et al. 2013; Zaepffel et al. 2013; Khanna and Carmena 2015). In our setup,  
770 bihemispheric tDCS reduced inter-hemispheric coherence of parietal beta oscillations.  
771 Arguably, the differential montage of tDCS electrodes, i.e. the excitatory anode over the right  
772 sensorimotor cortex and the inhibitory cathode over the left sensorimotor cortex, disrupted  
773 inter-hemispheric coordination of motor commands, reducing the rate of repetitive actions  
774 associated with whole body movements in dreams. A differential effect of bihemispheric  
775 tDCS was also observed in the phasic EMG activity of the arm muscles. While phasic EMG  
776 varied independently between the arms during sham stimulation, a strong negative correlation  
777 was observed following tDCS, i.e. it suppressed phasic muscle activity in one arm while  
778 increasing it in the other arm.

779 We expected that such destabilizing and hemisphere-specific effects of tDCS would also  
780 cause unilateral distortions of bodily sensations in dreams, i.e. stronger effects on one side of  
781 the dream body. However, the observed reduction of dream movement in dreams was  
782 independent of the laterality of stimulation. That is, the decrease of inter-hemispheric EEG  
783 coherence and the emergence of phasic EMG anticorrelation between arms did not translate  
784 into unilateral effects on the dream body. We can only speculate on the rather surprising lack  
785 of side-specific effects, and further studies will be important to understand underlying  
786 mechanisms. To detect effects on other modalities (e.g. body image distortion, vestibular  
787 sensations), a larger group of participants might be necessary. Moreover, the absence of  
788 modulatory effects of tDCS on somatosensory experiences, which were reported quite  
789 frequently by our participants, could be related to the placement of the tDCS electrodes that  
790 was specifically determined by the location of the hand area in the primary motor cortex.

791

792 **Implications for consciousness studies.**

793 Our study suggests a methodology for identifying, via causal manipulation, the neural  
794 correlates of specific types of dream experience. Thus, beyond dream and sleep research, our  
795 findings also have more general implications for consciousness research. First, they add  
796 another piece of evidence that the neural correlates of specific dream content match the  
797 neural correlates of corresponding cognitive and behavioural functions during wakefulness  
798 (Siclari et al. 2017). Going beyond mere correlation, our results provide *causal* evidence that  
799 the motor cortex is involved in the generation of movement sensations in dreams.

800 Our results also shed light on the phenomenological profile of self-representation in dreams.  
801 In simulation theories, the subjective sense of presence, or the experience of a self in a world,  
802 is central to dreaming. While this highlights the importance of self-simulation, the precise  
803 pattern of self-experience in dreams, as compared to wakefulness, raises questions (Windt  
804 2015). One possibility is that bodily experience in dreams replicates waking experience;  
805 another is that dreams are characterized by a comparative overrepresentation of movement  
806 and an underrepresentation of other types of bodily experience (e.g. tactile, thermal, or pain  
807 sensations). Our finding that tDCS selectively altered dream movement, taken together with  
808 the comparatively low frequency of other types of bodily experience in dreams, is consistent  
809 with the second possibility. Future studies could aim to further investigate this question by  
810 gathering reports of bodily experience in both dreams and wakefulness, enabling a more  
811 direct comparison.

812 A related question concerns the relation between bodily experiences in dreams and the  
813 sleeping physical body. It is commonly thought that dream experience, including bodily  
814 experience, is completely independent of outward muscular activity and stimulation of the

815 physical body. However, there are empirical and theoretical reasons for thinking that varying  
816 degrees of concordance between dream experience and the physical body exist, on both the  
817 levels of sensory input and motor output (Windt et al. 2016; Windt 2018). Lesion studies in  
818 cats have shown that pontine lesions, which eliminate REM-sleep related muscular atonia,  
819 induce organized motor behavior, such as searching and attacking, during REM sleep  
820 (Henley and Morrison 1974; Sastre and Jouvet 1979), possibly indicating dream behaviours.  
821 Further examples include (illusory) own-body perception, such as when stimulation to the  
822 sleeping body is incorporated in dreams (Nielsen 1993; Sauvageau et al. 1998), and dream  
823 enactment behaviors in humans, in which outward muscular activity corresponds to  
824 movement sensations in dreams. REM sleep behavior disorder, in which seemingly goal-  
825 directed behaviors during REM sleep (such as attacking one's sleeping partner, attempting to  
826 run, etc.) match subjective dream reports, is an extreme example (Schenck et al. 1986; Valli  
827 et al. 2012; Howell and Schenck. 2015). But REM sleep is also accompanied by subtler  
828 muscular activity in the form of twitching (Blumberg and Plumeau 2016). Its concordance  
829 with dream experience seems plausible but has not been systematically investigated.

