

1 **Title**

2 3-D deconvolution of human skin immune architecture with Multiplex Annotated Tissue
3 Imaging System (MANTIS)

4

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36 **Abstract**

37

38 Routine clinical assays, such as conventional immunohistochemistry, often fail to resolve the
39 regional heterogeneity of complex inflammatory skin conditions. Here we introduce MANTIS
40 (Multiplexed Annotated Tissue Imaging System), a flexible analytic pipeline compatible with
41 routine practice, specifically-designed for spatially-resolved immune phenotyping of the skin
42 in experimental or clinical samples. Based on phenotype attribution matrices coupled to α -shape
43 algorithms, MANTIS projects a representative digital immune landscape, while enabling
44 automated detection of major inflammatory clusters and concomitant single-cell data
45 quantification of biomarkers. We observed that severe pathological lesions from systemic lupus
46 erythematosus, Kawasaki syndrome or COVID-19-associated skin manifestations share
47 common quantitative immune features, while displaying a non-random distribution of cells with
48 the formation of disease-specific dermal immune structures. Given its accuracy and flexibility,
49 MANTIS is designed to solve the spatial organization of complex immune environments to
50 better apprehend the pathophysiology of skin manifestations.

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54 **Introduction**

55

56 The skin acts as a barrier organ that separates the body from the external environment. Upon
57 inflammation, blood-circulating immune cells are recruited to help orchestrate the cutaneous
58 immunity and are often nested nearby key structural elements (e.g., postcapillary venules, hair
59 follicles, dermal-epidermal junction, etc.)^{1,2}. In pathological settings, the nature and activation
60 status of the skin immune landscape often represent precious biological information that can
61 help establish an accurate diagnosis, apprehend interpatient heterogeneity and select the most
62 appropriate treatment. The use of imaging-based approaches to identify cutaneous immune cells
63 is still challenging because of the high level of autofluorescence arising from the tissue itself,
64 the potential spectral spillover when more than 4 fluorochromes are used simultaneously and
65 the entanglement of all cells within thick and polarized structural appendages.

66

67 The vast majority of microscopic diagnoses of inflammatory skin conditions relies on repeated
68 immunohistochemistry (IHC) analysis of one or two proteins and/or hematoxylin eosin (H&E)
69 staining in thin (2 to 5 μ m) formalin-fixed, paraffin-embedded (FFPE) specimens^{3,4}. While such

70 two-dimensional approaches are reproducible and suitable for routine practice, they do not
71 permit to apprehend the complex topology and heterogeneity of immune cells⁵, in particular
72 those nested in-between epidermal appendices. The development of image-based histo-
73 cytometry, which consists in analyzing segmented multicolor images with classical flow
74 cytometry gating strategies, has paved the way toward the development of sophisticated image-
75 generation systems coupled to computational imaging⁶. Recently, highly-multiplexed imaging
76 systems have significantly advanced our understanding of tissue-resident immune subsets and
77 of their spatial distribution with regards to tissue structures, with a strong focus on cancer
78 samples and tumor heterogeneity, such as CODEX^{7,8}, MIBI-TOF⁹, IMC¹⁰, MuSIC¹¹, CyCIF¹²,
79 Cell Dive¹³ and others¹⁴. While multiplexed imaging has an immense potential, there is a strong
80 need to democratize these methods with the use of inexpensive instrumentation compatible with
81 standard tissue processing and coupled to an analysis interface that is user-friendly enough to
82 be used in routine practice.

83

84 Here we present an integrated framework primarily designed for spatially-resolved immune
85 cells phenotyping in FFPE human skin biopsies. We first set up a simple and inexpensive
86 method to acquire 10 fluorescent signals simultaneously and in 3-D using a classical confocal
87 microscope. We next designed MANTIS (Multiplexed Annotated Tissue Imaging System), an
88 adaptable and interactive analytical system which automatically generates a digitalized version
89 of the skin immune landscape and enables single-cell quantitative data visualization. Based on
90 these settings, MANTIS could be implemented in most laboratories coupled to existing
91 confocal equipment to bridge the gap between sophisticated research tools and standard-of-care
92 diagnostic procedures with minimal human intervention.

93

94 **Results**

95

96 **Extraction of single-cell statistics from skin sections by combining conventional confocal 97 laser-scanning microscopy and computational imaging**

98 We developed a simple method to generate 3-D multiplexed fluorescent images from FFPE (20
99 µm thick) skin biopsies which could be implemented in most research or clinical laboratories
100 on existing equipment. Skin sections were first stained with different panels of commercially-
101 available fluorochrome-coupled antibodies added simultaneously, then quenched to avoid
102 excessive natural autofluorescence of skin structural elements (**Fig. 1A**). We acquired 3-D
103 fluorescent multiplexed images with a conventional inverted confocal laser-scanning

104 microscope equipped with 5 laser lines, 5 detectors and a 40X oil immersion objective, using a
105 strategy of sequential acquisition composed of fast consecutive steps (**Fig. 1B**; the detailed
106 description of optical paths and lasers of our 8-year-old Leica SP8 system is provided in the
107 Materials and Methods section). This setting enabled the acquisition of 8 to 10 fluorescent
108 channels, on a system primarily designed for 4 colors, over a skin section of the following 3
109 dimensions, 0.6 mm (x) x 0.4 mm (y) x 20 μ m (z) within 25 minutes. The obtained 3-D images
110 were then deconvoluted and compensated to correct 3-D fluorescent spectral spillovers (**Fig.**
111 **1C, D**) using the Huygens software (Scientific Volume Imaging), a strategy routinely applied
112 in flow cytometry to combine multiple fluorochromes simultaneously^{6,15}. Compared to classical
113 segmentation strategies based on nucleus expansion¹⁶, which often lead to under or over-
114 estimation of cellular cluster composition, we used the general immune biomarker CD45 as a
115 robust immune staining visualized in most skin-resident immune cells to constitute the core of
116 our cell segmentation strategy for future single immune cell statistics extraction (**Fig. 1E, F**).
117 Using the Isosurface algorithm of the Imaris software (Bitplane) we next modeled the 3D
118 fluorescence signal of CD45 for individual immune cells and exported a corresponding single-
119 cell database composed of the mean fluorescence intensity (MFI) of all individual biomarkers
120 and precise x, y, z tissue coordinates obtained with a resolution of 299 x 299 x 999 nm/voxel
121 (**Fig. 1F**). We found that CD45-based segmentation enabled an efficient isolation of single
122 immune cell characteristics, even when those were found aggregated around dermal structural
123 elements. Overall, we demonstrate that it is possible to extract a 10 parameter- single-cell
124 database using regular confocal equipment coupled to basic computational imaging steps.
125

126 **Analysis of the skin immune landscape using MANTIS phenotypes attribution matrices**
127 Based on the literature, we designed two panels composed of antibodies directed against
128 immune biomarkers suitable to generate a non-exhaustive overview of lymphoid and myeloid
129 cell landscape of the skin, with an average cost of approximately \$65 per sample. The
130 combination of CD45, CD3e, CD4, CD8, TCR $\gamma\delta$, CD20 and CD57 (a terminally sulfated
131 glycan carbohydrate epitope shared by NK and T cells with high cytotoxic potential^{17,18}) allows
132 to identify the following lymphoid cells: conventional CD4 and CD8 T cells (being CD57^{low} or
133 CD57^{high}), CD4⁺ CD8⁺ double positive (dp) T cells¹⁹, CD4⁻ CD8⁻ double negative (dn) T cells²⁰,
134 $\gamma\delta$ T cells, B cells and NK cells (**Table 1**). The combination of CD45, CD207, CD1c, HLA-
135 DR, CD123, Siglec-8, myeloperoxidase (MPO) and tryptase allows to identify the following
136 myeloid cells: Langerhans cells, Langerin⁺ (CD207⁺) dermal dendritic cells (dDCs) and
137 Langerin⁻ dDCs, eosinophils, basophils, neutrophils and mast cells (**Table 1**). The activation

138 status of DC, Langerin⁺ DC and LC was investigated using levels of HLA-DR expression. A
139 detailed list of excitation/emission/detection strategies is provided in **Table 2**.

