1   **Title**

2   The ascending arousal system shapes low-dimensional neural dynamics to mediate awareness

3   of intrinsic cognitive states

4

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14 **Abstract**

15 Models of cognitive function typically focus on the cerebral cortex and hence overlook
16 functional links to subcortical structures. This view neglects the highly-conserved ascending
17 arousal system's role and the computational capacities it provides the brain. In this study, we
18 test the hypothesis that the ascending arousal system modulates cortical neural gain to alter
19 the low-dimensional energy landscape of cortical dynamics. Our analyses of spontaneous
20 functional magnetic resonance imaging data and phasic bursts in both locus coeruleus and
21 basal forebrain demonstrate precise time-locked relationships between brainstem activity,
22 low-dimensional energy landscapes, network topology, and spatiotemporal travelling waves.
23 We extend our analysis to a cohort of experienced meditators and demonstrate locus
24 coeruleus-mediated network dynamics were associated with internal shifts in conscious
25 awareness. Together, these results present a novel view of brain organization that highlights
26 the ascending arousal system's role in shaping both the dynamics of the cerebral cortex and
27 conscious awareness.

28

29   **Main Text**

30   It is often difficult to see the forest for the trees, but to fully understand a concept typically

31   involves an accurate depiction of both. That is, we need to comprehend not only the detailed

32   workings of a specific system, but also how that system functions within a broader context

33   of interacting parts. Modern theories of whole-brain function exemplify this challenge. For

34   instance, activity in the brain has been shown to incorporate signatures of both local

35   computational specificity (e.g., specialized regions within the cerebral cortex) as well as

36   system-wide integration (e.g., the interactions between the cortex and the rest of the brain)[1,2].

37   Anatomical evidence suggests that the balance between integration and segregation is

38   mediated in part by the relatively fixed white matter connections between cerebral cortical

39   regions[1] – local connectivity motifs support segregated activity, whereas the axonal, re-

40   entrant connections between regions act to integrate the distributed signals via a highly

41   interconnected structural backbone[3]. However, how the human brain is also capable of

42   remarkable contextual flexibility given this relatively fixed connectivity remains poorly

43   understood.

44

45   During cognitive tasks, neural activity rapidly reconfigures the functional large-scale network

46   architecture of the brain to facilitate coordination between otherwise segregated cortical

47   regions. Precisely how this flexibility is implemented in the brain without altering structural

48   connectivity remains an open question in systems neuroscience. Although it is often

49   overlooked in theories of whole brain function, the neuromodulatory ascending arousal

50   system is well-placed to mediate this role[4]. The arousal system is comprised of a range of

51   nuclei spread across the brainstem and forebrain that send wide-reaching axons to the rest of

52   the central nervous system[5]. At their target sites, arousal neurons release neuromodulatory

53   neurotransmitters that shape and constrain a region's processing mode – altering their

54   excitability and responsivity without necessarily causing them to fire an action potential[4,6]. As

55   a result, subtle changes in the concentration of neuromodulatory chemicals can cause

56   massive alterations in the dynamics of the target regions, leading to nonlinear effects on the

57   coordinated patterns of activity that emerge from 'simple' neuronal circuits[4].

58

59   The ascending arousal system also contains substantial heterogeneity – unique cell

60   populations project in diverse ways to the cerebral cortex and release distinct

61 neurotransmitters. One key dichotomy is the distinction between adrenergic
62 neuromodulation (predominantly via the locus coeruleus [LC]), which promotes arousal and
63 exploratory behaviour[7], and cholinergic neuromodulation (such as via the basal nucleus of
64 Meynert [BNM]), which is associated with attentional focus and vigilance[8]. These highly
65 interconnected[9] structures both promote wakefulness and arousal[10,11], albeit via distinct
66 topological projections to the cerebral cortex: the LC projects in a diffuse manner that
67 crosses typical specialist boundaries, whereas the BNM projects in a more targeted, region-
68 specific manner[12] (Fig. 1A). The two systems have also been linked with distinct and
69 complimentary computational principles: the noradrenergic LC is presumed to modulate
70 interactions between neurons (response gain)[13], whereas the cholinergic BNM is presumed to
71 facilitate divisive normalization (multiplicative gain)[14]. Based on these anatomical and
72 computational features, we have hypothesized that the interaction between these two
73 neuromodulatory systems is crucial for mediating the dynamic, flexible balance between
74 integration and segregation in the brain[15].

75

76 Another crucial feature of the ascending arousal system is that the number of neurons that
77 project to the cerebral cortex is several orders of magnitude smaller than those that project
78 back to the brainstem and forebrain[16–18]. Based on this feature, we further hypothesize that
79 shifts in arousal are realized through a low-dimensional modulation of the ongoing neural
80 activity ('brain state')[17]. Conceptually, low-dimensional neural dynamics can be depicted as
81 evolving on a brain state energy landscape[19], where the energy of a given state corresponds
82 to the occurrence probability, e.g. high energy brain states have a low occurrence probability
83 (and *v. v.*). That is brain states evolve along the energy landscape topography, much like a ball
84 rolls under the influence of gravity down a valley and requires energy to traverse up a hill,
85 this corresponds to an evolution towards an attractive or repulsive brain state, respectively.
86 This technique can resolve what might otherwise be obscured states of attraction (and
87 repulsion) in a multi-stable system and has been successfully applied to the dynamics of
88 spiking neurons[20,21], blood oxygenation level dependent (BOLD) functional magnetic
89 resonance imaging (fMRI)[22,23], and magnetoencephalography (MEG)[24]. The approach offers
90 several conceptual advances, but perhaps most importantly, it renders the otherwise
91 daunting task of systems-level interpretation relatively intuitive. Importantly, this framework
92 is not a mere analogy[30], as the topography of the energy landscape shares a 1-to-1

93   correspondence with the generative equations required to synthesize realistic neural

94   timeseries data[25]. In this manuscript, we test these ideas by combining high-resolution resting

95   state fMRI data with analytic techniques from the study of complex systems.

96

97   ***Results***

98   To begin with, we extracted time series data from major subcortical hubs within the

99   noradrenergic LC[9] (Fig. 1A, red) and cholinergic BNM[26] (Fig. 1A, green) systems from 59

100   healthy participants who had undergone high-resolution, 7T resting-state functional

101   magnetic resonance imaging (fMRI; 2 mm^3 voxels; TR = 586 ms repetition time). Given the

102   known spatiotemporal interactions between the ascending arousal system and fluctuations in

103   cerebrospinal fluid, we first controlled for activity fluctuations in the nearby fourth ventricle,

104   which contains no neural structures, but nonetheless can cause alterations in the BOLD

105   signal over time. We next accounted for nearby gray-matter signals, by regressing the signal

106   from the nearby pontine nuclei. Using the residuals from these regressions from the LC

107   signal, τ_{LC}, and the BMN signal, τ_{BNM}, we focused on the difference between these signals

108   (τ_{LC-BNM} and τ_{BNM-LC}; concatenated across subjects) and then identified time points associated

109   with phasic bursts of LC activity that led to sustained adrenergic (versus cholinergic)

110   influence over evolving brain state dynamics (and *v.v.* for phasic bursts of BNM; see

111   Methods). Importantly, the phasic mode of firing within the noradrenergic arousal system

112   has been specifically linked to systemic influences that occur on time-scales relevant to

113   cognitive function[8,27]. Tracking the mean cortical BOLD response around these peaks

114   identified a spatiotemporal travelling wave (Fig. 1B; velocity = 0.13ms^{-1}) that propagated

115   from frontal to sensory cortices and tracked closely with the known path of the dorsal

116   noradrenergic bundle[9], albeit with a preserved 'island' within the parietal operculum (Fig.

