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4 Testing *in vitro* toxicity of nanoparticles in 3D cell culture with various

5 extracellular matrix scaffold

6 Short title: *In vitro* toxicity test of SiO₂ nanoparticles according to ECM type
7 using 3D cell culture model

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22 **Abstract**

23 Nanomaterials are used in a variety of fields and toxicity assessment is paramount for
24 their development and application. Although most toxicity assessments have been performed
25 in 2D (2-Dimensional) cell culture, the inability to adequately replicate the *in vivo* environment
26 and toxicity is a limitation. To overcome the limitation, a 3D (3-Dimensional) cell culture
27 method has been developed to make an environment closer to an *in vivo* system. In this study,
28 20 nm SiO₂ nanoparticles were dispersed in serum-containing (SC) and serum-free (SF) media
29 to compare 2D cell culture and 3D cell culture toxicity. The cells were subjected to a 3D cell
30 culture method in which HepG2, a human-derived liver cancer cell line, was mixed on a
31 scaffold. We found that nanoparticles induced toxicity in 2D cell culture, but toxicity was not
32 observed in 3D cell culture similar to *in vivo* environment. However, differences in toxicity
33 were observed between the three types of scaffolds in the absence of serum as the number of
34 cells decreased.

35

36 **Introduction**

37 Nanomaterials can be applied to diverse fields in a novel way or to provide enhanced
38 functionalities depending on their particle size and surface modifications and therefore have
39 been the subject of intense research in a wide range of fields, such as medicine, chemistry,
40 biotechnology, foods, and electronics. As it has become possible to apply nanomaterials to
41 various products and fields, many studies are underway investigating the effects that
42 nanoparticle exposure may have on the body. In particular, silica nanoparticles are incorporated
43 into various products, including drugs, cosmetics, food additives, and coatings, and are
44 extensively studied in the biochemical field regarding their application as drug carriers and/or

45 biomarkers [1, 2]. Cell cultures are used for such *in vitro* biochemical evaluation, and a variety
46 of cell culture models and platforms have been developed to study investigational products in
47 an environment that more closely mimic an *in vivo* system [3, 4]. Cell cultures are used in a
48 wide range of fields to study various biochemical and physiological events that may occur *in*
49 *vivo*, including the effects of drugs or toxic compounds on cells and development of mutations.
50 Two-dimensional (2D) cell culture, which has been used since the early 1900s, is a cell culture
51 method where cells are grown on flat surfaces optimized for cell attachment and growth.
52 Traditionally, 2D cell cultures have been widely used, and they are still used in many studies
53 because they allow simple cell observation and analysis. However, in 2D cell cultures, cells
54 adhere and grow on the surface of a culture dish, and these cells assume a different morphology
55 from cells grown *in vivo*. In addition, the 2D cultured cells differ from cells *in vivo* in a number
56 of ways that may affect the *in vitro* tests, such as surface area exposed to the investigational
57 product or cellular interactions [5]. S1 Fig shows the differences between 2D and 3D cell
58 cultures. As a result, 2D cell culture methods have the limitation that they do not accurately
59 reflect the *in vivo* environment, and as the cells grow and proliferate, the unnatural 2D
60 environment can also affect gene expression [6-10]. To overcome the limitations of these 2D
61 cell culture methods, a three-dimensional (3D) cell culture method has recently been developed
62 and used to grow cells in 3D and create an environment similar to the *in vivo* conditions [11,
63 12]. To cultivate cells in 3D *in vitro*, cells must self-assemble to form cell aggregates, or
64 scaffolds can be used to support 3D cell growth. Scaffold-based 3D cell culture technology
65 typically uses a matrix system called extracellular matrix (ECM). Used for 3D cell culture, the
66 ECM enables cell culture in a variety of spaces and can mimic cell-to-cell and cell-to-ECM
67 interactions, including paracrine signaling [13]. ECM is composed of a variety of polymers

68 such as collagen, enzymes, and glycoproteins and is known to support 3D cell growth and act
69 as mediator for cell growth, migration, differentiation, survival, homeostasis, and
70 morphogenesis [14-16]. In addition, moving away from 2D cell culture technology that uses
71 culture dishes for cell culture, allows cells cultured in 3D, using various newly developed
72 platforms, to be effectively applied to research. In this study, we compared the toxicity of silica
73 nanoparticles in two models, using a widely used 2D cell culture model and a newly developed
74 3D cell culture model. Fig 1 shows a micro-pillar/micro well platform for building 3D cell
75 culture techniques. Here, cells were mixed with ECM, dispensed into micro fillers, and cultured
76 in micro wells. Here, the ECM serves as a scaffold to support cell culture in 3D. In addition,
77 we evaluated the presence or absence of serum toxicity of ECM type nanoparticles using ECM
78 (alginate extracted from algae, Matrigel extracted from mouse tail, and collagen extracted and
79 purified from animals), and liver cancer cell line HepG2. Further, nanoparticle toxicity
80 assessments were performed on cultured cells (1×10^3 cells, 5×10^3 cells, and 1×10^4 cells) to
81 assess differences in toxicity by ECM type.

82

83 **Fig 1.** Micro Pillar / Micro Well Platform to Build 3D Cell Culture Technology.

84

85 **Materials and methods**

86 **SiO₂ nanoparticles**

87 In the present study, 20 nm SiO₂ nanomaterial, a certified reference material (CRM)
88 developed by the Korea Research Institute of Standards and Science (KRISS), was used. The
89 20 nm SiO₂ nanoparticles were prepared as previously reported [17]. The particles were
90 measured using both Mobile Particle Size Meter (SMPS) and Dynamic Light Scattering (DLS).

91 SMPS consisted of Differential Mobility Analyzer [(DMA), (TSI Inc., 3081)] and
92 Condensation Particle Counter [(CPC), (TSI Inc.)] with a Brookhaven Instruments system
93 having a BI9000AT digital correlator.

94

95 **Cell culture**

96 The HepG2 human liver cancer cell line purchased from the American Type Culture
97 Collection (ATCC) was used in this study. Prior to the experiment, HepG2 cells were thawed
98 and allowed to acclimate for three cycles. In the culture medium, 500 mL of Dulbecco's
99 Modified Eagle's Medium (DMEM) (WelgeneTM), 10% fetal bovine serum (HyCloneTM; FBS),
100 and 1% penicillin-streptomycin (WelgeneTM; PS) were diluted to prepare a serum-containing
101 medium (SC). Next, 15 mL of previously prepared DMEM was poured into a sterile T75 flask
102 purchased from Corning[®]. Cells were harvested in T75 flask with 0.05% trypsin-EDTA (1X)
103 purchased from Sigma Aldrich. Thereafter, cells were counted using Trypan blue 0.4%
104 purchased from Sigma Aldrich and placed in T75 flasks containing 15 mL DMEM at 2×10^6
105 cells/mL for incubation (37 °C/ 5% CO₂/ 95% humidity) for 2 days to reach approximately
106 80–90% confluence. Serum-free media (SF) was prepared by adding only 1% penicillin-
107 streptomycin (WelgeneTM; PS) to 500 mL of Dulbecco's Modified Eagle's Medium (DMEM)
108 (WelgeneTM).

109

110 **2D cell culture and 3D cell culture in scaffold**

111 S2 Fig shows the complete protocol of 2D and 3D cell culture. First, the HepG2 cells were
112 cultured in T75 flasks for 2 days, the culture medium was removed, and the cells were washed