140

141 We next aimed to develop an adaptable analytical system that could integrate and batch-process
142 extracted single-cell databases and enable an unsupervised phenotyping of immune subsets. To
143 address this latter challenge, we developed MANTIS, an interactive digital tool based on
144 phenotype attribution matrices inspired by the analytical logic of single-cell RNA sequencing
145 that identifies correlations between the single-cell database and the expression profiles of
146 different cell types (**Fig. 2A**). Such an analysis is possible by computing Spearman's Rho
147 correlation, which accommodates non-linear relationships in the expression values (i.e., in our
148 case the collected MFI of each biomarker). In practice, MANTIS runs instantaneously a
149 pairwise Spearman's correlation analysis, for each detected single-cell, against selected
150 combinations of biomarkers to identify the immune subsets annotated in the phenotype
151 attribution matrices. The output information is the attribution of specific Rho values per single
152 cell which then automatically finds the best match of cellular identity and generates associated
153 quantitative statistics (**Fig. 2A-C, Supp Fig. 1A, B**). As a proof of concept, we generated data
154 from two serial sections of an acral lesion from a patient with systemic lupus erythematosus
155 (SLE, i.e., lupus chilblains) stained with a lymphoid and a myeloid panel. The fast 3-D
156 acquisition of one region of interest (ROI) composed of 6 fields of view (i.e., 0.6 mm (x) x 0.4
157 mm (y) x 20 μ m (z)) enabled the annotation of 519 myeloid cells and 708 lymphoid cells for a
158 total of 19 different immune subsets identified (**Supp Fig. 1C, Fig. 2D**). One can then decide
159 to visualize annotated immune populations using either a heatmap, in which the MFI of
160 individual biomarkers is displayed per single cell (**Supp Fig. 1D**), or a graph-based
161 dimensionality reduction, i.e., t-distributed stochastic neighbor embedding (t-SNE), specifically
162 designed for visualizing clusters of populations and corresponding expression of biomarkers
163 per cluster (**Fig. 2E**).

164 A particularly challenging aspect of multiplexed imaging technologies is to circumvent the
165 spatial distribution of immune cells with respect to longitudinal and polarized structural
166 elements (e.g., epidermal appendages of the skin) in thick tissue sections. We developed an
167 interactive software interface that contextualizes the immune topology of the skin by replacing
168 all annotated single immune cells within their 3-D spatial context and leverages the natural
169 autofluorescence of keratinocytes to model the epidermal layer to facilitate biopsy orientation
170 (**Fig. 2F, Supp Fig. 1E, F**). The algorithm allows to use two complementary analytical
171 approaches and to switch from one to the other with a simple drawing tool (**Supp Video 1**).

172 The analysis can start from the visualization of the skin digital immune landscape, then be
173 pursued with the investigation of the immune composition of defined microregions via
174 instantaneous re-computation of drawn ROI. Conversely, it is also possible to start from all
175 annotated immune cells on a t-SNE graph, draw around subsets of interest, and immediately
176 visualize their anatomical distribution in the skin digital immune landscape (**Supp Video 1**,
177 **Fig. 2G**). Taken together, these data suggest that MANTIS interactive analytical system can be
178 used to compute the 3-D spatial organization of immune and structural elements of
179 inflammatory skin samples from patients.

180

181 **Quantitative validation of MANTIS annotation system using healthy-looking skin and** 182 **inflammatory pathological lesions**

183 With the constant increase in the number of cases, a large panel of putative skin manifestations
184 of COVID-19 have been observed worldwide^{21,22}, including an unprecedented high rate of acral
185 lesions which represent ~ 75% of all cases and commonly named “COVID-Toes”²³⁻²⁶. Such
186 manifestations (**Supp Fig. 2A**), compared to non-inflamed healthy-looking skin (**Supp Fig.**
187 **2B**), are associated with an important immune cell infiltration (**Supp Fig. 2C**) and tend to
188 develop in young patients with no or very mild respiratory symptoms^{26,27}. While some
189 pathological features of those lesions have been described^{28,3,29}, a precise analysis of their
190 spatial immune profile is currently missing, which impairs the development of a clear readout
191 to better diagnose and treat these rare cutaneous lesions. A possible explanation could be a
192 collateral clinical manifestation of an efficient anti-viral type 1 interferon response, since acral
193 lesions are also commonly observed in patients with interferonopathies, such as the Aicardi-
194 Goutières syndrome³⁰ ref and SLE³¹. With this in mind, we decided to benchmark the effective
195 performance of MANTIS to resolve the immune topology of skin lesions of similar clinical
196 severity from 5 patients with COVID-toes, 2 patients with the multi-system inflammatory
197 syndrome (MIS), which is clinically similar to Kawasaki syndrome (i.e., a rare severe systemic
198 inflammatory condition triggered by SARS-CoV-2 infection, named there after “Kawasaki
199 syndrome”) and 3 patients with SLE chilblains. Abdominal skin biopsies from 5 healthy-
200 looking controls were used to set the baseline of a natural steady-state immune environment,
201 albeit from a distant anatomical region.

202 We validated the quantitative performance of MANTIS to annotate immune cells by
203 calculations of statistical correlations with a supervised approach of histo-cytometry^{15,32} applied
204 on the same datasets for each antibody panel in all skin samples. This last method consists in a
205 manual gating of immune subsets on the same principle used in traditional flow cytometry. A

206 total of 20,464 single CD45⁺ immune cells were identified with the following distribution per
207 condition: 1,670 immune cells in 5 healthy-looking skin samples (i.e., with 895 myeloid and
208 775 lymphoid cells), 1,703 in 2 Kawasaki syndrome patients (i.e., with 932 myeloid and 775
209 lymphoid cells), 5,076 in 3 SLE chilblain patients (i.e., with 1,560 myeloid and 3,516 lymphoid
210 cells) and 12,015 in 5 COVID-toes patients (i.e., with 2,838 myeloid and 9,177 lymphoid cells).
211 A classical gating strategy based on mutually exclusive biomarkers was used to assess the
212 presence of myeloid (**Supp Fig. 3A**) and lymphoid (**Supp Fig. 4A**) cell subsets by histo-
213 cytometry. We identified a total of 19 different immune subsets and found very similar
214 distributions of cell counts by either supervised histo-cytometry or unsupervised MANTIS
215 algorithm (**Supp Fig. 3B-E, 4B-E**). The calculated R coefficients were between 0.75 and 1,
216 regardless of the antibody panel, the patients analyzed or the disease (**Supp Fig. 3F** and **4F**).
217 Importantly, we observed that all healthy-looking skin samples exhibited a proportion of
218 immune cells aligned with previously described skin-resident immune populations at steady
219 state in human^{1,33}. However, we noted a slightly higher tendency to detect rare populations of
220 blood-circulating CD45⁺CD3⁻CD20⁺ B cells or CD45⁺HLA-DR⁻CD123⁺Siglec8⁺ basophils,
221 only when 3-D images were computationally analyzed with MANTIS (**Supp Fig. 3B** and **4B**).
222 This is consistent with the fact that the skin is a highly-vascularized tissue and that recent studies
223 identified rare B cells in healthy skin³⁴.

