

Reversible and gain modulation of neuronal responses and sensorimotor behavior by mid-infrared stimulation

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23 **Abstract**

24 Neuromodulation serves as a cornerstone for brain sciences and clinical applications. Mid-infrared
25 stimulation (MIRS) has been recently reported to cause non-thermal modulation of brain functions.
26 However little knowledge of mechanisms hampers its application. Here we bridge across ion
27 channels, neuronal signals, and behavioral performances associated with sensorimotor
28 transformation to provide evidence of how the alternation of neuronal activity by MIRS guides the
29 change of behavioral performance in awake-behaving pigeons. We compared effects on visually-
30 guided eye movements by applying MIRS and electrical stimulation (ES) in the pretectal nucleus
31 lentiformis mesencephali (nLM). Distinct from ES, we found a specific gain modulation of MIRS
32 to alter behavior in a manner of the strength of visual inputs. Our simultaneous extracellular
33 recordings showed that MIRS can excite and inhibit the neuronal activity in the same pretectal
34 neuron based on its ongoing sensory responsiveness levels in awake-behaving animals. We further
35 applied computational simulations and found that MIRS can modulate the carbonyl group (-C=O)
36 enriched on the potassium channel to resonate, and could affect action potential generation, alter
37 neuronal responses to sensory inputs and then guide behavior. Our findings suggest that MIRS
38 could be a promising approach for brain researches and neurological diseases, with gene free
39 manipulation.

40

41 **Introduction**

42 Neuromodulation has long been employed to treat patients with brain disorders and answer
43 scientific questions on brain functions. It is consistently growing and evolving with innovations in
44 technology. Deep brain stimulation, and transcranial electromagnetic stimulation are thought to
45 effectively activate neuronal excitability and connectivity, and are applied commonly in clinical
46 treatments. Optogenetic stimulation shows power to selectively excite and inhibit specific groups
47 of neurons, but the genetic manipulation limited its clinical applications (Deisseroth, 2015). It
48 would be of great significance to clinical setting and neuroscience research if a neuromodulation
49 achieves reliable neural excitation and inhibition, with gene free manipulation.

50 Optical infrared neuronal stimulation is emerging as a potential neuromodulation because of the
51 ability to deliver focused energy through tissue even without direct contact. Initial studies showed
52 that near-infrared wavelength stimulation (NIRS) could excite neuronal responses *in vitro* (Izzo,
53 et al., 2008; Albert, et al., 2012; Shapiro, et al., 2012; Entwistle, et al., 2016) and *in vivo* (Wells, et
54 al., 2005; Wells, et al., 2007a; 2007b; Richter, et al., 2008; Xia, et al., 2014). Interestingly, there
55 are also limited cases observed that NIRS could inhibit neuronal firing (Cayce, et al., 2011; Duke,
56 et al., 2012; Duke, et al., 2013; Horváth Á, et al., 2020). Recently, there are rising evidence shed
57 light on that mid-infrared stimulation (MIRS) with a specific wavelength could lead to dramatic
58 changes: 1) *neuronal firing*. MIRS can exert non-thermal effects on ion channels, and lead to gain
59 modulation of action potentials based on current injections *in vitro* brain slices (Liu, et al., 2021).
60 MIRS can enhance neuronal spontaneous activities (Zhang, et al., 2021) and sensory responses
61 (Tan, et al., 2021) in anesthetized animals. 2) *behavioral performance*. MIRS can effectively
62 modulate behavior by accelerating associative learning in mice (Zhang, et al., 2021), and
63 regulating startle responses in larval zebrafish (Liu, et al., 2021). Although our understanding of

64 how MIRS neuromodulation impacts the brain is evolving, it is still left vacant to demonstrate how
65 MIRS alters *neuronal firing* in brain network, and then how the alternation guides *behavioral*
66 *performance* for lack of simultaneous recording in awake-behaving animals.

67 In this research, we aim to bridge across cellular and behavioral phenomena to provide evidence
68 of how alternations of neuronal activity by MIRS regulate behavioral performances in awake-
69 behaving pigeons. When birds fly, surrounding environment generates a large field of visual
70 motion across the entire retina, known as “optic flow” (Gibson, 1951). Their eyes reflex produce
71 optokinetic nystagmus (OKN) to maintain stabilization of image on the retina. OKN combines a
72 close tracking of a moving field by pursuit eye movement in slow phases, and a rapid resetting
73 back by saccadic eye movement in fast phases, producing a characteristic irregular sawtooth
74 waveform. In birds, the pretectal nucleus lentiformis mesencephali (nLM, homologous to the
75 nucleus of the optic tract) (Fite, 1985; McKenna and Wallman, 1985) is an essential encoder to
76 process horizontal visual information (Winterson and Brauth, 1985; Wylie and Frost, 1996; Fu, et
77 al., 1998; Wylie and Crowder, 2000; Cao, et al., 2004; Wylie, et al., 2018) and generate OKN eye
78 movements (Fite, et al., 1979; Burns and Wallman, 1981; Gioanni, et al., 1983; Cao, et al., 2006;
79 Yang, et al., 2008a; 2008b; Wylie, 2013; Ibbotson, 2017; Gutierrez-Ibanez, et al., 2018). Majority
80 of nLM neurons become excited by visual motion in the temporal-to-nasal direction and prefer
81 slow velocity, whereas other neurons are predominantly sensitive to the nasal-to-temporal, or
82 vertical motion. It transfers visual information from retina directly to multiple brain areas for
83 perception and motor control during self-motion, oculomotor and others (Cao, et al., 2006; Yang,
84 et al., 2008b; Wylie, 2013; Ibbotson, 2017; Wylie, et al., 2018).

85 In this study, we applied MIRS in the pretectal nLM and revealed neuromodulation effects in
86 awaking-behaving pigeons by evidence for several phenomena. First, we found a reversible and

87 gain regulation of pursuit velocity of OKN eye movements depending on the strength of visual
88 inputs. Second, we simultaneously recorded neuronal activities in the pretectal nLM, and found
89 that MIRS could facilitate and suppress firing activity based on levels of neuronal responses. Third,
90 we have applied computational simulations and found MIRS could preferentially enhance
91 potassium permeability through K^+ channels to alter action potential generation, which would
92 modulate neuronal signals in brain network and guide sensorimotor responses.

93

94 **Results**

95 **MIRS exerts gain modulation of pursuit depended on the strength of visual inputs**

96 We introduced a large-field grating motion to pigeons. Vision-evoked OKN eye movements were
97 recorded before, during and after ~120sec MIRS application in the left pretectal nucleus (Fig. 1A-
98 C). When pigeons viewed a grating motion of 8 deg/s in the temporo-to-nasal (T-N) direction (Fig.
99 1D top plots), they closely pursued moving gratings (Fig. 1E; velocity: 4.88 ± 0.29 deg/s; duration:
100 1.89 ± 0.26 s; amplitude: 8.44 ± 1.06 deg; mean \pm SEM, n=10) along the T-N direction, and then
101 quickly saccade back to reset eye position. Once MIRS was turned on, animals significantly fasted
102 their pursuit performances (velocity: 7.16 ± 0.60 deg/s; Wilcoxon signed-rank test, $p < 0.01$), but
103 kept similar pursuit durations and distances (duration: 1.71 ± 0.26 s; amplitude: 8.66 ± 0.95 deg,
104 $p > 0.05$). Conversely, when pigeons were introduced a grating motion of 8 deg/s in the nasal-to-
105 temporal (N-T) direction (Fig. 1D, bottom plots), animals tracked grating motion with far less
106 effective pursuit eye movements (Fig. 1E; velocity: -0.89 ± 0.09 deg/s; duration: 2.95 ± 0.47 s;
107 amplitude: -1.80 ± 0.16 deg). When MIRS was turned on, animals again significantly fasted their
108 eye movements to pursue in the N-T direction (velocity: -1.44 ± 0.09 deg/s; Wilcoxon signed-rank
109 test, $p < 0.01$), without significant changes in pursuit durations and distances (duration: 2.75 ± 0.39 s;
110 amplitude: -2.22 ± 0.22 deg, $p > 0.05$). There was asymmetry between the N-T and T-N OKN,
111 which has been widely observed in lateral-eyed vertebrates (rabbits: Collewijn, 1969; pigeons:
112 Zolotilina, et al., 1995 rats: Harvey, et al., 1997; mice: Kodama and du Lac, 2016). Although there
113 were massive asymmetric sensorimotor responses, MIRS significantly facilitated pursuit velocities
114 in slow phases evoked by 8 deg/s grating motion along both T-N and N-T directions, in the
115 individual and group animals.