113 once with phosphate buffered saline (PBS), 3 mL of 0.05% trypsin-EDTA (1X) was added,
114 and the cells were incubated for 2 min (37 °C/ 5% CO₂/ 95% humidity). To each T75 flask
115 containing cells, 7 mL of DMEM was added and the detached cells were centrifuged for 5 min
116 at 2500 rpm. The supernatant was removed and the cell pellet was resuspended in 1 mL of
117 DMEM. Thereafter, the cells were counted and seeded at a density of 1.0 x 10⁴ cells/well in
118 200 µL suspension in the wells B–G (3-6, 8-10) of a 96-well plate for 2D culture. S3 Fig (a)
119 shows a layout protocol in which 2D and 3D cell cultures were made to form in the B–G (3-6,
120 8-10) column. We prepared three plates in which 2D HepG2 cells were cultured. Further, 200
121 µL of PBS was added to wells in A and H columns to prevent evaporation of the culture
122 medium from the plate during culture. For 3D cell culture, cells were initially cultured in the
123 same way as 2D cell culture. In 3D cell culture, a 96-pillar plate (micro-pillar/micro well)
124 consisting of 0.2 mm diameter pillars was used, and cells were seeded in the same order as
125 seeded for 2D cell culture. Equal number of cells (1.0 x 10⁴ cells/pillar/2 µL) was used to
126 compare the toxicity levels in 3D and 2D cell cultures. To evaluate the toxicity in different
127 types of scaffolds used in 3D cell culture, cells were grown at densities 5.0 x 10³ cells and 1.0
128 x 10³ also. In this study, three types of ECM (alginate, Matrigel, and collagen) were used as
129 scaffolds for 3D cell growth. The first type of scaffold is 3% alginate, which is liquid at 4 °C,
130 but forms a gel at room temperature. To dilute 3% alginate to a final concentration of 0.75%,
131 3% alginate was diluted 1:1 in DMEM and further diluted in 1:1 ratio in DMEM containing
132 the prepared cells. To culture three plates for each cell density, an automated 3D cell culture
133 system (MBD model) was used to place the cells on a 96-pillar plate and let the gelation
134 proceed for 5 min at room temperature. Cells were placed in a 96-well plate containing 200 µL
135 of DMEM prepared in advance and incubated for 24 h (37 °C/ 5% CO₂/ 95% humidity).

136 Similarly, the 3D cell culture was carried out using two other scaffolds: 100% Matrigel
137 (Corning®) and collagen (Corning®). Matrigel is a liquid at 4 °C and quickly turns into a gel at
138 room temperature. Therefore, it was placed on ice for use in experiments. Here, Matrigel was
139 diluted in DMEM containing cells in a 1:1 ratio to grow cells in 3D at 50% Matrigel
140 concentration. Equal number of cells was seeded in the same order as alginate; cells were
141 transferred from the incubator to an empty 96 well plate, preheated, and gelation proceeded for
142 10 min. Then, cells were transferred to a 96-well plate containing 200 µL of DMEM, and
143 cultured for 24 h (37 °C/ 5% CO₂/ 95% humidity).

144

145 **Nanoparticle and chemical control process**

146 A CRM developed by the Korea Research Institute of Standards and Science (KRISS),
147 20 nm SiO₂ nanoparticles dispersed in sterile distilled water at a concentration of 10 mg/mL,
148 was used. As described above, the effect of corona protein was taken into consideration, SC
149 and serum-free (SF) media were separately prepared to have a final 20 nm SiO₂ concentration
150 of 1000 µg/mL. To compare the toxicity of nanoparticles, CdSO₄ (Cadmium sulphate) in the
151 powder form purchased from Sigma-Aldrich was used as the chemical control at varied
152 concentrations of 0, 9.4, 18.8, 37.5, 75 and 150 µM. In addition, CRM 20 nm SiO₂
153 nanoparticles at a concentration of 9.4 mg/mL were used and diluted to 0, 10, 50, 100, 500,
154 1000 µg/mL in 2D cell culture. In 3D cell culture, higher concentrations of 0, 62.5, 125, 250,
155 500, and 1000 µg/mL were prepared considering the penetration of nanoparticles into the
156 scaffold. Prior to experimentation, 20 nm SiO₂ diluted to each concentration in SC and SF
157 media was vortexed for 30 s to evenly disperse the particles. Using an electronic scale, 103 mg
158 of CdSO₄ was added to 40 mL of distilled water and vortexed for 30 s to prepare 10 mM CdSO₄,

159 which was diluted to a final concentration of 150 μ M and then further diluted in two-folds to
160 prepare various concentrations mentioned above. In this study, cytotoxicity was confirmed
161 using a toxicity test method based on absorbance measurement.

162

163 **Cell viability measurement through MTS assay**

164 After exposure of cells to nanoparticles for a 24 hr of time, toxicity was quantified by
165 MTS assay, which is one of the methods generally used to measure cell proliferation or toxicity
166 [18]. CellTiter96® AQueous One Solution Cell Proliferation Assay kit purchased from
167 Promega was used. MTS reagent was diluted in each culture medium (SC and SF) used in the
168 experiment at a ratio of 1:5 (MTS reagent : media), and 120 μ L of the mixture was added to
169 the cells following incubation. In 3D cell culture, diluted MTS reagent was added directly to
170 an empty 96-well plate and was transferred to the 96-pillar plate in which cells were seeded.
171 Cells were incubated with MTS reagent for 1 h for the 2D cell culture group and 2 h for the 3D
172 cell culture group considering the effects of ECM. The reaction was allowed to proceed in an
173 incubator (37 °C / 5% CO₂ / 95% humidity). The absorbance of these 96-well plates was
174 measured at 490 nm using a micro-plate reader. Cell viability was calculated from the following
175 equation, and IC₅₀ values were calculated using SoftMax Pro software.

176

$$177 \text{Cell viability (\%)} = \frac{\text{The absorbance value of each exposed cell}}{\text{Average absorbance value of unexposed cell}} \times 100\%$$

178

179 **Statistical Analysis**

180 Results of all the experiments were statistically analyzed and represented as the mean

181 with the standard error of the mean (SEM) of three or more independent experiments (n = 3).
182 The t-test was performed by dividing the equal variance and this variance through the F-test
183 using Excel, and the *p-value* was statistically processed as a value expressed in both directions.
184 In the 2D cell culture statistical comparisons were performed between two groups, and in 3D
185 cell culture, three groups were compared. While comparing the scaffolds, alginate was marked
186 with * and Matrigel with #. All *p-values* are expressed * as $p < 0.05$, ** as $p < 0.01$, and *** as
187 $p < 0.001$. IC₅₀ (inhibitory concentration 50) values were calculated using the SoftMax Pro
188 program.

189

190 **Results**

191 **Size changes in 20 nm SiO₂ with or without serum**

192 The particle size distribution is plotted in Fig 2 (a) and (b) showing hydrodynamic size
193 and mobility diameter, respectively. Fig 2 (c) and (d) respectively, show transmission electron
194 microscopy (TEM) images of 20 nm SiO₂ acquired on JEOL JEM-ARM200F and scanning
195 electron microscopy (SEM) images of 20 nm SiO₂ acquired at 200 kV accelerating voltage, at
196 an acceleration voltage of 10 kV each on the ZEISS Gemini SEM 500. As shown in Fig 2 (e),
197 particle size measurement by various methods revealed that the particle size data for 20 nm
198 SiO₂ obtained by electron microscopy (TEM and SEM) were similar to that obtained by
199 hydrodynamic methods (DLS and SMPS). This indicates that the nanoparticles were highly
200 monodisperse in aqueous suspension without aggregation.

201

202 **Fig 2.** Size Analysis of SiO₂ Nanoparticles by Different Methods. **(a)** Graphical representation
203 of Z-average diameter of 20 nm SiO₂ (avg 19.5 ± 2.4 nm) analyzed using DLS. **(b)** Graphical

204 representation of Z-average diameter of 20 nm SiO₂ (avg 21.5 ± 1.1 nm) analyzed using SMPS.
205 **c)** Representative TEM image captured at an acceleration voltage = 300 kV. **(d)** Representative
206 image of 20 nm SiO₂ nanoparticles observed using SEM. **(e)** Table shows the size of 20 nm
207 SiO₂ particles measured using different approaches.

208

209 To determine the cytotoxicity of the 20 nm SiO₂ nanoparticles, they were mixed with
210 culture media to expose cells to the nanoparticles. In addition, it has been reported that proteins
211 or polymers present in culture media get adsorbed to the nanoparticles and form protein corona
212 that can alter the size of the particles in an aqueous solution [19, 20]. Therefore, prior to
213 experimentation, particle size in the culture media with or without serum, in which the cells
214 were exposed to the nanoparticles, was determined using DLS. As shown in Fig 3, we were
215 able to confirm that the size of 20 nm SiO₂ nanoparticles dispersed in SC media increased to
216 as high as 158 nm because the serum led to the formation of protein corona around the
217 nanoparticles. In contrast, we found that the size of 20 nm SiO₂ nanoparticles dispersed in SF
218 media was 23 nm, which was similar to the original size.

219

220 **Fig 3.** Size of 20 nm SiO₂ Nanoparticles Dispersed in DMEM With and Without Serum
221 Analyzed Using DLS. **(a)** The size in serum-free DMEM is 23.23 ± 0.39 nm **(b)** The size in
222 serum-containing DMEM is 157.07 ± 1.07 nm.