224 Having validated the quantitative and qualitative performance of MANTIS-based annotation,
225 we next defined a high-level view of the complex immune environment of pathological lesions
226 from all 10 patients. Compared to healthy-looking samples, pathological lesions contained large
227 immune infiltrates confirming their inflammatory status (**Fig. 3A, B**). All three conditions were
228 associated with an infiltration of myeloid cells composed of a large number of neutrophils,
229 eosinophils, mast cells and conventional CD45⁺CD1c⁺CD207⁻HLA-DR⁺ dDCs (**Fig. 3A, C**).
230 While detected in relatively low numbers in all analyzed skin samples, no difference was
231 observed between healthy-looking and pathological samples for CD45⁺CD1c⁻CD207⁺HLA-
232 DR⁺ LCs or CD45⁺CD1c⁺CD207⁺HLA-DR⁺ dDCs populations.

233 Compared to Kawasaki syndrome patients, SLE and COVID-19 patients tended to have an
234 increased proportion of lymphoid cells (**Fig. 3B, C**), with an enrichment in conventional CD4⁺
235 or CD8⁺ T cells and NK cells, and to a lesser extent in $\gamma\delta$ T cells. Interestingly, we also observed
236 double-positive (dp) CD45⁺CD4⁺CD8⁺CD3⁺TCR $\gamma\delta$ ⁻ and double-negative (dn) CD45⁺CD4⁻
237 CD8⁻CD3⁺TCR $\gamma\delta$ ⁻ T cells in all inflamed and some healthy-looking samples, albeit in smaller
238 numbers (**Fig. 3B, C** and **Supp Fig. 3**). Such populations of T cells were often understudied, as

239 CD4 and CD8 biomarkers are thought to be mutually exclusive, however they have been often
240 reported in autoimmune and chronic inflammatory disorders^{19,35}, including SLE^{36,37}.
241 We next performed an unsupervised clustering of all patients and healthy-looking controls
242 based on the quantitative analysis of their immune signature using both a detailed heatmap
243 based on immune profiles (**Fig. 3C**) and a principal component analysis (PCA) per patient (**Fig.**
244 **3D**). Healthy-looking skin samples clustered together, with no apparent relationship with the
245 pathological samples (**Fig. 3C, D**). Kawasaki syndrome and COVID-toes patients had a
246 tendency to form disease-specific clusters, while SLE patients were distributed between both
247 conditions (**Fig. 3C, D**). Even though these data were obtained on a restricted number of
248 patients, they suggest that all analyzed pathological lesions displayed common quantitative
249 immune features (**Fig. 3C**), with nevertheless potential disease-intrinsic characteristics
250 suggested upon analysis with a dimensional reduction PCA (**Fig. 3D**). To explore further this
251 hypothesis, we refined our analysis by investigating the activation status of conventional CD4⁺
252 and CD8⁺ T cells based on their expression level of CD57, a biomarker classically associated
253 with a high cytotoxic potential (i.e., pro-tissue damage) during viral infections and autoimmune
254 disorders, including COVID-19³⁸. We found that, compared to other pathological conditions, 3
255 COVID-toes cases were particularly enriched in CD4⁺ and CD8⁺ T cells exhibiting high levels
256 of CD57 (i.e., CD57^{high}; calculated as CD57 MFI z-score, **Fig. 3E-G**).
257 During inflammatory skin conditions, cytotoxic immune cells can relocate nearby to/in contact
258 with keratinocytes and contribute to severe epidermal damage^{39,40}. In order to calculate the
259 anatomical location of all immune cells with respect to the epidermal layers, we acquired the
260 spatial coordinates of the modeled epidermis. We next incorporated into MANTIS a k-
261 dimensional tree algorithm^{41,42}, which automatically decomposes the structural element
262 coordinates (i.e., as exemplified here with the epidermis) into virtual subspaces and enables to
263 calculate the nearest neighbor to each immune cell (**Supp Fig. 5A**). A batch calculation of the
264 distance of each individual cell can then be visualized under the format of a heatmap, providing
265 a quick overview of the dataset (**Supp Fig. 5B**). We found that HLA^{high} dDCs (**Supp Fig. 5C**),
266 NK cells (**Supp Fig. 5D**) and CD8⁺ CD57^{high} T cells (**Supp Fig. 5E**) were all significantly
267 enriched near the epidermal layer in cases of COVID-toes. Importantly, CD8⁺ CD57^{low} T cells
268 were not found enriched in the epidermis (**Fig. 3 H-K**), suggesting a biological link between
269 the expression levels of CD57 and epidermal migration in CD8 T cells. Even though the
270 number of patients studied is limited, these findings strongly suggest the potential formation of
271 tissue damaging subepidermal inflammatory clusters composed of cytotoxic T cells and NK
272 cells in COVID-toes.

273

274 **MANTIS enables topographic exploration of skin lesions by solving the α -shape of *in situ* 275 immune substructures**

276 Inflammatory dermatoses are characterized by the presence of large inflammatory infiltrates 277 composed of specific immune cells and thought to be critical for the development of the 278 pathology (e.g., type 2 immune cells and eosinophils in atopic dermatitis). To better understand 279 the regional heterogeneity of pathological lesions from SLE, Kawasaki syndrome and COVID- 280 toes, we took advantage of alpha (α)-shape algorithms that enable, by tuning the α parameter, 281 to define a precise shape of sets of points by drawing bounding polygons based on the principle 282 of Delaunay triangulation⁴³. When combined with the digital immune landscapes generated 283 with MANTIS, α -shape algorithms automatically generate polymorphic α -shapes around n- 284 clusters composed of a minimum of 15 cells (**Fig. 4A**, i.e., 15 being the minimum number of 285 cells often found in clusters of inflammatory but not in healthy-looking samples). This method 286 enables to automatically detect and quantify the major inflammatory clusters (i.e., named 287 thereafter “ α ROIs”) to provide a high-level view of the *in situ* immune architecture of the skin 288 lesion for each patient and disease. We generated lymphoid (**Fig. 4B, C**) and myeloid (**Fig. 4D, 289 E**) α ROIs for all the samples. Healthy-looking controls displayed a few lymphoid α ROIs, and 290 4/5 controls did not show myeloid α ROIs. These data indicate that, in human skin at the steady- 291 state, lymphoid cells have a tendency to form aggregates (i.e., composed of perivascular T 292 lymphocytes¹), while myeloid cells are more likely to be randomly distributed. In line with the 293 data presented in **Fig. 3**, we found a higher proportion of both lymphoid and myeloid α ROIs in 294 pathological samples as compared to healthy-looking controls (**Fig. 4B-E**). Using global 295 unsupervised hierarchical clustering of α ROIs per disease, we can generate a high-level view 296 of inflammatory clusters composition and observe trends in disease-specific immune responses 297 (**Fig. 4F, G**). Notably, lymphoid α ROIs of both Kawasaki syndrome and COVID-toes exhibited 298 a significantly higher proportion of CD4⁺CD57^{low} T cells than that of SLE patients (**Fig. 4F, 299 H**). Interestingly, both COVID-toes and SLE lesions displayed significant clusters of 300 CD8⁺CD57^{high} cytotoxic T cells, highlighting the cytolytic aspect of pathological lesions 301 microenvironment in these conditions (**Fig. 4F, I**). We next analyzed myeloid α ROIs for all 302 cases. We found that, COVID-toes had a particularly high density of clusters enriched in 303 activated HLA-DR^{high} dDCs (**Fig. 4G,J**). Conversely, Kawasaki syndrome lesions showed an 304 enrichment in both HLA-DR^{high} LCs (**Fig. 4G,K**) and mast cells (**Fig. 4G,L**), while SLE lesions 305 displayed large aggregates of eosinophils (**Fig. 4G,M**). This finding is consistent with previous 306 reports of strong eosinophilia in SLE⁴⁴⁻⁴⁶. No significant differences were observed regarding

307 other immune cell subsets in α ROIs (unpublished). While the precise role played by specific
308 inflammatory clusters of immune cells in each disease remains elusive, these data strongly
309 suggest that combining MANTIS digital maps with α -shape-based algorithms can reveal a
310 significant non-random distribution of skin immune cells in skin lesions, with the presence of
311 disease-specific immune structures. MANTIS analytic pipeline can thus enable to quickly solve
312 the spatial organization of complex immune environments and open interesting perspectives for
313 future investigations in the field of dermatopathology.