117   1B). A block-resampling null model was applied to ensure that the results were not due to

118   spatial-autocorrelation (p < 0.05; see Methods). These results can be inverted for BNM

119   activity (relative to LC) as $\tau_{BNM-LC} = -\tau_{LC-BNM}$. Furthermore, these results confirm that

120   coordinated macroscale activity patterns align to fluctuations in activity within the ascending

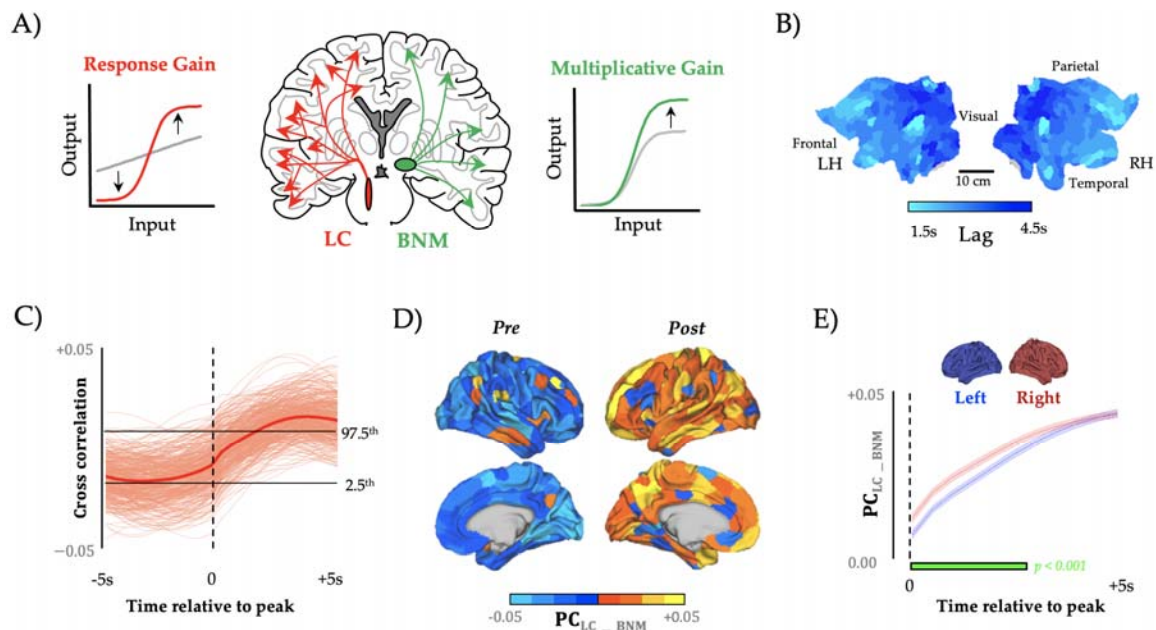121   arousal system of the brainstem[28].

122

123

124 **Figure 1. Sympathetic activity precedes network-level integration.** A) regional time series were extracted
125 from the locus coeruleus (red), which is thought to alter response gain, and the basal nucleus of Meynert
126 (green), which is thought to alter multiplicative gain, and compared to BOLD signal and topological signatures
127 during the resting state; B) we observed a anterior-to-posterior traveling wave (velocity ~ 0.13ms⁻¹) following
128 peaks in $\tau_{LC\text{-}BNM}$, which are shown on both the left (LH) and right (RH) hemispheres of a cortical flat map; C)
129 the lagged cross-correlation between ⠀⠀⠀ and PC – dotted line depicts the zero-lag correlation, and the
130 black lines depict the upper (lower) bounds of a block-resampled null model (95% CI); D) mean cortical
131 participation coefficient (PC) preceding (left) and following (right) the zero-lagged ⠀⠀⠀ value, only the
132 right hemisphere is shown (mirrored for 'Post'); E) the participation coefficient following peak ⠀⠀⠀ was
133 higher in the right- (red) vs. the left- (blue) hemisphere (p < 0.001; green bar).

134

Time-varying network topology

136 Based on previous empirical[29], modelling[30] and theoretical[15] work, we predicted that phasic
137 bursts in $\tau_{LC\text{-}BNM}$ would facilitate network-level integration by modulating increased neural
138 gain among regions distributed across the cerebral cortex. As predicted, we observed a
139 strong positive correlation between $\tau_{LC\text{-}BNM}$ and network-level integration (p < 0.05, block-
140 resampling null model; Fig. 1C) across the brain (Fig. 1D). An increase in phasic activity
141 within the LC (relative to the BNM) preceded an increase in the mean level of integration
142 within the cerebral cortex that was dominated by the frontoparietal cortices (Fig. 1D;
143 parcellated according to the 17 resting-state networks identified in[31]). Interestingly, this

6

144   global integration was opposed by a relative topological segregation of limbic, visual, and

145   motor cortices (Fig. S2). This increase in the synchronisation of the frontoparietal cortices

146   following an increase in sensory-limbic coordination and LC activity may reflect arousal-

147   enhanced processing of sensory stimuli[32,33]. Furthermore, regional integration occurred

148   earlier in the right- vs. the left-hemisphere (p<0.001; Fig. 1E), which is consistent with the

149   known anatomical bias of the LC system[34,35]. Together, these findings provide robust

150   evidence for the hypothesis that the balance between ascending noradrenergic and

151   cholinergic tone facilitates a transition towards topological integration across the

152   frontoparietal network of the brain[15].

153

Neuromodulation of the Energy Landscape

155   The results of our initial analysis demonstrate that coordinated distributed activity in the

156   cortex align with changes in small groups of neuromodulatory cells activity in the brainstem

157   and forebrain, which in turn are proposed to constrain brain dynamics onto a low-

158   dimensional energy landscape (Fig. 2A). The effects of noradrenaline and acetylcholine can

159   also be easily viewed through this lens: by integrating the brain, noradrenaline should flatten

160   the energy landscape (Fig. 2A, red) facilitating otherwise unlikely brain state transitions,

161   whereas in contrast, the segregative nature of cholinergic activity should act to deepen

162   energy valleys (Fig. 2A, green) decreasing the likelihood of a brain state transition. In

163   previous work, we have shown a correspondence between low-dimensional brain state

164   dynamics across multiple cognitive tasks and the heterogenous expression of metabotropic

165   neuromodulatory receptors[17]. This implies that neuromodulators act similar to catalysts in

166   chemical reactions, which lower (or raise) the activation energy (E_A) required to transform

167   chemicals from one steady state (or energy well) to another (Fig. 2B). In the context of the

168   interconnected, heterarchical networks that comprise the cerebral cortex, this would have

169   the effect of flattening (or deepening) the energy landscape, promoting variable (or rigid)