223

224 **Comparison of cell growth differences according to types in ECM
(Scaffold)**

226 In this study, cell growth rates in three types of ECM- alginate, Matrigel, and collagen were

227 compared prior to the nanoparticle toxicity evaluation test. For a more reliable comparison,
228 cells were cultured in SF media all day in an incubator (37 °C/5% CO₂/95% humidity) and then
229 observed with MTS analysis and Optical microscopy. Fig 4 shows 3D cultured HepG2 cells on
230 each scaffold observed after 24 h.

231

232 **Fig 4.** Different Types of Scaffolds (alginate, Matrigel, and collagen) Showed Differences in
233 the Growth of HepG2 Cells Under Serum-free Media Conditions for 24 h.

234

235 Observation under Optical microscope showed that in the case of alginate, the cells form a
236 single spheroid, and in the Matrigel, the cells gradually combine to form a small spheroid.
237 However, collagen appears to constitute a spheroid in which cells are completely coagulated.
238 MTS analysis showed that cell growth was promoted by collagen rather than alginate and
239 Matrigel. These results were similar to those reported previously, stating that collagen
240 promotes cell growth and is a useful ECM [21].

241

242 **Comparison of 2D and 3D cytotoxicity of nanoparticles with and**
243 **without serum**

244 The HepG2 cells grown in 2D and 3D modules were treated with varied concentrations of
245 SiO₂ nanoparticles (0 to 1000 µg/mL) and a chemical control- CdSO₄ (0 to 150 µM) dispersed
246 in SC and SF media. S3 Fig (b) shows nanoparticles and chemical control prepared for each
247 concentration. The nanoparticles prepared for each concentration were added to 96 well plates
248 (B–G, 8–12); among them, the wells without cells (B–G, 11–12) were used for nanoparticles
249 interference control. CdSO₄, a chemical control, was also treated in 96 well plates (B–G, 1–5),

250 and treatment in wells without cell (B–G, 1–2) acted as the chemical interference control. In
251 addition, only media replaced cell control in B–G, column 6 of the 96 well plate. No cells
252 present in B–G, row 7 of a 96 well plate, acted as the background media control. MTS assay
253 was used for toxicity analysis, and the results were quantified using a microplate reader. Based
254 on the quantified data, IC_{50} (inhibitory concentration 50) values were calculated using the
255 SoftMax Pro program to determine the concentration at which 50% cell death occurred. Fig 5
256 shows the cell viability of the 2D cultured HepG2 cells after exposure to $CdSO_4$ and 20 nm
257 SiO_2 nanoparticles in media with or without serum.

258

259 **Fig 5.** Toxicity Analysis of $CdSO_4$ and 20 nm SiO_2 Nanoparticles Dispersed in DMEM With
260 or Without Serum Against 2D Cultured HepG2 Cells Analyzed by MTS Assay. The data is
261 represented as standard error of the mean (SEM) of 3 independent experiments ($n = 3$)
262 statistical significance is analyzed by t-test. The *p-value* is denoted as* $p < 0.05$, ** $p < 0.01$,
263 and *** $p < 0.001$.

264

265 For $CdSO_4$, the IC_{50} value was 36.33 μM in the SC and 14.62 μM in SF media,
266 indicating that in the absence of serum, IC_{50} value was lowered, indicating that it caused more
267 toxicity. In the 2D cell culture model, the IC_{50} value of the toxicity of nanoparticles was 710.5
268 $\mu g/mL$ in the SC, and 34.5 $\mu g/mL$ in SF media. Similarly, toxicities were compared when three
269 types of scaffolds (ECM) at 1.0×10^4 cell density were used for HepG2 3D cell culture as
270 shown in Figs 6 and 7. First, in the chemical control $CdSO_4$, the IC_{50} in alginate was 70.3 μM
271 in the SC and 29.17 μM in SF media. The IC_{50} value in Matrigel was 108.6 μM in the SC and
272 21.09 μM in SF conditions. In addition, the IC_{50} value in Collagen was 94.5 μM in the SC and

273 21.87 μ M in SF media. For the toxicity of nanoparticles, the IC₅₀ values of alginate, Matrigel,
274 and collagen could not be determined regardless of the presence or absence of serum. These
275 results suggest that in the presence of serum, protein coronas are formed around the
276 nanoparticles, increasing the particle size, preventing the particles from entering the HepG2
277 cells in the scaffold, and thus reducing the toxicity compared to 2D cultured cells. This suggests
278 that even in the absence of serum, cytotoxicity was markedly reduced in 3D cell culture due to
279 the influence of cell resistance and scaffold. In addition, the results obtained from 3D cell
280 cultures using synthetic ECM as scaffolds to create conditions similar to the *in vivo*
281 environment are shown to differ from those obtained from 2D cell cultures traditionally used
282 for *in vitro* studies.

283

284 **Fig 6.** Toxicity of 20 nm SiO₂ Nanoparticles Under Serum Containing Media Conditions Was
285 Compared by Changing the HepG2 Cell Count for Each Type of Scaffold (alginate, Matrigel,
286 and collagen). The standard error of the mean (SEM) of 3 independent experiments (n = 3) was
287 statistically analyzed as a *p-value* via t-test. The *p-value* is denoted as* *p* <0.05, ** *p* <0.01,
288 and *** *p* <0.001. Comparisons with alginate are indicated by *, and comparisons with
289 Matrigel are indicated by #.

290

291 **Fig 7.** Toxicity of 20 nm SiO₂ Nanoparticles Under Serum Free Media Conditions Was
292 Compared by Changing the HepG2 Cell Count for Each Type of Scaffold (alginate, Matrigel,
293 and collagen). The standard error of the mean (SEM) of 3 independent experiments (n = 3) was
294 expressed as a *p-value* via T-test. The *p-value* is denoted as* *p* <0.05, ** *p* <0.01, and *** *p*

295 <0.001. Comparisons with alginate are indicated by *, and comparisons with Matrigel are
296 indicated by #.

297 **Comparison of cytotoxicity of nanoparticles in different 3D**
298 **scaffolds**

299 Since standards for 3D cell culture have not yet been established, various 3D cell
300 culture methods have been adopted and various hydrogels have been developed for use as ECM.
301 Therefore, we created conditions for growing HepG2 cells as spheroids in 3D cell culture using
302 three ECM, alginate, Matrigel, and collagen, which are commonly used as scaffolds in 3D cell
303 culture. The effect of ECM types on the cytotoxicity of nanoparticles was compared in the
304 same way as in the above experiment using 3D cell culture plates grown on different ECM. In
305 addition, the difference in toxicity of 20 nm SiO_2 to 3D cell culture was confirmed by the
306 presence or absence of serum. Fig 6 shows the toxicity of CdSO_4 and 20 nm SiO_2 nanoparticles
307 as a function of the number of HepG2 cells grown on three different scaffolds in the presence
308 of serum. In the presence of serum, the size of the nanoparticles is increased by a large number
309 of proteins present in the medium getting adsorbed on the particles, increasing the original size
310 of the nanoparticles. Therefore, cell uptake has not taken place, resulting in no toxicity. In
311 contrast, for the control chemical CdSO_4 , IC_{50} values can be obtained on three different
312 scaffolds as the concentration increases. In addition, it was confirmed that smaller the number
313 of cells, lower the external resistance between cells, resulting in a significant decrease in the
314 IC_{50} value. Fig 7 shows the toxicity of CdSO_4 and 20 nm SiO_2 nanoparticles as a function of
315 the number of HepG2 cells grown on three different scaffolds in the absence of serum. Based
316 on the DLS results shown above, it was confirmed that the change in the size of the
317 nanoparticles was not large in SF media and that the cytotoxicity appeared to be greater than
318 when serum was present due to cell uptake. In the case of 1.0×10^4 cells, it was confirmed that
319 there was no toxicity to the extent that the IC_{50} value could not be determined, as in Fig 6,

320 where serum was present, but the cell viability (%) value was slightly reduced. In addition, as
321 the number of cells decreased, the IC_{50} value decreased significantly in alginate and collagen.
322 Alternately, with Matrigel, the IC_{50} values could not be obtained regardless of the number of
323 cells. Based on these results, it was found that the toxicity results of nanoparticles differ
324 depending on the type of scaffold used in 3D culture even under identical conditions. Other
325 studies have reported that differences in toxicity of nanomaterials in 3D culture using Matrigel,
326 collagen, and gelatin are caused by ECM type. This is because each ECM has its own structure
327 and function [22].