314

315 **Discussion**

316 Here we propose a general framework for 3-D quantitative and spatial analysis of skin immune
317 cells at the cellular level. We first describe a simple method to perform a fast 3-D acquisition
318 of up to 10 biomarkers simultaneously and extract a single-cell database containing the
319 biological identity (including spatial coordinates) of skin lymphoid and myeloid cells. We then
320 analyze the extracted databases using an automated and interactive analytic pipeline composed
321 of phenotype attribution matrices coupled with cell-to-structure distance calculations and α -
322 shape algorithm-based detection of major inflammatory clusters. Our analysis was focused on
323 FFPE samples as it is still the most easily-available source of pathological tissues and can
324 enable analysis of patients' skin-sampled in routine clinical practice. However, the use of cryo-
325 preserved samples is compatible with the approach we describe here, and enables the analysis
326 of thicker tissue sections (unpublished data).

327 We identified that the first steps of the process, which consists in the generation of good quality
328 3-D multiplexed images with a significantly high ratio signal over autofluorescent background
329 and no spectral spillover, were not necessarily obvious, while being critical for the rest of the
330 study. This is why we emphasized the capability of a conventional 8-year-old (non-custom-
331 built) confocal laser-scanning system to acquire 10 different fluorochromes simultaneously.
332 This method of acquisition can be democratized to most academic/clinical facilities since they
333 involve a conventional equipment coupled to basic spectral spillover compensation and single-
334 cell data extraction strategies, via the use of commercially-available softwares (Huygens and
335 Imaris; described in detail in the Methods section).

336 Single-cell segmentation is also very critical as it will constitute the very core of the future
337 analysis of immune subpopulations and expression of biomarkers. Possible mistakes made at
338 this step, e.g. the inability to separate immune cells in large infiltrates, would then result in
339 misinterpretation of MANTIS-generated results. We tested different approaches to
340 automatically segment healthy-looking and inflammatory skin samples, including random

341 forest-based classifiers (e.g., Ilastik machine learning). While such a method was suitable to
342 segment healthy-looking images with a low concentration of immune cells, it failed to segment
343 complex inflammatory lesions, where large and packed immune clusters were present
344 (unpublished). We thus opted for a semi-supervised segmentation of single immune cells using
345 the software Imaris, in which the segmentation of each inflammatory cluster was quality-
346 controlled manually and in 3-D (**Fig. 1F**). While this approach is probably more time-
347 consuming, we could ensure a precise 3-D segmentation and further extraction of an accurate
348 single-cell database to be processed with MANTIS. A recent study has reported the use of an
349 analysis pipeline, including a new segmentation strategy, adapted from the field of astronomy
350 named “AstroPath”⁴⁷. Using this approach and only six biomarkers, they could identify
351 important pathological features in biopsies from melanoma patients. These results, in line with
352 our findings, highlight the importance of carefully selecting a list of biomarkers to be studied
353 and of having the right analytic pipeline to draw reliable insights.

354 Because immunologists are more commonly used to identify immune cell populations with
355 manual gating of populations based on flow cytometry, we validated the quantitative
356 performance of MANTIS by analyzing the extracted single-cell databases for the 15 patients
357 analyzed with the conventional flow cytometry software, FlowJo. We found that the MANTIS-
358 based analysis on 3-D images generated with two different panels, and just a minimal number
359 of 10 antibodies per panel, were sufficient to distinguish 19 immune subsets and identify
360 disease-specific trends in skin lesions.

361 Because MANTIS attribution matrices can be quickly adjusted to any sets of markers, they
362 could be compatible with single-cell databases generated using technology with high
363 multiplexing capabilities such as CODEX^{7,8}, MIBI-TOF⁹, IMC¹⁰, MuSIC¹¹, CyCIF¹², Cell
364 Dive¹³ and others¹⁴. We included in MANTIS the α -shape algorithm that enables us to define
365 the precise shape of inflammatory immune clusters based on the principle of Delaunay
366 triangulation⁴³. When applied to digital immune landscapes, the α -shape algorithm
367 automatically identifies and quantifies dermal and epidermal inflammatory clusters (i.e.,
368 α ROIs) composed of a minimum of 15 immune cells (**Fig. 4A**). This method enables one to
369 directly analyze the major α ROIs to provide a fast high-level view of the skin immune
370 architecture in a given lesion. Using this method, we could quickly identify that immune subset
371 (e.g., mast cells, HLA-DR^{high} dDCs, CD8⁺CD57^{high} cytotoxic T cells, eosinophils etc.) were
372 specifically enriched in dermal areas only in some patient subgroups. These preliminary
373 observations suggest that, depending on their etiology, pathological lesions could be due to
374 distinct pathological mechanisms. This type of analysis opens interesting perspectives for the

375 3-D cartography of complex inflammatory skin lesions and should be pursued by additional
376 studies on a larger number of patients. Importantly, while 2D immune landscapes are
377 represented here to facilitate the visual assessment on Figures (3-D graphs are hardly
378 perceivable on static pictures), the single-cell segmentation and extraction of cellular spatial
379 coordinates were all performed in 3-D.

380 Based on CODEX high multiplexing capacity, previous studies^{8,48} have shown that it is possible
381 to generate a high-level view of the cell-to-cell interaction landscape based on the principle of
382 the Delaunay neighborhood graph⁴⁹. The MANTIS α -shape algorithm is complementary, as it
383 automatically identifies major immune structures while deciphering their cellular composition.
384 Combining α -shape and neighborhood approaches could help to quickly solve the biology of
385 major inflammatory clusters in the skin, by drawing the ligand-receptor interactome of immune
386 and structural cells within the identified cluster. Such a high dimensional analysis of the skin
387 immune architecture could provide a promising avenue for understanding the complexity of
388 inflammatory skin manifestations with potential benefits for patient stratification and/or
389 diagnosis.

390 There is a strong need to design new tools to assist clinical decision making and/or better
391 apprehend the complexity of inflammatory dermatoses. While very promising processes have
392 been made in the field of spatial biology⁵⁰⁻⁵², there is an unmet need for a non-expensive and
393 standardized multiplexed imaging analytical framework capable of automatically resolving the
394 immune architecture of an inflamed skin. Here we show that the MANTIS analytical system is
395 uniquely positioned to examine numerous questions in the fields of skin immuno-biology and
396 should lay the foundation for a fast and automated analysis pipeline of relevant *in situ*
397 inflammatory environments in both research and clinical facilities.

398

399 Materials and Methods

400 **Human skin samples.** Control normal skin biopsies were obtained from Genoskin SAS
401 (<https://www.genoskin.com/>). Genoskin has obtained all legal authorizations necessary from
402 the French Ministry of Higher Education, Research and Innovation (AC-2017-2897) and the
403 Personal Protection Committee (2017-A01041-52). Skin biopsies from patients with lupus
404 erythematosus were obtained from Toulouse University Hospital. Biopsies of COVID-toes
405 were obtained from Toulouse, Reims and Lyon University Hospitals. Skin biopsies of multi-
406 system inflammatory syndrome were obtained from Reims University Hospital.

407 **Skin section preparation, histology, and staining.** Human skin samples were either frozen in
408 optimal cutting temperature compounds (OCT, Tissue-Tek, unpublished) or formalin-fixed and
409 paraffin embedded (FFPE). 10 μ m FFPE-tissue sections were heated at 95°C for 20 minutes.
410 Sections were subsequently immersed into Xylene for 30 minutes, washed in a graded series of
411 ethanol (100%, 95%, 70%, 50% and 30% for 5 minutes each) and abundantly washed with
412 distilled water. They were then treated using a heat-induced epitope retrieval method as
413 previously described⁵³.