116 Next, we conducted ES experiments with a classic frequency used in deep brain stimulation as a
117 comparative research. Similarly, a grating motion of 8 deg/s was introduced to pigeons, and a
118 ~120sec ES was applied in the similar way as MIRS (Fig. 1F). Distinct from MIRS, ES effectively
119 deflected eye movements to pursue toward the T-N direction, independent of visual motion
120 directions of the T-N or N-T (Fig. 1F and G, T-N OKN in top plots, before: 4.84 ± 0.12 deg/s; ES:
121 8.19 ± 0.42 deg/s; N-T OKN in bottom plots, before: -0.80 ± 0.14 deg/s; ES: 2.43 ± 0.59 deg/s; mean
122 \pm SEM; Wilcoxon signed-rank test, n=6, p<0.05).

123 To verify differences in the modulation of MIRS and ES, we compared effects of MIRS and ES
124 on pursuit movements of OKN. Pigeons sensitively produced OKN to large-filed grating motions
125 of different directions and velocities, or spontaneously made saccades when they freely viewed
126 stationary gratings (Fig. 2). When the grating moved at a faster velocity of 8 deg/s, MIRS
127 significantly facilitated the pursuit eye movements along the grating motion direction. When the
128 grating moved at a lower velocity of 2 deg/s or kept still (0 deg/s), changes of pursuit velocity by
129 the same MIRS were insignificant (Fig 2A, T-N OKN, before: 1.97 ± 0.05 deg/s; MIRS: 2.15 ± 0.22
130 deg/s; N-T OKN, before: -0.40 ± 0.11 deg/s; MIRS: -0.47 ± 0.11 deg/s; spontaneous saccades, before:
131 -0.09 ± 0.07 deg/s; MIRS: 0.03 ± 0.12 deg/s; Wilcoxon signed-rank test, p>>0.05). The effects of ES
132 on OKN were consistent across different visual conditions: ES deflected pursuit eye movements
133 towards the T-N direction, regardless of the visual motion information (directions or velocities of
134 grating motion) (Fig. 2C, Wilcoxon signed-rank test, p<0.05). We further compared pursuit data
135 that had been normalized to the top 10 trials with highest pursuit velocities before MIRS/ES under
136 each visual condition. This could eliminate individual animal bias from population analysis. Data
137 showed that gain modulation intensity of MIRS on pursuit depended on the strength of visual
138 inputs (Fig. 2B and D): when the visual motion was “faster”, MIRS facilitated the pursuit eye

139 movements of OKN significantly; however, when the visual motion was “slower”, MIRS failed to
140 regulate oculomotor behavior.

141 **MIRS excites and inhibits neuronal responses in the same pretectal neuron**

142 To examine effects of MIRS on neuronal responses, we performed extracellular recording and
143 tested 31 nLM neurons in awake-behaving pigeons before, during and after MIRS irradiation. 16
144 of them increased firing rates to a grating motion in the T-N direction (“preferred direction”), while
145 decreased in the N-T direction (“null direction”). The other 15 neurons showed an opposite
146 direction selectivity. All recorded nLM cells have been modulated by corollary discharge signals
147 during saccadic eye movements (Yang, et al., 2008a): their firing rates were inhibited during
148 saccades. To investigate how nLM neurons coding sensory information to guide pursuit eye
149 movements, we aligned the spiking activity to the onset of pursuit eye movements of OKN. The
150 following data analysis focused on an interval from 0-600 ms after the onset of pursuit. Visual
151 responses of 28 neurons were significantly modified during MIRS (Wilcoxon signed-rank test,
152 $p<0.01$). Among them, only 3 neurons were suppressed firing rates under all conditions tested. We
153 focused on the left 25 pretectal neurons for further data analysis.

154 An example nLM neuron with a preferred direction of N-T was shown in Figure 3. During MIRS,
155 neuronal activities were modified by positive and negative effects linked with excitation and
156 inhibition of visual responses. When the pigeon viewed a grating motion of 8 deg/s in the neuronal
157 preferred direction (N-T), visual responses were excited to 31.09 ± 6.80 spikes/s (mean \pm SD). Once
158 MIRS was turned on, neuronal excitation was further facilitated to 37.95 ± 11.32 spikes/s (Student’s
159 t-test, $p<0.001$, Fig. 3C and E) and fasted pursuit velocity toward N-T direction (Fig. 2A). When
160 the pigeon viewed a grating motion in the null direction (T-N), neuronal responses were inhibited
161 to 26.25 ± 6.73 spikes/s. Interestingly, the same MIRS showed an opposite effect and further

162 significantly enhanced neuronal inhibition to 18.40 ± 6.87 spikes/s (Student's t-test: $p < 0.001$, Fig.
163 3D and F), and speeded up pursuit eye movements to the T-N direction (Fig. 2A). Our data showed
164 positive and negative modulations of neuronal responsiveness occurred in the same recorded
165 neuron, depending on the level of visual responses.

166 Next, we compared neuronal population responses before, during and after MIRS while they were
167 evoked by grating motions of 8 deg/s in preferred or null directions. All tested neurons are excited
168 to their preferred direction (mean firing rates: 55.99 ± 24.02 spikes/s, $n=21$) or inhibited to their
169 null direction (mean firing rates: 28.93 ± 24.19 spikes/s, $n=14$) before stimulations. We defined
170 the ratio of firing rates by normalization to visual responses before MIRS for each cell. Our data
171 suggested that MIRS could significantly facilitate neuronal excitation in the preferred direction
172 and enhance neuronal inhibition in the null direction. These bidirectional effects of MIRS occurred
173 reversibly (Fig. 4A-C, Wilcoxon signed-rank test, $p < 0.01$).

174 Further, we statically analyzed neuronal activities across population under different visual inputs.
175 Pretectal nLM neurons' firing rates can be evoked to different responsiveness by grating motions
176 at 2 or 8 deg/s in preferred and null directions: when the grating motion speeded up from 2 deg/s
177 to 8 deg/s in preferred or null directions, visual responses increased from ~ 40 to ~ 55 spikes/s or
178 decreased from ~ 25 to ~ 15 spikes/s (Our unpublished data, also reported by (Cao, et al., 2004)).
179 Visual inputs evoked neuronal initial discharges at different levels of high- or low-frequency. The
180 percentage change of visual responses was correlated with the strength of visual inputs, even in
181 individual neurons (Fig. 4D, each gray line presents the same tested neuron). When the grating
182 moved at a higher velocity of 8 deg/s in the preferred direction, the percentage change of visual
183 responses by MIRS ($14.31\% \pm 2.10\%$, $n=21$) was larger than ones when the grating moved at a
184 lower speed of 2 deg/s ($0.84\% \pm 4.62\%$, $n=7$) and in null direction ($-14.86\% \pm 2.32\%$, $n=6$ for 2

185 deg/s, Wilcoxon rank-sum test, $p < 0.01$; $-18.81\% \pm 4.43\%$, $n=14$ for 8 deg/s; Wilcoxon rank-sum
186 test, $p << 0.01$). These results supported that MIRS exerts gain modulation of neuronal signals, in a
187 manner that is itself sensory responses dependent.

188 **MIRS preferentially regulates permeation of K^+ channels**

189 To explore the potential molecular mechanism underlying the gain modulation of neuronal
190 responses by MIRS, we constructed models of voltage-gated K^+ and Na^+ channels. Recently,
191 models of biomimetic ion channels have been widely used to investigate the translocation events
192 of K^+ and Na^+ ions (Long, et al., 2005; Zhang, et al., 2012). In our model (Supplementary Fig. S1),
193 we constructed K^+ channels containing the whole protein placed at the middle of phospholipid
194 bilayer (DPPC molecules) to separate water and ions on each side, in which the model could
195 provide a more authentic and informative simulation of the function of MIRS on ion channels. We
196 started to define the absorption spectrum of ion channels to MIRS based on classical molecular
197 dynamics (MD) method. The MD simulation showed a remarkable absorption finger of K^+
198 channels located between 30 to 40 THz, while just out of the strong absorption spectral ranges by
199 water molecules (Heyden, et al., 2010) and Na^+ channels. The specific frequency of 34.88 THz
200 applied in the study was closed to the maximum absorption spectrum, at least within half-height
201 width of the finger (Fig. 5A).

202 The protein structures of K^+ and Na^+ channels were tetramers, consisting of a single chain and
203 include a narrow pore region (i.e. selective filter), playing a decisive role of the permeation
204 efficiency of K^+ and Na^+ ions. Therefore, by considering the calculation requirements of quantum
205 chemistry method, we further simplified the ion channel structure into a filter model. We identified
206 the specific absorption modes of ion channels during MIRS (Supplementary Fig. S2) according to
207 the filter structure extracted from the model of K^+ and Na^+ channels, the intrinsic spectrum was

208 further calculated by using Gaussian 09 software based on density functional theory (DFT) at
209 B3LYP/6-31G(d) level. It needed to be noted here that the absorption finger of $-\text{OH}^-$ groups at
210 the filter region of Na^+ channels are distant from ~ 34.88 THz (Supplementary Fig. S2), indicating
211 that MIRS was mainly absorbed by $-\text{C}=\text{O}$ groups at the inner wall of the filter region of K^+
212 channels. These data demonstrated that the effect of MIRS with 34.88 THz could enhance the
213 resonance absorption of K^+ channels: the $-\text{C}=\text{O}$ groups are frequency-sensitive due to their
214 collective resonance to the K^+ channels, while these effects seldom occurred in Na^+ channels or
215 water molecules.