328

329 **Conclusions**

330 To overcome the limited ability of 2D cell culture to adequately express the *in vivo*
331 environment, this study aimed to determine the toxicity of nanoparticles using 3D cell culture
332 technology. Among various methods for culturing cells in 3D, a method of distributing cells
333 mixed with ECM acting as a scaffold in a column was used in this study. The toxicity of
334 nanoparticles in 3D cell culture method used in this study was compared to 2D cell culture.
335 The results showed that the HepG2 cells grown in 3D are less susceptible to toxicity regardless
336 of protein-corona formation. In addition, it was found that there were differences in toxicity
337 according to the scaffold (ECM) type and cell number suggesting that 3D cell culture needs
338 more research and development. Cells grown in 2D are designed to mimic *in vivo* conditions.
339 However, the environment is significantly different with regard to morphology, exposed
340 surface area, and intercellular signals and interactions. Previous reports have revealed that the
341 evaluation of nanoparticle toxicity between 2D and 3D cultured cells is different, and the results
342 of 3D cell culture are similar to *in vivo* environments and closely related to animal experiments

343 [23]. Thus, in this study, 3D cell culture technology can also help to bridge the gap between
344 the toxicity results of traditional *in vitro* 2D cell culture and *in vivo* assays, and is useful for
345 developing experimental systems similar to actual *in vivo* conditions. In addition, based on the
346 experiments conducted in this study, in future we aim to evaluate the toxicity of various
347 nanoparticles using 3D cell cultures grown over long term to form single spheroids, which
348 would mimic the *in vivo* environment more precisely.

349

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356

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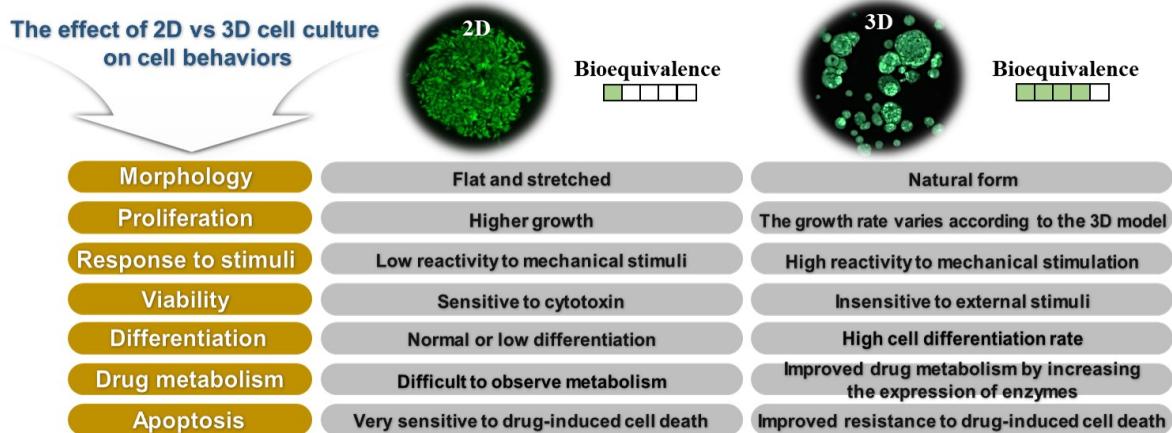
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418 Supporting information

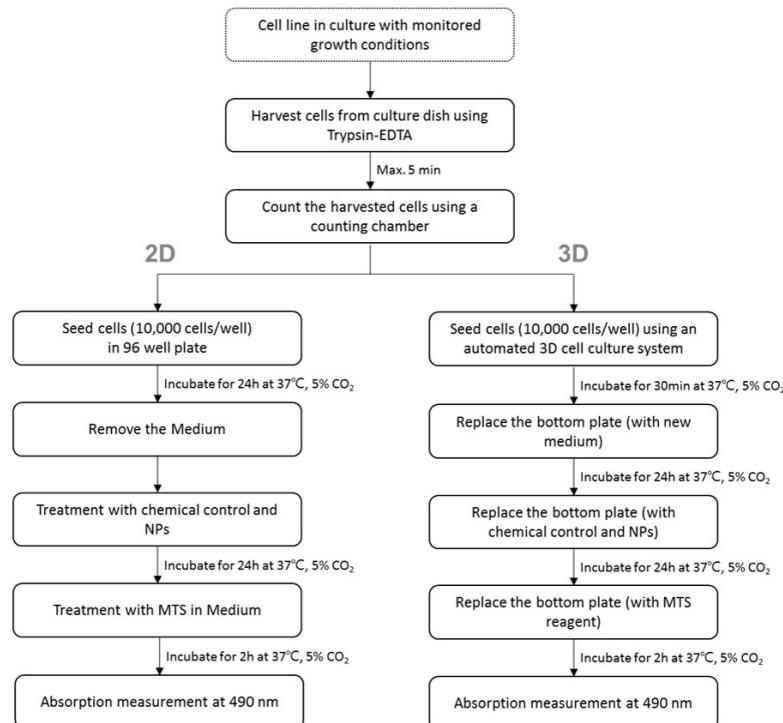
419 S1 Fig. This is the S1 figure legend.



S1 Fig. Comparison of 2D and 3D cell culture characteristics.

420

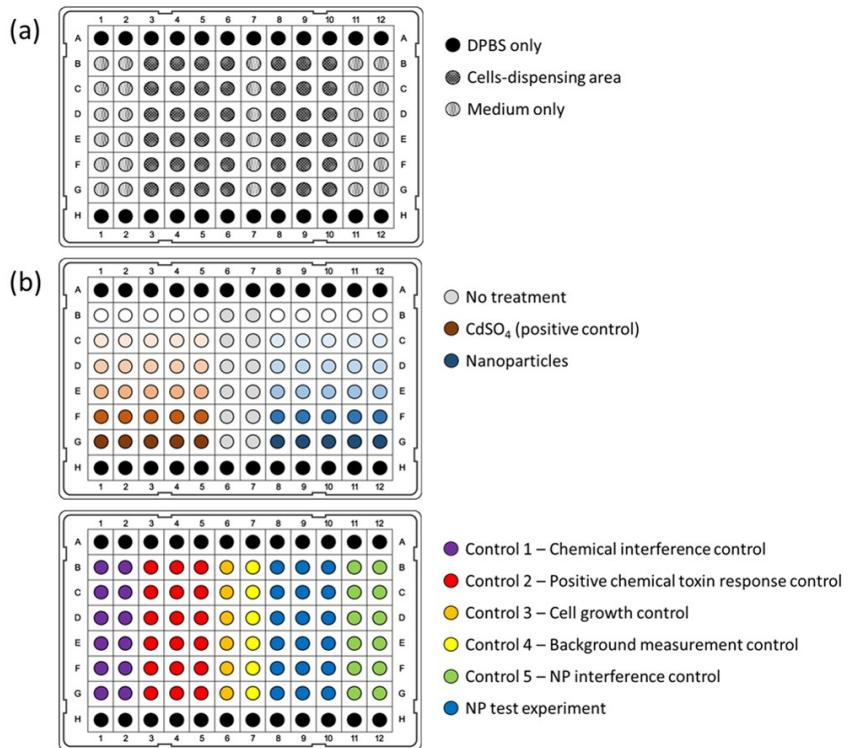
421 S2 Fig. This is the S2 figure legend.



S2 Fig. Shows the overall protocol for 2D and 3D cell culture experiments.