414 FFPE-tissue sections were blocked and permeabilized with PBS 0.5 % (w/v)% BSA (Sigma-
415 Aldrich), 0.3 % Triton X-100 (Merck) for 30 to 60 minutes at room temperature, then incubated
416 with fluorophore-coupled antibodies or unconjugated antibodies overnight at 4°C in the dark.
417 The sections were then washed three times in PBS 0.5 % (w/v)% BSA, 0.3 % Triton X-100 and
418 incubated, if needed, with secondary antibodies in PBS 0.5 % (w/v)% BSA, 0.3 % Triton X-
419 100 for 2 hours at room temperature in the dark. Finally, samples were treated with an
420 autofluorescence quenching solution named TrueView (Vector Lab) for 5 minutes. The slides
421 were mounted in Mowiol medium (Sigma-Aldrich) and sealed with a coverslip.

422 All conjugated and unconjugated antibodies used in this study were validated in single
423 immunostainings of human skin and tonsils (unpublished), and are listed in **Supplementary**
424 **Table 1.**

425 **Acquisition.** 512x512 pixel Z-Stack Images were acquired using an 8-year-old confocal
426 microscope SP8 (Leica Microsystems) equipped with a HC PL APO CS2 with 40X NA 1.3 oil
427 objective, a UV diode (405nm) and four lasers in visible range wavelengths (405, 488, 532, 552
428 and 635nm). The setup was made up of five detectors (three hybrid detectors with high quantum
429 yield compared to classical photomultiplier (PMTs) detectors, and two PMTs). Mosaic
430 sequential images were acquired using the between-stack configuration in order to
431 simultaneously collect individual 7/8 channels and tiles before merging them to obtain one
432 single image. Use of the between-stack configuration and the modulation of the detectors'
433 detection windows help to reduce the leaking of fluorophores. Finally, a digital zoom of 1.9
434 was applied during the acquisition and a mosaic multicolor image was obtained and exported
435 into a .lif format. Detection windows and microscope configuration used in our study are listed
436 in **Supplementary Table 2.**

437 **Image deconvolution and correction of spectral spillover.** 3-D mosaic images were then
438 imported into Huygens SVI software, in order to correct the signal by applying deconvolution
439 and crosstalk correction. Two deconvolution methods were used: the express deconvolution
440 (theoretical and fast) or the deconvolution wizard (possibility to use experimental or theoretical
441 parameters and to adjust the background value). Automatic crosstalk correction estimation was
442 obtained and the coefficients were slightly adjusted manually, if needed, for optimal spillover
443 correction.

444 **Segmentation.** 3-D mosaic images were imported into Imaris software to separate objects
445 (cells) using a 3-D surface segmentation. Before creating the surface objects in Imaris, classical
446 image processing was required. For instance, defining a threshold, adding a median filter,
447 and/or normalizing the layers were sometimes applied in order to clean the background. Images
448 were either cleaned using the CD45 surface objects or other channels by applying appropriate
449 masks for each channel. Then, segmentation was applied on the CD45 channel surface.
450 Statistics were exported into .csv format.

451 **Segmentation troubleshooting.** In some cases, the surface creation parameters were not
452 efficient to automatically obtain good object creation, or the module was not sensitive enough
453 to detect low intensity objects. In this case, the creation of small objects was done manually and
454 the threshold selection was also reduced. If the detected object was below 1 μm , a manual object
455 unification with surrounding objects of same intensity was performed.

456 **Statistical data exportation.** Statistical properties of each segmented object (cell) in the
457 processed 3-D Imaris Multiplex image were automatically calculated. Object *Volume*,
458 *Sphericity*, *Area*, *xyz Position* and *Mean Fluorescence Intensity (MFI)* in all channels were
459 exported as a .csv table.

460 **FlowJo analysis and gating strategies.** Identification and density assessment of immune cell
461 subsets were analyzed using classical histo-cytometry³².

462 Immune cell populations were gated in FlowJo software as follows:

463 B cells: CD45⁺ CD20⁺

464 NK cells: CD45⁺ CD20⁻ CD3⁻ CD57⁺

465 CD4⁺ T cells: CD45⁺ CD20⁻ CD3⁺ TCR $\gamma\delta^-$ CD4⁺ CD8⁻ CD57^{low or high}

466 CD8⁺ T cells: CD45⁺ CD20⁻ CD3⁺ TCR $\gamma\delta^-$ CD4⁻ CD8⁺ CD57^{low or high}

467 $\gamma\delta$ T cells: CD45⁺ CD20⁻ CD3⁺ TCR $\gamma\delta^+$

468 dn T cells: CD45⁺ CD20⁻ CD3⁺ TCR $\gamma\delta^-$ CD4⁻ CD8⁻
469 dp T cells: CD45⁺ CD20⁻ CD3⁺ TCR $\gamma\delta^-$ CD4⁺ CD8⁺
470 Mast cells: CD45⁺ Tryptase⁺
471 DC: CD45⁺ CD1c⁺ CD207⁻ HLA-DR^{low or high}
472 LC: CD45⁺ CD1c⁻ CD207⁺ HLA-DR^{low or high}
473 DC CD207⁺: CD45⁺ CD1c⁺ CD207⁺ HLA-DR^{low or high}
474 Neutrophils: CD45⁺ CD1c⁻ CD207⁻ Tryptase⁻ Siglec8⁻ MPO⁺
475 Eosinophils: CD45⁺ CD1c⁻ CD207⁻ MPO⁻ Tryptase⁻ Siglec8⁺ CD123⁻
476 Basophils: CD45⁺ CD1c⁻ CD207⁻ MPO⁻ Siglec8⁺ CD123⁺
477

478 **Tissue annotation**

479 **Implementation of MANTIS reference panels.** In order to enable cell identification, we built
480 a binary table containing a literature-based theoretical signature of biomarkers expressed in
481 each cell population identified by the used panel (naturally depending on the used set of
482 antibodies), known as the reference attribution panel. If a cell population is positive for a
483 marker, the value is set to 1, otherwise it is set to 0. If a cell population can be positive for a
484 marker, there are two columns, one with the value set to 1, the other with the value set to 0 (i.e.,
485 $\gamma\delta$ T cells can express CD4 or not). Two reference tables were implemented and designated by
486 lymphoid and myeloid reference attribution matrices.

487 **Dynamic adaptation of reference matrices.** Sample heterogeneity led to different acquisition
488 parameters (laser power, gain, etc.). In order to standardize data processing, we scaled the
489 reference tables and dynamically adapted, for each sample, the table values according to the
490 MFI values. In practice, the value “1” in the binary table was replaced by the maximum MFI
491 value acquired in the corresponding channel from the tested sample.

492 **Automatic cell type identification.** To annotate the segmented objects, a correlation matrix
493 between the MFI table and the adapted reference panel was generated by performing a pairwise
494 Spearman’s Rank Correlation using the R software (2021). Each object was then phenotypically
495 assigned to the cell type having the highest correlation coefficient. Objects with multiple highest
496 correlation coefficients were assigned as “Other” cell types.

497 **Accuracy validation.** The accuracy of MANTIS automatic cell identification was verified by
498 comparing quantification results to classical histo-cytometry³². Briefly, linear regression of cell

499 type density was computed between both attribution methods and regression coefficients were
500 calculated. Regression coefficients ranging between 0.75 and 1 reflect MANTIS technique
501 robustness.