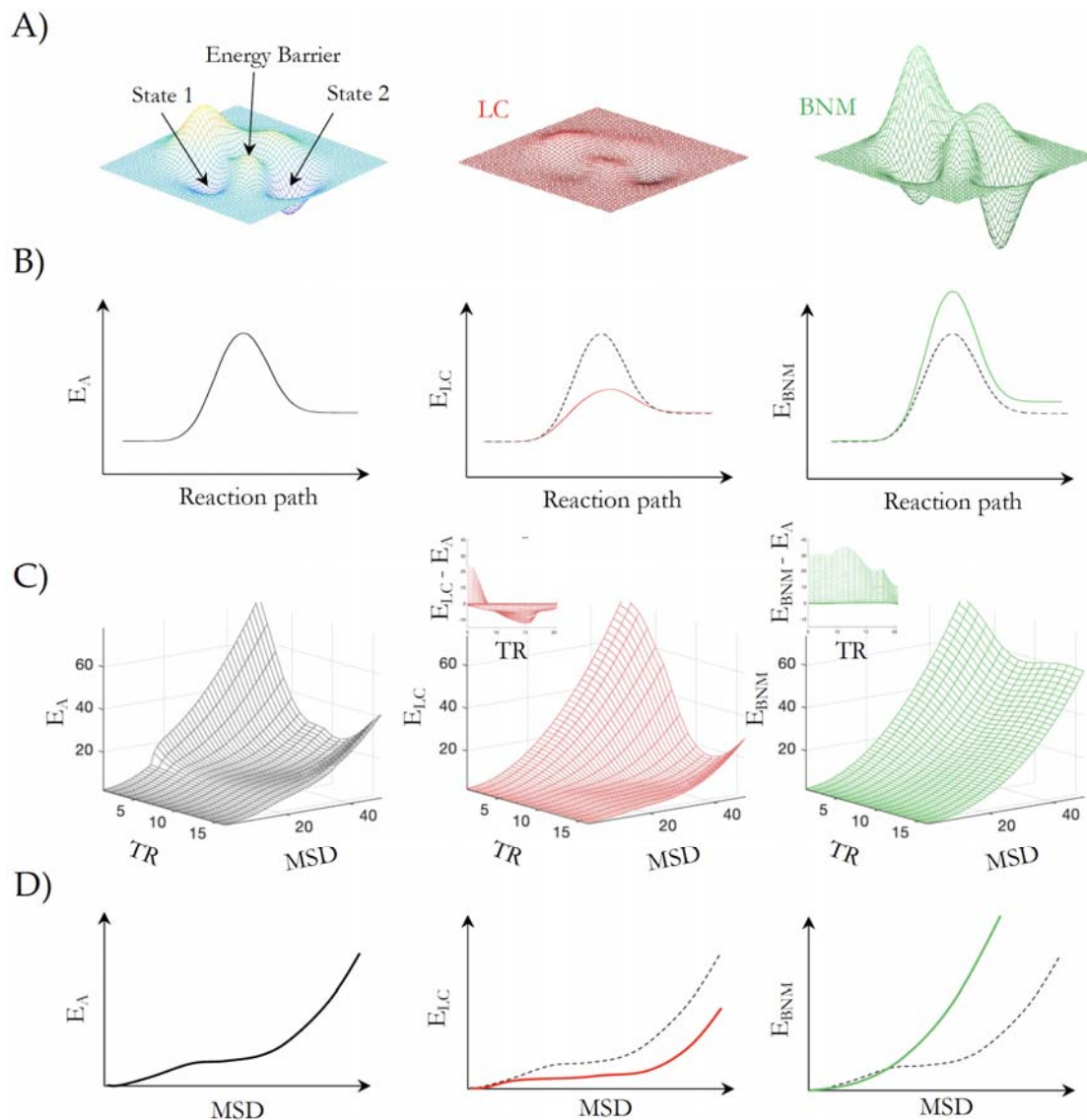170   brain states[36] (Fig. 2A).

Figure 2 – LC and BNM mediated shifts in energy landscape brain state space dynamics. A) an energy landscape, which defines the energy required to move between different brain states: by increasing response gain, the LC should flatten the energy landscape (red); by increasing multiplicative gain, the BNM should deepen the energy wells (green); B) the topography of the energy landscape can be conceptualized as similar to the activation energy (E_A) that must be overcome in order to convert one chemical to another; C) Empirical BOLD trajectory energy as a function of MSD and TR of the baseline activity (E_A, black) and after phasic bursts in LC (E_{LC}, red) and BNM (E_{BNM}, green) – relative to the baseline energy landscape phasic bursts in LC (E_{LC} - E_A, red inset) lead to a flattening or reduction of the energy landscape, whereas peaks in BNM (E_{BNM} - E_A, green inset) lead to a raising of the energy landscape. D) Empirical activation energy as a function of MSD averaged over lags   TR during base baseline activity (E_A, Left) and following phasic bursts in LC (E_{LC}, red) and BNM (E_{BNM}, green).

8

184   To elucidate the role of phasic activity from the neuromodulatory system in modifying the

185   energy landscape, we first estimated the energy of BOLD signal transitions across the

186   cerebral cortex. Importantly, the term 'energy' here is used in reference to its definition in

187   statistical physics and hence does not represent the biological use of the term, which instead

188   stands for the energy used by the brain to maintain or change neural activity. Specifically, we

189   define the energy landscape, E, as the natural logarithm of the inverse probability of

190   observing a given BOLD MSD at a given time-lag t, $\mathrm{P}(MSD, t)$, calculated as $\mathrm{E} =$

191    $\ln \frac{1}{\mathrm{P}(MSD, t)}$, where $MSD_{t, t_0} = \langle |x_{t_0 + t} - x_{t_0}|^2 \rangle_r$ is the mean-squared displacement (MSD) of

192   BOLD signal, $x_t = [x_{1,t}, x_{2,t}, \ldots, x_{r,t}]$ across r voxels and t is the number of time-lags of

193   size TR from a reference timepoint t_0 [20]. The probability of a BOLD signal transition,

194    $\mathrm{P}(MSD, t)$, was estimated from the sampled MSD_{t, t_0}, and we used a Gaussian kernel

195   density estimation $\mathrm{P}(MSD, t) = \frac{1}{4n} \sum_{i=1}^{n} K\left(\frac{MSD_{t, i}}{4}\right)$, where $K(u) = \frac{1}{2\sqrt{\pi}} e^{-\frac{1}{2} u^2}$ (see

196   Methods). Our analysis is consistent with the statistical mechanics interpretation that the

197   energy of a given state, E_σ, and its probability are related $P_\sigma = \frac{1}{Z} e^{-\frac{E_\sigma}{T}}$, where Z is the

198   normalisation function and T is a scaling factor equivalent to temperature in

199   thermodynamics, where we set $T = 1$ and $Z = 1$ [20]. In this framework, a highly probable

200   relative change in BOLD (as quantified by the MSD) corresponds to a relatively low energy

201   transition (i.e., low E_A), whereas an infrequently visited state will require the most energy

202   (i.e., high E_A).