216 In response to a signal, neurons emit action potentials mainly generated by the ion permeability
217 events of sodium ions through Na^+ channels and potassium ions through K^+ channels. To compare
218 the modulation of neuronal electrical activity by MIRS, we computed potential of mean force
219 (PMF) as potential energy needed to cross configurations during ion permeability (Bernèche and
220 Roux, 2001; Li, et al., 2021). By applying identical computational methods, the PMF before MIRS
221 showed a higher potential energy at the entrance than at the exit of selectivity filter for both K^+
222 channels and Na^+ channels (blue lines in Fig. 5B and C). It implied that potassium ions and sodium
223 ions could permeate the selectivity filter with comparable energetic potential. A further MD
224 simulation showed that the potential energy difference of potassium ions through the filter became
225 enlarged dramatically during MIRS, while the energy of sodium ions changed slightly through the
226 filter configuration of Na^+ channels (red lines in Fig. 5B, C). This indicated a selectively enhanced
227 K^+ permeability. To statically characterize the effect on ion permeability by MIRS, we defined the
228 PMF ratio of $\Delta P_{\text{MIRS}} / \Delta P_{\text{before}}$ (ΔP_{before} , ΔP_{MIRS} represent for the case before and during MIRS)
229 as the change of ion permeability of potassium and sodium ions, respectively. Data showed that
230 MIRS could increase the PMF ratio of K^+ channels about 1.4-fold at the site around $\xi = 1.1$ nm,

231 while the ratio of Na^+ channels was kept closely to 1 at the site around $\xi = 0.5$ nm. Together, our
232 simulation data demonstrated that MIRS with frequency of 34.88 THz could be selectively
233 absorbed by K^+ channels, and thus improved the efficiency of K^+ permeability, while might not
234 affect Na^+ channels effectively. Therefore, MIRS could have a potential to alter neural discharge
235 activities by selectively and significantly enhancing potassium permeability through K^+ channels.
236

237 Discussion

238 Our study provides several lines of evidence that MIRS could cause reversible and gain modulation
239 on neuronal activity and sensorimotor behavior, by simultaneously recording neuronal and
240 behavioral responses in awaking-behaving pigeons (Fig. 6). Our results showed that MIRS could
241 achieve neuronal excitation and inhibition in the same pretectal neuron and cause gain modulation
242 on pursuit eye movements of OKN. These alternations depended on the level of ongoing firing
243 rates evoked by the directions and velocities of visual motion. Further computational simulations
244 revealed that MIRS may effectively enhance K^+ permeance through the selectivity filter of
245 potassium channels (Fig. 5, 6B). Therefore, MIRS with 34.88 THz could be a specific
246 neuromodulation approach to excite and inhibit neuronal firing and then alter sensorimotor
247 behavior in a manner of the strength of sensory inputs.

248 OKN consists of pursuit eye movements during slow phases tracking in the direction of large-field
249 motions and saccadic eye movements in fast phases resetting back into the opposite direction.
250 OKN responses are highly sensitive to the velocity of visual motion. We found that MIRS applied
251 in nLM induced gain modulations on pursuit eye movements based on the visual motion: MIRS
252 can significantly speed up pursuit eye movements induced by a faster visual grating motion, but
253 failed to significantly modulate pursuit when OKN was evoked by a slower visual grating motion.
254 Note that if the grating was stationary (0 deg/s), pigeons only made spontaneous saccadic eye
255 movements to search surrounding instead of pursuing visual motion, MIRS also failed to initiate
256 any pursuit eye movements. Compared with MIRS, the classical ES in nLM can effectively deflect
257 eye movements toward the T-N direction isolated from directions of grating motion. Even pigeons
258 well pursued a grating motion in the N-T direction or freely searched still gratings without any
259 pursuit, eye movements were deflected and driven to pursuit in the T-N direction immediately

260 once ES applied. Comparison behavioral evidence from MIRS and ES, we found that MIRS could
261 induce gain modulations to regulate oculomotor behavior depending on the strength of sensory
262 inputs.

263 Neuronal circuitry for OKN has been studied for decades. In birds, the pretectal nLM plays
264 complementary roles in encoding vision information of a large-field optic flow and guiding pursuit
265 eye movements in slow phases of OKN (Cao, et al., 2004; Yang, et al., 2008b). Major neurons in
266 the pretectal nLM encoded visual information of horizontal motion (Wylie and Frost, 1996; Wylie
267 and Crowder, 2000). Visual responses of nLM were sensitively tuned by the velocity of grating
268 motion. There were more than half pretectal neurons excited their visual responses to the T-N
269 directional motion and inhibited their firing rates to the N-T directional motion. Once the grating
270 moved from 2 deg/s to 8 deg/s in both preferred and null directions, firing rates of pretectal neurons
271 could be activated at different visual responsiveness levels, emitting neuronal discharges into high-
272 or low-frequency. These paved a fundamental basement to specifically investigate the
273 neuromodulation effects of MIRS according to levels of neuronal visual responses. Our results
274 showed that MIRS can further excite or inhibit neural firing occurred in the same neuron in a
275 manner of its level of visual responses, respectively. Meanwhile, when animals viewed a given
276 grating motion, the same MIRS could facilitate neuronal activity in one nLM neuron and suppress
277 firing rates in the other neuron in a manner that the grating motion excited or inhibited neuronal
278 discharges of that cell. Therefore, MIRS can cause reversible and multiplicative gain modulations
279 on neuronal signals depending on the ongoing levels of visual responses or the strength of sensory
280 inputs, which could follow the rule of “when strong is strong, when weak is weak” (Fig. 6C).

281 Traditional views thought infrared neuronal stimulation could cause local thermal heat by water
282 absorption, which changes capacitance of the transmembrane to excite cells (Shapiro, et al., 2012),

283 or activate thermosensitive TRPV channels to depolarize cells(Albert, et al., 2012). Recently,
284 experimental evidence in *vitro* demonstrated that MIRS with a specific wavelength (5.6 μm) will
285 cause nonthermal effect on ion channels and neuronal functions, especially when the distance was
286 greater than 300 μm . Our evidence from behavioral and neurophysiological results are consistent
287 with the nonthermal effect of MIRS. First, the distance between the MIRS fiber tip and recording
288 sites was kept about $850 \pm 300 \mu\text{m}$ (Fig.1B), which was limited thermal changes within 3°C(Tan,
289 et al., 2021). Second, the modulation of pursuit eye movements by MIRS depends on the sensory
290 inputs, which is not consistent with the thermal effect. MIRS increased pursuit velocities under a
291 grating motion of 8 deg/s. If we assumed it was caused by local thermal heat of MIRS, then this
292 heating effect should keep working to speed up oculomotor behavior when gratings move at lower
293 velocities or keep still. Obviously, behavioral results showed a clear sensory-input depended
294 modulation to against the thermal effect. Third, visual responses of the same recorded neuron can
295 be increased by MIRS only when it was excited by motion in the preferred direction, and decreased
296 by the same MIRS when it was inhibited by motion in the null direction. These positive and
297 negative effects depended on the evoked excitatory or inhibitory visual responses in individual
298 neurons. While we are not able to eliminate the thermal effect induced neuronal activity changes
299 or vasodilation as contributing factors, experimental evidence observed demonstrate consistently
300 that the bidirectional and gain modulation of MIRS on neuronal responses and behavioral
301 performances depends on the strength of sensory inputs (Fig. 6C).