502 **Activation status detection.** MANTIS panels were designed to not only include discriminant
503 markers for cell attribution but also non-discriminant and informative markers, for instance,
504 activation markers. The cell populations of interest (CD4⁺ and CD8⁺ T cells in the lymphoid
505 panel, DCs, LCs and CD207⁺ DCs in the myeloid panel) as well as the activation markers that
506 reflect the activation status of these populations (CD57 in the lymphoid panel, and HLA-DR in
507 the myeloid panel) were defined in the MANTIS algorithm. This latter automatically computes
508 the MFI density curve associated with the activation markers within the selected populations.
509 Subsequently, the MFI corresponding to the first peak of the density curve is defined as the
510 MFI value above which the cell is considered positive for the activation marker.

511 **Alpha (α)-shape calculation.** α -shape was calculated using the alphashape Python package.
512 Briefly, Delauney triangulation of a given set of points formed a bounding polygon that contains
513 all the points of the set. The α parameter was defined by the value α , and a circle with $1/\alpha$ radius
514 was drawn in such a way that two points of the dataset are located on the boundaries of the
515 circle and the circle is empty. For each empty circle found, the line between the two points
516 formed a side of the bounding polygon, i.e., the α shape. As α decreased, the alpha shape
517 changed from a convex hull (e.g., epidermis α shape, $\alpha = 0.4$) to a more tightly-fitting bounding
518 box resulting in more refined alpha shapes (e.g., region of interest alpha shape [α ROI], $\alpha = 0.1$).

519 **Cell to structure distance calculation and nearest neighbor search.** x-y coordinates of
520 epidermis α -shape contours were stored using the k-dimensional tree method, which allows
521 data ranking and structuration. Briefly, data points were classified based on nodes and branches
522 space-partitioning, allowing a fast nearest neighbor calculation. For a given point (cell) of the
523 dataset, the nearest neighbor in the epidermis alpha shape was found and the distance defined
524 by r was calculated using the *scipy.spatial* Python package⁴¹. The distance of cells contained in
525 the epidermis α shape was set to 0.

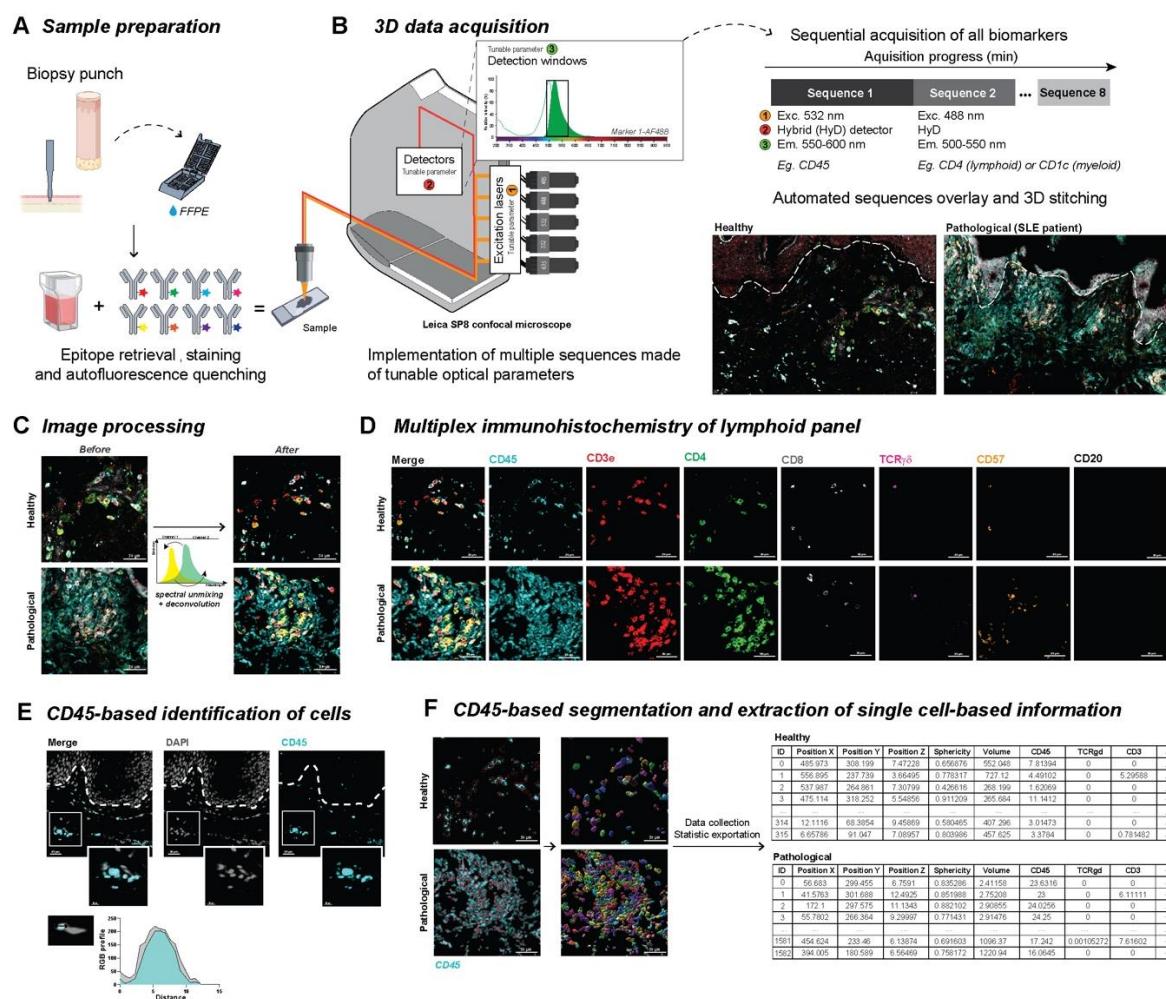
526 **Data clustering and α ROI analysis.** Regions of interest (α ROI, i.e., inflammatory cell
527 clusters) were identified using the α shape algorithm with a tuned α parameter ($\alpha = 0.1$),
528 allowing correct detection of high cell density areas. α ROI with less than 15 cells were removed
529 from the analysis. For each selected α ROI, specific characteristics were calculated and

530 extracted, such as area, total number of cells, cell number, proportion by cell type and α ROI
531 center coordinates.

532 **Data visualization.** Visualization charts were obtained using the *ggplot2*, *Pigengene* &
533 *ComplexHeatmap* R packages, and *matplotlib* & *seaborn* Python packages. t-Distributed
534 Stochastic Neighbor Embedding (tSNE) was computed with Rtsne.

535 **Statistics.** Statistical tests were performed using Prism 8 (GraphPad Software), the *Rstats* and
536 *rstatix* R packages. One-way ANOVA with Tukey's test for multiple comparisons or Mann-
537 Whitney test were performed on samples as noted in the respective figure legends. A p-value
538 of less than 0.05 was considered statistically significant.