203

204   By treating energy as inversely proportional to the probability of brain state occurrence, our

205   approach resembles other studies that have been applied to spiking dynamics of neuronal

206   populations, spiking neurons[20,21], BOLD fMRI[22,23], MEG[24], and natural scene[37]. However,

207   these studies binarized continuous signals to reduce the brain state space (to 2^r states),

208   however this approach requires the fitting of a threshold, which can be problematic in

209   continuously recorded data. In contrast, our approach reduces the dimensionality by

210   analysing the likelihood of a change in BOLD activity (i.e., the MSD), and thus retains the

211   dimensionality of the underlying signal without the need for thresholding. This approach

212   overcomes a major limitation inherent to previous energy landscape studies that require a

213   large sample size to sufficiently sample the brain state space.

214

215   With this in mind, we turned our attention to the relationship between the ascending arousal
216   system dynamics and the MSD energy landscape. To test the hypothesis that the
217   neuromodulatory system alters the topography of the energy landscape, we calculated BOLD
218   MSD energetics following phasic bursts of both LC relative to BNM (τ_{LC-BNM}), E_{LC}, and
219   BNM relative to LC (τ_{BNM-LC}), E_{BNM}, i.e., t_0 was the onset of a phasic burst, and compared
220   these to sampled brain evolutions without large changes in LC and BNM arousal i.e., t_0 was
221   all timepoints outside of a phasic burst in LC and BNM, analogous to the baseline energy
222   landscape E_A. We identified phasic bursts as peaks in the second derivative of the arousal
223   BOLD signals τ_{LC-BNM} and τ_{BNM-LC} that lead to a sustained increase in BOLD activity for
224   each individual (see Methods) and using these criteria, we identified 148 τ_{LC-BNM} time points
225   and 130 τ_{BNM-LC} time points.

226

227   The energy landscapes for these three states are defined by the energy for a given BOLD
228   MSD at a given TR delay. Figure 2C demonstrates the baseline energy landscape (Fig. 2C,
229   black), which corresponds to the reaction pathway in Fig. 2B, and the MSD energy
230   landscape following phasic bursts in the LC (Fig. 2C, red) and BNM (Fig. 2C, green). These
231   figures demonstrate an MSD energy landscape across displacement and time, wherein the
232   energy relates to the likelihood of seeing a given mean change in bold activity (i.e., MSD) at a
233   given temporal displacement (i.e., TR). For example, all the MSD energy landscapes have a
234   high energy peak for large MSD at a short timescale as it is extremely unlikely that the bold
235   activity would change significantly (quantified by a large MSD) in one TR (~0.5s), and
236   neuromodulation increases the energy of such an initial change. The utility of the MSD
237   energy landscape can be seen when comparing large phasic bursts of LC and BNM relative
238   to baseline fluctuations. We found the largest change occurs around 10-15 TR (~6-9s)
239   following a phasic burst that typically corresponds to a peak in the LC or BNM BOLD
240   signal. At this ~6-9s temporal delay we see direct evidence that a phasic burst of LC
241   flattened the energy landscape (decreased the energy relative to baseline Fig. 2C, red inset),
242   thus making previously unlikely large MSD trajectories far more probable (Fig. 2D red),
243   whereas a phasic burst of BNM activity (increased energy relative to baseline Fig. 2C, green
244   inset) caused the energy landscape to be elevated, thus promoting local trajectories, and
245   making large MSD deviations unlikely (Fig. 2D green). These patterns are analogous to

246   modulating a physical landscape in which towns sit within valleys separated by impassable

247   mountains – when BNM is high, the towns remain isolated, whereas when LC is high, the

248   towns are separated by easily navigated rolling plains and transitions between towns (novel

249   combinations of consecutive brain states) can be easily realised.

250

251   We next asked whether LC and BNM combined synergistically to alter the energy landscape.

252   To achieve this, we isolated simultaneous phasic peaks in both LC and BNM (τ_{LC+BNM}). We

253   found that the LC + BNM energy landscape differed from either independent LC or BNM

254   activation, shifting the brain state into divergent regimes than could be explained by the

255   HRF. By comparing the MSD energy topography for a given TR slice we found that the

256   landscape switched from an anti- to de-correlation with the HRF. In other words, the

257   cooperative behaviour between the noradrenergic and cholinergic systems allowed the brain

258   to reach unique BOLD MSDs that neither could facilitate individually. To examine how

259   simultaneous LC+BNM activity altered the energy landscape, we compared the energy

260   relative to the two individual landscapes. As demonstrated in Fig. S3, the energy landscape

261   following phasic bursts of LC+BNM differed in magnitude from that expected from a linear

262   superposition of the LC and BNM energy landscape – i.e., LC+BNM ≠ (LC) + (BNM).

263   Furthermore, to explore the dominance of either LC or BNM in this signal, we minimised

264   the relationship LC+BNM = α LC + β BNM (conditional upon α and β being positive

265   constants) and found that $\alpha = 0.16$ and $\beta = 0.84$ gave the best match to the LC+BNM

266   energy landscape. That is, the BNM dynamics dominates the simultaneous LC+BNM energy

267   landscape, which is consistent with the unidirectional synaptic projections from the LC that

268   synapse upon the BNM on their way through to the cortex[12], and suggests that phasic

269   LC+BNM bursts may be initiated by the LC in order to elicit a cascade of BNM activity.

270

271   ***Conscious awareness of shifts in BOLD state***

272   Interpreting the relationship between neuroimaging data and conscious awareness is

273   notoriously challenging. For instance, it is currently not possible to directly determine the

274   contents of self-directed thought without intervening, and thus altering, the contents of

275   consciousness[38]. Although we can't determine the contents of consciousness directly, we can

276   use task designs to modulate the state of consciousness. To this end, we leveraged data from

277   a group of 14 expert meditators who were asked to meditate during an fMRI scanning

278   session[39], and to press a button when they noticed that their focus had drifted from their

279   breath (Fig. 3A). At this point, there is a mismatch between expectation and conscious

280   awareness, which is an internal state that has been previously linked to the activation of the

281   noradrenergic system, both in theoretical[40,41] and computational[42] work. Based on these

282   studies, we predicted that the switch in internal conscious awareness would be facilitated by

283   increases in locus coeruleus-mediated integration and subsequent reconfiguration of low-

284   dimensional brain states. Analysing time-resolved network data with a finite impulse

285   response model, we observed a peak in locus coeruleus activity (Fig. 3B), TR-to-TR mean

286   squared displacement (Fig. 3C) and elevated network-level integration (Fig. 3D) surrounding

287   the change in conscious awareness (all p_{PERM} < 0.05; 95% CI of null distribution). These

288   results confirm that the locus coeruleus mediates energy landscape reconfigurations and that