302 The multiformity of ionic channels allows neurons to encode and transfer information by
303 generating action potentials with a wide range of shapes, patterns and frequencies. This process
304 must involve complex interactions with ion channels. A recent research in brain slices found that
305 multiplicative modulations of the action potential generation by MIRS depended on the strength

306 of current pules in *vitro*, and an increase in K^+ currents (not Na^+ currents) could lead to the gain
307 modulation (Liu, et al., 2021). Consistent with previous reports, our ion channel simulations
308 indicated that MIRS can cause the carbonyl group (-C=O) enriched on the K^+ channel selective
309 filter to resonate, thereby decreasing in input resistance and increasing in potassium ion flow,
310 which could also work to modulate neuronal responses to sensory inputs in *vivo* (Fig. 6B).
311 Potassium channels commonly playing a major part in the repolarization of action potentials. The
312 increase in potassium ion flow by MIRS could cause a faster and/or earlier repolarization, and lead
313 to a shortened action potential duration (Supplementary Fig. S3; (Liu, et al., 2021)) and an enlarged
314 afterhyperpolarization. Once there were “stronger” stimuli (i.e. pretectal neurons were excited in
315 the preferred direction in our case), these might cause faster recovery from inactivation of sodium
316 channels (Bean, 2007) and the prior action potential’s refractory period. Then the neuron can be
317 facilitated to initiate a subsequent action potential, which resulting in fastening of high-frequency
318 firing. Once there were “weaker” stimuli (i.e. pretectal neurons were inhibited in the null direction),
319 the raising K^+ permeability might hinder the depolarization and retard the threshold potential of a
320 subsequent action potential, which resulting in slowing of low-frequency firing. Although the
321 computational simulations have not listed a full description from ion channels to generations of
322 action potentials, our data provided evidence that suggest ionic mechanisms underlying MIRS:
323 MIRS could preferentially modify permeation of K^+ channels, leading to alternations of action
324 potential generation in a manner of ongoing firing levels depended on sensory inputs to guide
325 behavioural performances.

326 Distinct from the electrical stimulation that would activate neuronal firing and cause unidirectional
327 deflections in behaviour (Fig. 6D), MIRS produces positive and negative modulations on visual
328 responses in the same neuron, and then lead to gain modulations on behavioral performances (Fig.

329 6C-E). Distinct from the optogenetic stimulation that would require application of light-sensitive
330 genes, our results showed that MIRS could selectively activate or inhibit neuronal responses by
331 controlling the strength of sensory inputs in an individual or population cells, with gene free
332 manipulation. Moreover, our results demonstrated that effects of MIRS occur reversibly in
333 neuronal and behavioral responses in awake-behaving animals. These findings together suggested
334 that MIRS could be used as a promising neuromodulation approach to excite and inhibit neuronal
335 firing in brain researches and clinical applications.

336

337 **Methods**

338 **Animal preparation**

339 We conducted experiments on 16 awake, behaving adult pigeons of either sex (*Columba livia*,
340 body weight: 300-500g). 10 of animals contributed for MIRS experiments combining recording in
341 the pretectal nLM, while 6 of them were used for electrical stimulation experiments. We performed
342 experiments using techniques that have been described in detail before(Yang, et al., 2008a; 2008b;
343 Yang, et al., 2017). Procedures were in accordance with the guidelines for the care and use of
344 animals established by the Society for Neuroscience and approved by the *Institutional Animal*
345 *Administration Committee* at the Institute of Biophysics, Chinese Academy of Sciences.

346 **Visual conditions**

347 A large-field square wave grating was generated by MATLAB program and projected to a screen
348 subtended a visual field of 130° by 140°. The grating consisted equal-width black and white stripes
349 with spatial frequency of 0.16 cycles/degree. The meridians of the visual field were rotated by 38°
350 (Britto, et al., 1990; Fu, et al., 1998) to match pigeons' normal viewing conditions (Erichsen, et
351 al., 1989). Animals produced saccades and OKN when they viewed stationary gratings (0 deg/s)
352 and moving gratings. The grating moved at 2 deg/s and 8 deg/s in the T-N and N-T directions to
353 elicit OKN, respectively (Gioanni, et al., 1983; Yang, et al., 2008b).

354 **Mid-infrared stimulation and Electrical stimulation**

355 The MIRS was performed using a quantum cascade mid-infrared laser (Daylight solution Inc.,
356 model MIRcat) with a radiation wavelength of 8.6 μm, frequency of 34.88 THz, and a power of
357 80 mW. The pulse train was applied for 120 seconds with a mark of 2 μs and a space of 3 μs. An
358 infrared fiber (IRF-S-9, IRflex) with a diameter of 600 μm was used for coupling. The fiber was

359 inserted vertically into the left pretectal nLM. The distance between recording microelectrodes and
360 fiber tips was about $850 \pm 300 \mu\text{m}$ (mean \pm SD, Fig.1 B). There were \sim 10 minute intervals between
361 any two MIRS to get a recovery from the prior stimulation.

362 The ES was generated by an isolated pulse stimulator (A-M Systems, model 2100) and applied for
363 120 seconds in the pretectal nLM, with parameters of 0.2 mA, 100 μs pulse width, 133 Hz(Elias,
364 et al., 2020). The stimulation electrodes were glass-insulated tungsten bipolar electrodes with an
365 exposed tip of 60 μm and a distance of 400 μm between the two tips. The electrodes were advanced
366 into the brain following the same method as optical fibers in the MIRS.

367 **Data acquisition and analysis**

368 *Extracellular recording.* We introduced homemade glass-insulated tungsten microelectrodes into
369 the pretectal nLM, with an impedance of 1-3 $\text{M}\Omega$ (Gioanni, et al., 1983; Yang, et al., 2008b). We
370 amplified extracellular action potentials, filtered them with a bandpass of 300 Hz to 5 kHz (A-M
371 Systems, Model 1800), and digitized at 25 kHz (CED, Power 1401 Cambridge electronic design
372 limited,) for off-line spike sorting (Spike2, Cambridge electronic design limited). At the end of
373 each experiment, recording sites were marked by electrical destruction (positive current of 30-40
374 μA for 20-30 seconds).

375 *Electrooculogram recording (EOG).* Eye position changes were recorded by an electrooculogram
376 system (Wohlschläger, et al., 1993; Yang, et al., 2008a; 2008b), sampled at 2.5kHz and stored
377 simultaneously with neuronal signals. EOG signals were smoothed by a low-pass filter with a cut-
378 off frequency of 5 Hz, and differentiated into eye velocity. For calibration purposes, eye
379 movements were video graphed by an infrared video camera simultaneously with EOG recording

380 (Niu, et al., 2006; Yang, et al., 2008a; 2008b). Eye movement data were defined as positive values
381 for T-N direction and negative values for N-T direction.

382 Eye movements and neuronal spikes were calculated in an interval from 0-600 ms after the onset
383 of pursuit eye movement in OKN. The choice of the interval ensures that our measures are related
384 to the visual response to grating motions during pursuit of OKN. The onset and offset of pursuit
385 eye movement were determined with a customized MATLAB code according to characteristic
386 oscillations in avian saccadic eye movements, and then manually rechecked. Data were excluded
387 if the period of pursuit was shorter than 600 ms, although this probability was negligible under
388 tested visual conditions (Fig. 1E). Neuronal activities were collected before, during and after MIRS
389 for about 120 seconds, and smoothed by a Gaussian Kernel filter with an h value of 25. We defined
390 neuronal firing to be facilitated or suppressed by MIRS if they were significantly higher or lower
391 than activities before MIRS (Wilcoxon signed-rank test, $p<0.05$).

392 **Molecular dynamics simulation**

393 The simulation was carried out to obtain an understanding of the power of ions permeation, and
394 aimed to compare the permeability of K^+ and Na^+ ions during MIRS at nano-scale spatial and
395 femto-second time resolution. Based on the eukaryotic model of voltage-gated K^+ channels (PDB
396 ID: 2a79, Supplementary Fig. S1) (Long, et al., 2005) and Na^+ channels (PDB ID: 4dxw,
397 Supplementary Fig. S2) (Zhang, et al., 2012), respectively. In our simulations, the force field of
398 CHARMM 36 and periodic boundary conditions were used (Mackerell and Nilsson, 2008). The
399 connection element algorithm Ewald was used to deal with the electrostatic interaction (Leeuw, et
400 al., 1980). The Velocity-Verlet algorithm (Andersen, 1983) was performed to solve the motion
401 equation, with the time step of 2 fs. All bond lengths were limited by the Lincs algorithm (Swope
402 and William, 1982). In particular, for K^+ channels, the truncation of Lennard-Jones interaction and

403 the real space part of Ewald sum were 1.90 nm, the convergence factor of Ewald sum was 1.65
404 nm, and the radius of K-space section was 10.4 nm. Meanwhile, for Na^+ channels, the truncation
405 of Lennard-Jones interaction and the real space part of Ewald sum were 1.623 nm, Ewald and
406 convergence factors were 1.65 nm, and the radius of K-space section was 10.4 nm. The process of
407 the ion permeation events was divided into two stages according to before and during MIRS. First,
408 we fixed the phospholipid bilayer and protein (except the filter region of K^+ and Na^+ channels) in
409 the system to research the process of ion permeation through the filter domain under the NVT
410 ensemble at room temperatures 300 K. Second, to combine effects of the electromagnetic wave on
411 the ion channel, MIRS with frequency of 34.88 THz was added into the whole simulation system
412 (Wu, et al., 2020). The intensity ratio of the electromagnetic component of an electromagnetic
413 wave is equal to the speed of light. In the formula:

414
$$E(t) = A * u * \cos(\omega t + \varphi) \quad (1)$$

415 where A represented the maximum amplitude of the electric field to determine the electric field
416 strength of electromagnetic wave, and u and φ represented the polarization direction and phase,
417 thus set to (0, 0, 1) and 0 respectively. The electromagnetic wave frequency was computed as a
418 function of the angular frequency ω by the equation $\gamma = \omega/2\pi$. The total time was ~ 10 ns, and the
419 trajectory is saved every 0.1 ps for subsequent data analysis.