539 **Figures and legends**



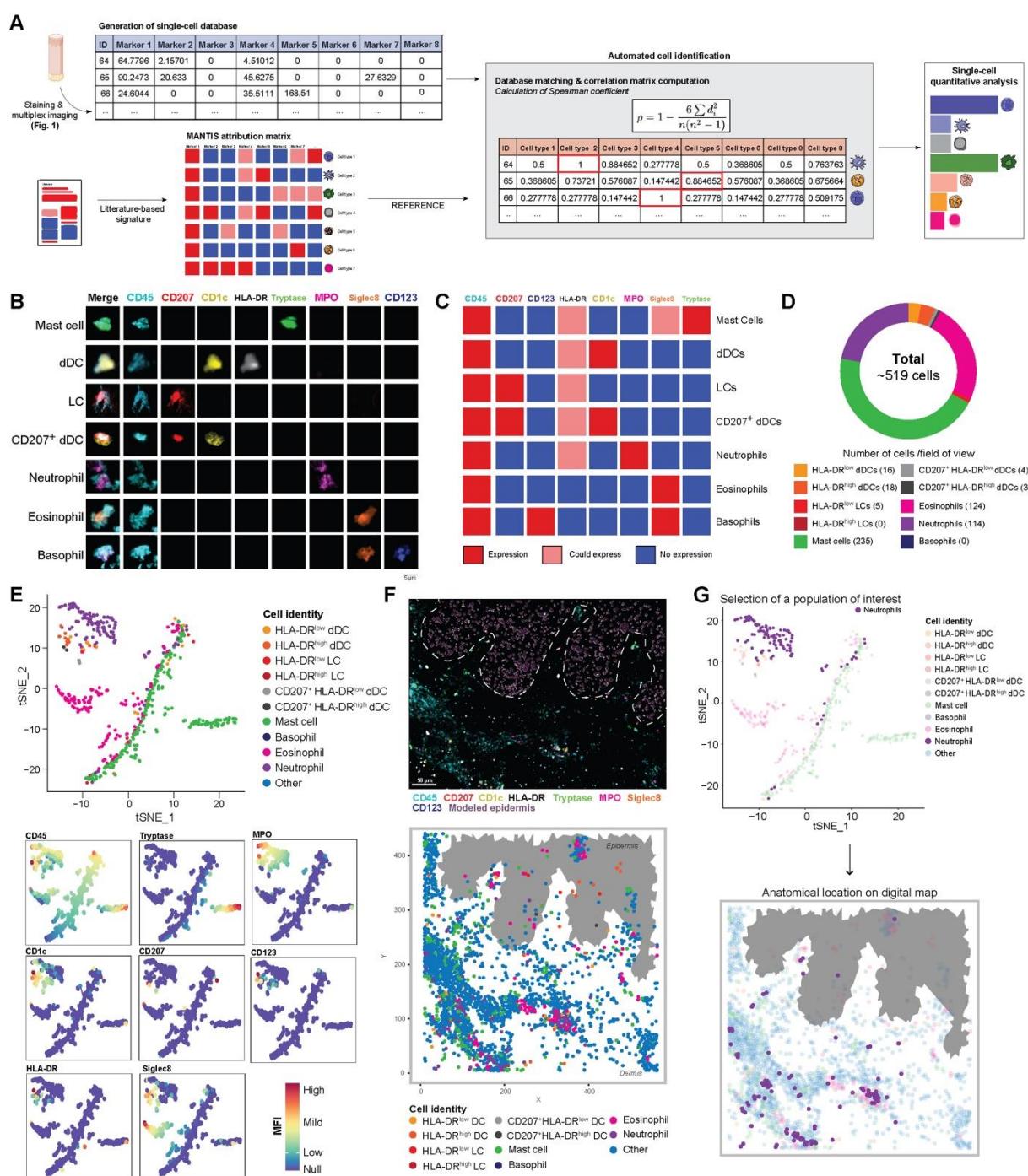
540

541 **Figure 1. Between-stack microscope configuration allows sequential acquisition of 7+**

542 **channels with classical image processing. A, Sample preparation.** FFPE-skin sections were
543 cut and stained for myeloid and lymphoid panels after appropriate epitope retrieval and
544 autofluorescence quenching. Sample images were then acquired using a SP8 confocal
545 microscope from Leica Microsystems as described in B. **B, Microscope configuration and**
546 acquisition settings. Mosaic sequential images were acquired using the between-stack
547 configuration with tunable detection windows. Sequences were overlaid and 3-D-stitched. An
548 example of data acquisition is given for healthy (left panel) and pathological (lupus
549 erythematosus [SLE], right panel) skin. **C, Deconvolution of regions of interest and spectral**
550 **unmixing.** Acquired 3-D images were deconvoluted and compensated to correct optical

Main manuscript

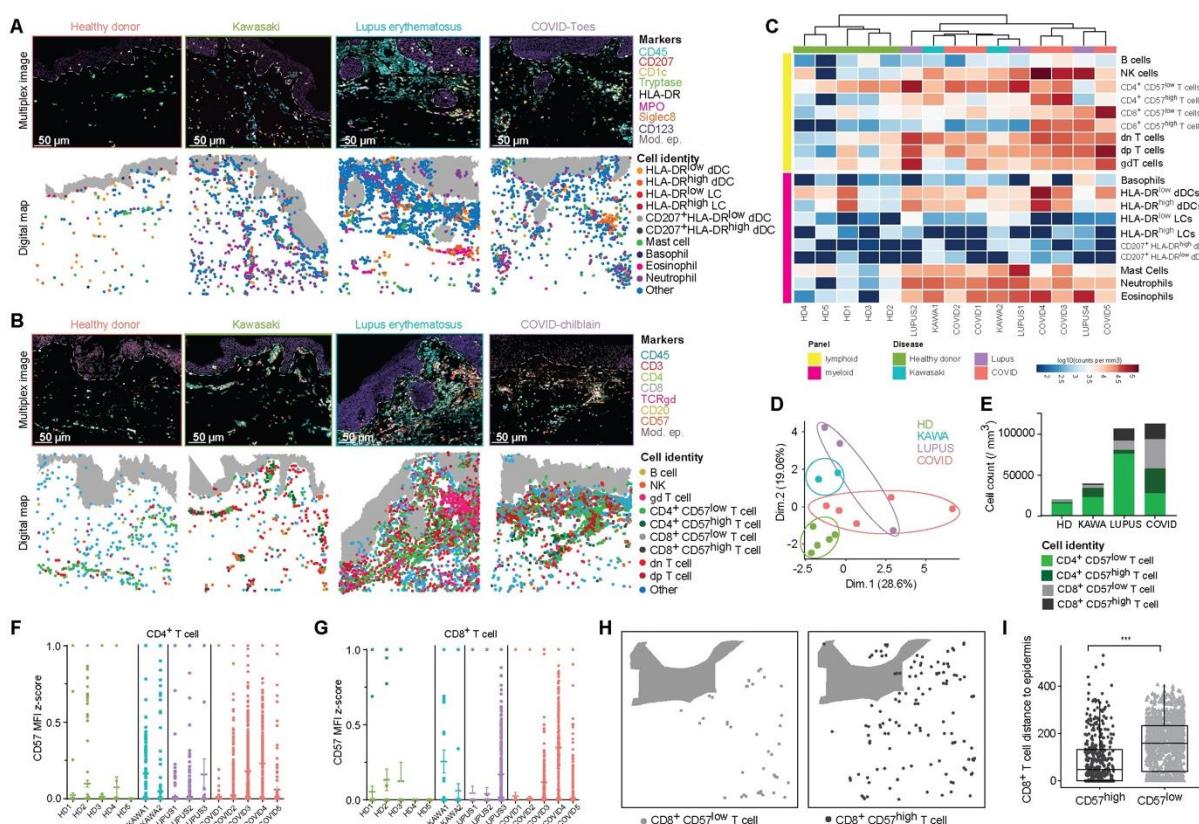
551 aberrations and 3-D fluorescent spectral spillovers. **D**, Representative 3D multiplex image of
552 healthy (upper panel) and pathological SLE (lower panel) skin sample for lymphoid panel,
553 staining CD45, CD3, CD4, CD8, TCR $\gamma\delta$, CD57 and CD20. **E**, Co-localization of DAPI and
554 CD45 staining and respective RGB profiles. **F**, Segmentation and single-cell database creation.
555 Cell segmentation using the CD45 fluorescence channel allowed efficient isolation of
556 individual objects, i.e., immune cells. Individual object statistics (*xyz* coordinates, sphericity,
557 volume and Mean Fluorescence Intensity) were extracted for each sample.