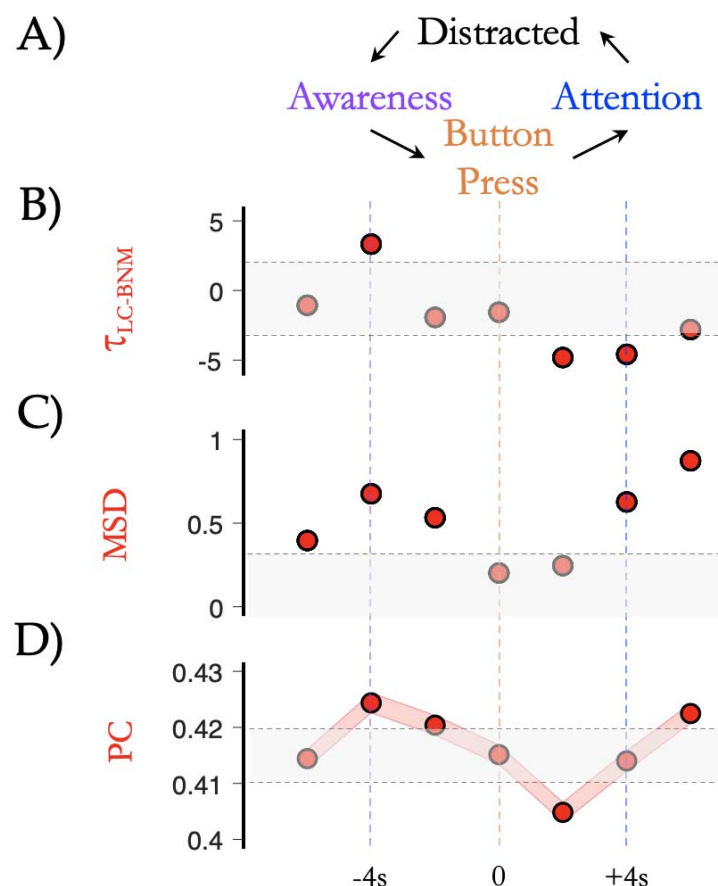289   these changes modulate internal states of conscious awareness.

290

291   **Figure 3 – Awareness of intrinsic state changes.** A) participants performing breath-awareness meditation

292   (Focus; blue) were trained to respond with a Button Press (orange) when they became Aware (purple) that they

293   had become Distracted (i.e., their attention had wandered from their breath) and to then re-focus their

294   Attention (blue) on their breath; B) we observed a peak in τ_{LC-BNM} (i.e., LC > BNM; red) ~4 seconds before

295   the button press, which then returned to low levels (i.e., BNM > LC) in the 2-4 seconds following the button

296   press; C) the Mean Squared Displacement (MSD; dark orange) of TR-to-TR BOLD signal was increased above

297   null values around the peak in τ_{LC-BNM}, as well as following the re-establishment of attentional focus (in

298   panels B & C, grey shading depicts 95% CI of block-resampled null distribution); D) we observed a peak in

299   mean participation coefficient (PC) ~4 seconds (2 TRs) prior to the Button Press during the task. All: grey

300   shading depicts 97.5th and 2.5th percentile of null distribution i.e., outside grey shading indicates a value

301   different than null [p < 0.05]; and lower: red shading represents SEM error bars).

302

Discussion

304   Our results provide evidence for an arousal-mediated macroscopic network and energy

305   landscape reconfiguration which tracks with moment-to-moment alterations in conscious

306   awareness. By tracking fluctuations in BOLD signal within the noradrenergic LC and the

307   cholinergic BNM, we were able to demonstrate fundamental ways in which the low-

308   dimensional, dynamic, and topological signature of cortical dynamics was related to changes

309   within the ascending arousal system. Furthermore, we demonstrated a link between these

310   dynamic reconfigurations and alterations in conscious awareness in a cohort of experienced

311   meditators. In this way, our results provide a novel, systems-level perspective on the

312   distributed dynamics of the human brain.

313

314   There is growing evidence that distributed neural dynamics in the brain are well described by

315   relatively low-dimensional models[17,18,43–45], however the biological constraints that impose

316   these features on the brain remain poorly understood. Due to the low number of cells in the

317   arousal system and their broad projections to the rest of the brain, we theorized that

318   neuromodulatory regions are well-placed to shape and constrain the vast number of neurons

319   in the cerebral cortex into low-dimensional dynamic modes. Our results support this

320   prediction by showing that patterns of activity in key regions within the brainstem and

321   forebrain relate to fundamental alterations in a dynamically evolving energy landscape. In

322   other words, neural state space trajectories are a powerful framework that extends beyond

323   that of mere analogy, and the ascending arousal system is well-placed to mediate

324   deformations in the energy landscape.

325

326   Much in the same way that there are many different reference frames for navigation – e.g.,

327   egocentric (i.e., straight, left, right directions), which is independent of the environment; and

328   allocentric (i.e., following compass directions and visual cues), which is dependent on the

329   environment – we can interrogate energy landscapes using different vantage points on

330   BOLD dynamics. Our displacement framework is consistent with an egocentric (or 'first-

331   person') frame of reference, wherein MSD is used to track BOLD trajectories from an initial

332   state which maps out the topology of the energy landscape (i.e., a BOLD MSD implies a

333   BOLD trajectory). Nonetheless, the method does not distinguish between two different

334   neural trajectories that possess the same MSD. In comparison, other methods have evaluated

335   the energy landscape for a given pre-defined state estimated from thresholded BOLD

336   timeseries[22,23] a framework consistent with an allocentric (or 'third-person') reference frame.

337   This framework has the advantage of calculating energy for a given state, however, it also

338   requires substantial exploration of the state-space – which is typically unfeasible – or the

339   need to resort to severe coarse-graining (such as the binarization of BOLD activity) which

340   further diminishes interpretability. Furthermore, the allocentric view does not provide

341   insights into the transitions between each energy state, whereas this information is inherent

342   to the egocentric reference. Along these lines, we found that the egocentric reference frame

343   clearly demonstrated the flattening and deepening of the energy landscape, providing indirect

344   evidence that the ascending arousal system is well set-up to control brain-state dynamics

345   'egocentrically' (as opposed to specific neural activity patterns). Nevertheless, given

346   improvements in recording length and novel analytic techniques to probe the brains

347   dynamical landscape, we expect that the field will ultimately discover even more optimal

348   mappings between neurobiology and low-dimensional brain state dynamics.

349

350   The results of our state-space analysis have important implications for the biological

351   mechanisms underlying cognition. For instance, the concept of locus coeruleus-mediated

352   energy landscape flattening is reminiscent of the α1 receptor-mediated notion of a 'network

353   reset'[40]. By increasing response gain (Fig. 1A) through the modulation of second-messenger

354   cascades[4], noradrenaline released by the LC would augment inter-regional coordination[30].

355   Importantly, this capacity could confer adaptive benefits across a spectrum, potentially

356   facilitating the formation of flexible coalitions in precise cognitive contexts[46], while also

357   forcing a broader landscape flattening (i.e., a 'reset') in the context of large, unexpected

358   changes[27,40]. Similarly, the idea that phasic cholinergic bursts deepens energy wells is

359   consistent with the idea that the cholinergic system instantiates divisive normalization within

360   the cerebral cortex[14]. Numerous cognitive neuroscience studies have shown that heightened

361   acetylcholine levels correspond to improvements in attentional precision[8,8]. By deepening

362   energy wells, acetylcholine from the BNM could ensure that the brain remains within a

363   particular state and is hence not diluted by other (potentially distracting) brain states.