420 We simulated the absorption spectrum of K^+ and Na^+ channels by using molecular dynamics
421 methods based on the classical GROMACS package (Abraham, et al., 2015)(Fig. 5A). The
422 absorption spectrum was calculated according to the Fourier transform of the velocity
423 autocorrelation function of the total charge current of our simulation systems (Heyden, et al., 2010).
424 We set the time interval of spectrum sampling as 1 fs, and the total time of sampling as 50 ps. The

425 absorption spectra were calculated based on the Fourier transform of the autocorrelation function
426 of the total charge current (Heyden, et al., 2010):

427
$$J(t) = \sum_i q_i v_i(t) \quad (2)$$

428 where q_i represented the charge of the i -th atom, and $v_i(t)$ stood for the velocity of the i -th atom at
429 time t .

430 We further simulated the potential of mean force (PMF) as potential energy needed to cross
431 configurations during ion permeability (Bernèche and Roux, 2001; Li, et al., 2021)(Fig. 5B and
432 C). Umbrella sampling (US) is a method that a series of initial configurations are sampled along a
433 reaction coordinate defined between two groups, then we simulated in the group of K^+/Na^+
434 harmonically restrained against the other fixed group via an umbrella biasing potential. Initially, a
435 K^+ or Na^+ ion was placed in the z direction at the entrance of the selectivity filter. The Cl^- ion was
436 in line with the center of the protein channel. It was initially frozen and taken as the reference
437 group. The simulated K^+ or Na^+ ion was pulled by a force constant of 2000 kJ/mol/nm^2 along the
438 filter for 1.5 ns at a pulling rate of 0.01 \AA per ps. All residues of filter were set flexible during
439 pulling. The initial configurations for the US simulations were extracted from the pulling process
440 at an interval of approximately 0.2 \AA (COM distance between the reference Cl^- ion and the
441 simulated K^+ or Na^+ ion) along the ion conductance path. Pressure equilibration was carried out
442 for 1.0 ns for all sampled windows, followed by 3.0 ns trajectory generation for a reliable PMF
443 calculation. In each umbrella sampling simulation, the simulated ion was restrained harmonically
444 with a force constant of 5000 kJ/mol/nm^2 along the z -axis. During the US process, the protein
445 (except for the key SF residues) was restrained, so the shift of the whole protein due to system
446 thermal and pressure fluctuations can be negligible. The free energy profile was calculated with
447 the WHAM method implemented in GROMACS based on the US data.

448 In general, the critical factor to determine the permeability of ions concern to the filter region of
449 ion channels (Kopec, et al., 2018). The selective filter of K⁺ channels composed of 24 residues
450 (sequence index of 75~80) (Long, et al., 2005), and 12 residues for Na⁺ channels (sequence index
451 9~11) (Zhang, et al., 2012). According to the filter structure extracted from the model of K⁺ and
452 Na⁺ channels, the intrinsic spectrum was further calculated by using Gaussian 09 software (Frisch,
453 et al., 2009) based on density functional theory (DFT) at B3LYP/6-31G(d) level (Zhang, et al.,
454 2012), thus to explore the specific absorption modes of ion channel during MIRS (Supplementary
455 Fig. S2).

456

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465

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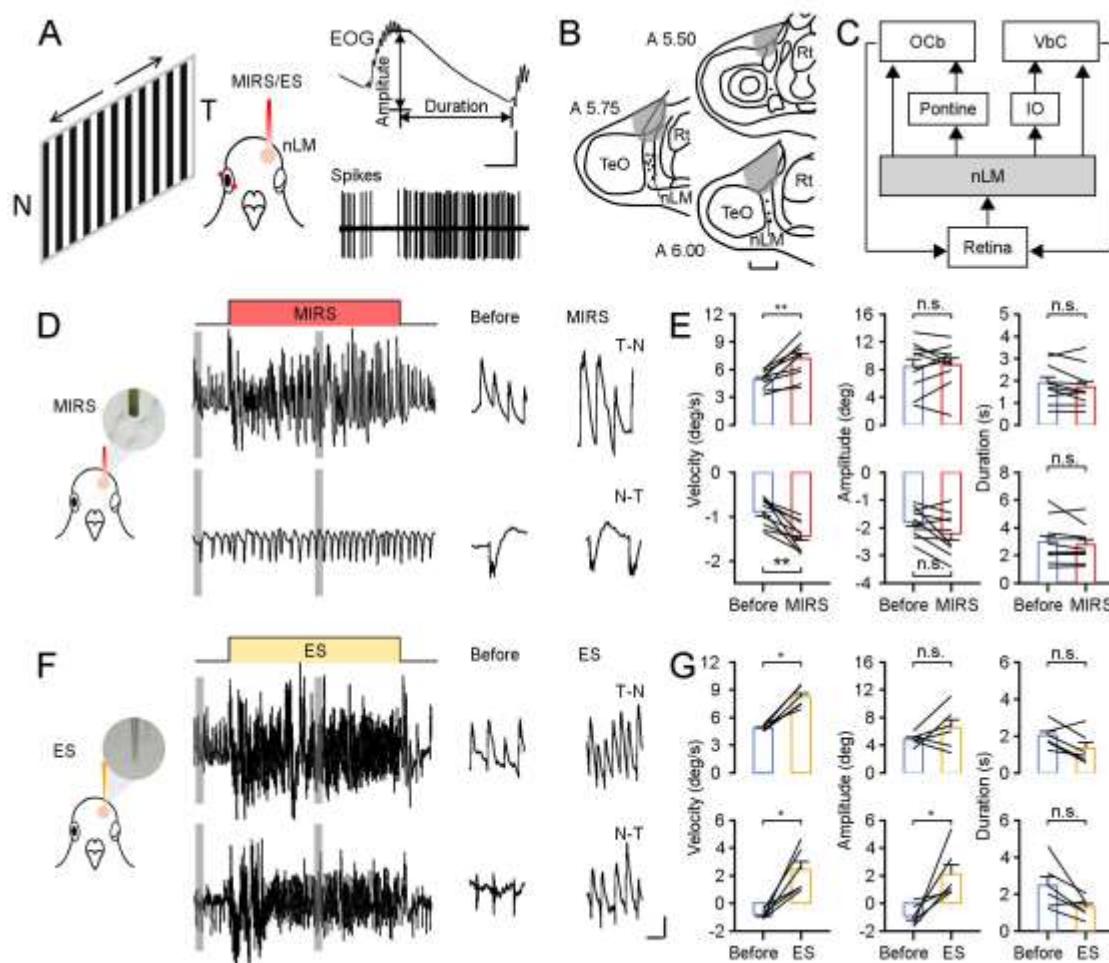
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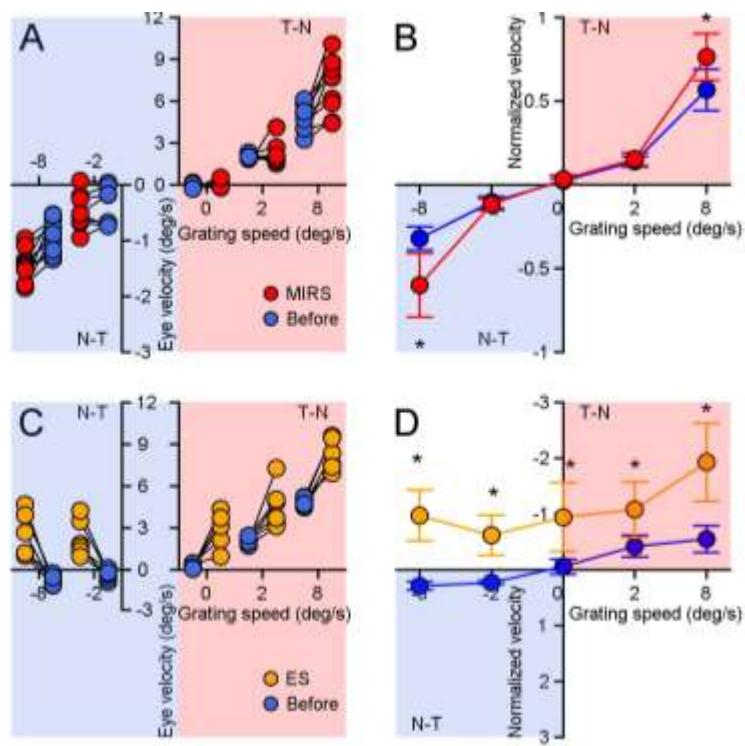
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641 **Figure 1. Modulation of sensorimotor behavior by MIRS in pigeons.** **A:** Schematic drawing of
642 neuronal activities and behavioral performances recording system, with visual stimuli of grating
643 motions (T-N and N-T direction), from top to bottom: EOG traces of OKN, and action potentials
644 of an example nLM neuron. **B:** Marked recording sites (dots) and MIRS/ES sites (gray shading)
645 in the prethalamic nLM cross brain sections under study (A 5.5-6.0). **C:** Optic flow pathways from
646 nLM to the cerebellum for generation of OKN in birds. Abbreviations are: OCb, ocularmotor
647 cerebellum; VbC, vestibular cerebellum; IO, inferior olive; nLM, the prethalamic nucleus lentiformis
648 mesencephali. **D, F:** MIRS (**D**) and ES (**F**) modulated OKN eye movements based on grating
649 motion directions in example animals (top to bottom traces: T-N and N-T direction motion). **E, G:**
650 Comparison of pursuit eye movement parameters to T-N and N-T grating motion (top and bottom
651 plots) before and during MIRS (**E**, n=10) and ES (**G**, n=6). * P<0.05, ** P<0.01, Wilcoxon signed-
652 rank test. Error bars represent SEM. Black lines represent data from individual animals. Scale bars
653 in A: 0.3s, 12deg; B: 1mm; D and F: top-left 12s, 4deg; top-middle and top-right, 2s, 4deg; bottom-
654 left 12s, 1deg; bottom-middle and bottom-right, 2s, 1deg.