558

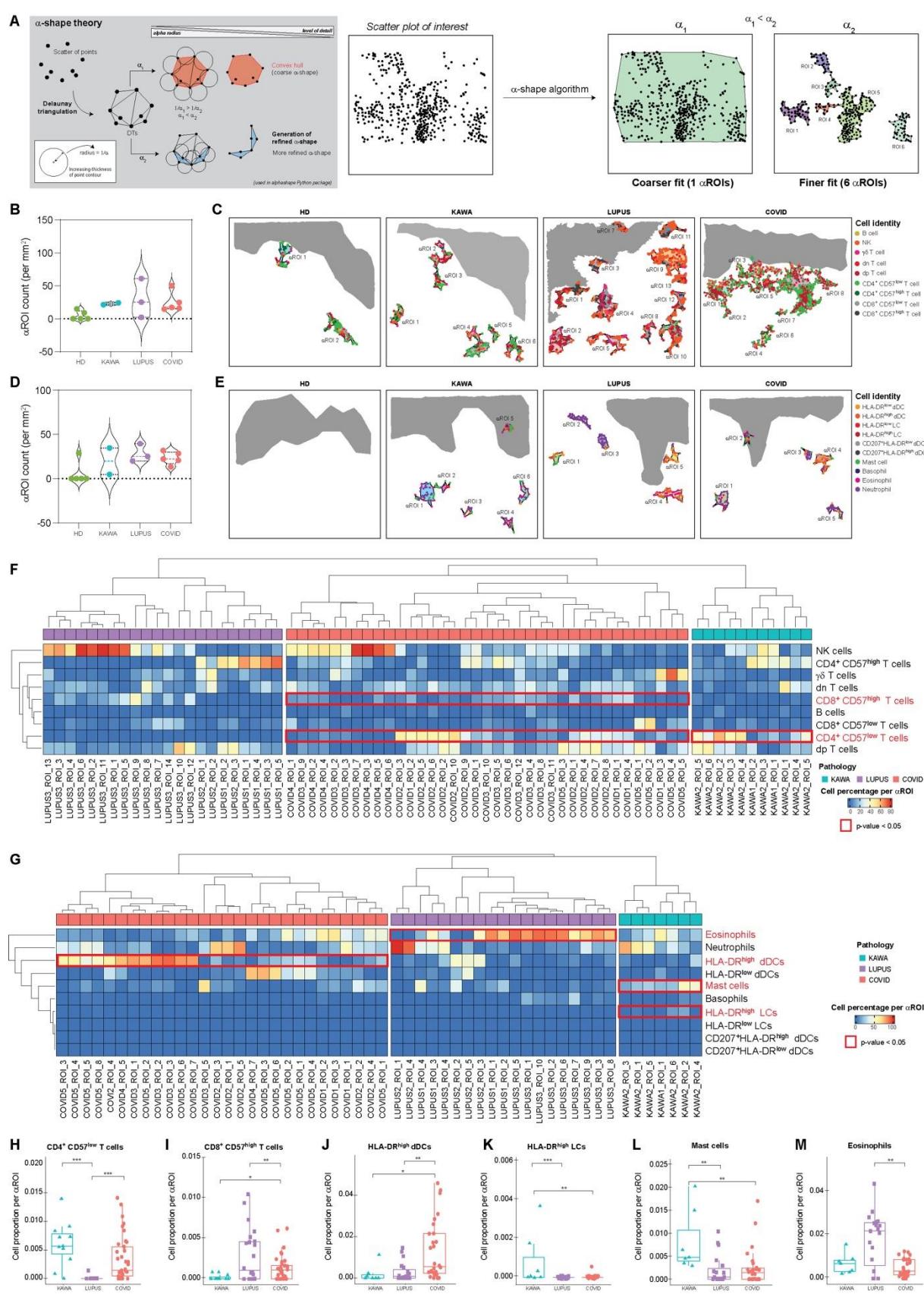
559 **Figure 2. MANTIS algorithm allows automated cell type attribution and interactive**
 560 **exploration of skin myeloid immune topology. A, Automated tissue annotation. A reference**
 561 **attribution matrix defining the literature-based theoretical signature of a particular cell type was**
 562 **constructed and designated as MANTIS attribution matrix. A correlation matrix calculating**
 563 **Spearman coefficient between the single-cell database and MANTIS attribution matrix was**
 564 **computed. Each segmented cell was annotated to the cell type having the highest correlation**

565 coefficient, and cell type proportions were extracted. **B**, Single-cell staining of all used
566 biomarkers in identified myeloid cells. **C**, MANTIS simplified attribution matrix for myeloid
567 panel. **D**, Tissue annotation and cell proportion of pathological (SLE) skin. **E**, Representative
568 t-SNE plot of myeloid cell populations (upper panel) and MFI levels of used markers (colored
569 intensity scale, lower panel). **F**, Representative 3D confocal multiplex image (upper panel) and
570 associated digital map (lower panel) of pre-designed MANTIS myeloid panel of pathological
571 (SLE) skin. **G**, Interactive reverse-gating. A population of interest (neutrophils) was selected
572 on the tSNE plot. Recomputation of the corresponding digital map enabled the visualization of
573 the anatomical distribution of this particular population in the skin biopsy.



574

575 **Figure 3. 3-D quantitative and spatial analysis of skin immune cells at the cellular level**
 576 **provide insight into disease signatures. A, B, Representative 3-D confocal multiplex images**
 577 **(upper panel) and associated digital maps (lower panel) of pre-designed MANTIS myeloid (A)**
 578 **and lymphoid (B) panels of healthy and pathological skin. C, Representative heatmap of**
 579 **lymphoid and myeloid cell densities in logarithmic scale with hierarchical clustering. D,**
 580 **Principal Component Analysis (PCA) of immune signatures of healthy and diseased skin. E,**
 581 **Cell count per mm³ of CD57^{low} and CD57^{high} T cells. F, G, Dotplot of CD57 Mean Fluorescence**
 582 **Intensity (MFI) z-score in CD4⁺ (F) and CD8⁺ (G) T cells in healthy and diseased skin. H, I,**
 583 **Representative digital map (H) and mean distance to epidermis (in µm [I]) of CD8⁺ CD57^{low}**
 584 **(left panel) and CD57^{high} (right panel) T cells in COVID skin lesions.**



585

586 **Figure 4. Automatic detection of α -regions of interest (aROI) enables exploration of**
 587 **inflammatory cluster topography in healthy and diseased skin. A, Alpha shape algorithm.**

588 Delauney triangulation of a given set of points formed a bounding polygon that contains all the
589 points of the set. The alpha parameter was defined by the value α , and a circle with $1/\alpha$ radius
590 was drawn around each point of the dataset. The line between two circles meeting points formed
591 a side of the bounding polygon, i.e., the alpha shape. α value defines the detail level of the alpha
592 shape and allows modeling of voluminous structures ($1/\alpha_1$) or smaller structures ($1/\alpha_2$) having
593 $1/\alpha_1 > 1/\alpha_2$. **B, C**, Violin plot (B) and representative digital maps (C) of lymphoid α -ROI density
594 in healthy and pathological skin. **D, E**, Violin plot (D) and representative digital maps (E) of
595 myeloid α -ROI density in healthy and diseased skin. **F-K**, Mean proportion of $CD4^+ CD57^{\text{low}}$
596 T cells (F), $CD8^+ CD57^{\text{high}}$ T cells (G), HLA-DR^{high} dDCs (H), HLA-DR^{high} LCs (I), mast cells
597 (J) and eosinophils (K) per α ROI in diseased skin. Mean \pm SEM; *P<0.05, **P<0.01,
598 ***P<0.001 One-way ANOVA (F-K). **L, M**, Representative heatmaps of cell proportions in
599 lymphoid (L) and myeloid (M) α ROIs in pathological skin. A hierarchical clustering was
600 applied on rows and on each pathology's column.

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