830 In our study, bihemispheric tDCS during REM sleep modulated not only dream movement  
831 but also outward muscular activity in the arms. Due to the absence of movement reports in  
832 several participants, we could not reliably relate individual variance in subjective movement  
833 reports to electrophysiological measures. However, our findings are consistent with the  
834 possibility that changes in dream movement are related to changes in outward muscular  
835 activity during REM sleep. A promising avenue for future research could be to investigate the  
836 relevance of bihemispheric tDCS for several movement-related sleep disorders. REM sleep  
837 behaviour disorder would be a good place to start because of the match between dream  
838 movements and outward physical activity. Other disorders that could benefit from the

839 inhibition of motor activity include sleep walking and restless leg syndrome. Here, however,  
840 the association with dream experience is less clear and should be investigated more directly.

841

842 **Limitations and outlook.**

843 Despite these promising results, the current study has several limitations. First, the effects of  
844 tDCS on mental states have been repetitively challenged by replicability difficulties  
845 (Tremblay et al. 2014; Horvath et al. 2015a, 2015b) and should thus be treated with caution.  
846 Nevertheless, given that motor cortex tDCS during wakefulness provides the most reliable  
847 effects (Horvath et al. 2015b; Buch et al. 2017), we expect the same to hold during REM  
848 sleep. Second, due to the very complicated and time-intensive protocol of the study, we could  
849 only recruit a rather small number of participants. Thus, larger samples and replication  
850 studies will be needed in future (Minarik et al. 2016). Furthermore, and again due to the  
851 complexity of the setup, we did not include a control stimulation site nor did we switch the  
852 side of the bihemispheric stimulation (to left anodal, right cathodal stimulation), which would  
853 be especially interesting to disentangle hemisphere-specific effects. Future studies with a  
854 larger sample of participants should also explore whether bihemispheric tDCS during REM  
855 sleep interferes with a wider range of EEG frequencies involved in motor processing,  
856 including alpha and gamma bands as well as broadband responses (Ball et al. 2008; Babiloni  
857 et al. 2016).

858

859 **Conclusions.**

860 To conclude, this study provided, in a controlled setup, evidence that stimulation over the  
861 sensorimotor cortex modulates dream content in healthy participants during REM sleep. This  
862 has important implications for various research fields, including consciousness research, and

863 sleep and dream research. Future studies will have to pinpoint more specifically which neural  
864 mechanisms underlie the inhibition of repetitive movements of the dream self and whether  
865 the observed subjective and neurophysiological effects are sufficiently long-lasting to warrant  
866 clinical studies in, for example, parasomnia patients.

867

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874

## 875 **Author Contributions.**

876 V.N., J.M.W., A.A.K., T.B. and B.L. conceived the study and designed the experiments.  
877 V.N., T.S. and R.P. conducted experiments. V.N., T.B., B.L. analyzed and interpreted EEG  
878 data. M.K. and T.B. analyzed and interpreted EMG data. V.N., J.M.W., K.V. and B.L.  
879 analyzed and interpreted dream data. V.N., J.M.W., M.K., K.V., T.S., R.P., A.R., T.B., and  
880 B.L. prepared the manuscript.

881

## 882 **Declaration of Interests**

883 The authors declare no competing interests.

884

885

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1139 **SUPPLEMENTARY MATERIALS**

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1141 **Content analysis of movement sensations in verbal dream reports: Results.**

1142 Movements were reported in 49.8% (SEM=10) of dreams following sham-stimulation and  
1143 54.9% (SEM=10.9) of dreams following tDCS. Repetitive actions were the most common  
1144 type of movement, followed by single actions, with passive movements being the least  
1145 common (see Tables S1 and S2), replicating the pattern observed in the BED Questionnaire  
1146 data. However, there were no significant differences between the sham-stimulation and tDCS  
1147 conditions (see Table S2), in contrast to the effects observed in the questionnaire data (see  
1148 Table 1). The discrepancy could be due to a considerably smaller proportion of explicitly  
1149 expressed movements in free dream reports compared to the BED Questionnaire answers, i.e.  
1150 participants tended to omit movements from the spontaneous verbal reports unless asked  
1151 about them explicitly.