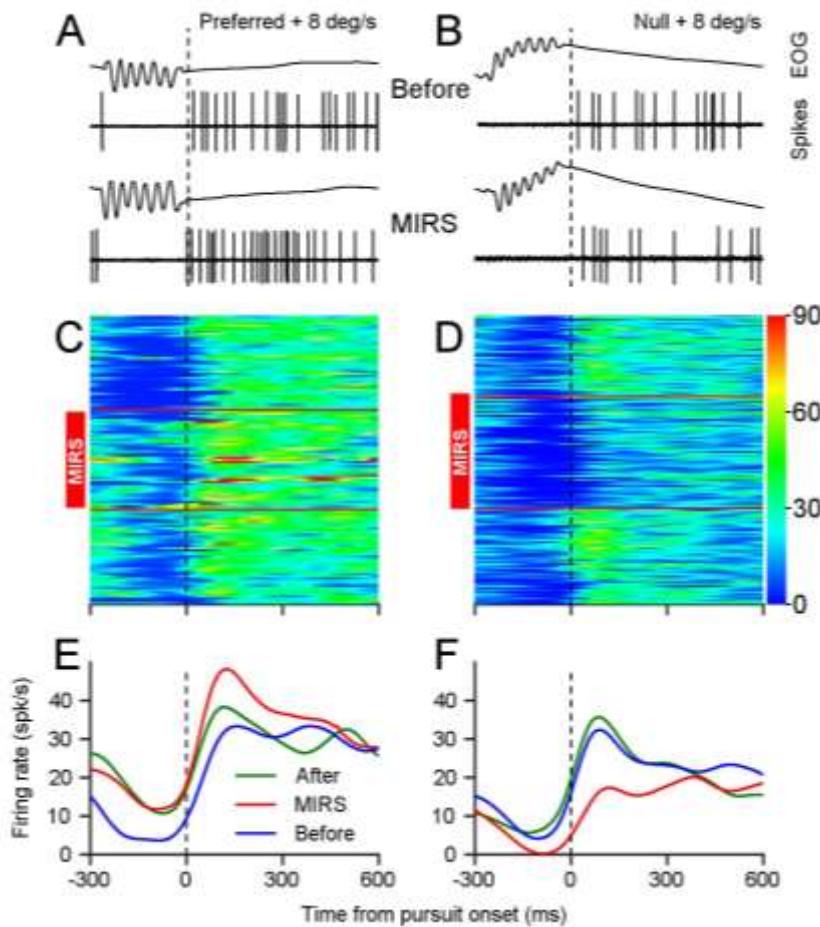
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656 **Figure 2. Comparison of modulation effects by MIRS and ES on OKN eye movements under**
657 **different directions and velocities of grating motions. A, C: MIRS(A) and ES(C) modulated**
658 **pursuit eye velocities based on grating motions. Black lines show data from individual animals**
659 **(blue symbols: before stimulation; red symbols: during MIRS; yellow symbols: during ES). B, D:**
660 **Pursuit eye velocity data had been normalized to average values from the top 10 trials with highest**
661 **peak velocities before MIRS(B) and ES(D) under each visual input. Wilcoxon signed-rank test, ***
662 **P<0.05. Error bars represent 1 SEM.**

663

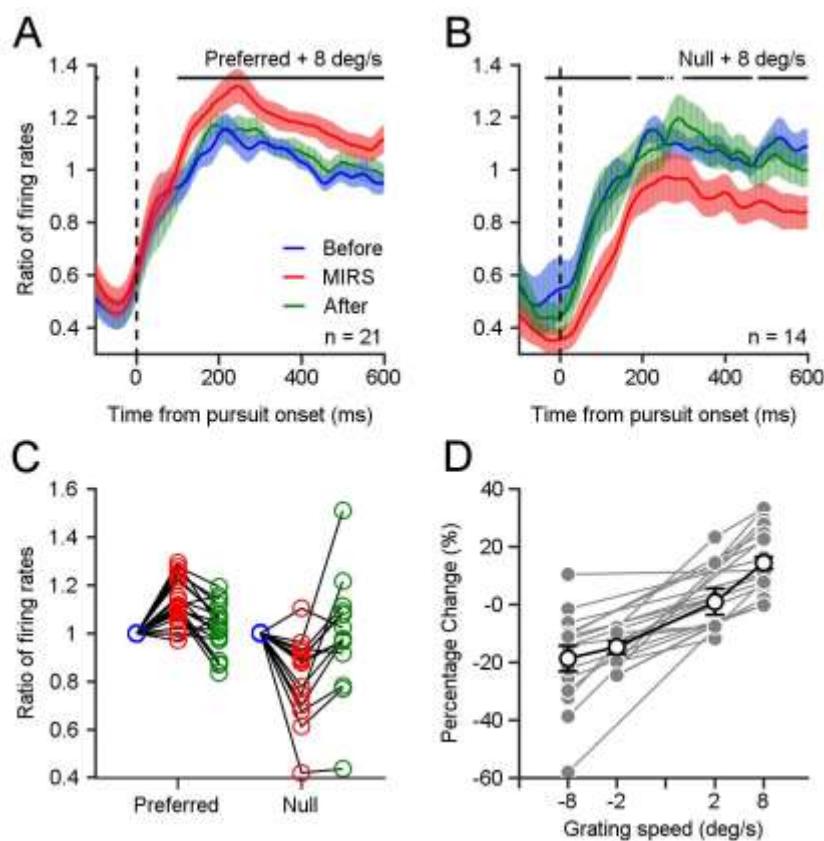
664



665 **Figure 3. MIRS exerts positive and negative modulation of visual responses during pursuit**
666 **in slow phases of OKN in an example nLM neuron. A, B:** Representative eye movements and
667 spiking responses to grating motion at 8 deg/s in the preferred (A) and null direction (B) of an
668 example neuron. From top to bottom: EOG traces of OKN, and action potentials of the neuron
669 before and during MIRS. **C, D:** Visual responses of the cell before, during and after MIRS are
670 color-coded with a scale (spikes/s) on the right. MIRS facilitated neuronal excitation during pursuit
671 to grating motion in preferred direction (C). The same MIRS enhanced neuronal inhibition during
672 pursuit to grating motion in null direction in the same neuron (D). Each horizontal colored line
673 shows neuronal firing rates during pursuit in one OKN. Red horizontal lines show the period of
674 MIRS application. **E, F:** Mean firing rates of the example cell, as a function of time from the onset
675 of pursuit. Blue, red and green traces show data obtained before, during and after MIRS,
676 respectively.