364   Determining the specific rules that govern the links between the neuromodulation of the

365   energy landscape and cognitive function[47–49] is of paramount importance, particularly given

366   the highly integrated and degenerate nature of the ascending arousal system[50].

367

368   Our results also provide a systems-level perspective on an emerging corpus of work that

369   details the microscopic circuit level mechanisms responsible for conscious phenomena[51]. In

370   particular, a number of recent studies have highlighted the intersection between the axonal

371   projections of the ascending arousal system and pyramidal cell dendrites in the supragranular

372   regions of the cerebral cortex as a key site for mediating conscious awareness. For instance,

373   optogenetic blockage of the connections between the cell bodies and dendrites of thick-

374   tufted layer V pyramidal cells in the sensory cortex causally modulated conscious arousal in

375   mice[52]. Other work has shown that both the noradrenergic[53] and cholinergic[54] systems alter

376   this mechanism, albeit in distinct ways: noradrenaline would promote burst firing due to the

377   α2a receptor-mediated closure of Ih HCN leak-channels[53], whereas the cholinergic system

378   instead prolongs the time-scale of firing via M1 cholinergic receptor activation on pyramidal

379   cell dendrites[54]. In this way, coordinated activity in the ascending arousal system can mediate

380   alterations in microcircuit processing that ultimately manifest as alteration in macroscopic

381   brain network dynamics.

382

383   The vascular nature of the T2* fMRI signal is such that it is impossible to rule out the role of

384   haemodynamics in the results we obtained in our analysis. Indeed, there is evidence that

385   noradrenaline causes a targeted hyperaemia through the augmentation of G-protein-coupled

386   receptors on vascular smooth muscle cells[55,56]. However, it is also clear that the

387   haemodynamics and massed neural action in the cerebral cortex are inextricably linked[57,58]. In

388   addition, there is evidence that stimulation of the locus coeruleus leads to the high-

389   frequency, low-amplitude electrophysiological activity patterns characteristic of the awake

390   state[10]. Together, these results argue that the locus coeruleus mediates a combination of

391   haemodynamic and neural responses that facilitate integrative neural network interactions

392   and subsequently mediate alterations in conscious awareness.

393

394   In this manuscript, we have argued that the ascending arousal system provides crucial

395   constraints over normal brain function, however there are numerous examples wherein

396   pathology within the ascending arousal system leads to systemic impairments in cognition. In

397   addition to disorders of consciousness[59], dementia syndromes are also crucially related to

398   dysfunction within the ascending arousal system. For instance, Alzheimer's disease has been

399   linked to tau pathology within the BNM[26], however individuals with Alzheimer's disease also

400   often have pathological involvement of the LC as well[60]. Similarly, individuals with

401   Parkinson's disease often have extra-dopaminergic pathology in the LC[61], as well as in the

402   cholinergic tegmentum[62]. Given the pathological processes at play in these disorders, we

403   expect that other neuromodulatory systems will also be impaired, and in turn effect the

404   macroscopic dynamics of the system in ways that remain to be elucidated.

405

406   In conclusion, we leveraged a high-resolution 7T resting state fMRI dataset to test the

407   hypothesis that activity within the ascending arousal system shapes and constrains patterns

408   of systems-level network reconfiguration. Our results support specific predictions from a

409   recent hypothetical framework[15], and further delineate the manner in which the autonomic

410   nervous system shapes and constraints ongoing, low-dimensional brain state dynamics in the

411   central nervous system in a manner that supports changes in conscious awareness.

412

413 ## Methods

414 ### 7T resting state fMRI

415 Sixty-five healthy, right-handed adult participants (mean, 23.35 years; SD, 3.6 years; range
416 18–33 years; 28 females) were recruited, of whom 59 were included in the final analysis (four
417 participants were excluded due to MR scanning issues, one participant was excluded due to
418 an unforeseen brain structure abnormality, and one was excluded due to inconsistent BOLD
419 dynamics following global-signal regression). Participants provided informed written consent
420 to participate in the study. The research was approved by The University of Queensland
421 Human Research Ethics Committee. These data were originally described in Hearne et al.,
422 2017[63]. 1050 (~10 minutes) whole-brain 7T resting state fMRI echo planar images were
423 acquired using a multiband sequence (acceleration factor = 5; 2 mm^3 voxels; 586 ms TR;
424 23 ms TE; 40^0 flip angle; 208 mm FOV; 55 slices). Structural images were also collected to
425 assist functional data pre-processing (MP2RAGE sequence – 0.75 mm^3 voxels 4,300 ms TR;
426 3.44 ms TE; 256 slices).

427

428 DICOM images were first converted to NIfTI format and realigned. T1 images were
429 reoriented, skull-stripped (FSL BET), and co-registered to the NIfTI functional images using
430 statistical parametric mapping functions. Segmentation and the DARTEL algorithm were
431 used to improve the estimation of non-neural signal in subject space and the spatial
432 normalization. From each grey-matter voxel, the following signals were regressed: linear
433 trends, signals from the six head-motion parameters (three translation, three rotation) and
434 their temporal derivatives, white matter, and CSF (estimated from single-subject masks of
435 white matter and CSF). The aCompCor method (Behzadi et al., 2007) was used to regress
436 out residual signal unrelated to neural activity (i.e., five principal components derived from
437 noise regions- of-interest in which the time series data were unlikely to be modulated by
438 neural activity). Participants with head displacement > 3 mm in > 5% of volumes in any one
439 scan were excluded ($n = 5$). A temporal band pass filter ($0.01 < f < 0.15$ Hz) was applied to
440 the data.

441

442 ### Brain parcellation

443 Following pre-processing, the mean time series was extracted from 400 pre-defined cortical
444 parcels using the Schaefer atlas (Schaefer et al., 2018). Probabilistic anatomical atlases were

445   used to define the location of the noradrenergic LC[64] and the cholinergic BNM (Ch4 cell

446   group)[65]. The mean signal intensity from each region was extracted and then used for

447   subsequent analyses. To ensure that the BOLD data were reflective of neuronal signals, we

448   statistically compared LC and BNM time series with a number of potential nuisance signals

449   from: i) the cerebrospinal fluid; ii) the cortical white matter; iii) mean framewise

450   displacement; and iv) a $2mm^3$ sphere in the fourth ventricle (centred at MNI co-ordinates: 0

451   -45 -30)[66]. All signals were unrelated to LC and BNM activity ($|r| < 0.05$ in each case),

452   however given the spatial proximity of the LC to the fourth ventricle, we opted to use a

453   linear regression to residualize the signal from the fourth ventricle. To ensure that BOLD

454   signals from nearby grey matter structures were not influencing the locus coeruleus

455   timeseries, we extracted the mean activity of the locus coeruleus mask after shifting the mask

456   anteriorly such that it overlapped with an area of the pons that harbours the nuclei (i.e.,

457   +8mm in the Y direction). In the same manner in which we previously regressed the

458   dynamics of the fourth ventricle, we regressed the activity of this non-LC pontine region,

459   and then re-analysed our data. Each of the results was statistically identical following this

460   approach, providing confidence that the original conclusions were not biased by a lack of

461   regional specificity.