1152 The difference between questionnaire results and dream report analyses has also been found  
1153 for emotions. The frequency of emotions increases 10-fold if participants are asked to report  
1154 emotions on a line-by-line basis, as compared to free dream reports (Merritt et al. 1994).  
1155 When participants are asked to rate the kinds of emotions experienced in their dreams, they  
1156 specifically report more positive emotions than when their dream reports are analyzed by  
1157 independent judges (Sikka et al. 2014, 2017). This discrepancy raises important  
1158 methodological issues that to date have not been fully resolved, and both methods likely have  
1159 weaknesses and suffer from different kinds of bias (Sikka et al. 2017). One reason for the  
1160 discrepancy, however, could be that free dream reports lack the focus to allow independent  
1161 judges to pick up on specific aspects of dream phenomenology, such as emotions or  
1162 movements. By contrast, when participants' focus is directed to these aspects, such as

1163 through use of questionnaires, this leads to more precise reporting. In our data, similar  
1164 proportions of different types of movements between external ratings and questionnaire  
1165 responses, together with the fact that movements are reported more frequently in the  
1166 questionnaire data, makes us lean towards this interpretation. There are also likely differences  
1167 in what is reported: in free dream reports, individual movements need to be described in some  
1168 detail for them to be rated by external judges. By contrast, in the questionnaire, participants  
1169 rate the occurrence and frequency of specific movement types over the entire dream. Again,  
1170 this may lead to a more comprehensive picture, but also bears the danger of overgeneralizing.

1171 Nevertheless, the proportion of repetitive actions correlated strongly between the free dream  
1172 reports and the BED Questionnaire answers in the sham-stimulation condition (Spearman  
1173 rank order correlation:  $\rho=0.81$ ,  $p_{B-8}=0.033$ ), indicating a strong convergence between these  
1174 two types of measurement. Interestingly, this association did not hold in the tDCS condition  
1175 ( $\rho=-0.19$ ,  $p_{B-8}=1$ ). No other correlations were significant.

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## Supplementary tables

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1193 **Table S1.** Examples of different types of movement reported in verbal dream reports

<i>Movement types</i>	<i>Sham</i>	<i>tDCS</i>
Single actions	“I [...] took away the wires” (P4, N2, A2)	“I was diving” (P1, N1, A1)
	“I was putting together some board” (P10, N2, A2)	“I was [...] to take a pose” (P5, N2, A1)
	“We [...] sat down” (P10, N2, A2)	“I painted a sunset and there was a ship” (P6, N2, A3)
	“I hugged her” (P10, N2, A3)	“I jumped there to the movie” (P7, N1, A1)
Repetitive actions	“I remember rubbing quite hard [...] my leg” (P1, N2, A1)	“I was swimming in a pool” (P1, N1, A1)
	“I was walking there” (P3, N2, A2)	“I [...] was writing something” (P3, N1, A1)
	“we are running away from him” (P4, N2, A1)	“we [...] went to the bathroom” (P5, N2, A2)
	“I had been sleepwalking” (P4, N2, A2)	“I was cleaning a table” (P5, N2, A2)

	“I was digging the vegetable garden” (P6, N1, A3)	“I was climbing upstairs” (P7, N2, A2)
	“I was coming out from some room” (P10, N2, A2)	“I was scratching [our cat]” (P8, N2, A3)
Passive movements	“we were coming from Lappeenranta with a train” (P4, N2, A1)	“our father was driving me and my brother [...] with a car” (P6, N2, A1)
	“they somehow forced to put my hand to fist” (P7, N1, A1)	“he took my hand and pulled me to the middle” (P6, N2, A1)

1194 *Note.* P – participant (1-10), N – night (1-2), A – awakening (1-3).

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1207 **Table S2.** Dream content analysis: Percentage of dream reports containing movement  
1208 sensations following sham-stimulation and tDCS during REM sleep

	<i>Sham</i>	<i>tDCS</i>	<i>Statistical test</i>	
	<i>M (SEM)</i>	<i>M (SEM)</i>	<i>t/Z</i>	<i>p</i>
<i>Movement</i>				
	49.8 (10)	54.9 (10.9)	$t(9) = 0.31$	0.77
<i>Movement sub-scales</i>				
Single actions	21.6 (10.5)	24.9 (8.6)	$t(9) = 0.19$	0.85
Repetitive actions	38.2 (12.7)	43.2 (9.4)	$Z = 0.54$	0.59
Passive movements	16.6 (7)	8.3 (5.7)	$Z = 0.76$	0.45

1209 *Note.* t: paired samples t test; Z: Wilcoxon signed-rank test. Uncorrected p values.

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1219 **Table S3.** Balance of awakenings between the first and the second night and between the  
1220 sham-stimulation and tDCS conditions

<i>Participant</i>	<i>1<sup>st</sup> night, N</i>	<i>2<sup>nd</sup> night, N</i>	<i>Sham, N</i>	<i>tDCS, N</i>
1	2	3	3	2
2	2	3	2	3
3	2	2	2	2
4	3	2	2	3
5	3	2	3	2
6	3	3	3	3
7	3	3	3	3
8	3	3	3	3
9	2	3	3	2
10	3	2	2	3
<i>Total:</i>	25	25	25	25

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