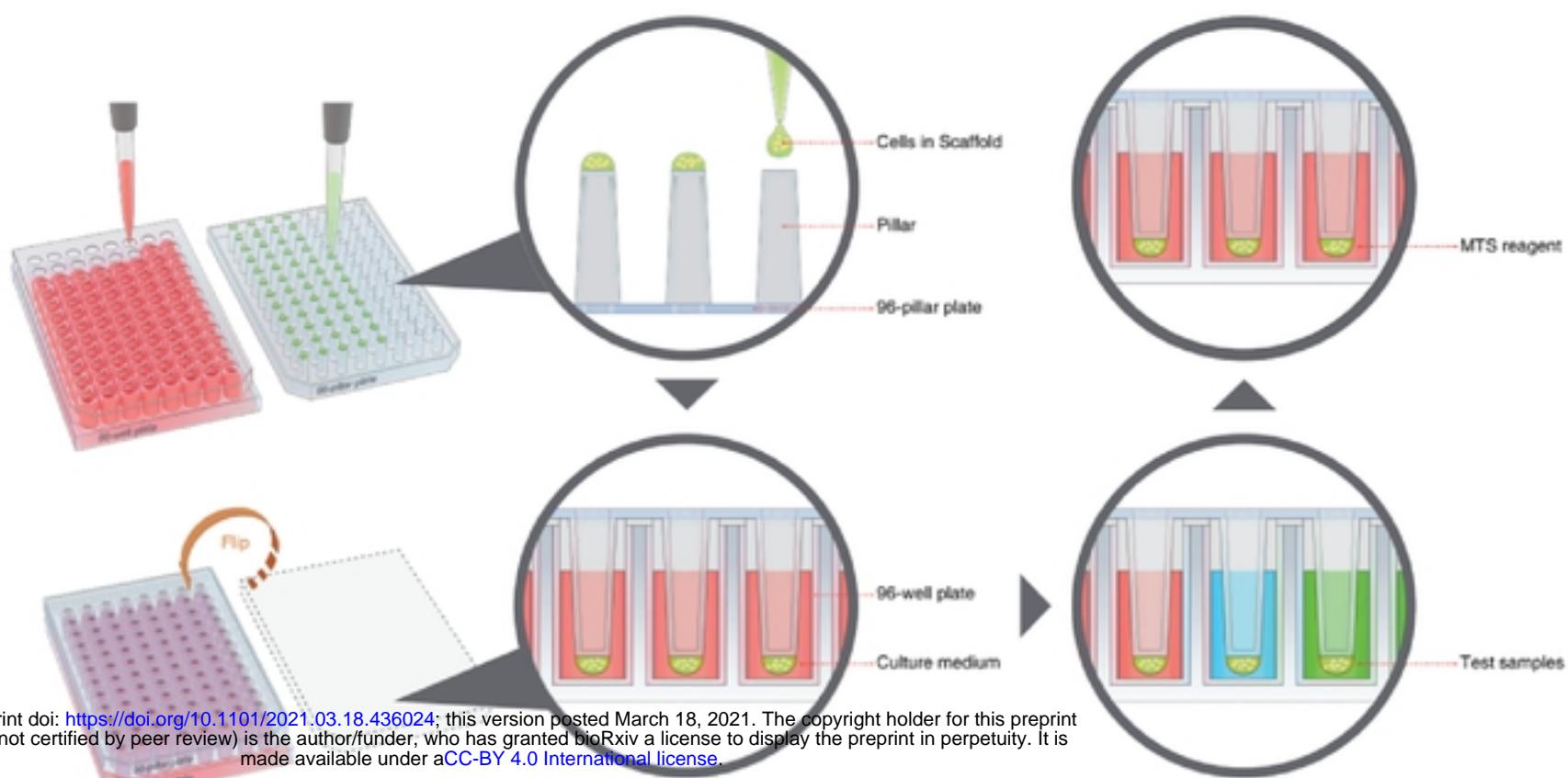
422

423 **S3 Fig. This is the S3 figure legend.**



S3 Fig. (a) shows the lay out of the protocol for 96 column/well plates, **(b)** shows the concentration and chemical control of the nanoparticles used in the experiment, and the control for each well is shown.

424



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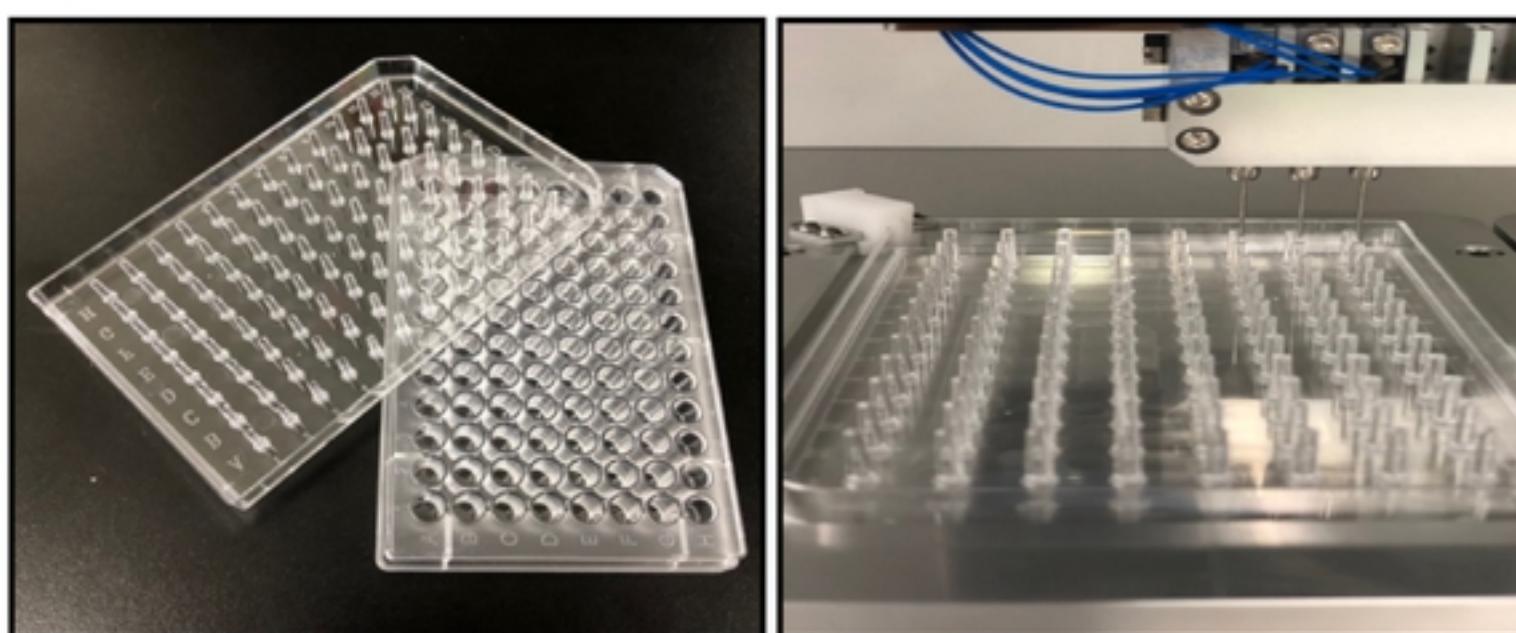