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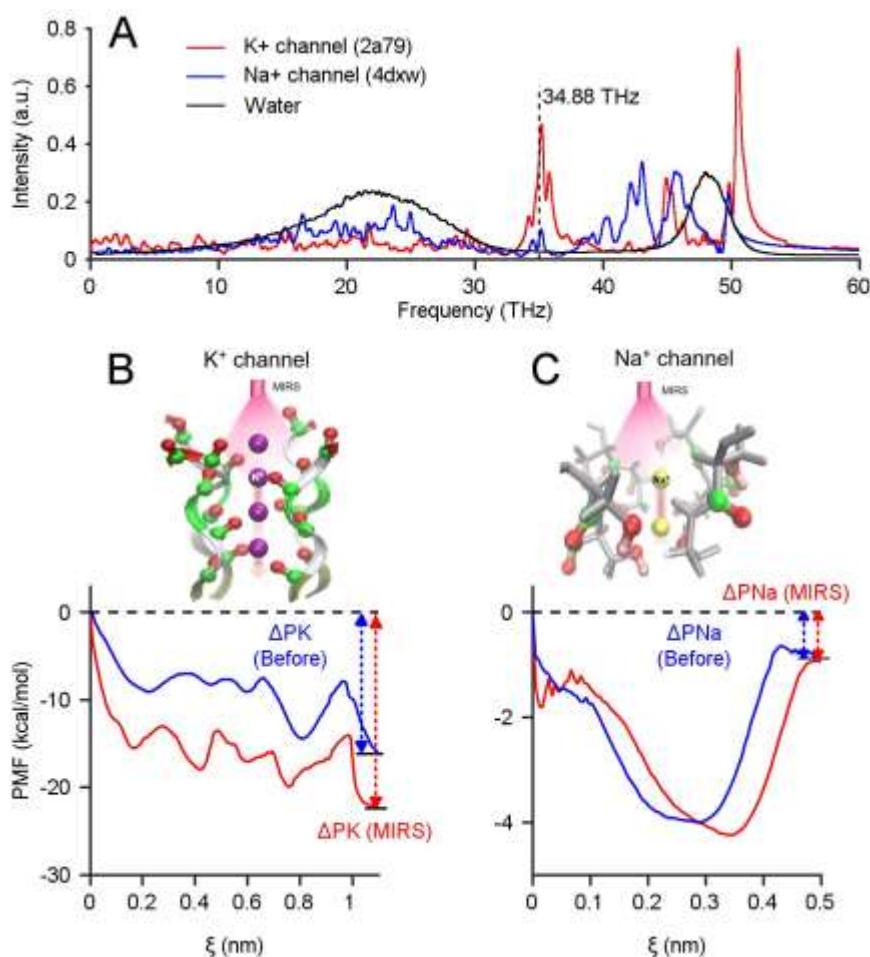
678



679 **Figure 4. MIRS alters sensory coding in pretectal neurons associated with the level of visual**
680 **responses. A, B:** Comparison of neuronal population responses before, during and after MIRS
681 while neurons were evoked by grating motions of 8 deg/s in the preferred (A) and null (B)
682 directions. Data during and after MIRS were normalized to neuronal firing rates before stimulation.
683 Black stars on the top showed that MIRS significantly increased(A) and decreased(B) neuronal
684 responses (Wilcoxon signed-rank test, * P<0.05). **C:** Ratio of neuronal responses in A and B
685 showing the effect of MIRS in preferred and null directions. Black lines show data from individual
686 neurons. Blue, red and green symbols show data from before, during and after MIRS. **D:** The
687 percentage change of visual responses across populations was correlated with the strength of visual
688 inputs. Gray symbols and lines show data from individual neurons. Open symbols with black line
689 show the average across populations. Error bars represent 1 SEM.

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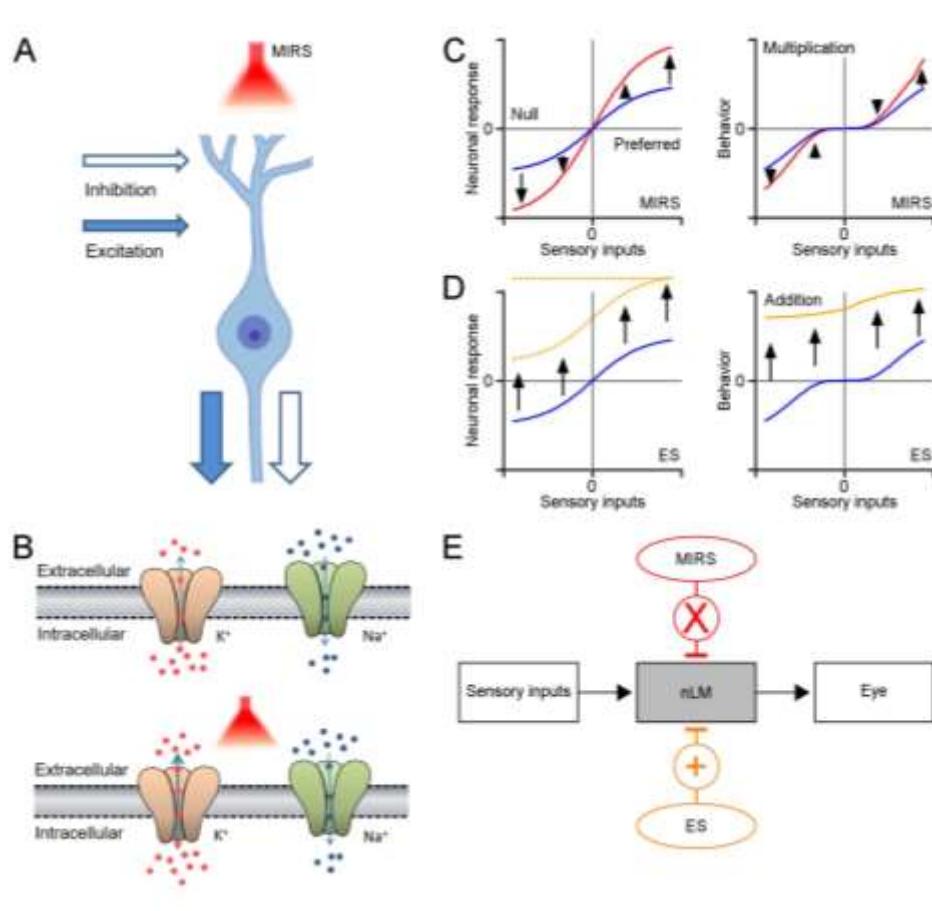
691



692 **Figure 5. Computational simulations reveal preferential regulation of K⁺ channels by MIRS.**
693 A: Absorption spectra of K⁺ and Na⁺ channels were calculated by using molecular dynamics
694 simulation, respectively. The vertical dashed line of 34.88 THz was closed to the maximum
695 absorption finger located between 30 to 40 THz, at least within half-height width of the finger. B,
696 C: The potential of mean force (PMF) of K⁺ and Na⁺ ions permeate through ion channels, before
697 and during MIRS with frequency of 34.88 THz (blue and red lines), respectively. The field strength
698 was E₀=2.5 V/nm.

699

700



701 **Figure 6. Schematic diagrams showing modulations of MIRS and ES suggested by our data.**
702 **A:** MIRS produces positive and negative modulations on visual responses in the same pre-tectal
703 neuron. **B:** MIRS preferentially regulates permeation of K⁺ channels, instead of Na⁺ channels. **C:**
704 MIRS exerts multiplicative gain modulations on neuronal responses to sensory and behavior
705 performances, suggested by our experimental data. Blue and red lines present neuronal and
706 behavior responses before and during MIRS. **D:** ES could exert additive modulations on neuronal
707 firing, and cause unidirectional deflections in behaviour in our results. Blue and yellow lines
708 present neuronal and behavior responses before and during ES. Dashed lines present the possible
709 changes in neuronal firing by ES suggested by prior researches. **E:** Summary of different effects
710 of MIRS and ES on sensorimotor transformation: gain modulation by MIRS, and additive
711 modulation by ES.
712

Supplementary Figures:

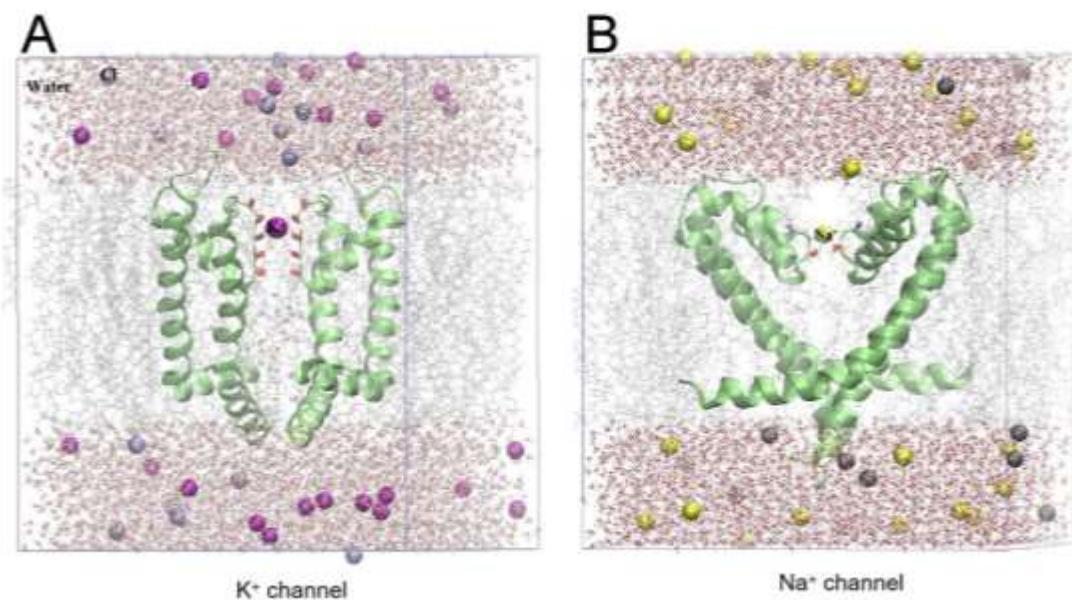


Figure S1. The composite atomic models contain the K⁺ channel (A) and the Na⁺ channel (B).