462

463   **Phasic increases in neuromodulatory BOLD signal**

464   To identify phasic increases in neuromodulatory BOLD signal, we calculated the second

465   derivative (i.e., the acceleration) of the LC and BNM time series, and then identified points

466   in time that fulfilled three criteria: 1) value greater than or equal to 2 s.d. above the mean

467   acceleration; 2) value of the original time series, i.e., LC or BNM, was greater than or equal

468   to 2 s.d. above the mean of the time series within the following 10 TRs (i.e., 5.8 seconds);

469   and 3) the time point was not present within the first or last 20 TRs of an individual subjects'

470   trial (so as to avoid potential boundary effects). Using these criteria, we identified 148 $\tau_{LC\text{-}BNM}$

471   time points, 130 $\tau_{BNM\text{-}LC}$ time points and 316 τ_{LC+BNM} time points across all 59 subjects. To

472   ensure that the choice of 2 s.d. threshold was reflective of the underlying dynamics, we

473   altered this threshold between 1-3 s.d. and found robustly similar patterns. For subsequent

474   analyses, we identified time points in the 21 TR window surrounding these peaks, and then

475   used these to conduct statistical comparisons of the low-dimensional, complex network

476   signature of brain network dynamics as a function of phasic ascending arousal system

477   activity. Each of these patterns was confirmed using a lag-based cross-correlation analysis,

478   which demonstrated similar phenomena to those that we present in the manuscript.

479

480   To monitor the propagation of cortical signals with respect to $\tau_{LC\text{-}BNM}$, $\tau_{BNM\text{-}LC}$ and τ_{LC+BNM}, we

481   extracted the time-to-peak of the cross-correlation between these signals and each of the 400

482   cortical parcels within the 10 TR (i.e., 5.8 second) windows following each identified phasic

483   peak. These patterns were mapped onto the cortex (Fig. 1B) for visualization and clearly

484   demonstrated anterior-to-posterior direction for the wave. We then used the volumetric

485   MNI co-ordinates of the Schaefer parcellation scheme to calculate the average velocity of the

486   travelling wave (0.13m s^{-1}).

487

488   In order to obtain an appropriate null model against which to compare our data, we

489   identified 5,000 random timepoints within the concatenated dataset that did not substantially

490   overlap with the already identified $\tau_{LC\text{-}BNM}$, $\tau_{BNM\text{-}LC}$ and τ_{LC+BNM} time series, and used these to

491   populate a null distribution[67]. Outcome measures were deemed significant if they were more

492   extreme than the 95th (or 5th) percentile of the null distribution. Crucially, this ensured that

493   our data could not be explained by the characteristic spatial and temporal autocorrelation

494   present in BOLD timeseries data.

495

496   **Time-resolved functional connectivity.**

497   To estimate functional connectivity between the 400 regions of interest, we used the

498   multiplication of temporal derivatives (MTD) technique. Briefly, MTD is computed by

499   calculating the point-wise product of temporal derivative of pair-wise time series. The

500   resultant score is then averaged over a temporal window, w (a window length of 20 TRs was

501   used in this study, though results were consistent for w = 10–50 TRs).

502

503   **Modularity Maximization**

504   The Louvain modularity algorithm from the Brain Connectivity Toolbox (BCT[73]) was used

505   on the neural network edge weights to estimate community structure. The Louvain

506   algorithm iteratively maximizes the modularity statistic, Q, for different community

507   assignments until the maximum possible score of Q has been obtained:

$$Q_T = \frac{1}{v^+} \sum_{ij} \left(w_{ij}^+ - e_{ij}^+\right) \delta_{M_i M_j} - \frac{1}{v^+ + v^-} \sum_{ij} \left(w_{ij}^- - e_{ij}^-\right) \delta_{M_i M_j},$$

508   where v is the total weight of the network (sum of all negative and positive connections), w_{ij}

509   is the weighted and signed connection between regions i and j, e_{ij} is the strength of a

510   connection divided by the total weight of the network, and δ_{MiMj} is set to 1 when regions are

511   in the same community and 0 otherwise. '+' and '−' super-scripts denote all positive and

512   negative connections, respectively. The modularity of a given network is therefore a

513   quantification of the extent to which the network may be subdivided into communities with

514   stronger within-module than between-module connections.

515

516   For each epoch, we assessed the community assignment for each region 500 times and a

517   consensus partition was identified using a fine-tuning algorithm from the Brain Connectivity

518   Toolbox (BCT; http://www.brain-connectivity-toolbox.net/). We calculated all graph

519   theoretical measures on un-thresholded, weighted and signed connectivity matrices[73]. The

520   stability of the γ parameter was estimated by iteratively calculating the modularity across a

521   range of γ values (0.5-2.5; mean Pearson's r = 0.859 +-0.01) on the time-averaged

522   connectivity matrix for each subject – across iterations and subjects, a γ value of 1.0 was

523   found to be the least variable, and hence was used for the resultant topological analyses.

524

525   **Participation Coefficient**

526   The participation coefficient, *PC*, quantifies the extent to which a region connects across all

527   modules (i.e., between-module strength) and has previously been used to successfully

528   characterize hubs within brain networks (e.g. see [75]). The PC for each region was calculated

529   within each temporal window as,

$$\text{PC} = 1 - \sum_{s=1}^{n_M} \left(\frac{\kappa_{isT}}{\kappa_{iT}}\right)^2$$

530   where k_{isT} is the strength of the positive connections of region i to regions in module s at

531   time T, and k_{iT} is the sum of strengths of all positive connections of region i at time T.

532   Negative connections were discarded prior to calculation. The participation coefficient of a

533   region is therefore close to 1 if its connections are uniformly distributed among all the

534   modules and 0 if all of its links are within its own module.

535

536

Brain State Displacement and the Energy Landscape

To quantify the change in BOLD activity following phasic bursts of neuromodulation we calculated the BOLD mean-squared displacement (MSD). The MSD is a measure of the deviation in BOLD activity, $\boldsymbol{x}_t = [x_{1,t}, x_{2,t}, \ldots, x_{r,t}]$ for r parcels, with respect to the activity at the phasic onset, t_0. The MSD is calculated as the average change of each voxel

$$MSD_{t,t_0} = \langle |\boldsymbol{x}_{t_0+t} - \boldsymbol{x}_{t_0}|^2 \rangle_r,$$

and it is calculated for different t_0, where t_0 are the onset of a subcortical phasic burst, across t TRs. We are interested in the probability, P_{MSD}, that we will observe a given displacement in BOLD at a given time-lag t. We estimated the probability distribution function $P(MSD, t)$ from n MSD_{t,t_0} samplings, — e.g., the identified n phasic bursts of subcortical structures (as above) — using a Gaussian kernel density estimation $P(MSD, t) = \frac{1}{4n} \sum_{i=1}^{n} K\left(\frac{MSD_{t,i}}{4}\right)$, where $K(u) = \frac{1}{2\sqrt{\pi}} e^{-\frac{1}{2}u^2}$ and we display the results for t between 1 to 15 TR and MSD between 0 to 50. As is typical in statistical mechanics the energy of a given state, E_σ, and its probability are related $P(\sigma) = \frac{1}{Z} e^{-\frac{E_\sigma}{T}}$, where Z is the normalisation function and T is a scaling factor equivalent to temperature in thermodynamics [20]. In our analysis $\sum_\sigma P_\sigma = 1$ by construction and we can set $T = 1$ for the observed data. Thus, the energy of each BOLD MSD for a given at a given time-lag t, E, is then equal to the natural logarithm of the inverse probability, $P(MSD, t)$, of its occurrence:

$$E = \ln \frac{1}{P(MSD, t)}.$$

554

Meditation Dataset

Fourteen healthy right-handed non-smoking meditation practitioners (11 female; age 28-66) underwent Siemens 3T MRI scanning (T1: TR = 2600 msec, TE = 3.9 msec, TI = 900 msec, FOV = 24 cm, 256 x 256 matrix, voxel dimensions = 1 x 1 x 1 mm³; T2*: weighted gradient-echo pulse sequence, TR = 1500 msec, TE = 30 msec, flip angle = 90 deg, FOV = 192 cm, 64 x 64 matrix, voxel dimensions = 3 x 3 x 4 mm³). All participants signed a consent form approved by the Institutional Review Board at Emory University and the Atlanta Veterans Affairs