Figure 1

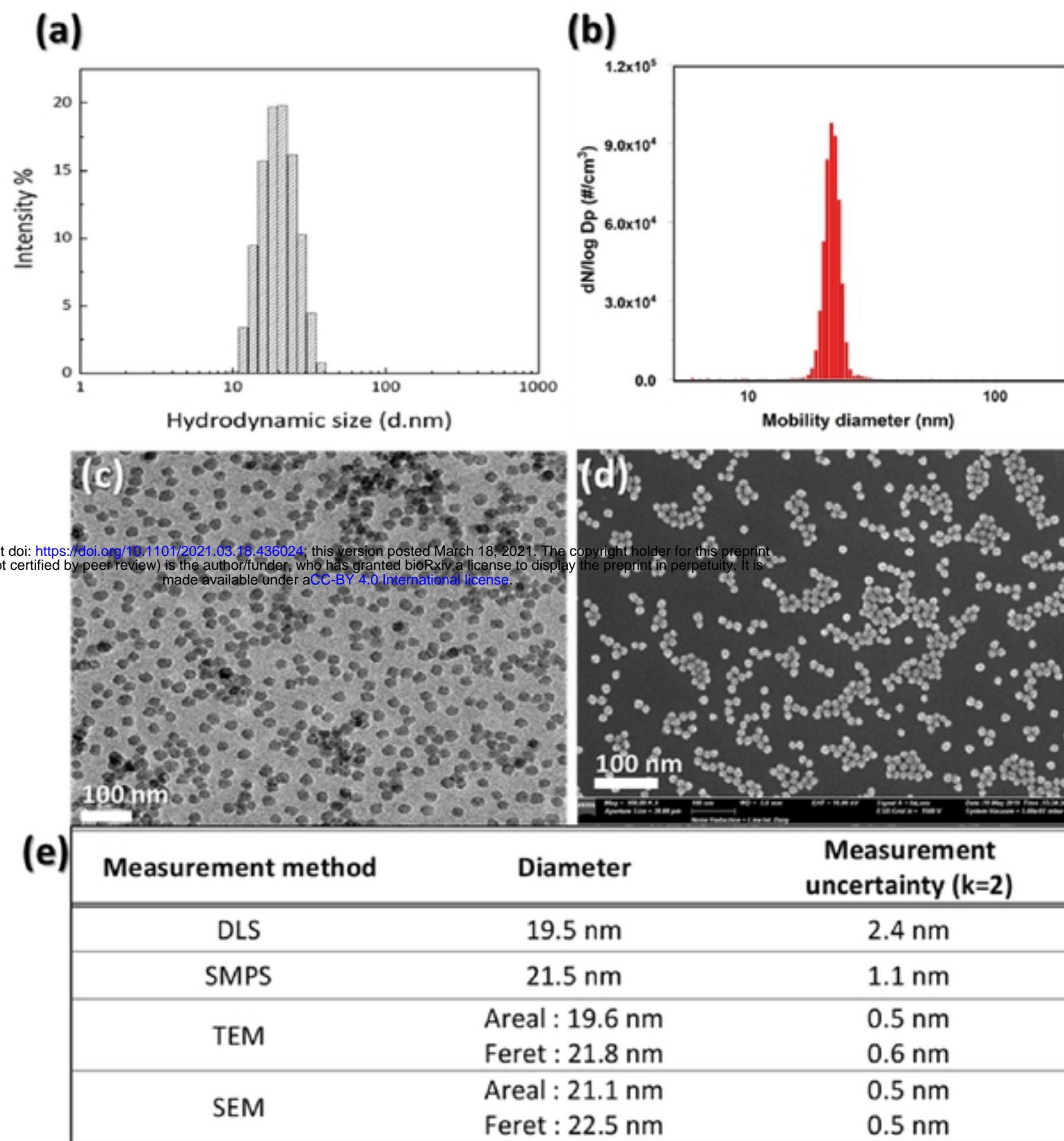


Figure 2

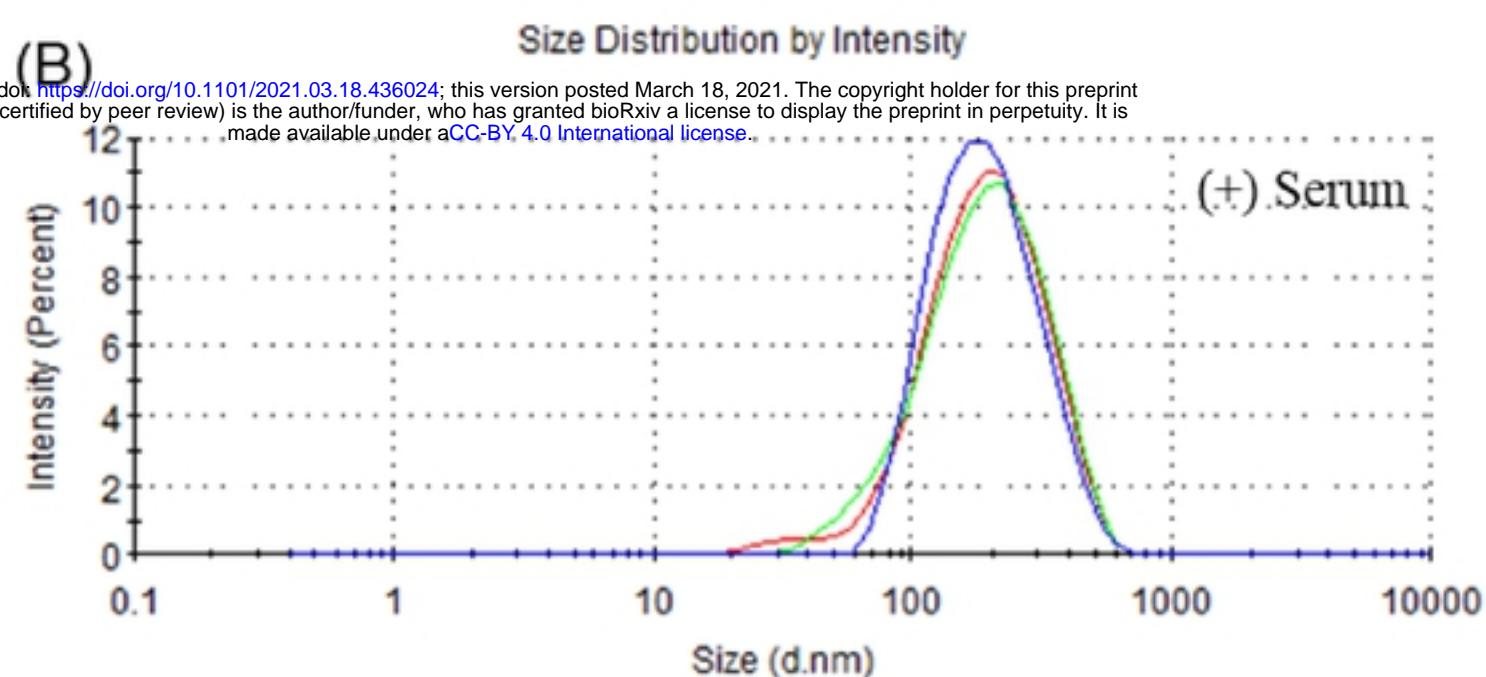
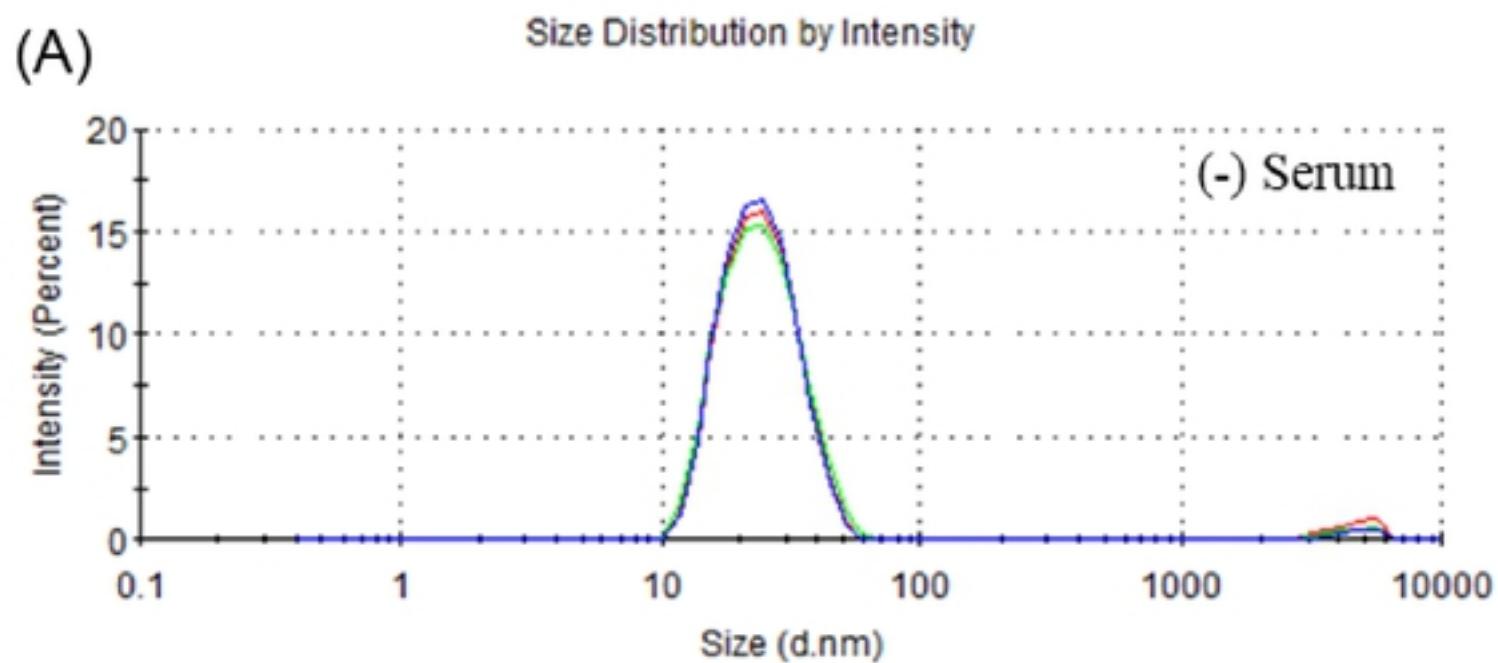
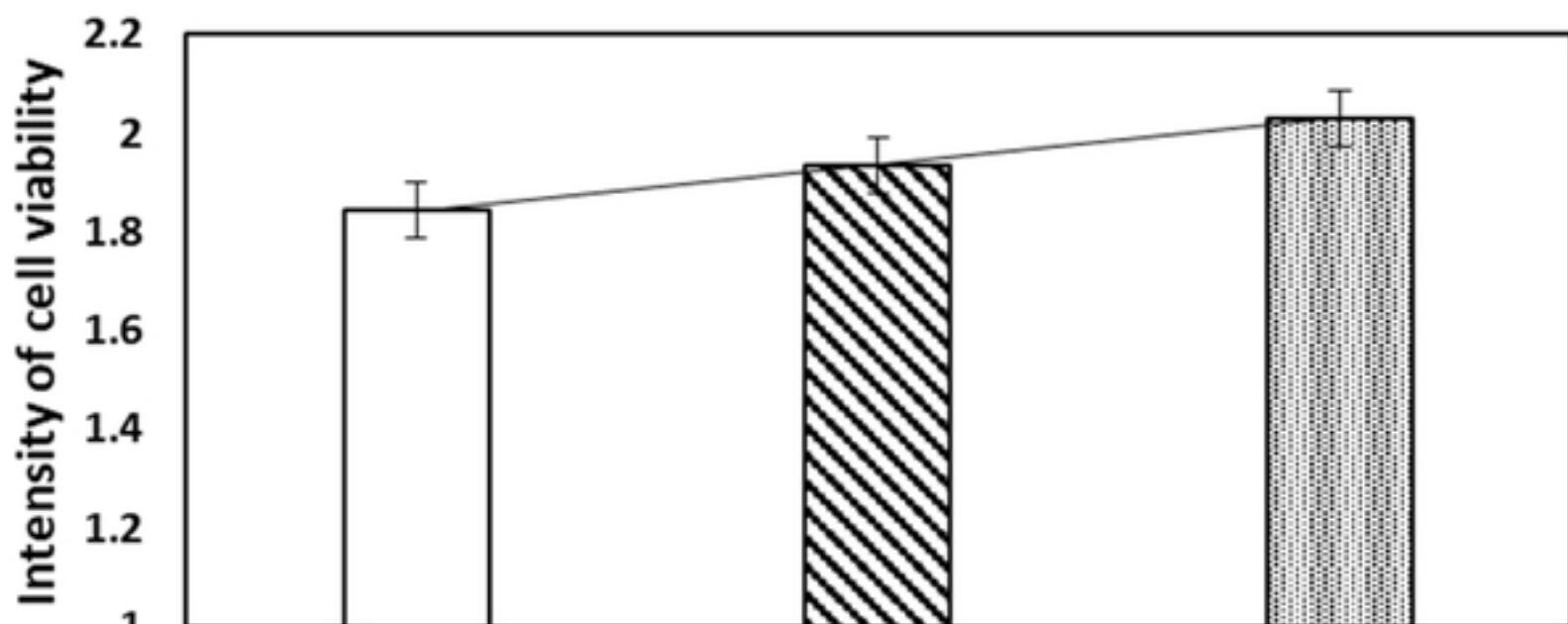