In our models, we constructed channels containing the whole protein placed at the middle of phospholipid bilayer to separate water and ions on each side. There are 12 potassium, 12 sodium ions and 20 chloride ions for K⁺ channels, and 14 sodium ions, 14 potassium ions and 24 chloride ions for Na⁺ channels, respectively. Both the water thickness of K⁺ and Na⁺ channels are ~0.3 nm. **A:** The K⁺ channel (PDB ID: 2a79) contains 10,294 atoms, including 2,725 TIP3P water molecules, 12 K⁺ and 20 Cl⁻ ions, thus the concentration of a salt solution is 0.15 M. The protein has four negative charges, the addition of four counterbalance ions ensures that the whole system is electrically neutral. The size of the PBC box is 5.04 nm × 5.16 nm × 6.25 nm. **B:** The Na⁺ channel (PDB ID: 4dxw) contains 14,922 atoms, including 4,067 water molecules, 14 Na⁺ and 24 Cl⁻ ions, thus the concentration of a salt solution is 0.15 M. Similarly, the addition of four counterbalance ions also ensures that the whole system is electrically neutral. The size of the PBC box is 5.40 nm × 5.40 nm × 7.30 nm. The purple atom represents K⁺, the yellow atom represents Na⁺, and the gray atom represents Cl⁻. The TIP3P water molecule is displayed in the format of a red ball stick. Green stripes show K⁺ and Na⁺ channels, red stripes show -C=O groups located at the inner wall of the filter region, blue stripes show -OH⁻ groups of the filter, and light gray lines show a phospholipid bilayer, respectively.

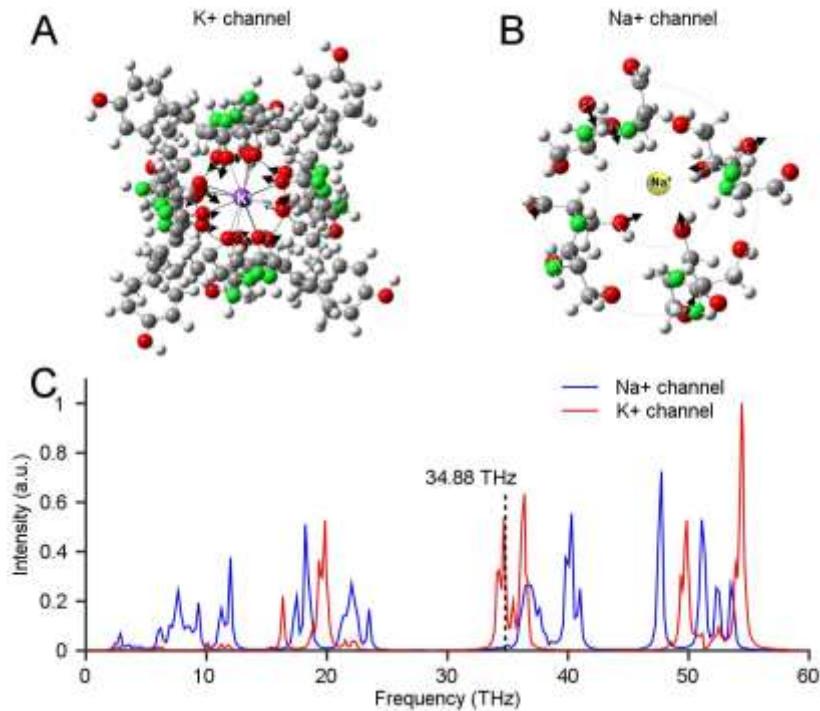


Figure S2. The eigen-modes and intrinsic spectrum calculation for K^+ and Na^+ channels. A and B: Calculations on the eigen-mode frequencies of $-\text{C}=\text{O}$ groups for K^+ channels, and $-\text{C}=\text{O}$, $-\text{OH}^-$ groups for Na^+ channels according to the filter structure extracted from the model of K^+ channels (PDB ID: 2a79) contain 284 atoms (A) and Na^+ channels (PDB ID: 4dxw) contain 96 atoms (B). **C:** The intrinsic spectrum was calculated by using Gaussian 09 software based on density functional theory (DFT) methods at B3LYP/6-31G(d) level.

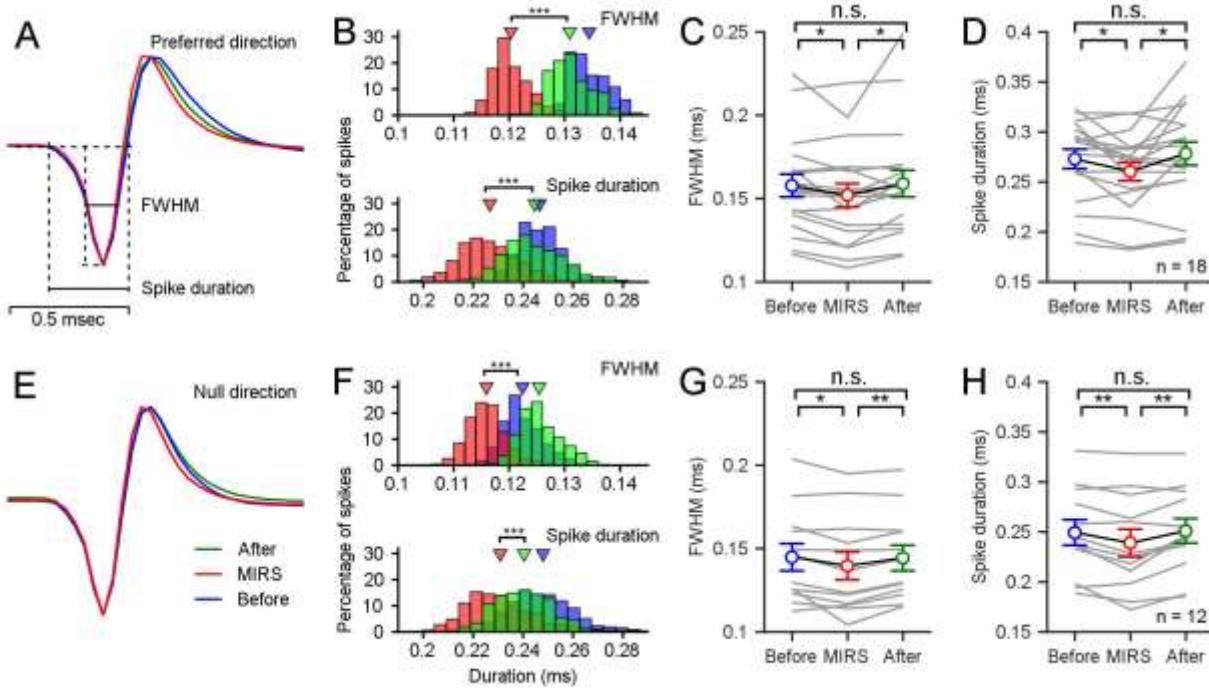


Figure S3. Extracellular recordings showed shortened action potential durations of pretectal nLM neurons during MIRS in the preferred direction (A-D) and the null direction (E-H). A and E: mean action potential traces from an example pretectal neuron before, during and after MIRS in both directions. B and F: Distributions of the full width at half maximum (FWHM) and the duration of spikes' negative phases (Spike duration) of the example pretectal neuron's action potentials (Student's T-test, * $P<0.001$). C, D, G, and H: Statical summarization of the full width at half maximum and the duration of spikes' negative phases across population neurons (n=18 in C and D; n=12 in G and H; Paired Student's T-test, * $P<0.05$, ** $P<0.01$; Error bars represent 1 SEM). In order to reduce the influence of recording noises on the definition of durations, we analyzed data from recorded neurons with the signal-to-noise ratio above 4:1 in Figure 4A and B.**