562   Research and Development Committee as an indication of informed consent. Participants

563   were asked to meditate for 20 min in the MRI scanner by maintaining focused attention on

564   the breath and keeping the eyes closed. They were instructed to press a button whenever

565   they realized their mind had wandered away from the breath, and then return their focus to

566   the breath. The epoch of time immediately prior to the button press was thus the moment in

567   time in which each individual recognized that their focus had deviated from their breath.

568   This information was used to construct a finite impulses response model that mapped the 5

569   TRs prior-to and following each button press. We then modelled LC>BNM activity, low-

570   dimensional dynamics and network topology around this epoch to construct a model of

571   state-space reconfiguration as a function of intrinsic conscious awareness. Non-parametric,

572   block-resampling null distributions were utilized for statistical testing ($p < 0.05$).

573

574   **Data availability**

575   The BOLD data was obtained from (Hearne et al., 2017)[63] and

576   The BOLD data that support the findings of this study were obtained from (Hearne et al.,

577   2017)[63] and they are available from the authors upon reasonable request. The subcortical

578   timeseries (τ_{LC} and τ_{BNM}) that support the findings of this study are available at

579   (github.com/Bmunn/BSI).

580

581

582   **Code availability**

583   All the code required to conduct the analysis can be found on Github at

584   (github.com/Bmunn/BSI).

585

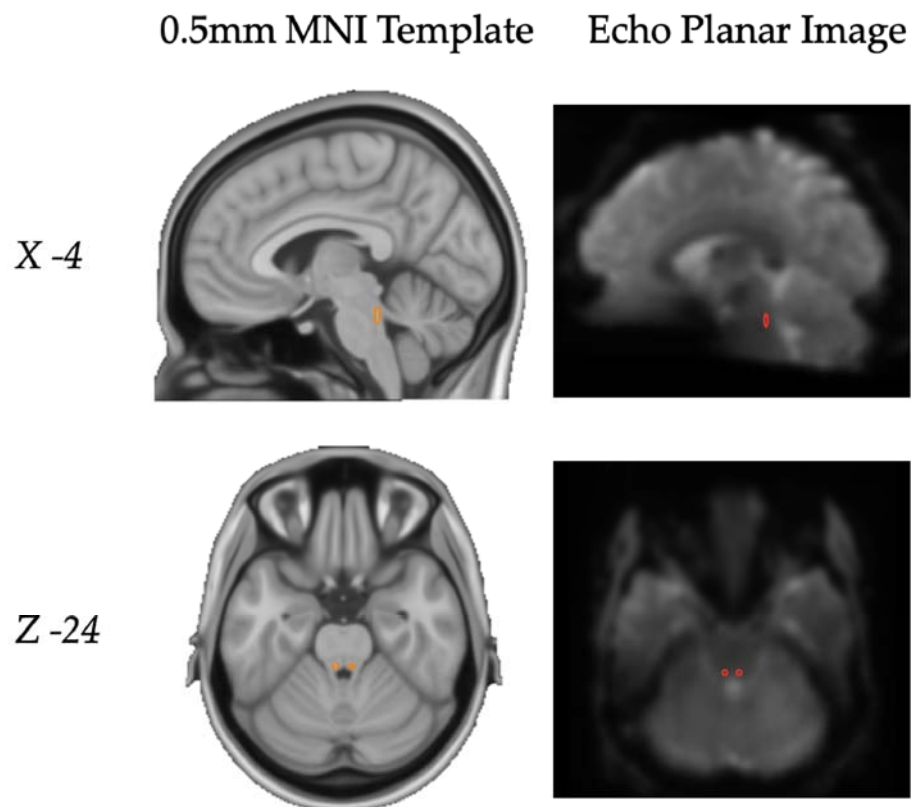586   **Supplementary Figures**

587

588   **Figure S1**. The locus coeruleus. Left: The anatomical locus coeruleus mask projected onto MNI 0.5mm

589   standard brain (orange); Right: The anatomical locus coeruleus mask down-sampled onto an example 7T Echo
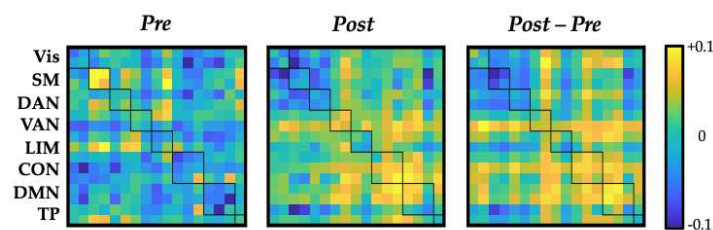
590   Planar Image from a single subject (red).

591

592   **Figure S2. Time-varying correlations**. Average correlation preceding (left) and following (middle) the zero-

593   lagged   value, along with the difference between the two (right); squares represent eight pre-defined

594   sub-networks: Vis – visual, SM – somatomotor, DAN – dorsal attention, VAN – ventral attention, LIM –

595   limbic, CON – control, DMN – default and TP – temporal pole.
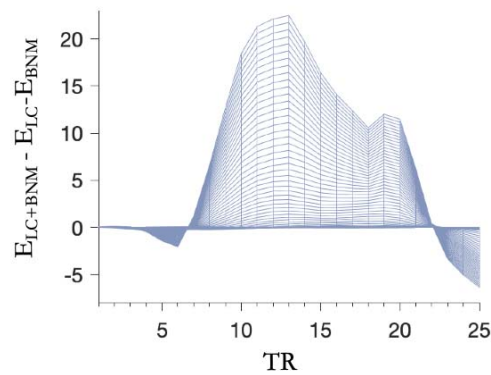
596

Figure S3 – LC and BNM move dynamics to differing regimes than unaroused activity and their simultaneous combination LC+BNM. The energy landscape of simultaneous LC+BNM phasic bursts relative to their linear superposition, suggesting the simultaneous combination may allow the system to reach particularly unique brain-states that neither individually could reach.

601

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602

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Author contributions

MS conceived, funded, and directed the project. MS Curated the data. BM, EM, MS Conducted the analysis. BM, MS Wrote the original draft. BM, EM, GW, MS Reviewed and edited the manuscript.