Figure 3

HepG2 cell growth control for 24 h



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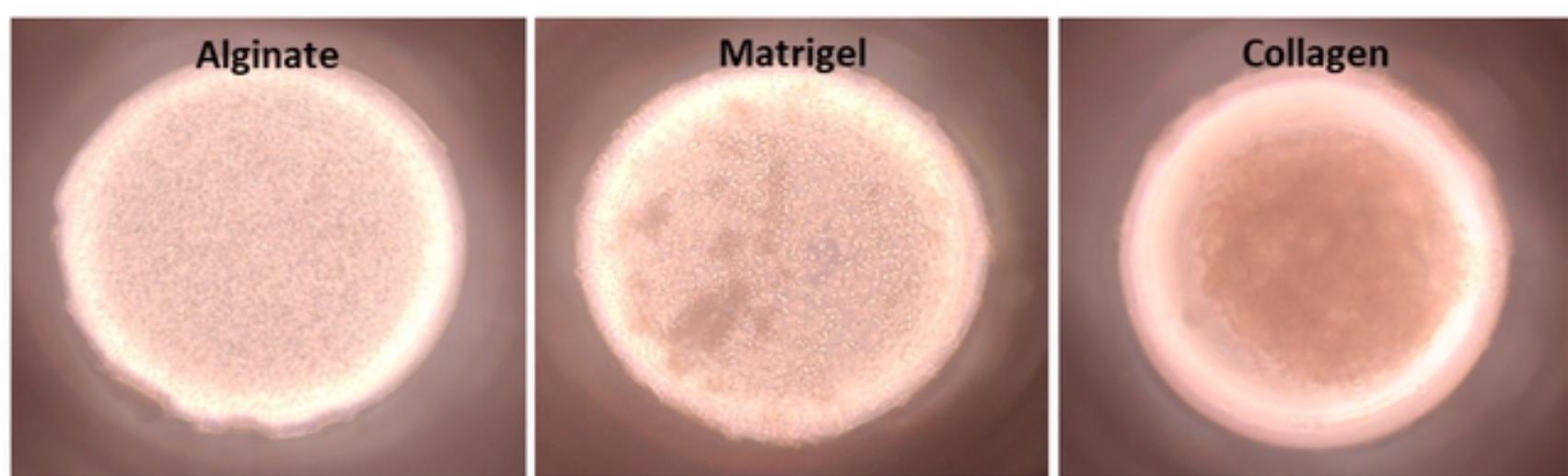
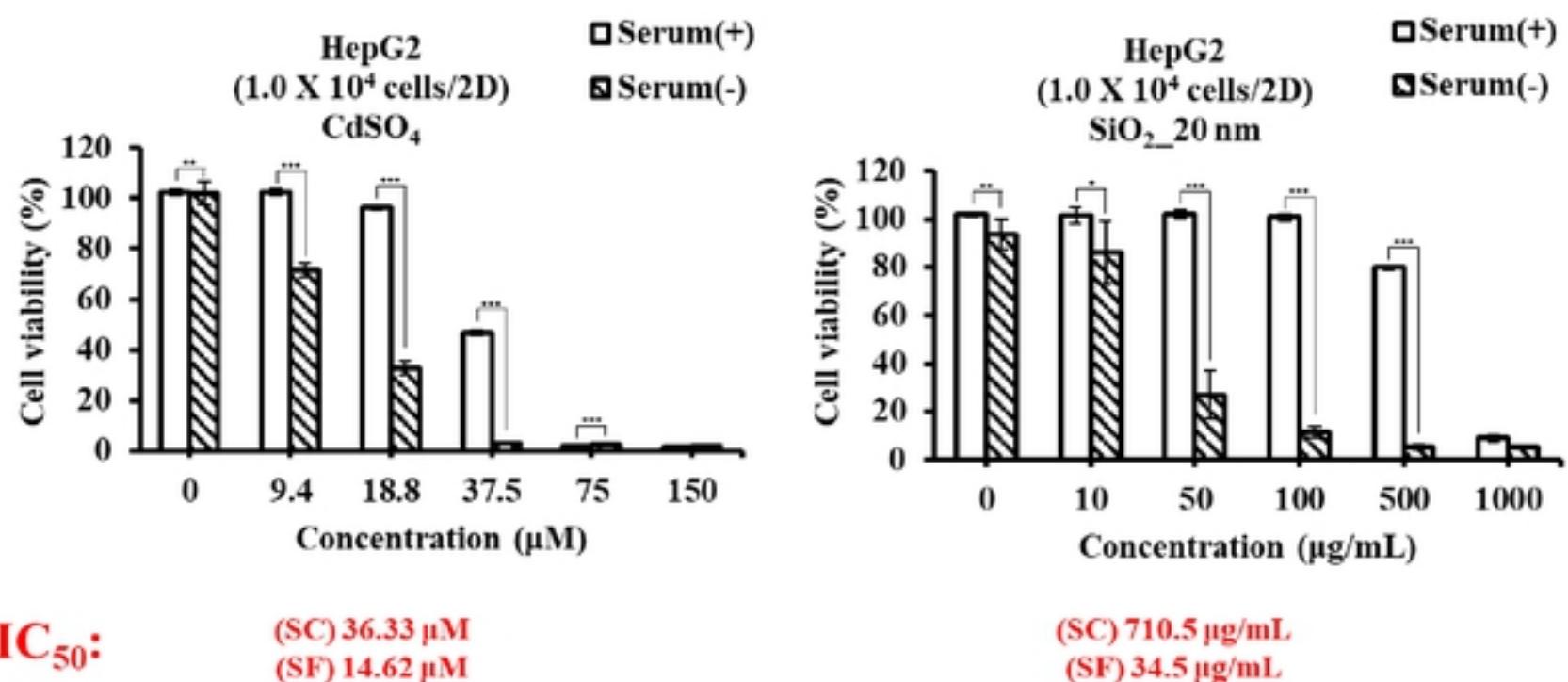


Figure 4



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Figure 5

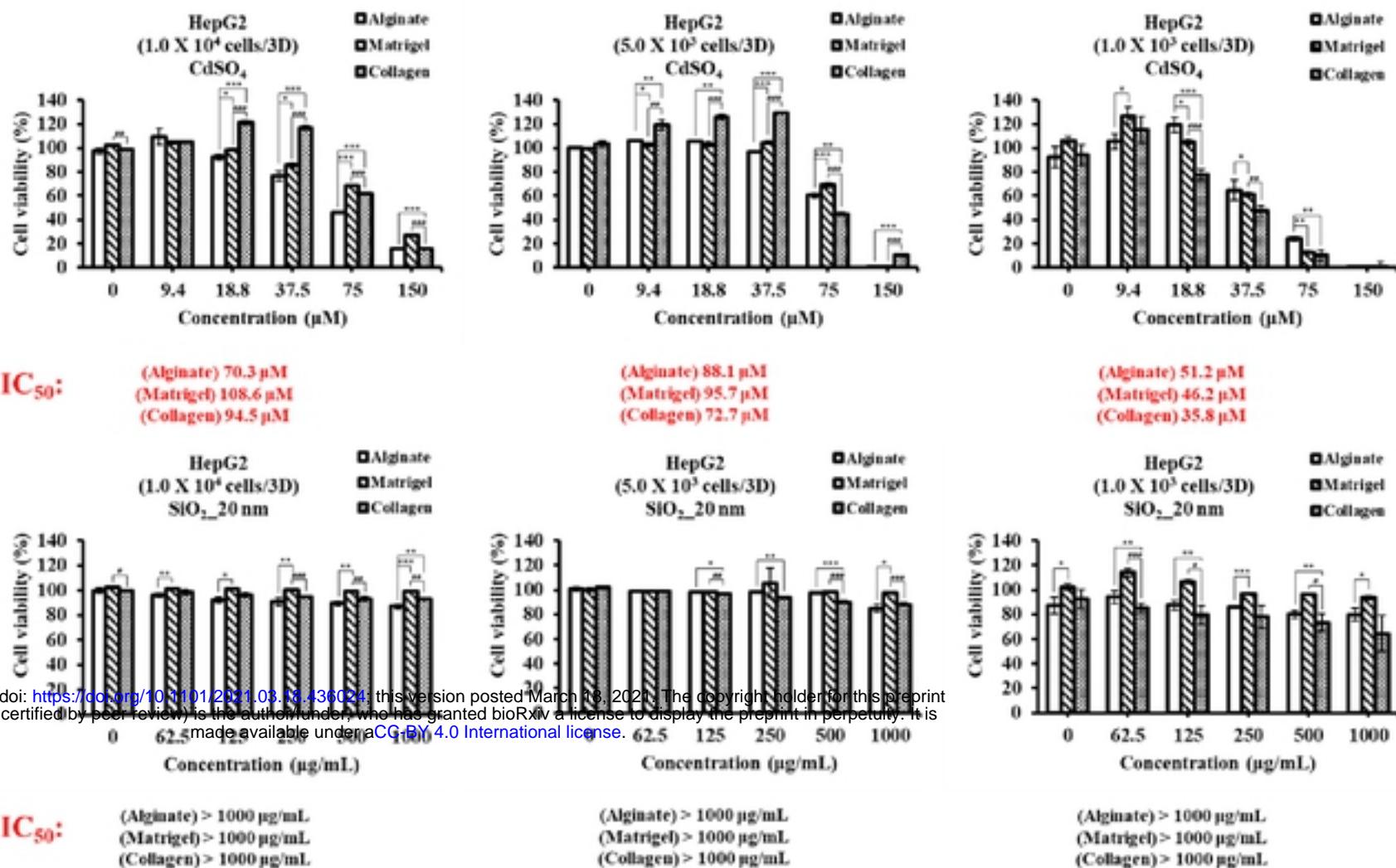


Figure 6

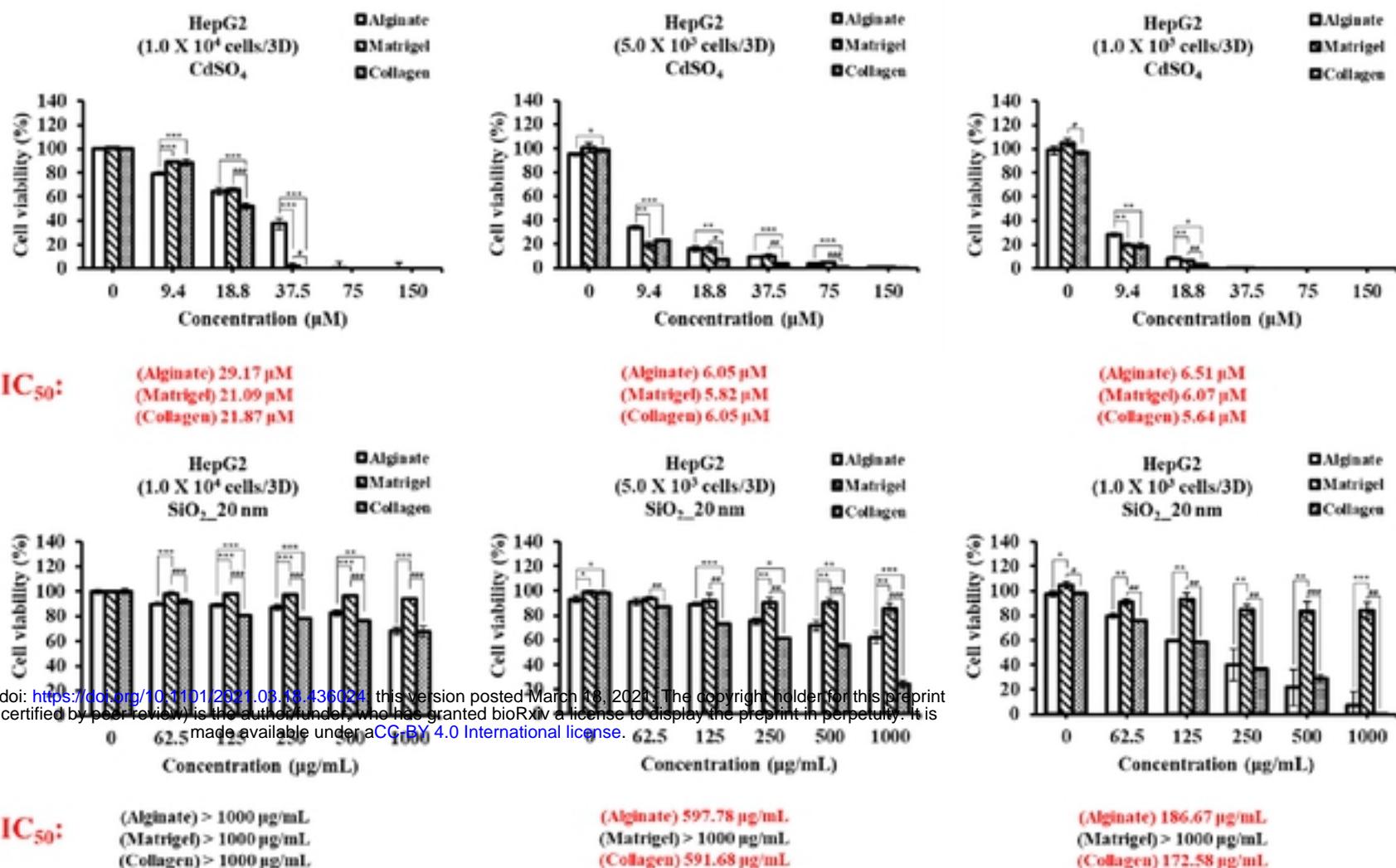


Figure 7